

# How Much Neuronal Information Can We Extract With fMRI?

Advancing fMRI Utility

Peter A. Bandettini, Ph.D

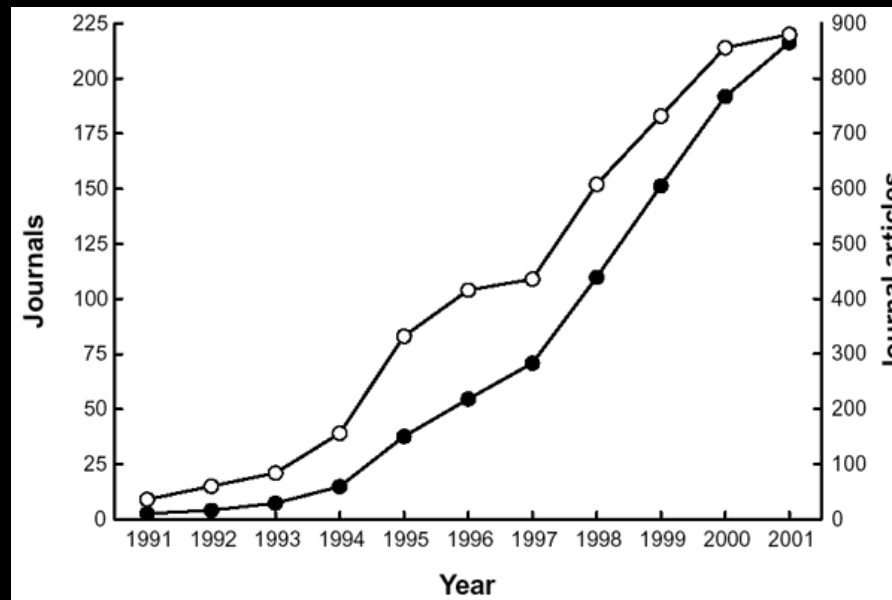
bandettini@nih.gov

Unit on Functional Imaging Methods  
&  
Functional MRI Facility

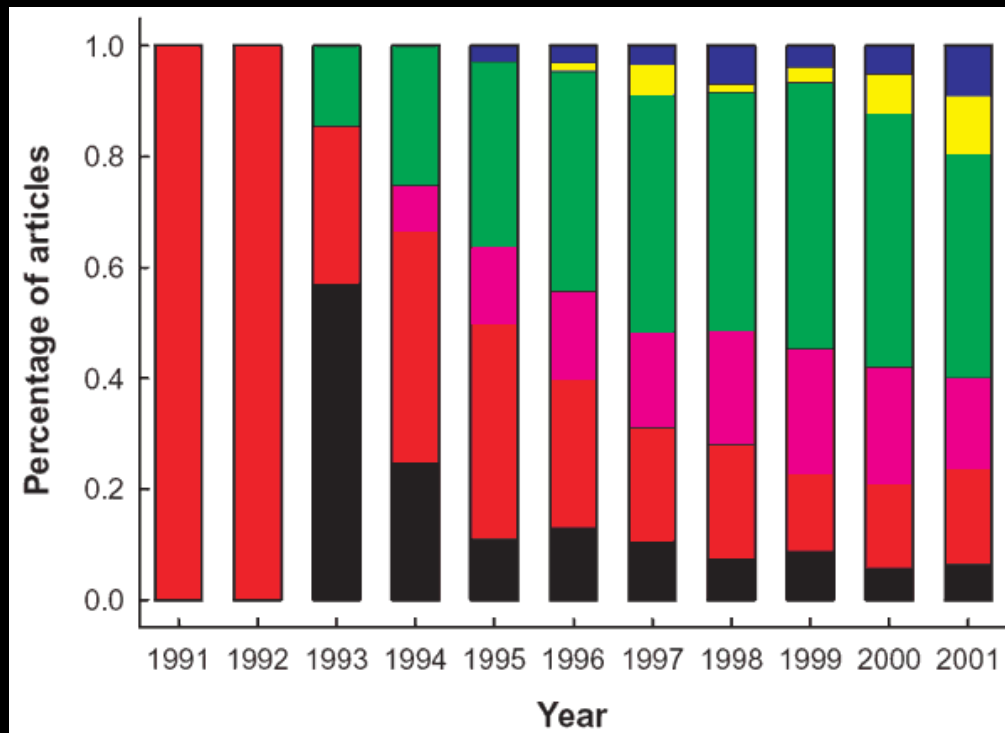
Laboratory of Brain and Cognition  
National Institute of Mental Health



J. Illes, M. P. Kirschen,  
 J. D. E. Gabrielli,  
 Nature Neuroscience,  
 6 (3) p.205



Motor (black)  
 Primary Sensory (red)  
 Integrative Sensory (violet)  
 Basic Cognition (green)  
 High-Order Cognition (yellow)  
 Emotion (blue)



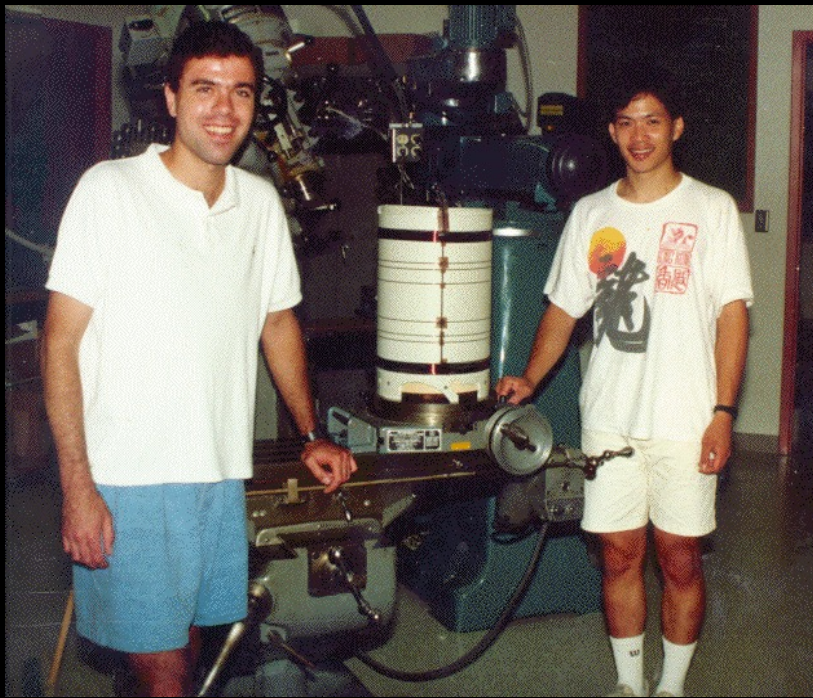
# Most fMRI studies since 1992:

## Minimum necessary:

- Whole Brain EPI
- Field strength of 1.5T or greater
- Basic stimulus delivery and feedback
- Software for image transfer, analysis, and display

## Typical advanced features:

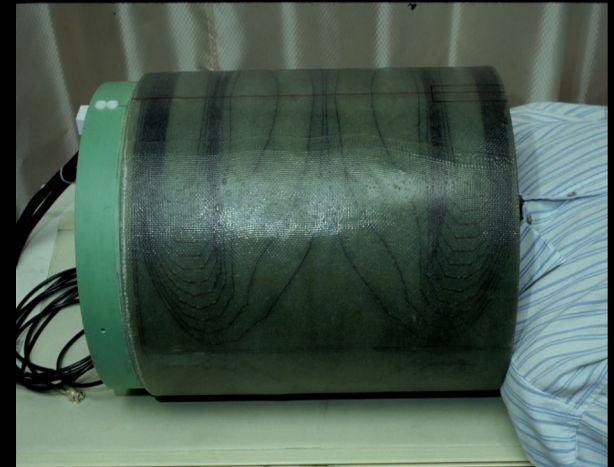
- Higher resolution whole brain EPI, spiral, or multi-shot
- Field strength of 3T to 7T
- Quadrature and Surface coils (single, multiple)
- Susceptibility correction
- ASL (perfusion imaging)
- Multiple subject interface devices, including EEG, SCR, eye position.
- Multi-subject analysis, more rigorous statistics, more sophisticated display methods, exploratory analysis



**1991-1992**



**1992-1999**





# Technology

MRI  
 EPI  
 Local Human Head Gradient Coils  
 BOLD  
 ASL  
 Spiral EPI  
 Multi-shot fMRI  
 1.5T,3T, 4T  
 EPI on Clin. Syst.  
 Nav. pulses  
 Diff. tensor  
 Real time fMRI  
 Quant. ASL  
 Dynamic IV volume  
 Simultaneous ASL and BOLD  
 Mg<sup>+</sup>  
 Venography  
 Z-shim  
 Baseline Susceptibility  
 7T  
 SENSE  
 "vaso"  
 >8 channels  
 Current Imaging?

# Methodology

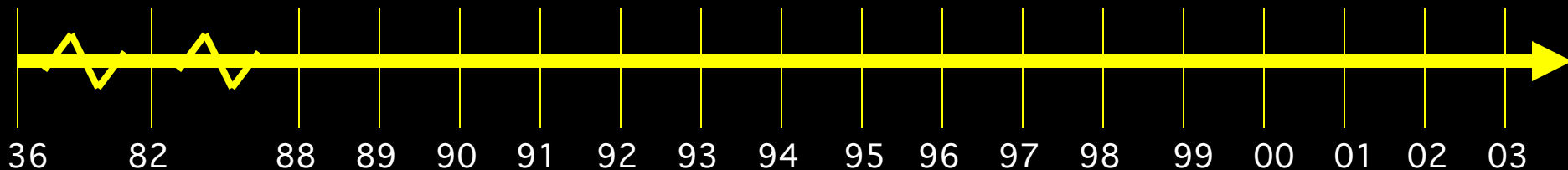
Baseline Volume  
 IVIM  
 Correlation Analysis  
 Parametric Design  
 Surface Mapping  
 Phase Mapping  
 Linear Regression  
 Event-related  
 Motion Correction  
 Multi-Modal Mapping  
 ICA  
 Free-behavior Designs  
 Mental Chronometry  
 Deconvolution  
 Fuzzy Clustering  
 CO<sub>2</sub> Calibration  
 Latency and Width Mod  
 Multi-variate Mapping

# Interpretation

Blood T2  
 Hemoglobin  
 BOLD models  
 B<sub>0</sub> dep.  
 TE dep  
 SE vs. GE  
 NIRS Correlation  
 Veins  
 PET correlation  
 IV vs EV  
 Pre-undershoot  
 Resolution Dep.  
 Post-undershoot  
 CO<sub>2</sub> effect  
 Inflow  
 ASL vs. BOLD  
 PSF of BOLD  
 Extended Stim.  
 Linearity  
 Fluctuations  
 Balloon Model  
 Layer spec. latency  
 Excite and Inhibit  
 Metab. Correlation  
 Optical Im. Correlation  
 Electrophys. correlation

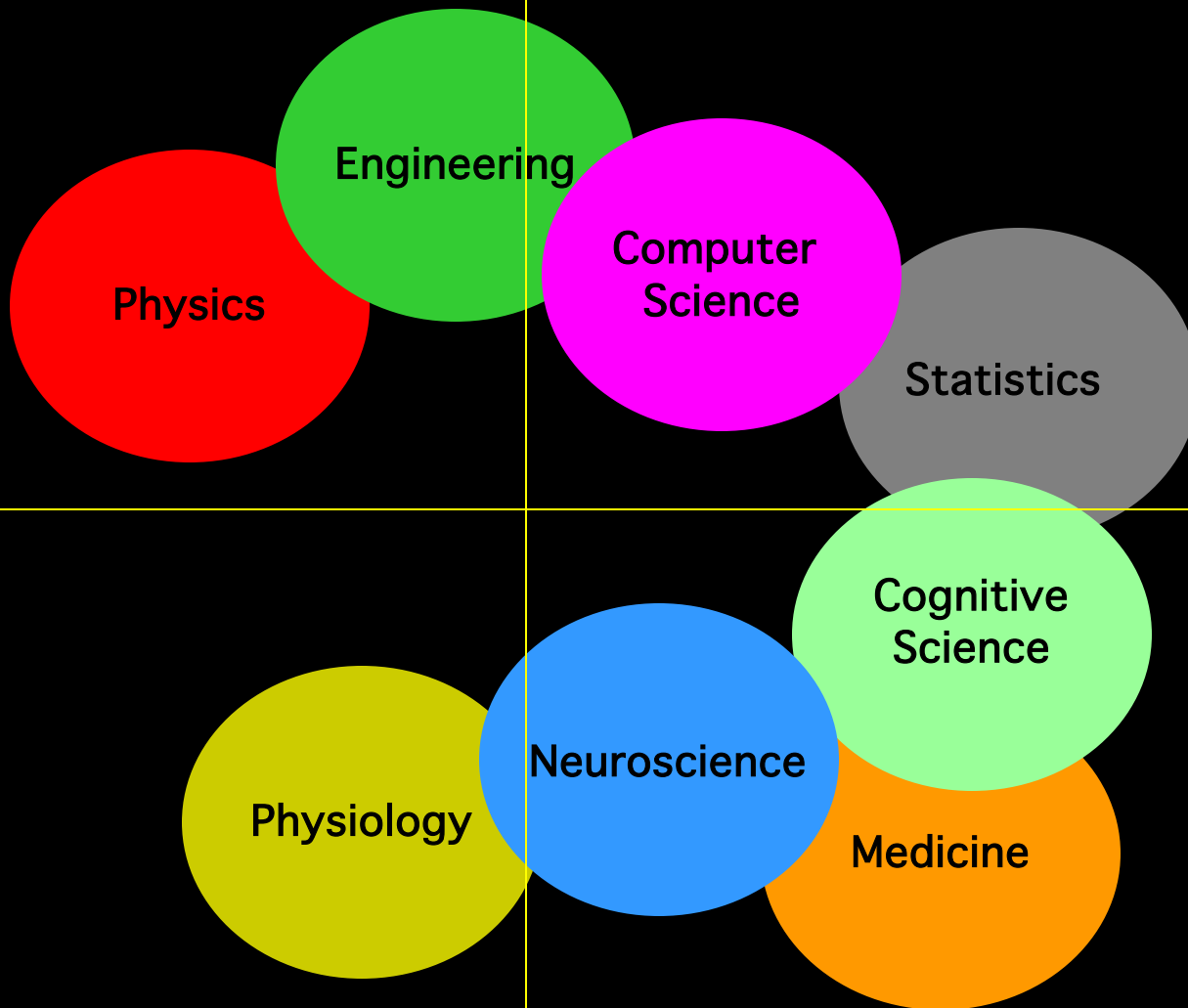
# Applications

Complex motor  
 Language  
 Imagery  
 Memory  
 Emotion  
 Epilepsy  
 Motor learning  
 Children  
 Tumor vasc.  
 Drug effects  
 Mirror neurons  
 BOLD -V1, M1, A1  
 Presurgical  
 Attention  
 Ocular Dominance  
 Volume - Stroke  
 V1, V2..mapping  
 Priming/Learning  
 Clinical Populations  
 Δ Volume-V1  
 Plasticity  
 Face recognition  
 Performance prediction



**Technology**

**Methodology**



**Interpretation**

**Applications**

# What are the biggest unknowns/challenges?

1. Technology

2. Methodology

3. Interpretation

# What are the biggest unknowns/challenges?

1. Technology

2. Methodology

3. Interpretation

# Technology

- Field strength
- Signal to noise
- Resolution
- Shimming

# Field strength

## Plusses

- SNR proportional to  $B_0$
- Contrast proportional to  $B_0$

## Minuses

- Susceptibility effects increase
- RF penetration problems
- SAR problems
- Fluctuations increase

## Bottom Line

- SNR buys resolution when technology catches up
- Fluctuations may be increasingly interesting



# Signal to noise

## Methods to increase

- Increase  $B_0$
- Smaller RF coils (arrays)
- Reduce noise

## Issue:

- Temporal SNR is most important

# More SNR...More “signal” is there...

## The spatial extent of the BOLD response

Ziad S. Saad,<sup>a,b,\*</sup> Kristina M. Ropella,<sup>b</sup> Edgar A. DeYoe,<sup>c</sup> and Peter A. Bandettini<sup>a</sup>

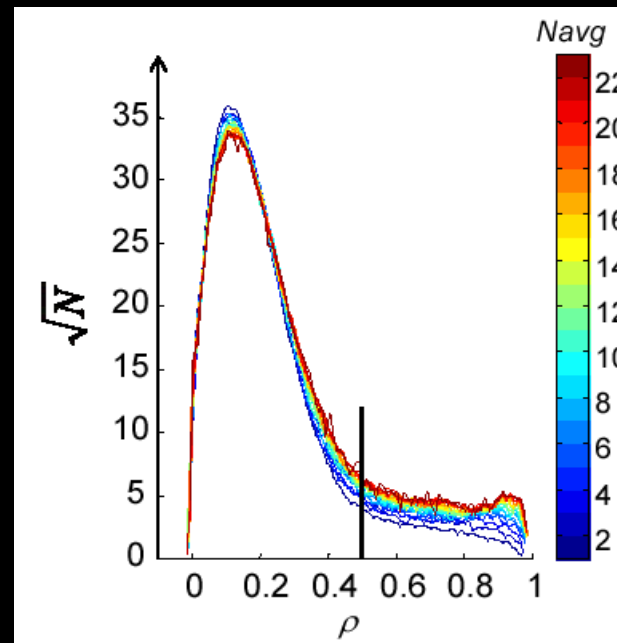
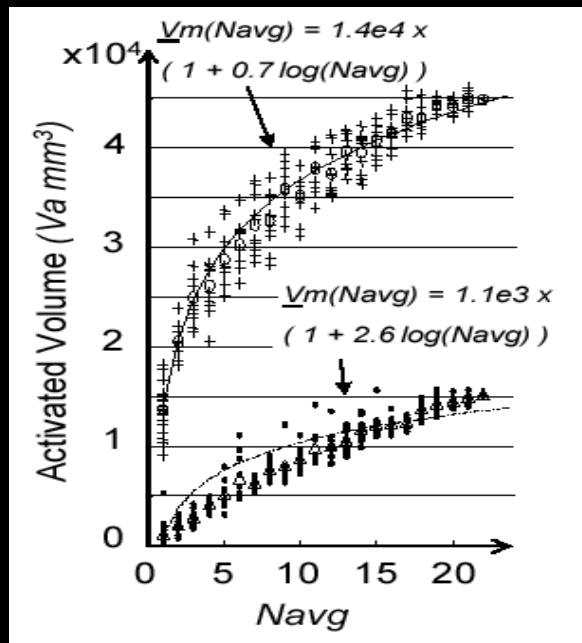
<sup>a</sup> Laboratory of Brain and Cognition, National Institute of Mental Health, NIH, Bethesda, MD 20892-1148, USA

<sup>b</sup> Department of Biomedical Engineering Marquette University, Milwaukee, WI 53233, USA

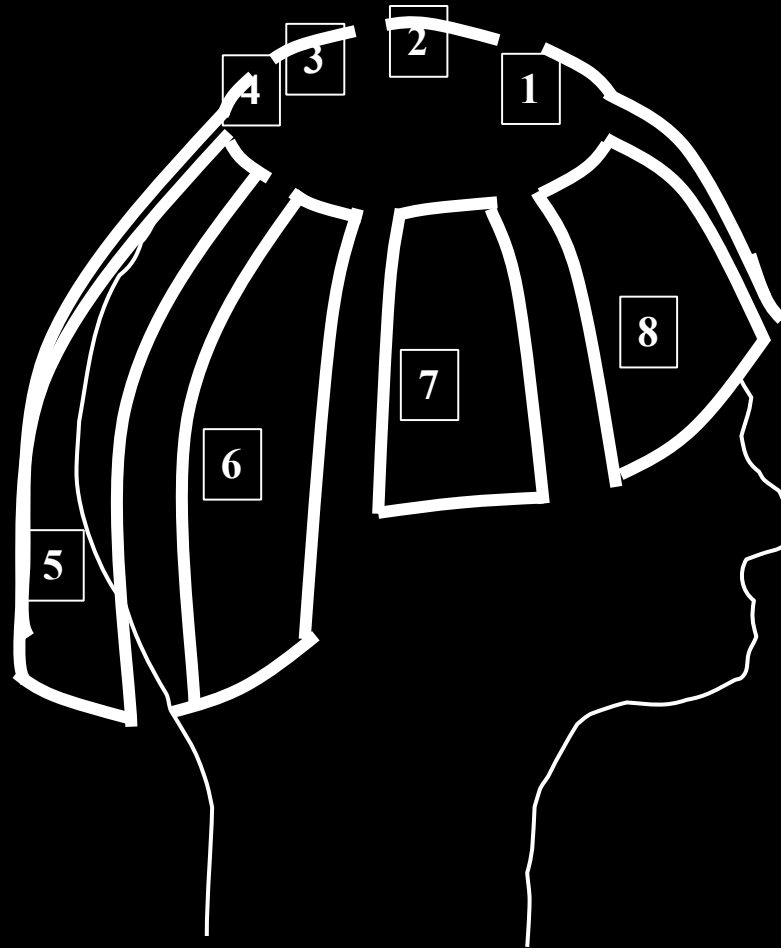
<sup>c</sup> Department of Cell Biology, Neurobiology and Anatomy, Medical College of Wisconsin, Milwaukee, WI 53226, USA

Received 16 August 2002; revised 29 October 2002; accepted 21 November 2002

NeuroImage



# General concept



# MRI Reception Hardware – 16 channels

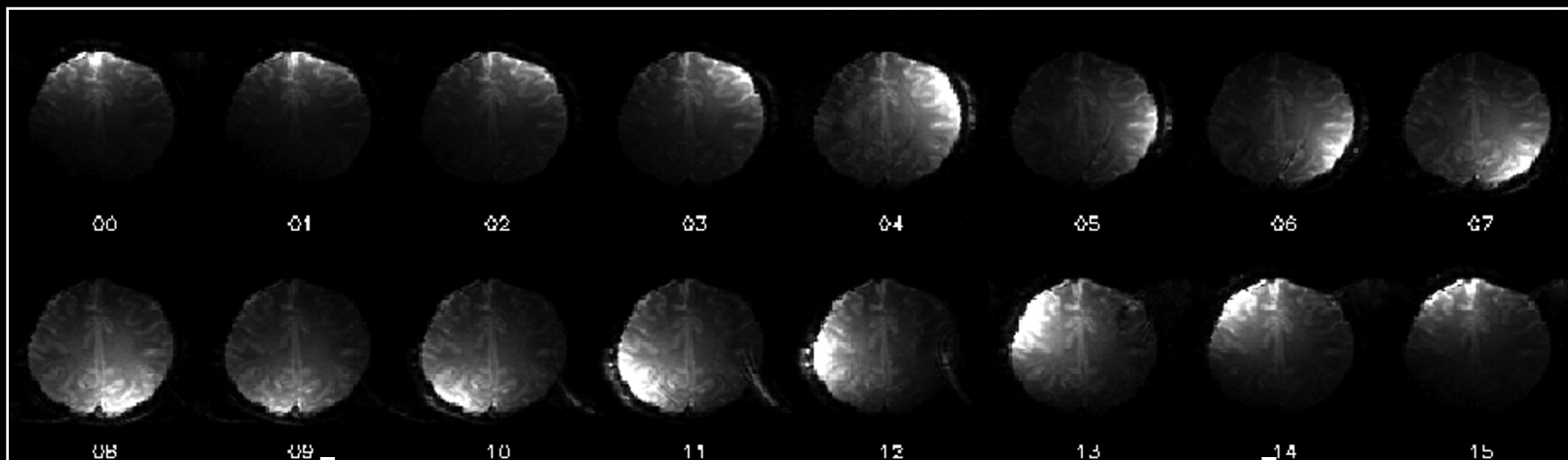
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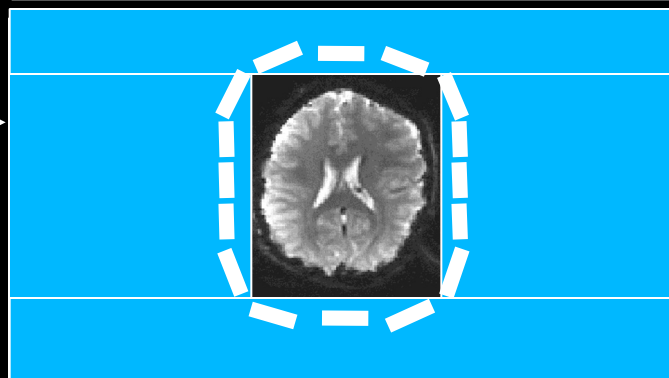
Built by Nova Medical Inc.

de Zwart et al. MRM 51:22 (2004).

# Individual coil images



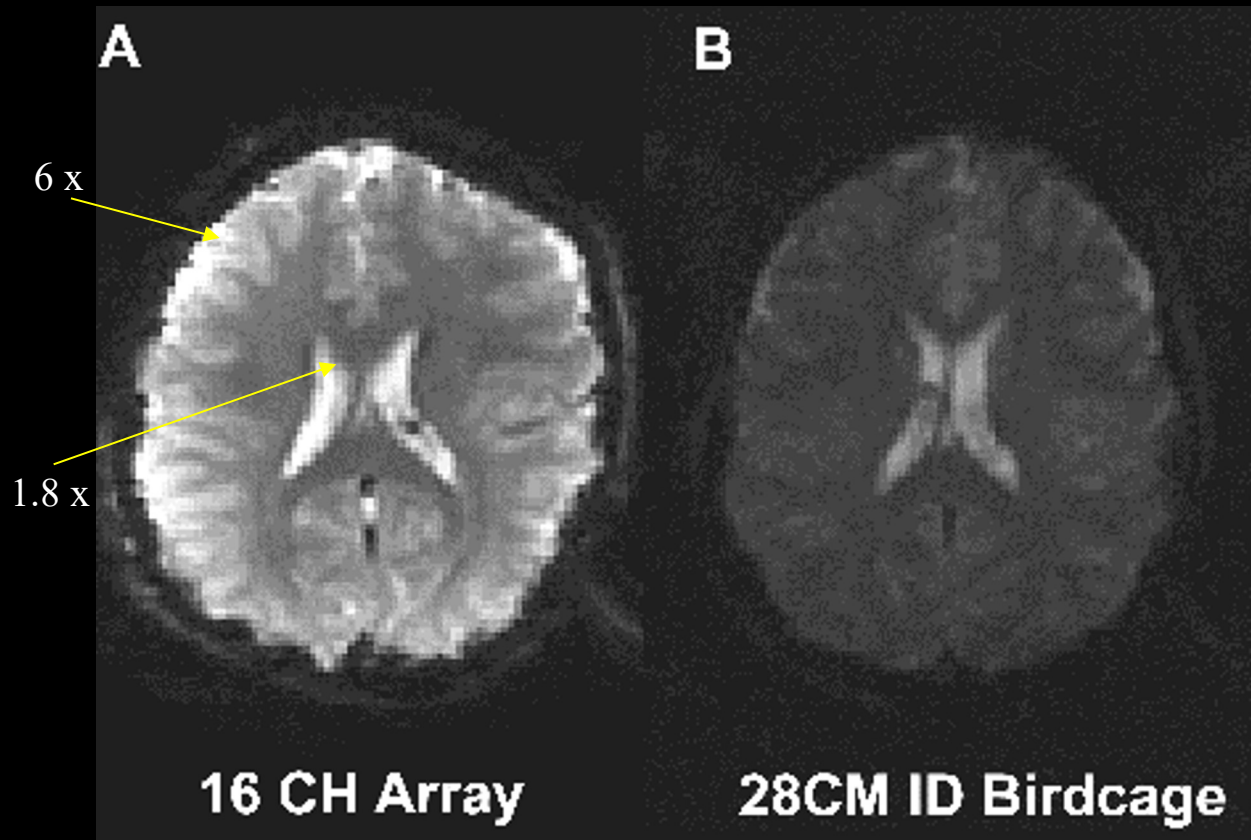
Single combined image



# Experimental Data

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## SNR comparison



Both images are in the same scale.  
Relative intensity corresponds to SNR.

3-fold SNR improvements

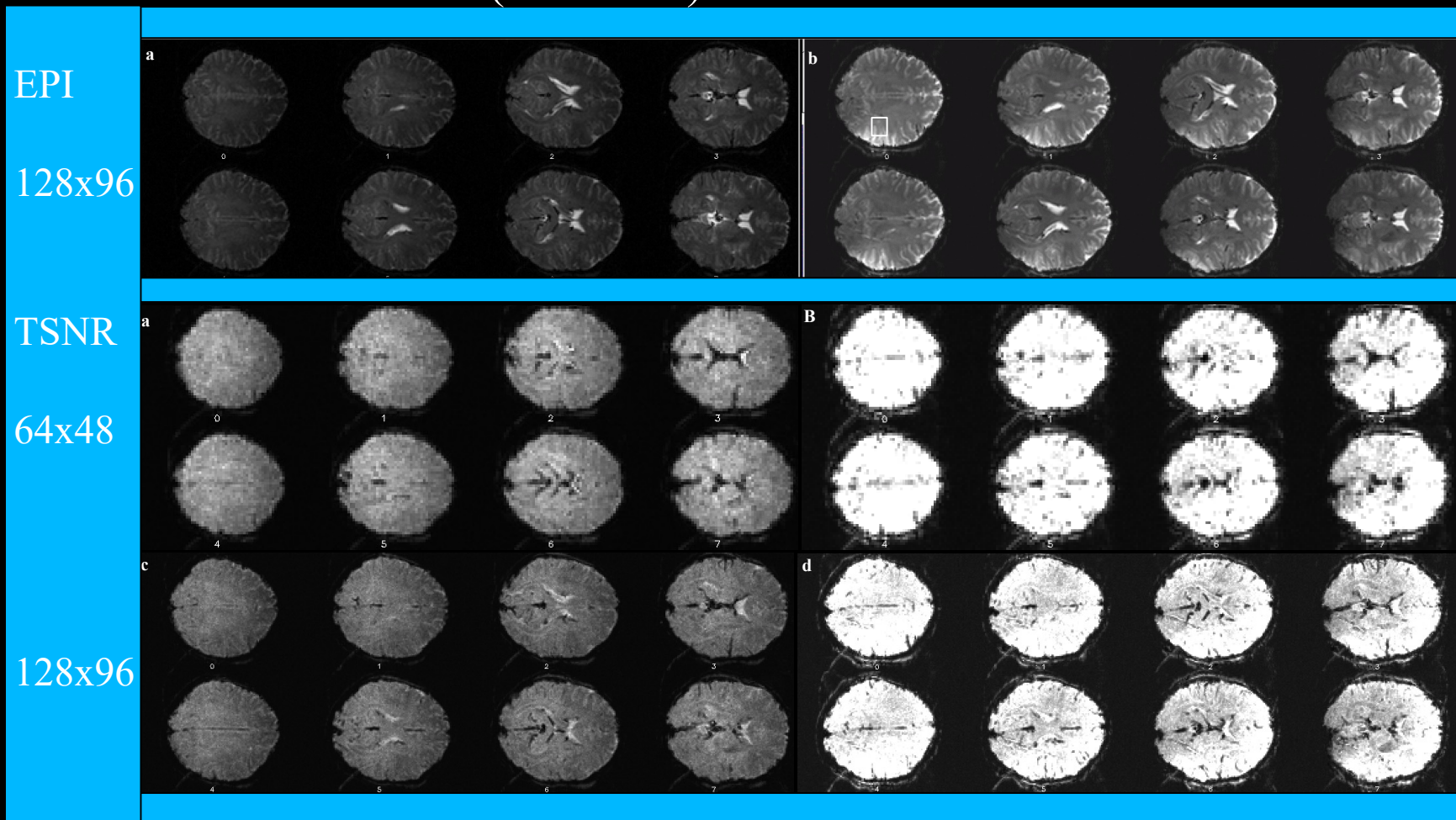


# Experimental Data

TSNR comparison

1 channel (MAI coil)

16 channel

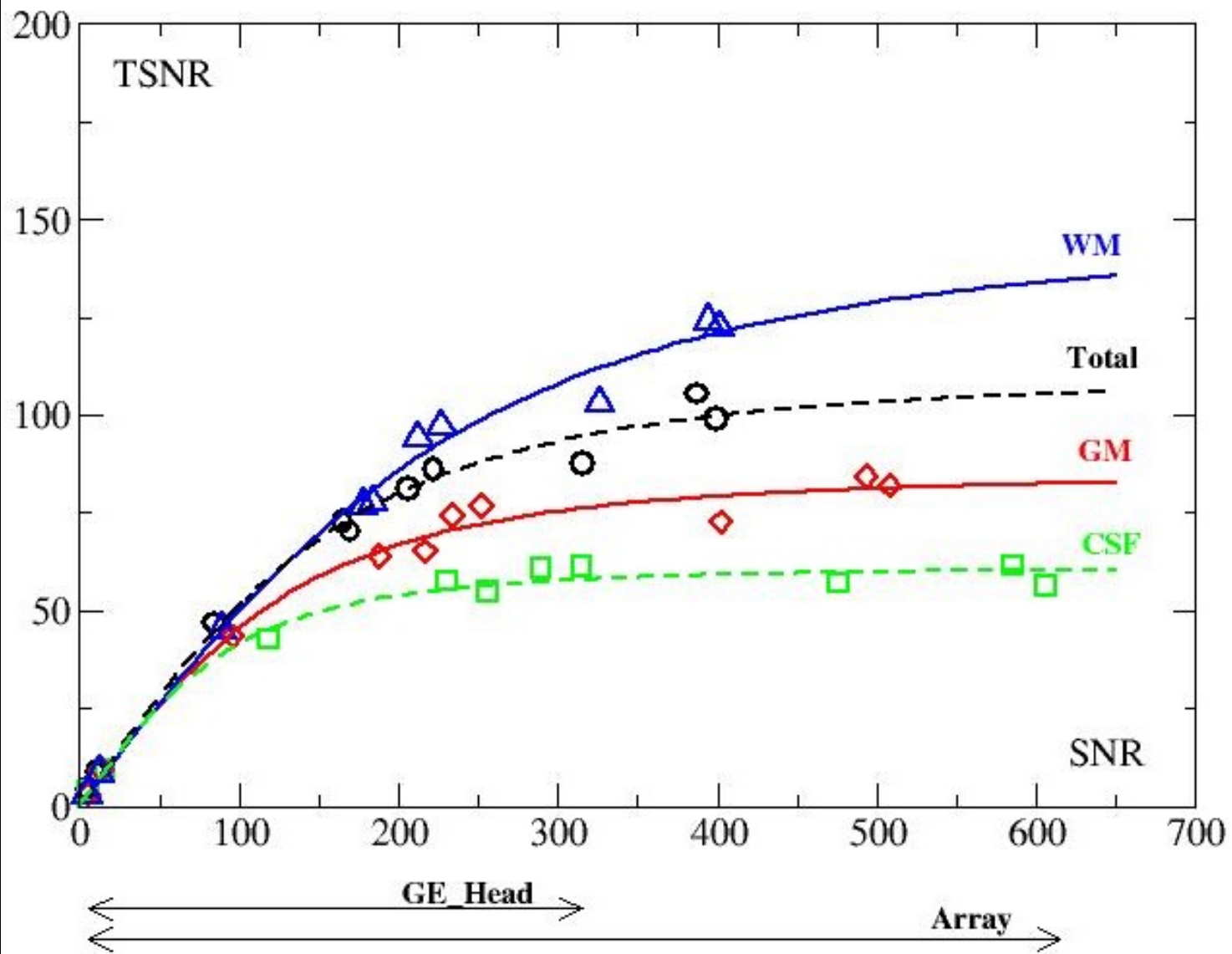


$TSNR_{16}/TSNR_1 :$

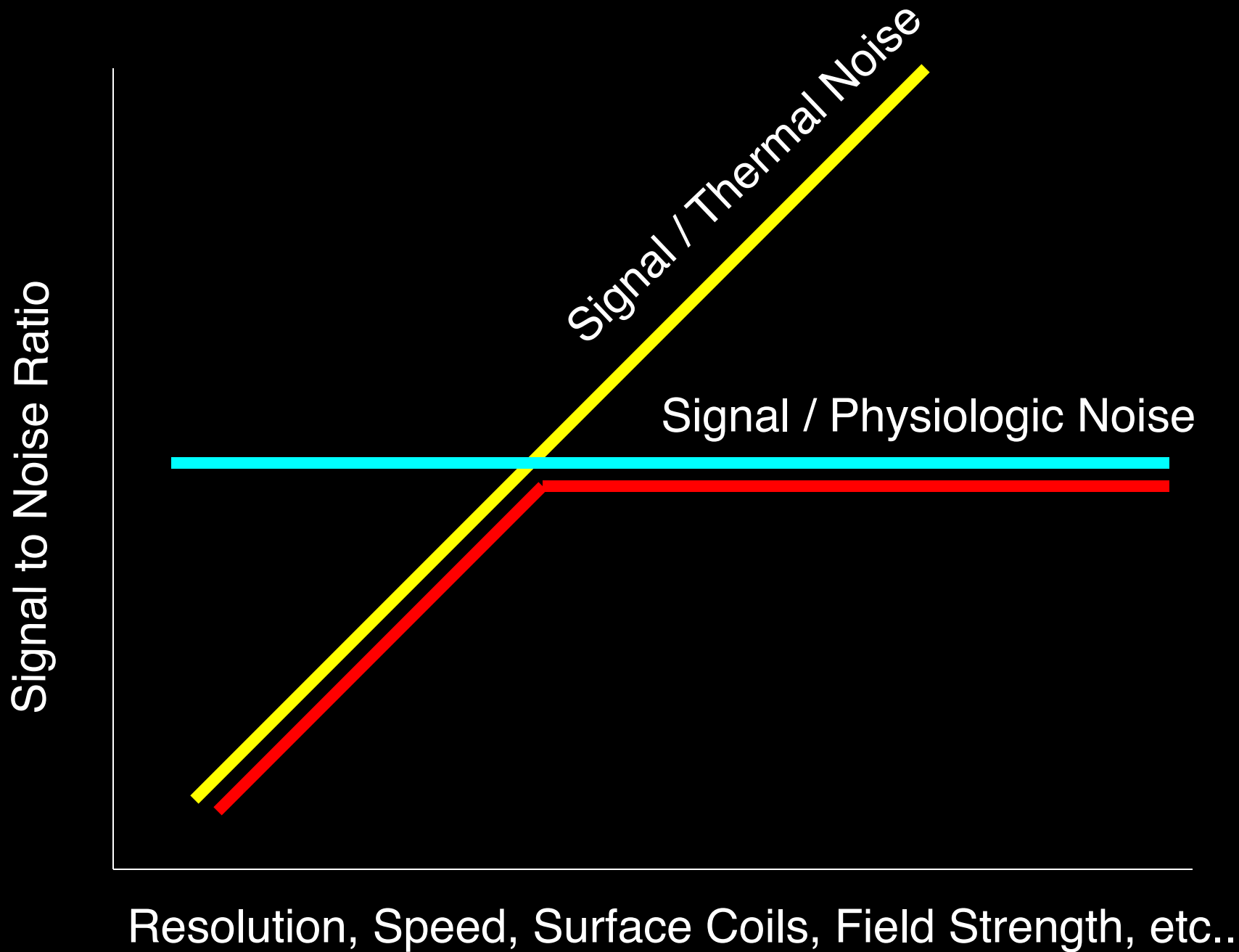
ROI: 64x48  $\rightarrow$  1.98 +/- 0.52

128x96  $\rightarrow$  2.2 +/- 0.53

An average over all slices for both resolutions  $\rightarrow$  1.7 +/- 0.3



Bodurka et al.



# Resolution

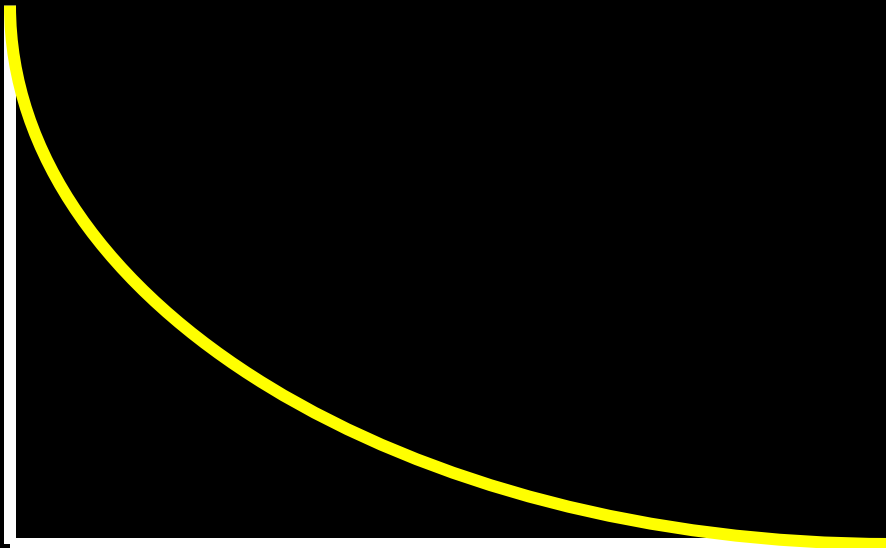
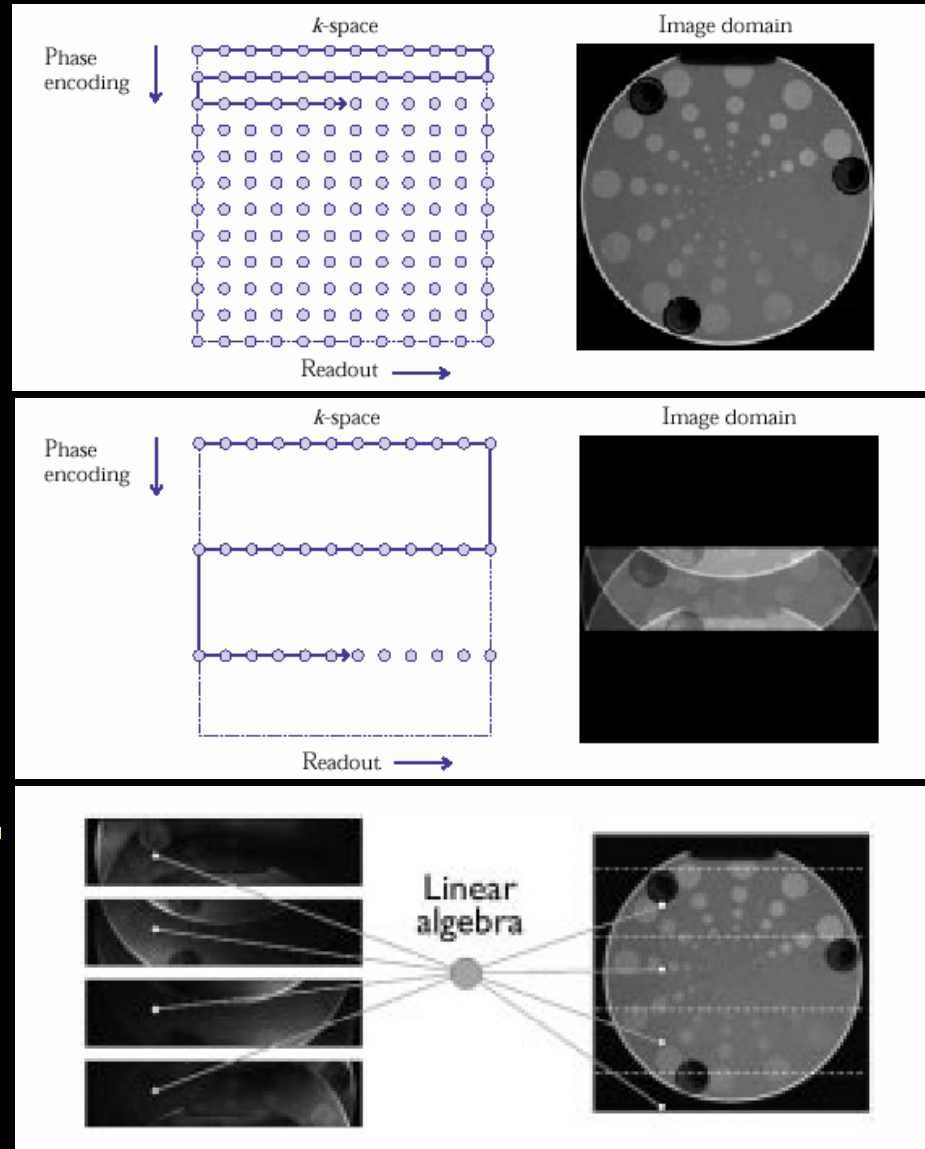
## Methods to increase:

- Faster sampling rate per image
- Faster gradient switching
- Longer readout window
- Partial k-space
- Multi-shot techniques
- Parallel Imaging

## Bottom Line:

- Up against limits in most methods
- Multi-shot still problematic (time, stability)
- Parallel imaging is most promising

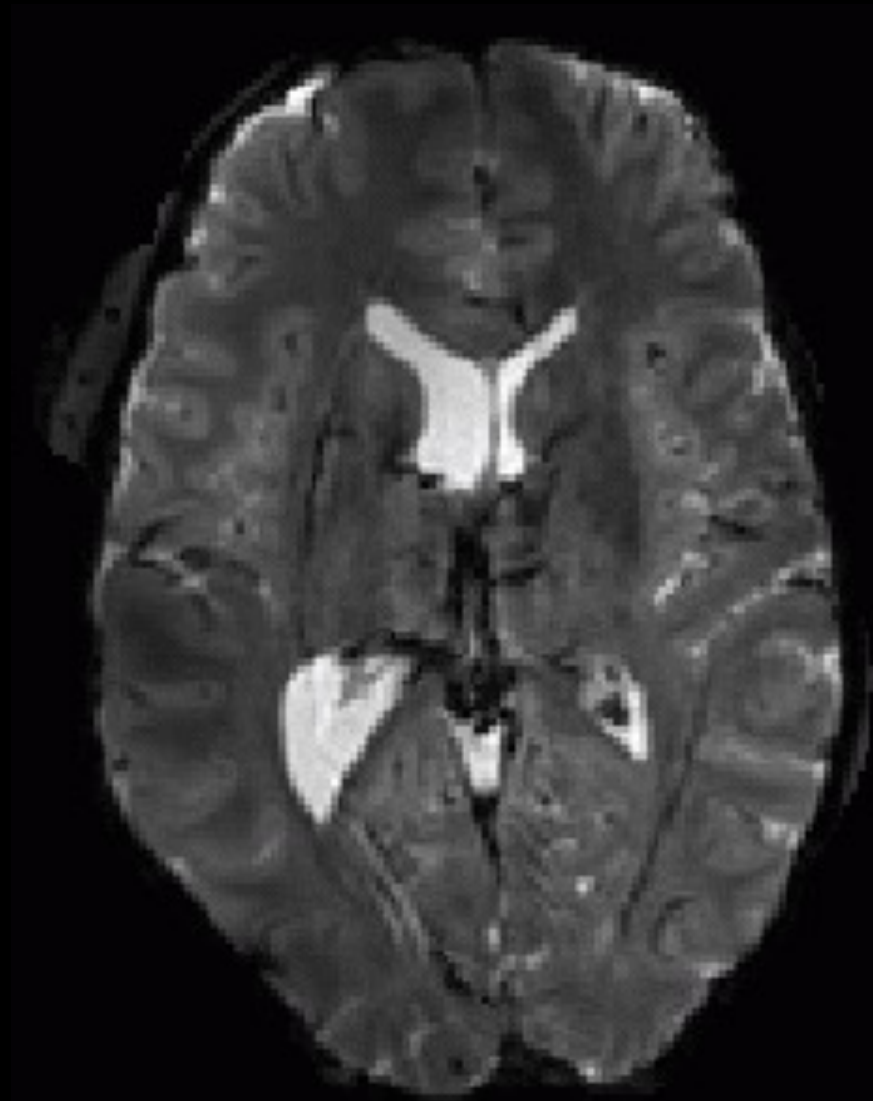
# SENSE Imaging



$\approx 5$  to  $30$  ms

Pruessmann, et al.

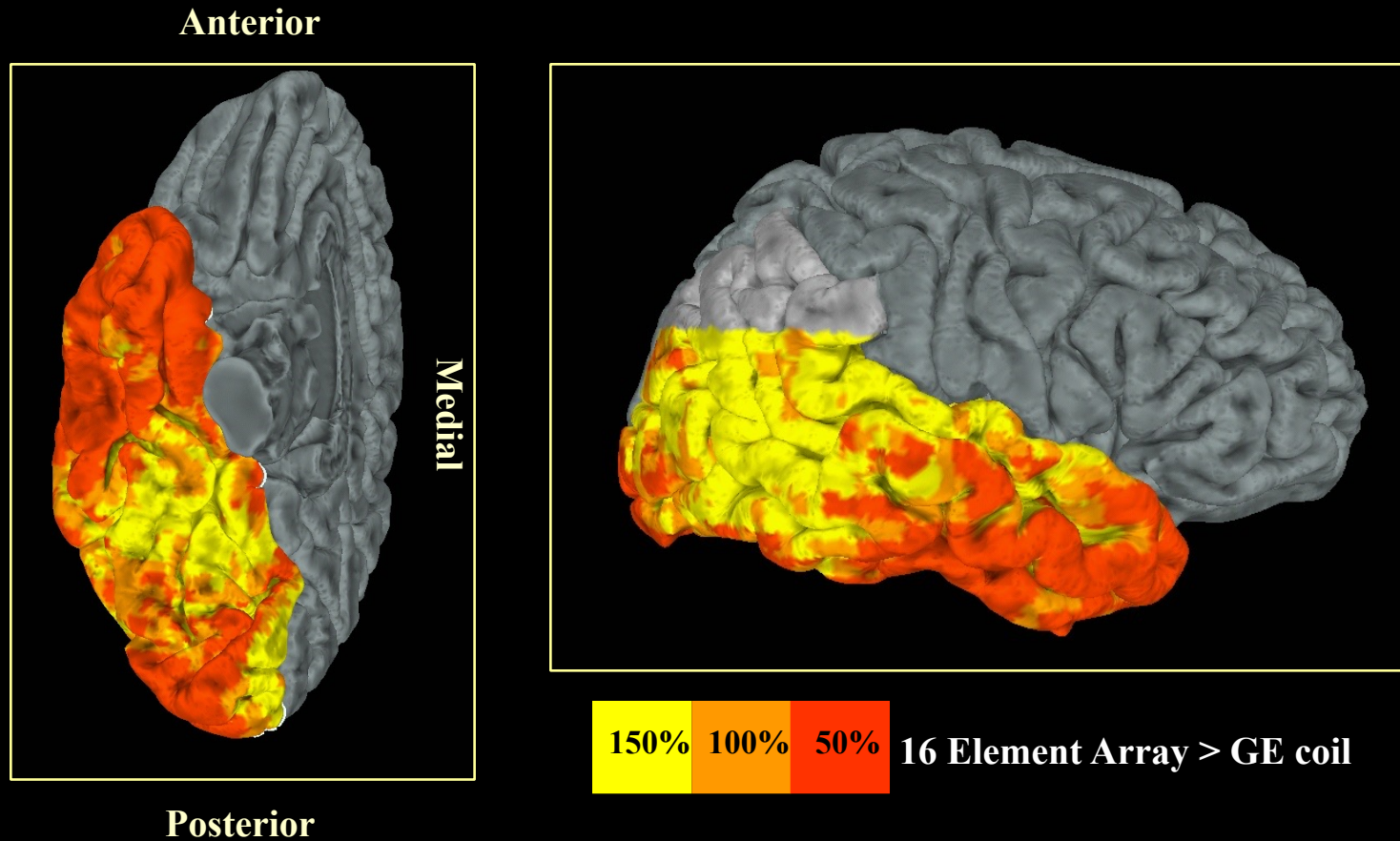
Axial-oblique single  
shot SENSE EPI  
using 16-channel  
reception. 192x144 :  
1.25x1.25x2mm





# Average Temporal Signal-to-Noise ratio Comparison Between Coils

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# Shimming

A solvable problem:

- more shim coils and/or coil designs
- increased shim currents
- higher resolution (fixes dropout)
- shorter readout window (fixes distortion)
- shim inserts
- z-shim methods

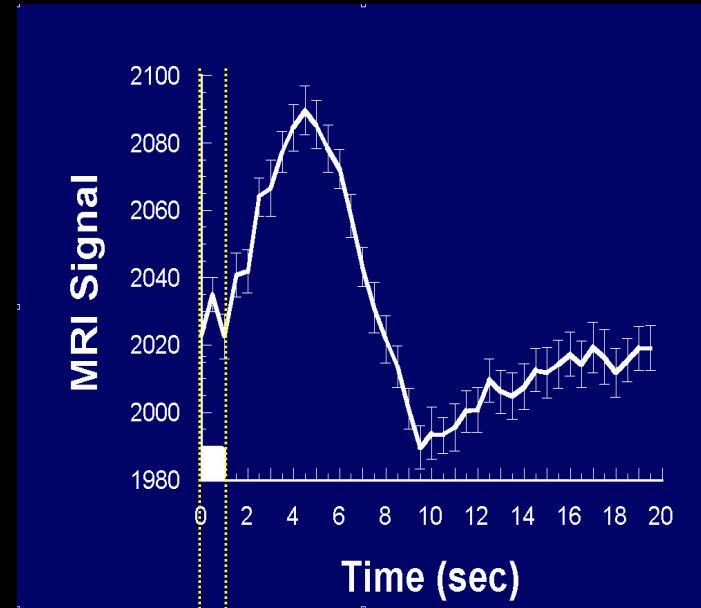
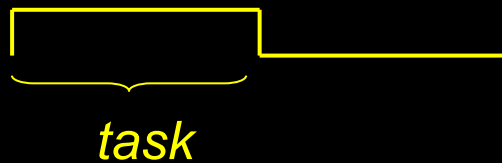
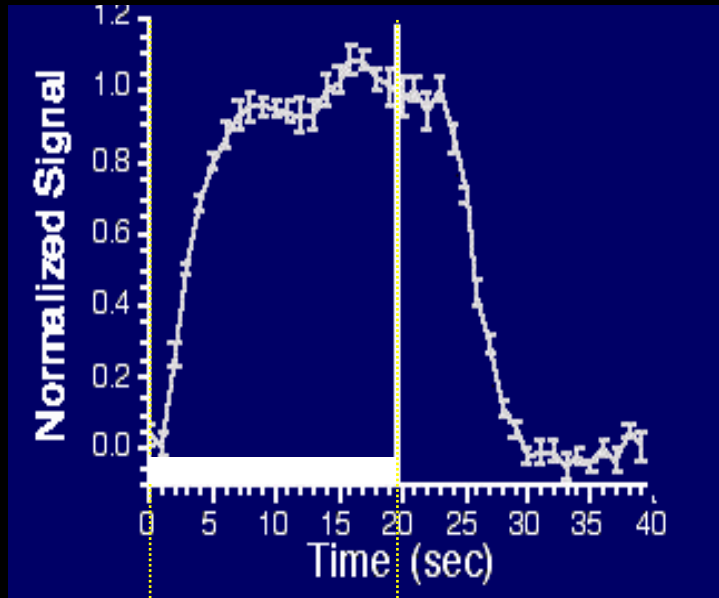
## Methodology

- Temporal resolution
- Spatial specificity
- Magnitude Calibration
- Multi-subject averaging/normalization at very high resolution
- Paradigm design
- Motion (very slow and motion correlated)
- Scanner acoustic noise effect removal
- Individual Map “Classification”
- Local pattern effect mapping and classification
- Exploratory analysis techniques (ICA, PCA..)
- Temporal fluctuations (removal and use)
- Simultaneous measures with fMRI
- Baseline susceptibility mapping
- Non-invasive blood volume imaging
- Multimodal integration
- Functional Connectivity mapping
- Real time fMRI
- Neuronal Current MRI

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# Temporal resolution

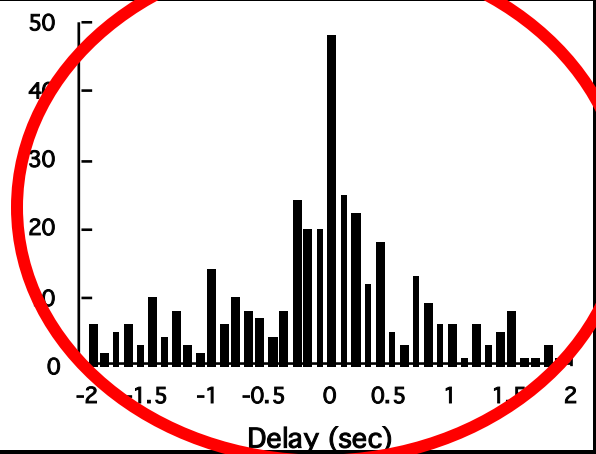
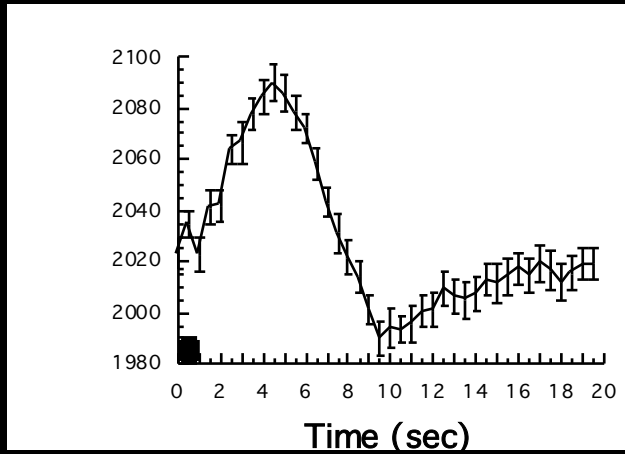
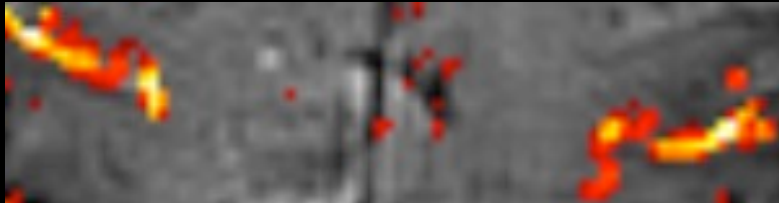
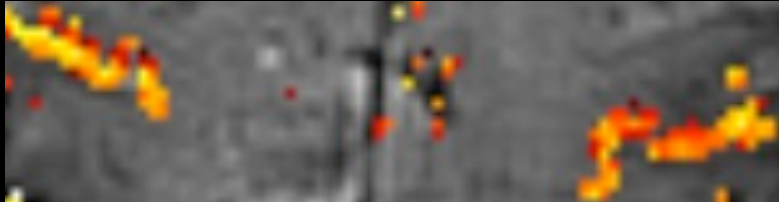


The major obstacle in BOLD contrast temporal resolution:

Latency

Magnitude

Venogram

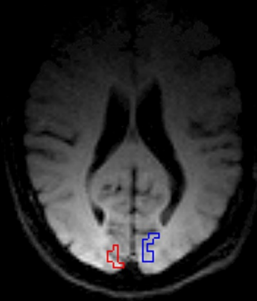


P. A. Bandettini, The temporal resolution of Functional MRI in "Functional MRI" (C. Moonen, and P. Bandettini., Eds.), p. 205-220, Springer - Verlag,. 1999.

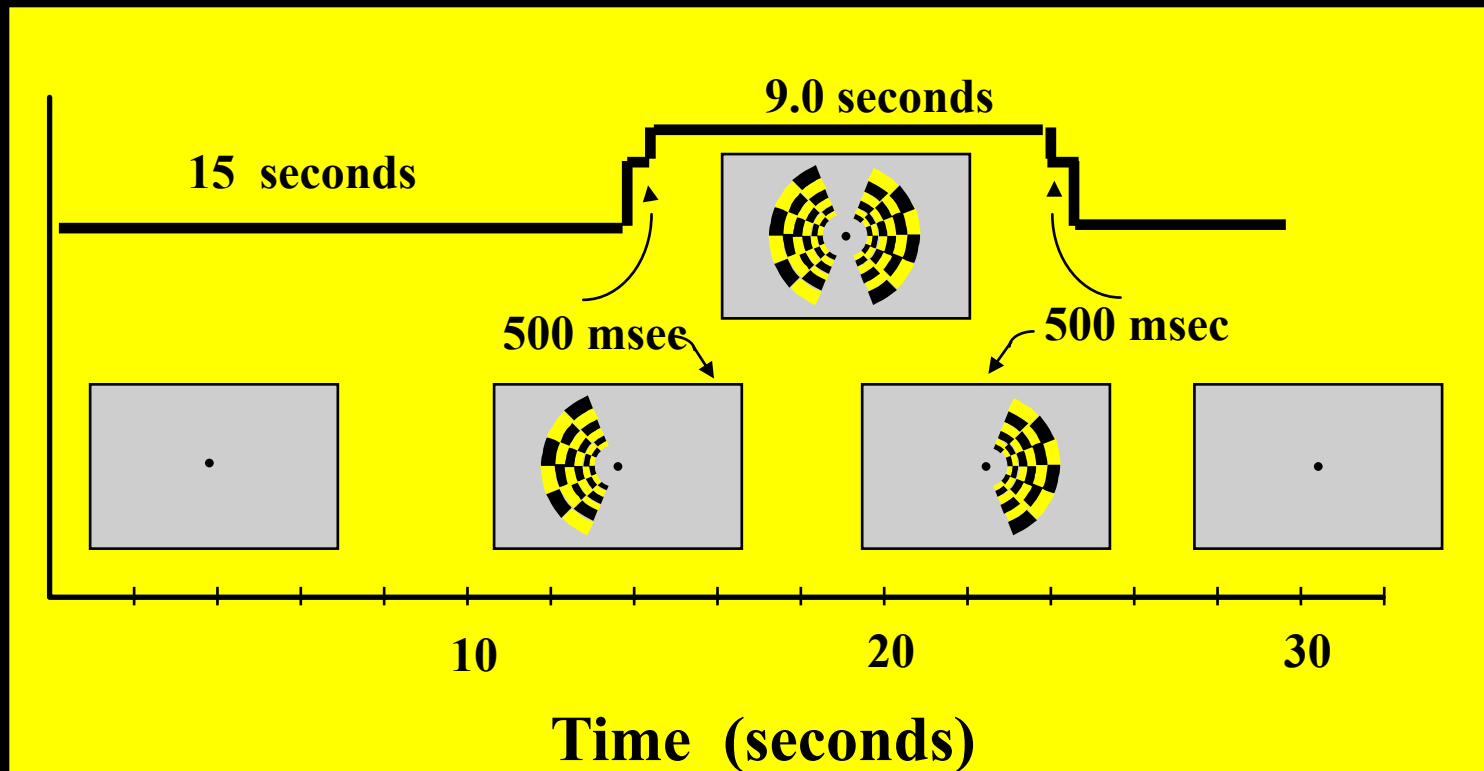


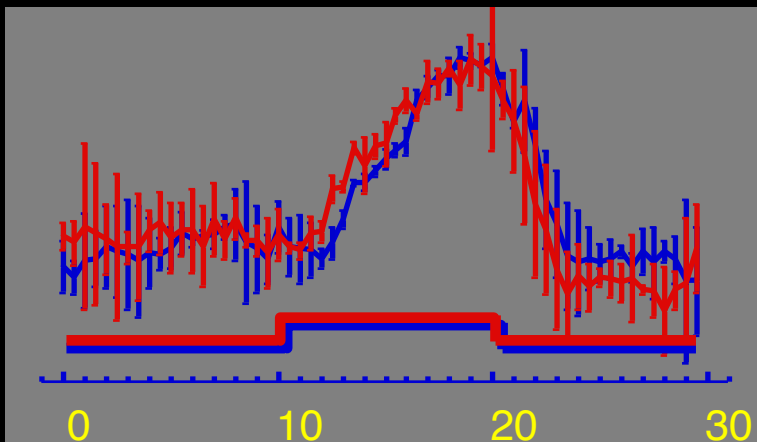
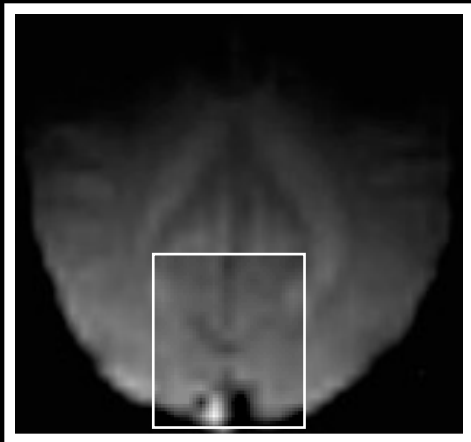
# Hemi-Field Experiment

**Right Hemisphere**



**Left Hemisphere**





500 ms

||



500 ms

||



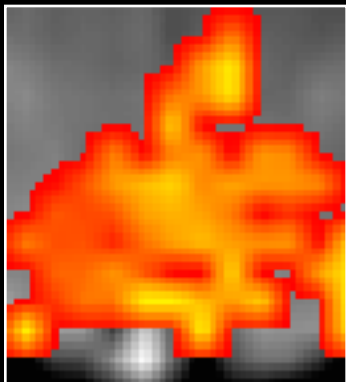
Right Hemifield

Left Hemifield

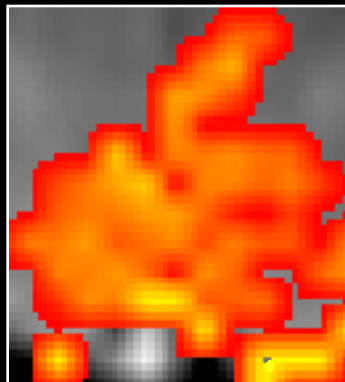
+ 2.5 s

0 s

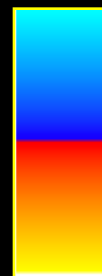
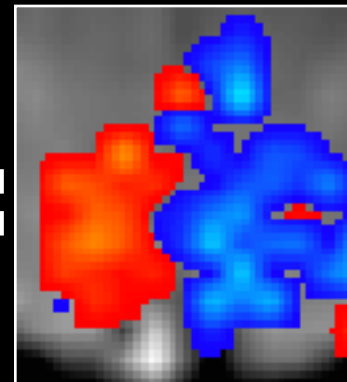
- 2.5 s



-



=



# Cognitive Neuroscience Application:

## Understanding neural system dynamics through task modulation and measurement of functional MRI amplitude, latency, and width

PNAS

P. S. F. Bellgowan<sup>\*,†</sup>, Z. S. Saad<sup>‡</sup>, and P. A. Bandettini<sup>\*</sup>

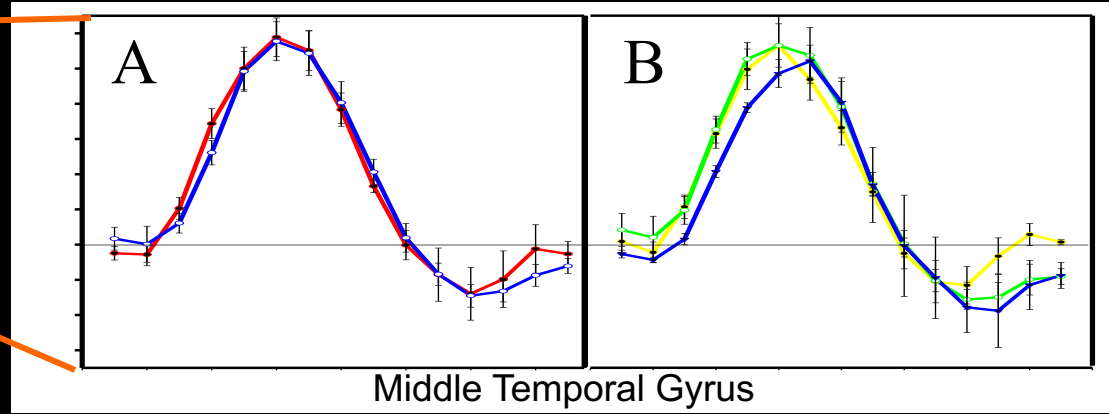
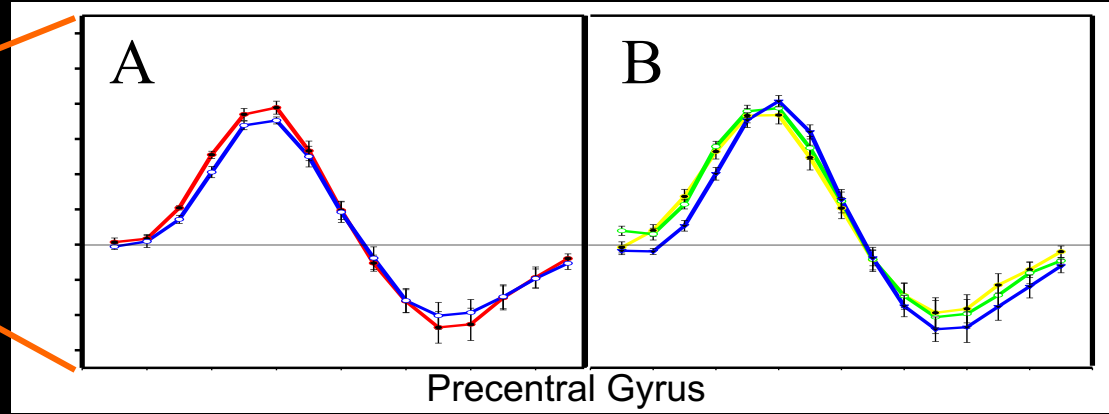
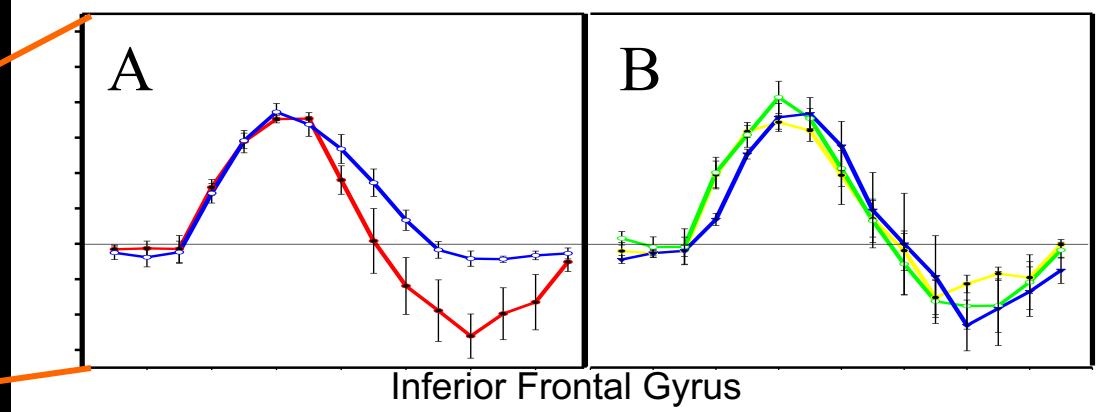
<sup>\*</sup>Laboratory of Brain and Cognition and <sup>†</sup>Scientific and Statistical Computing Core, National Institute of Mental Health, Bethesda, MD 20892

Communicated by Leslie G. Ungerleider, National Institutes of Health, Bethesda, MD, December 19, 2002 (received for review October 31, 2002)

		Lexical Delay		
		Words	Non-Words	Mean Reaction Time
Rotational Delay	0°	smudge	dierts	823 ms
	60°	frollic	cuhlos	891 ms
	120°	sloach	gednus	1446 ms
Mean Reaction Time		986 ms	1219 ms	

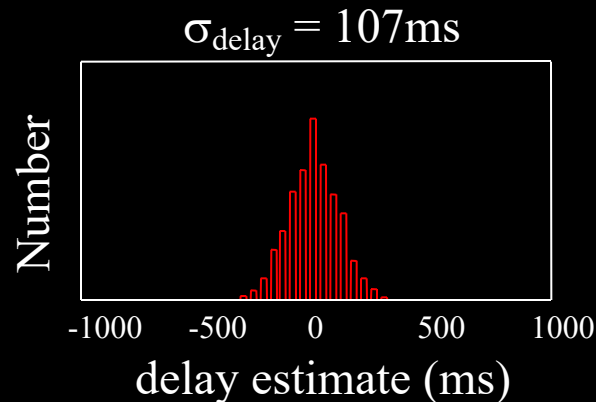
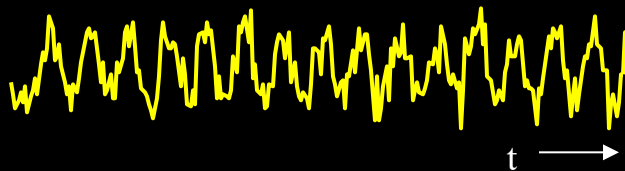
**Word vs. Non-word**    **0°, 60°, 120° Rotation**

**Regions of Interest**

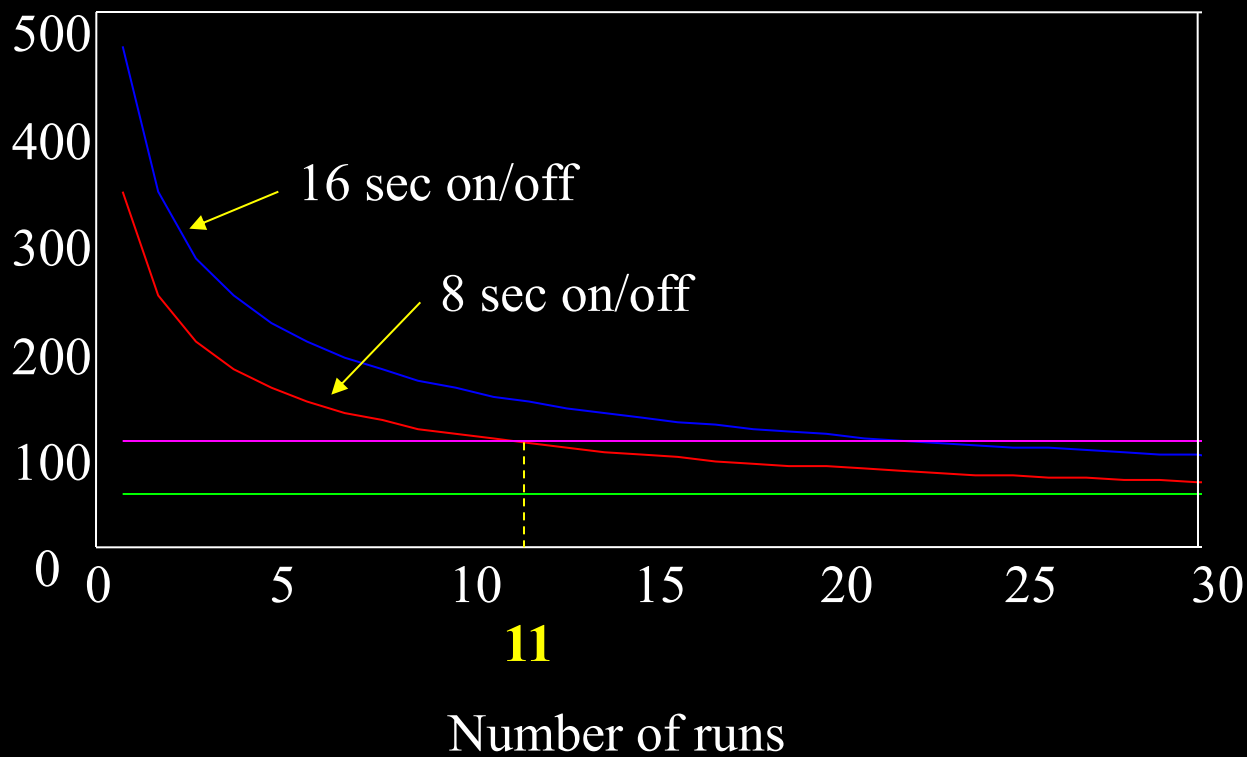


1 run:

1% Noise  
4% BOLD  
256 time pts /run  
1 second TR



Smallest latency  
Variation Detectable  
(ms) ( $p < 0.001$ )



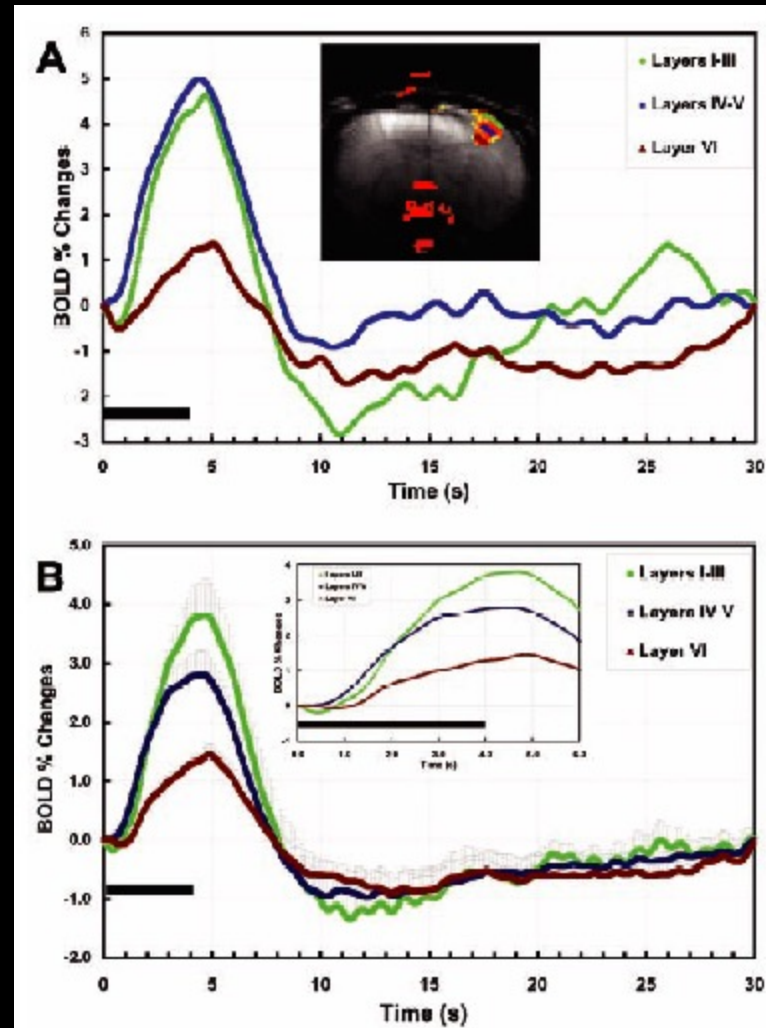
# Laminar specificity of functional MRI onset times during somatosensory stimulation in rat

Afonso C. Silva\* and Alan P. Koretsky

Laboratory of Functional and Molecular Imaging, National Institute of Neurological Disorders and Stroke, Bethesda, MD 20892

15182-15187 | PNAS | November 12, 2002 | vol. 99 | no. 23

No calibration



11.7 T

# Paradigm Design

1. Block Design

2. Parametric Design

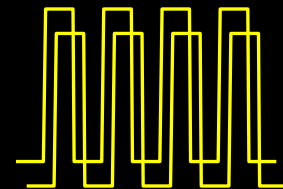
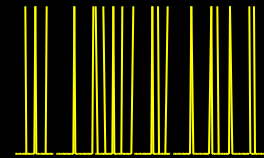
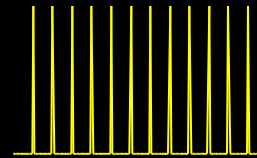
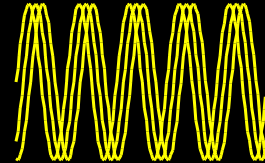
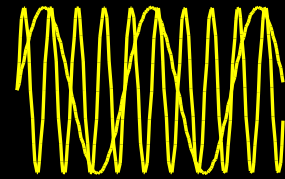
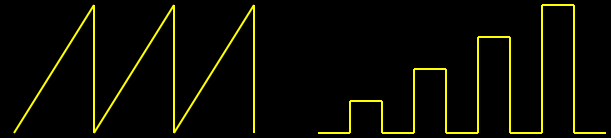
3. Frequency Encoding

4. Phase Encoding

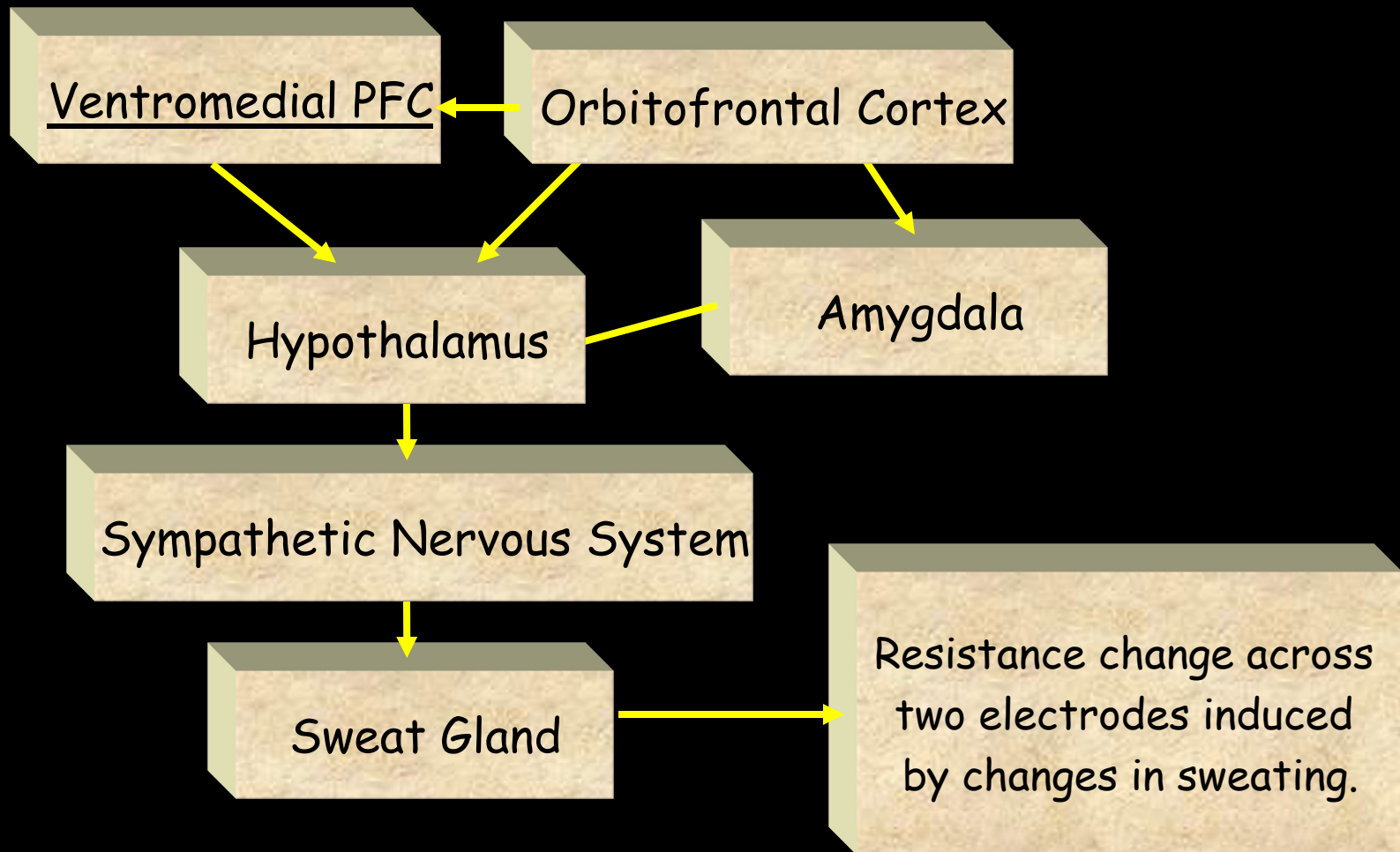
5. Event Related

6. Orthogonal Design

7. Free Behavior Design

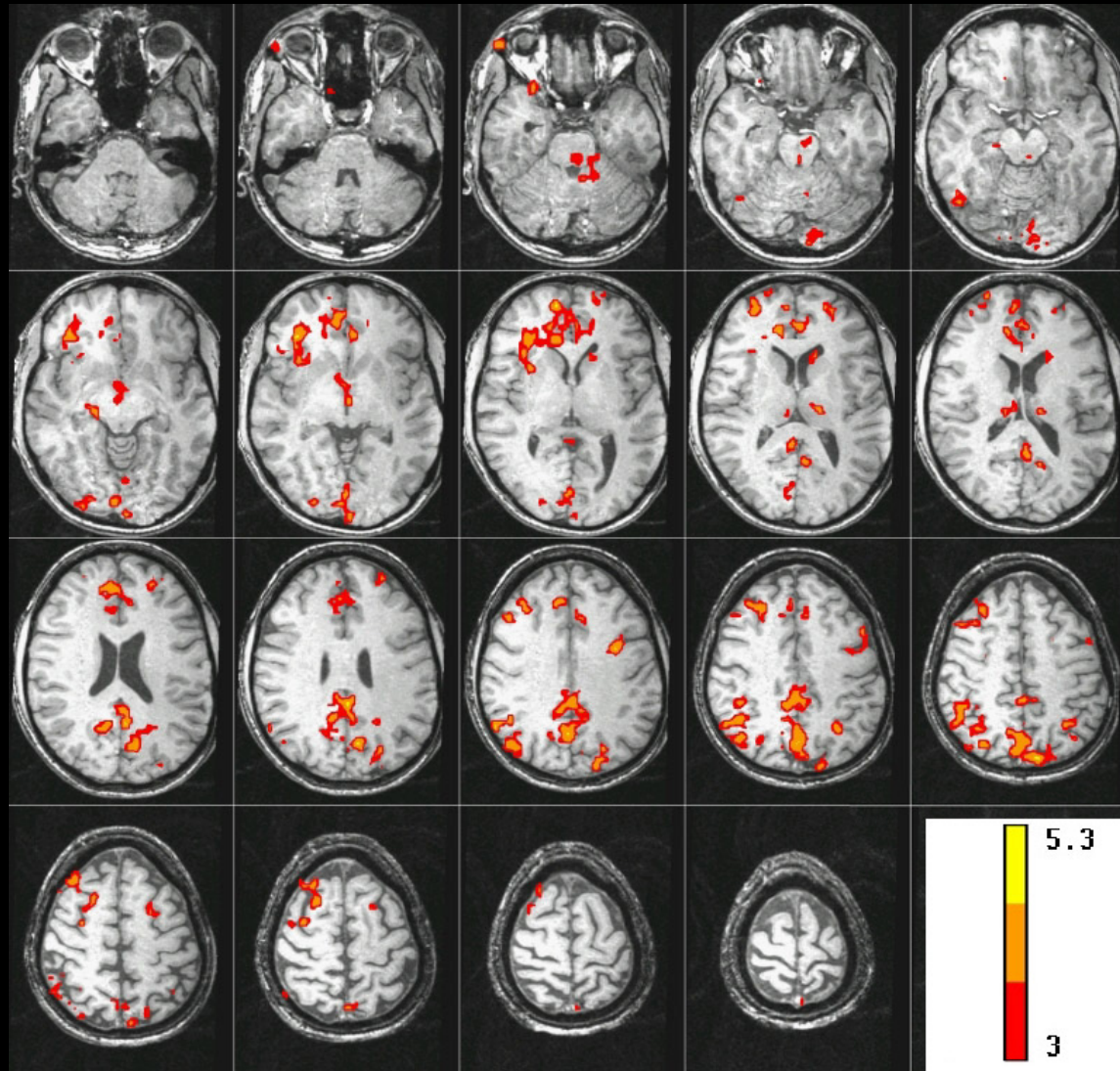


# The Skin Conductance Response (SCR)





# Brain activity correlated with SCR during “Rest”



J. C. Patterson II, L. G. Ungerleider, and P. A. Bandettini, Task - independent functional brain activity correlation with skin conductance changes: an fMRI study. *NeuroImage* 17: 1787-1806, (2002).

# Simultaneous EEG and fMRI of the alpha rhythm

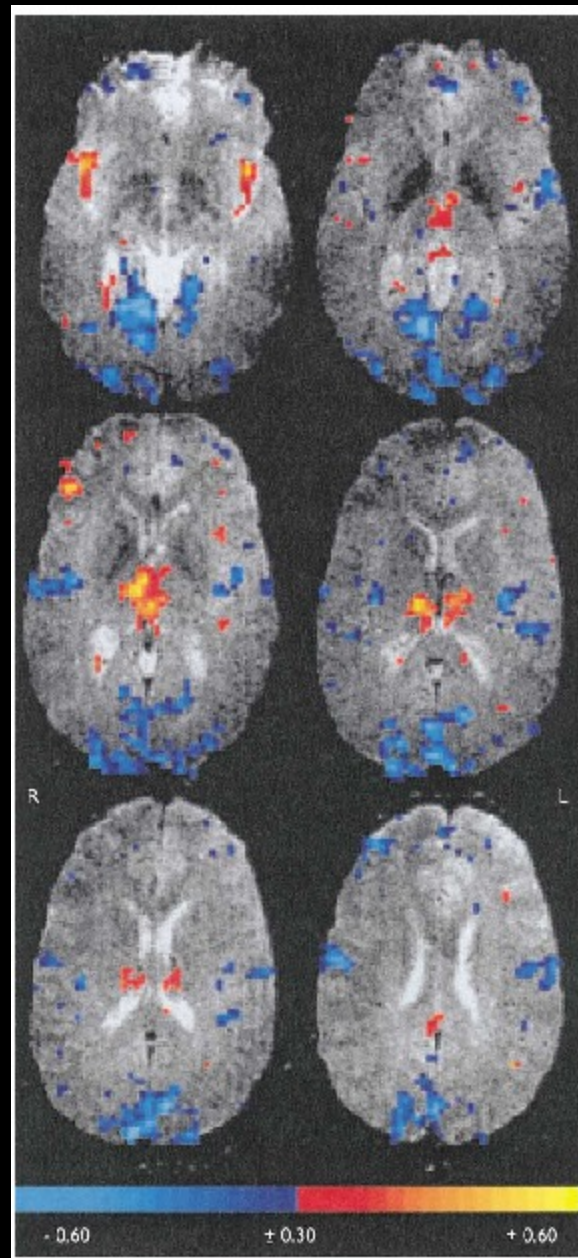
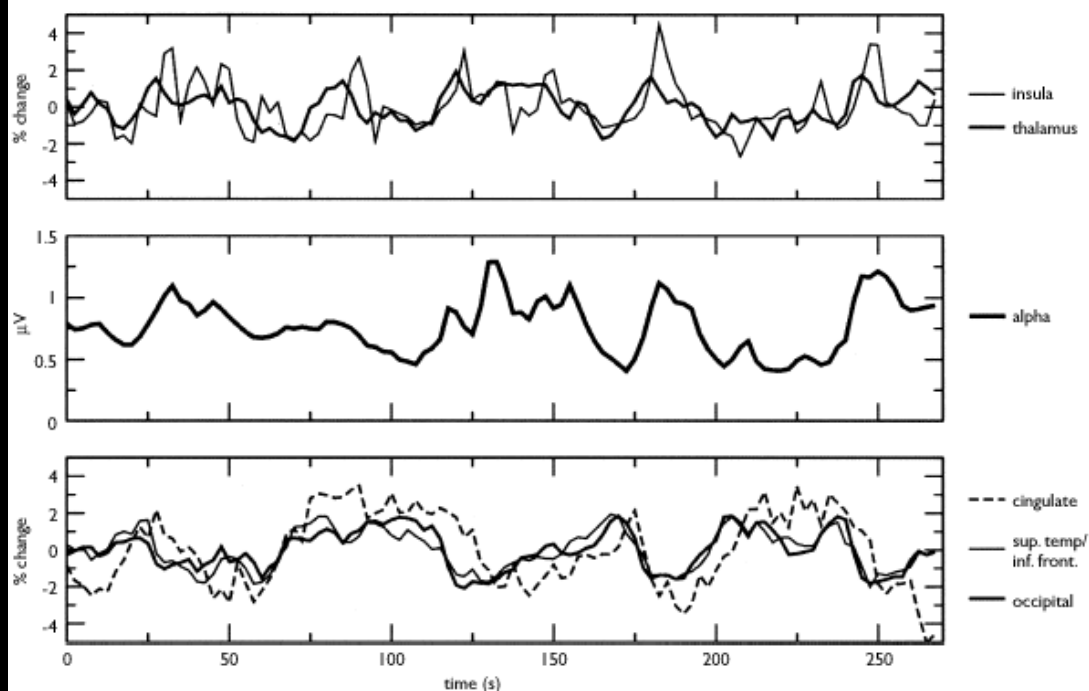
Robin I. Goldman,<sup>2,CA</sup> John M. Stern,<sup>1</sup> Jerome Engel Jr<sup>1</sup> and Mark S. Cohen

Ahmanson-Lovelace Brain Mapping Center, UCLA, 660 Charles Young Drive South, Los Angeles, CA 90095; <sup>1</sup>Department of Neurology, UCLA School of Medicine, Los Angeles, CA; <sup>2</sup>Hatch Center for MR Research, Columbia University, HSD, 710 W. 168th St., NIB-1, Mailbox 48, NY, NY 10032, USA

<sup>CA,2</sup>Corresponding Author and Address: rg2146@columbia.edu

Received 28 October 2002; accepted 30 October 2002

DOI: 10.1097/01.wnr.0000047685.08940.d0



# Motion (very slow and activation correlated)

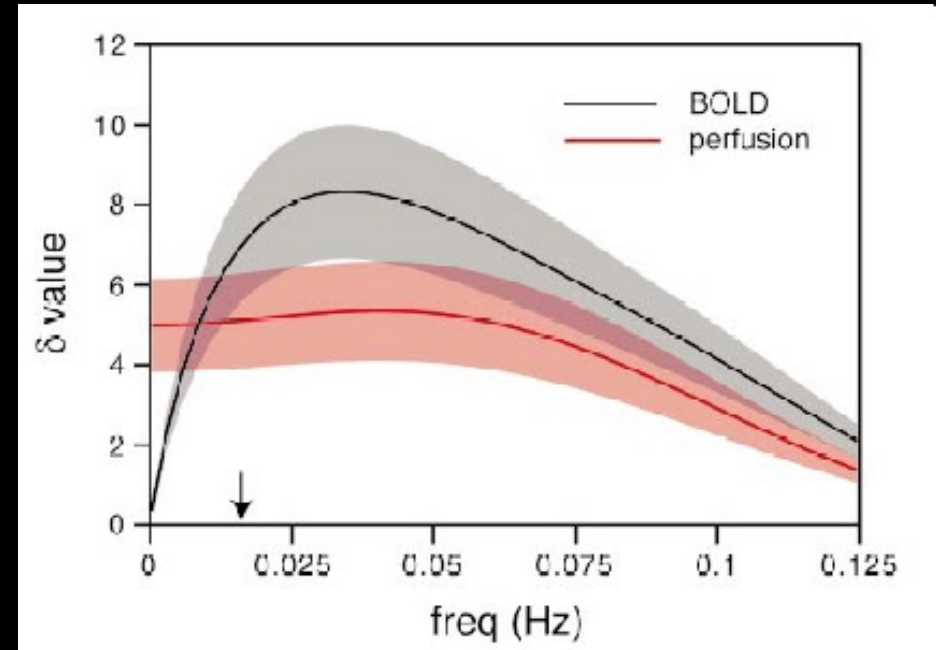
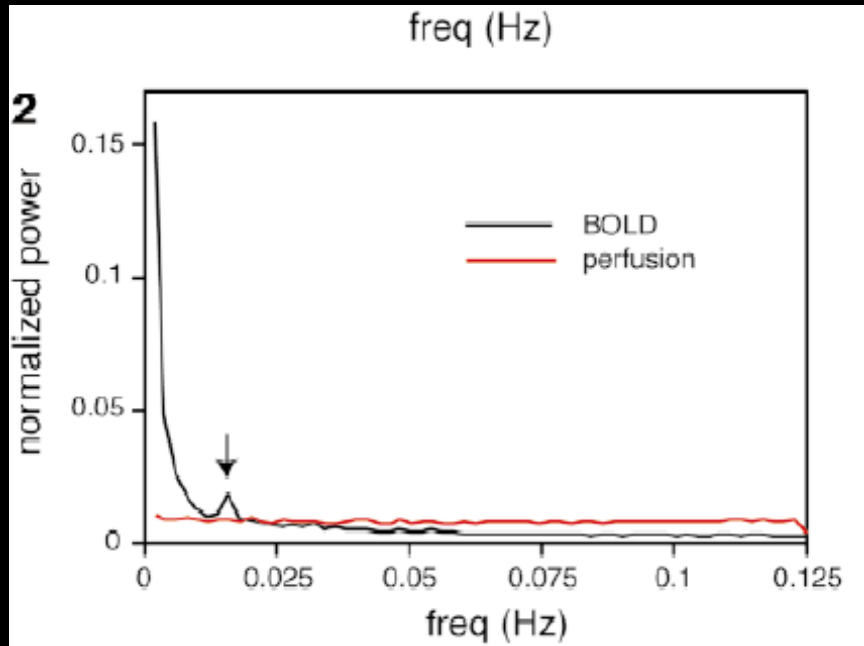
Very slow:

- a problem when looking at slow state changes
- one solution: ASL techniques

Activation correlated:

- separable from hemodynamic response

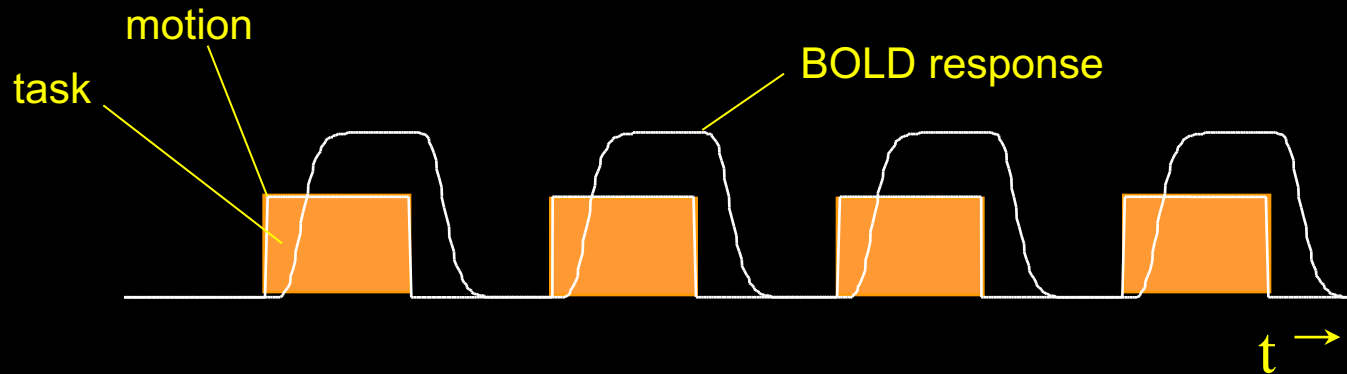
# ASL Techniques show more temporal stability



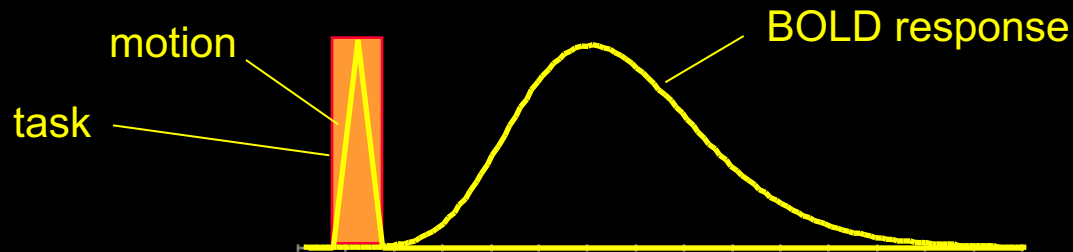
Experimental design and the relative sensitivity of BOLD and perfusion fMRI Aguirre GK, Detre JA, Zarahn E, Alsop DC, NEUROIMAGE 15 (3): 488-500 MAR 2002

# fMRI during tasks that involve brief motion

## Blocked Design



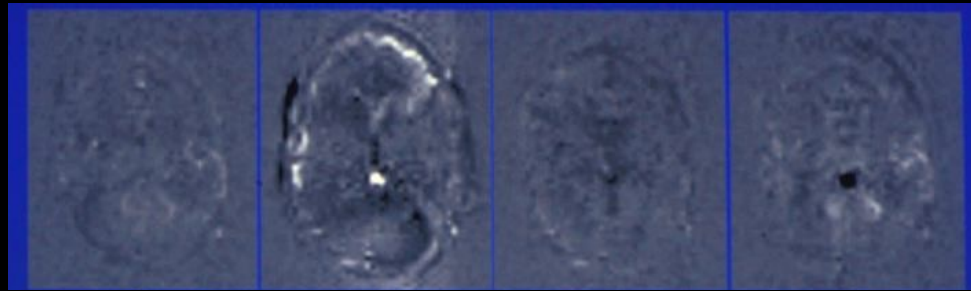
## Event-Related Design



R. M. Birn, P. A. Bandettini, R. W. Cox, R. Shaker, Event - related fMRI of tasks involving brief motion. *Human Brain Mapping* 7: 106-114 (1999).



# Overt Word Production

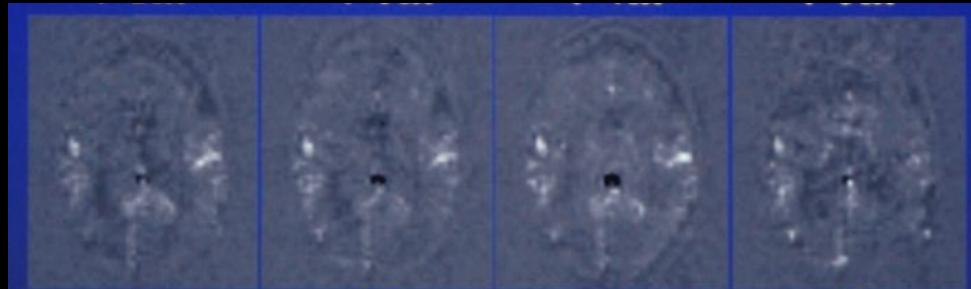


2

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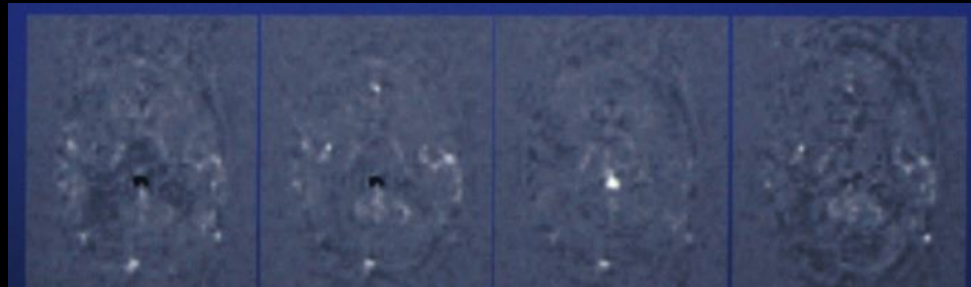


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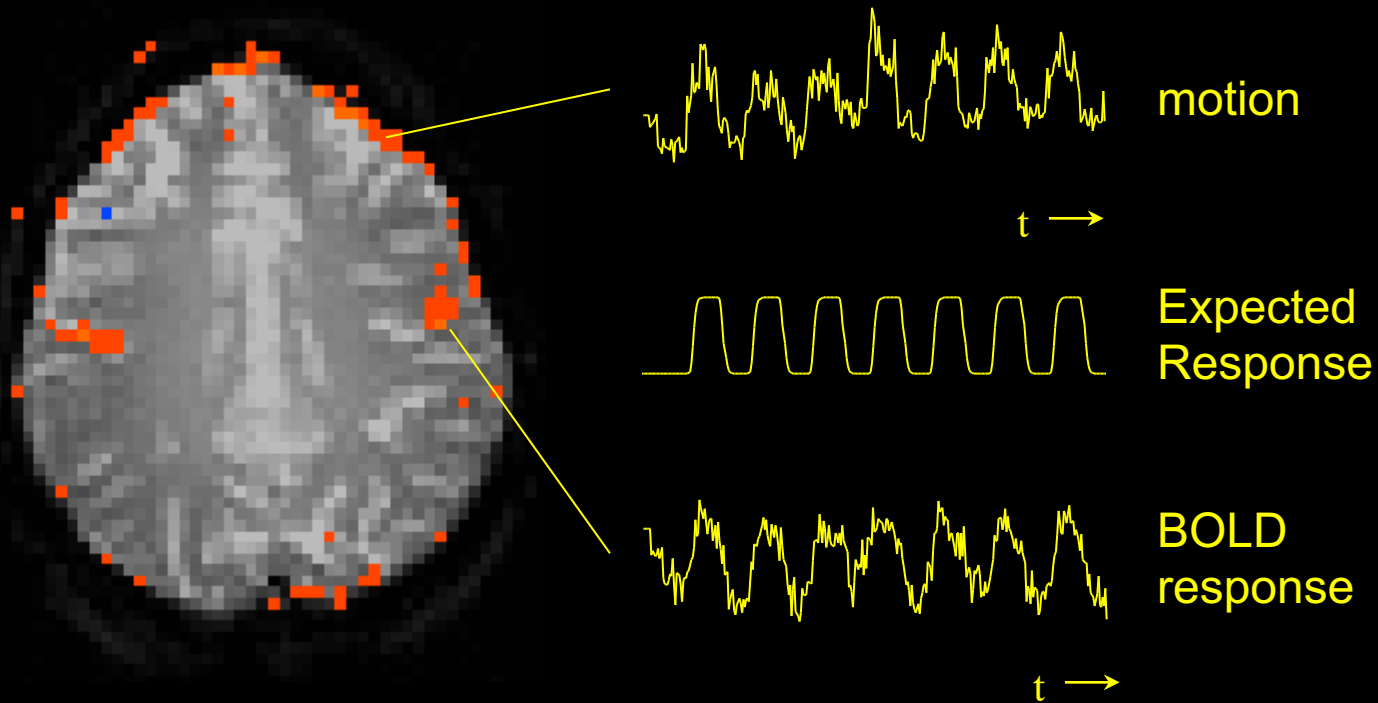
12

13

R. M. Birn, P. A. Bandettini, R. W. Cox, R. Shaker, Event - related fMRI of tasks involving brief motion. *Human Brain Mapping* 7: 106-114 (1999).

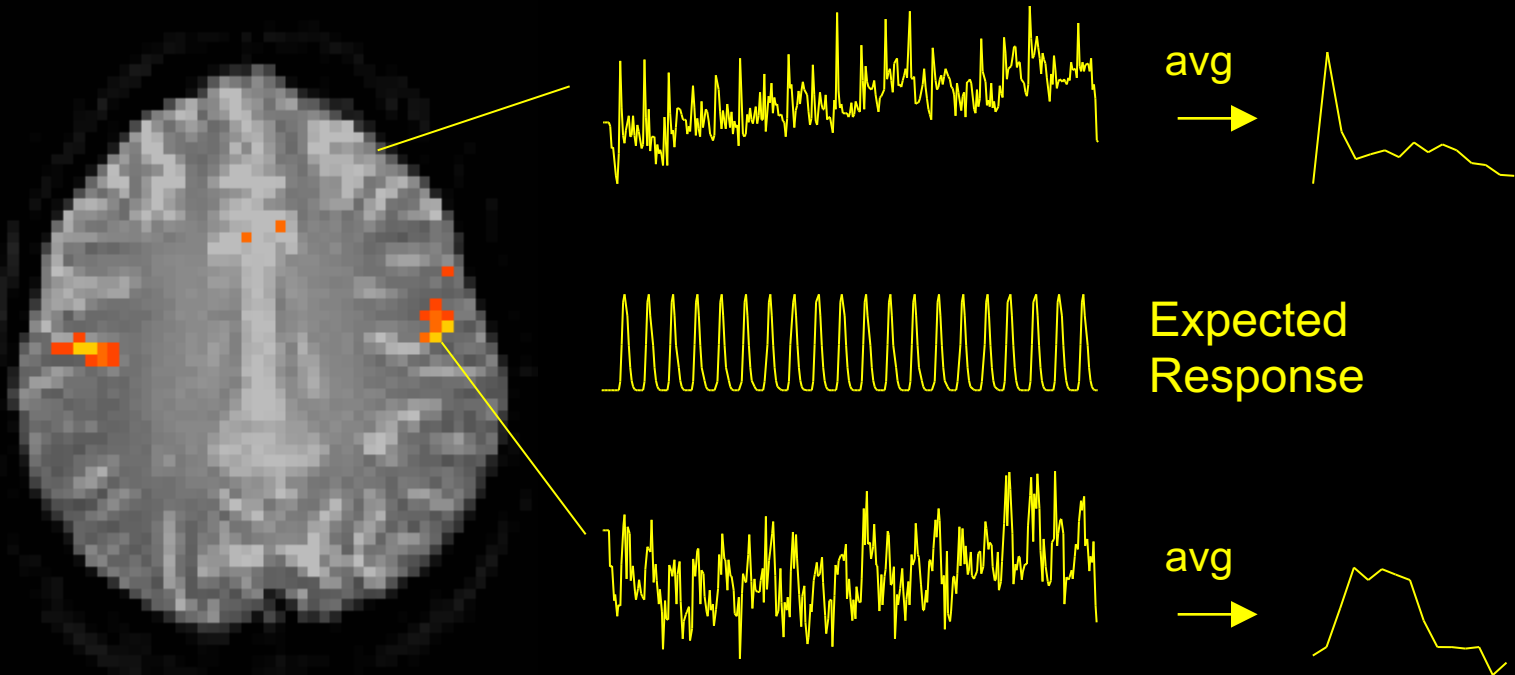
# Speaking – Blocked design

*R.M. Birn, et al. Human Brain Mapping 7(2), 106-114, 1999*



# Speaking – Event related design *Constant ISI*

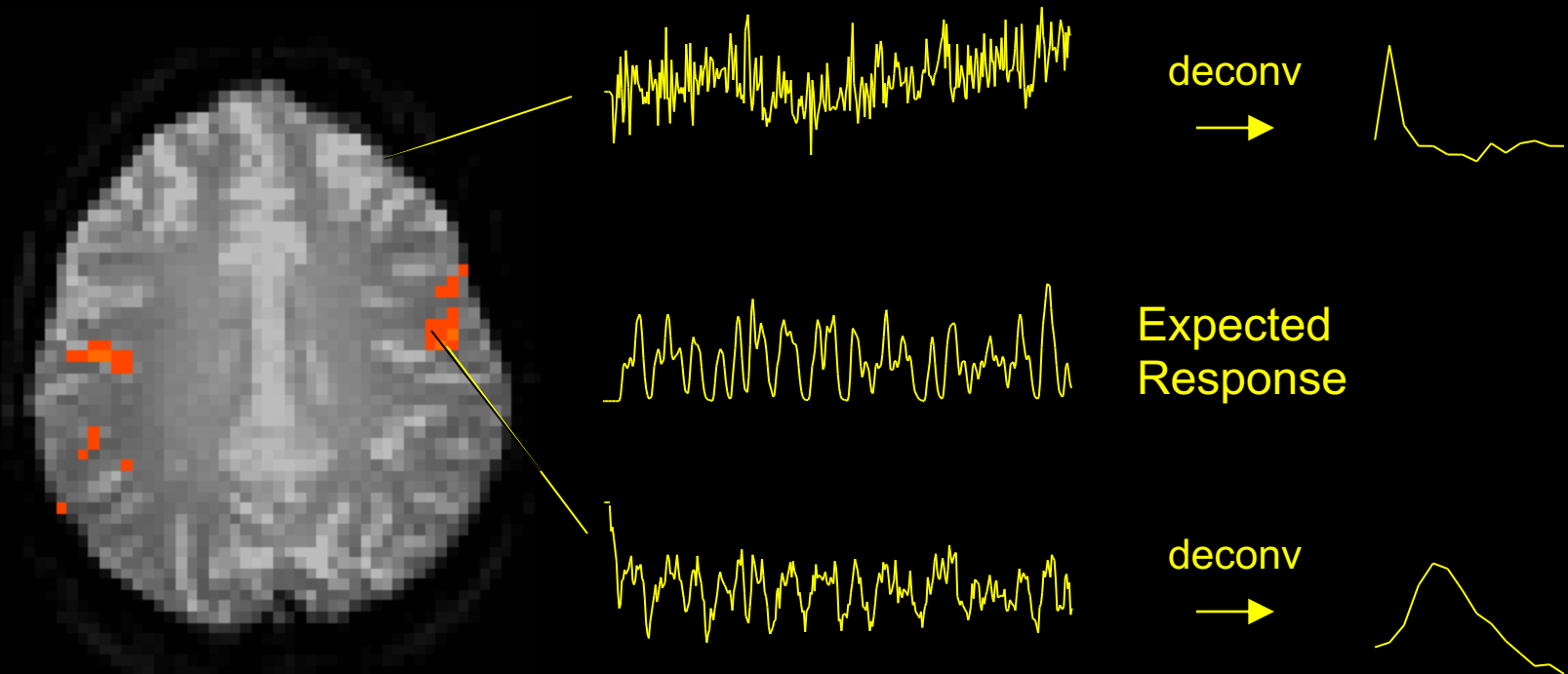
*R.M. Birn, et al. Human Brain Mapping 7(2), 106-114, 1999*





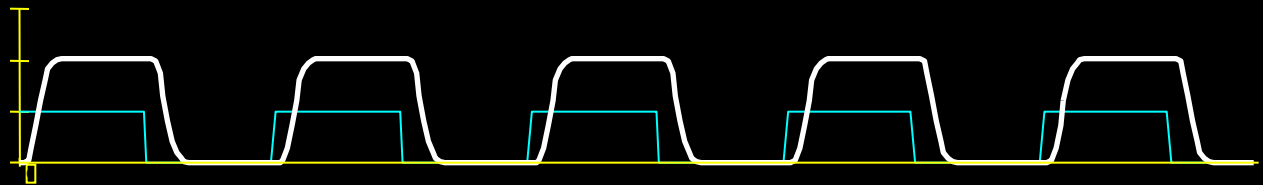
*Variable ISI*

# Speaking - ER-fMRI

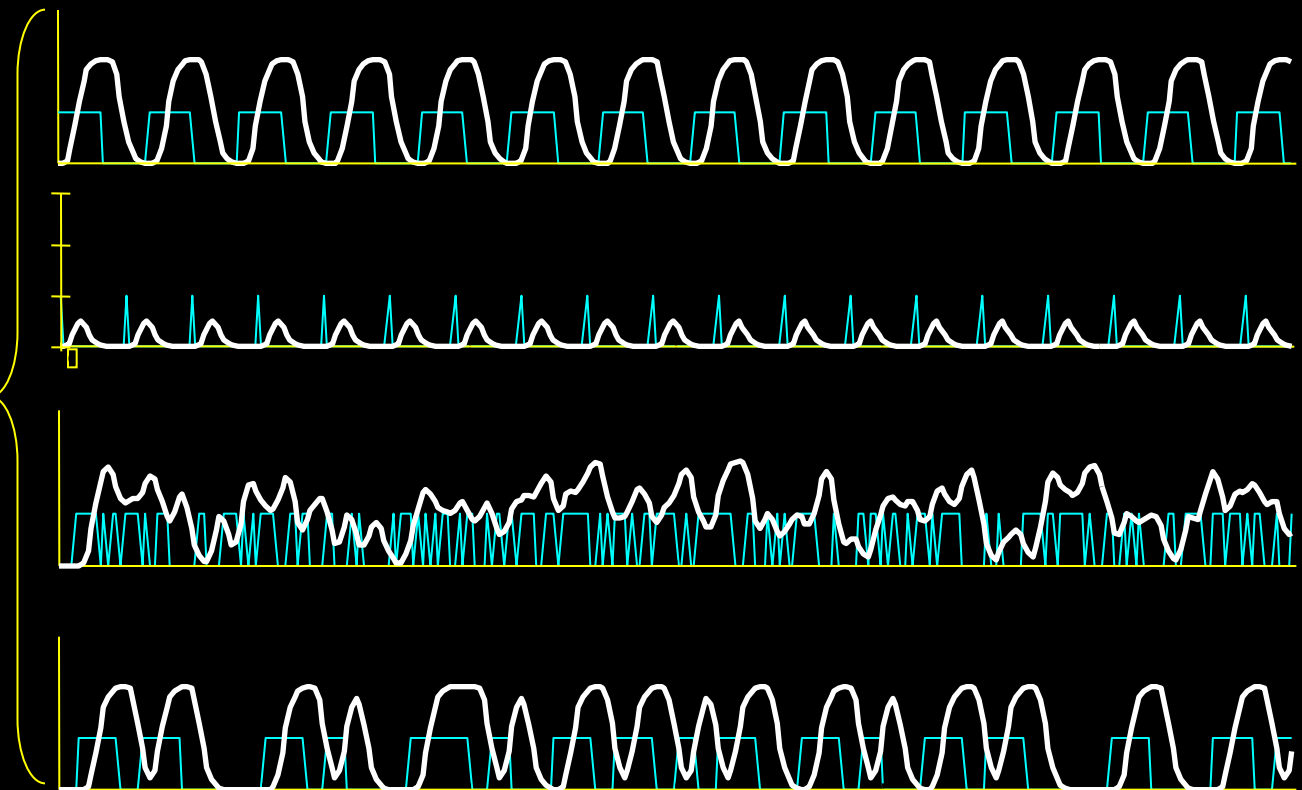


# Optimizing the stimulus paradigm

Blocked  
(motion highly  
correlated)

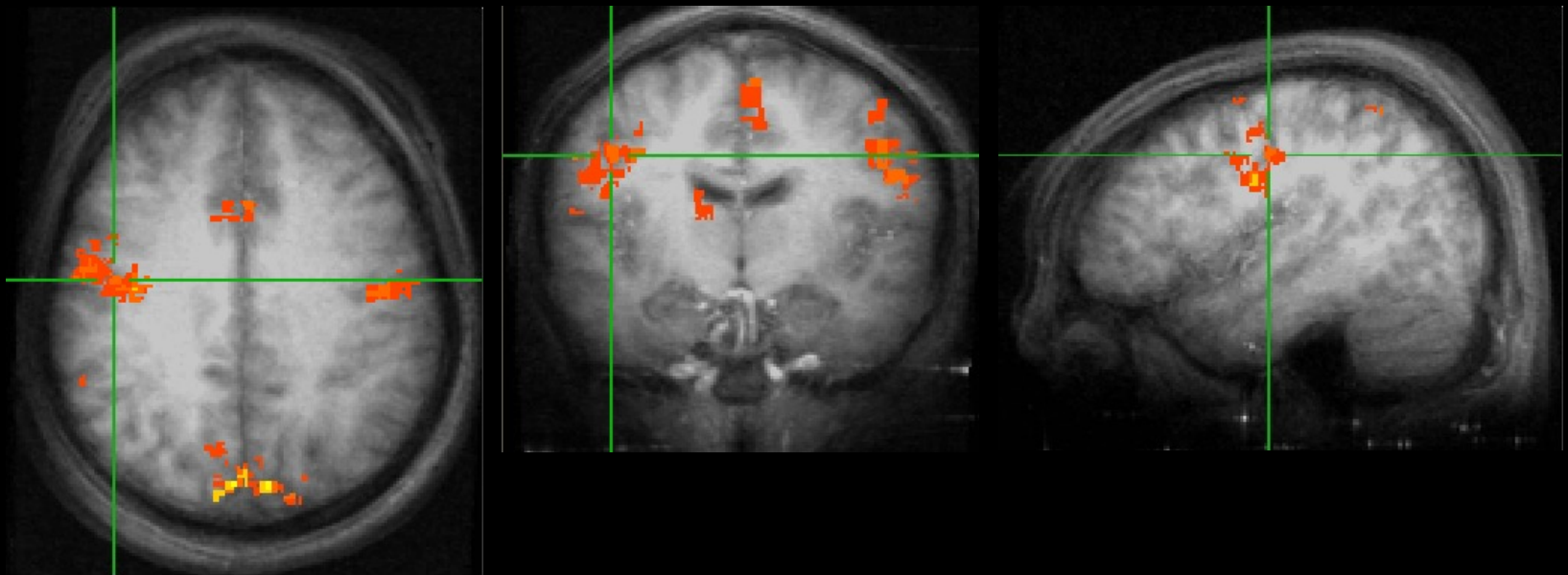


Blocked /  
Event-Related  
(low correlation  
w/ motion)



# Swallowing - Event-Related

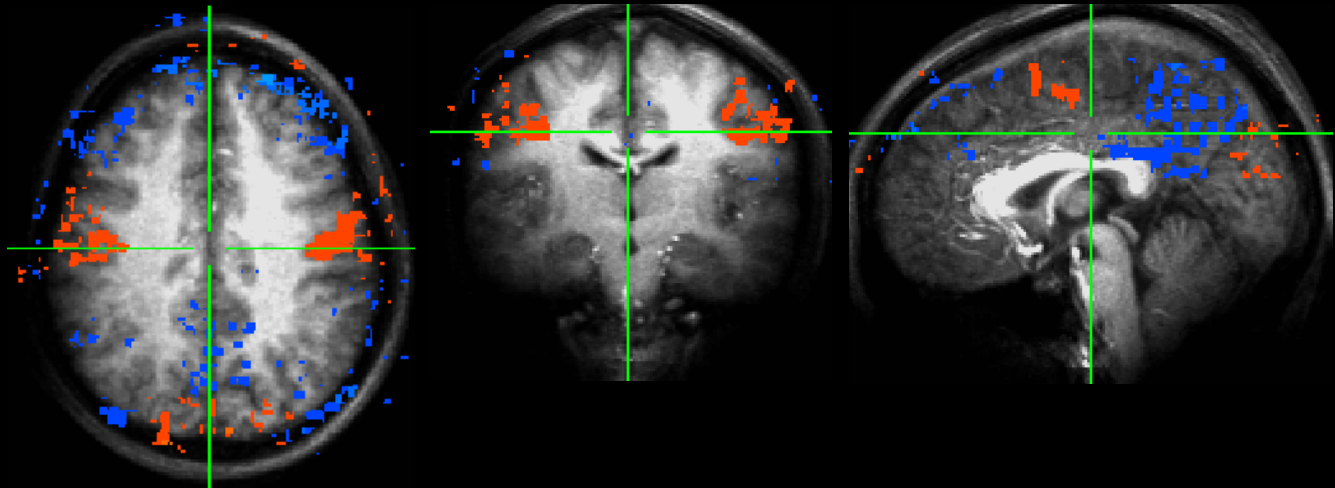
*M.K. Kern, R.M. Birn, S. Jaradeh, et al., Am J Physiol Gastrointest Liver Physiol, 280(4), G531-538, 2001.*



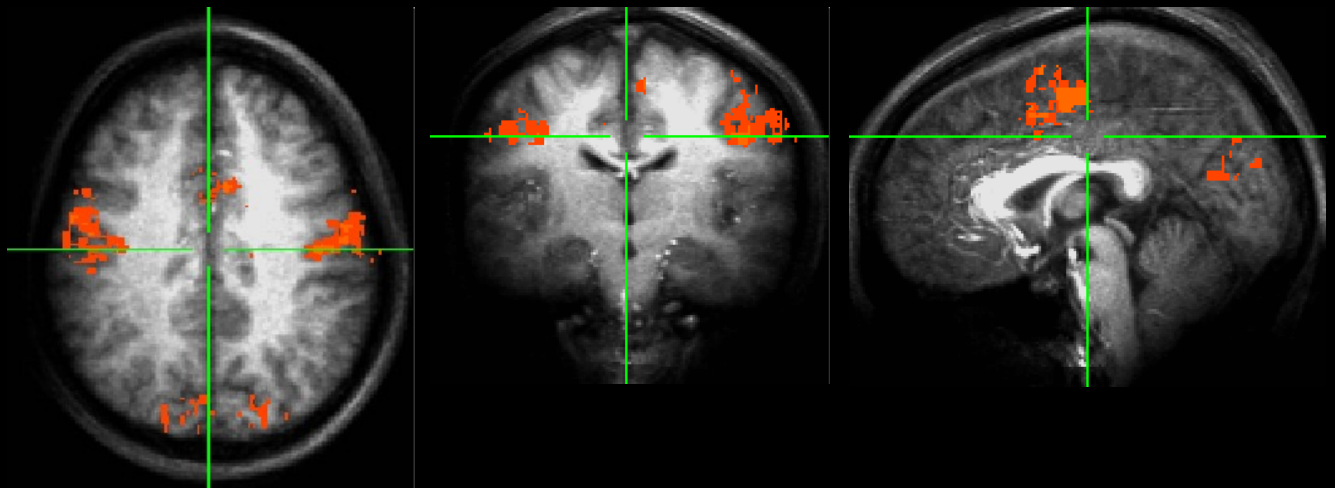
# Facial muscle movement

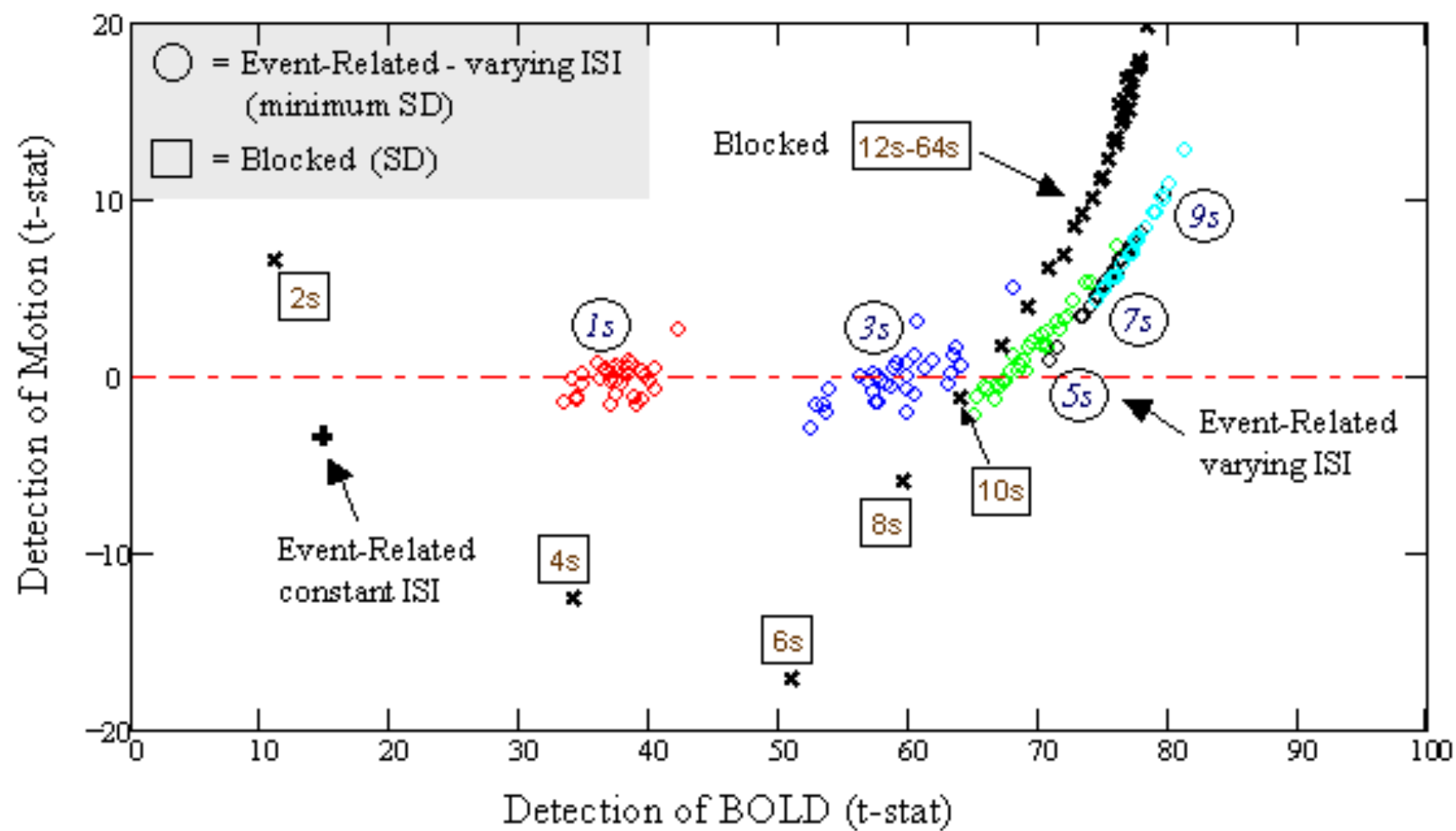
*R.M. Birn, et al. Human Brain Mapping 7(2), 106-114, 1999*

Blocked  
design



Event -  
Related  
design



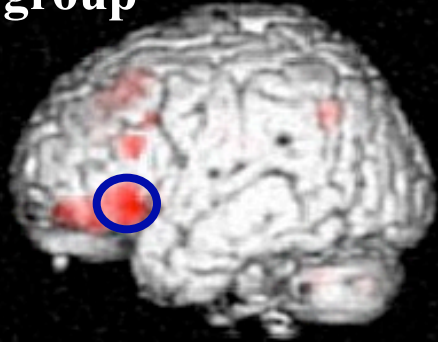


# Individual Map “Classification”

The issue: We can make inferences about groups when averaging individual maps, but can we make inferences which group an individual belongs to?

Not yet. Requires extensive classification techniques.

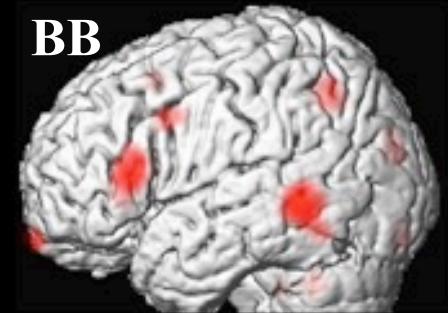
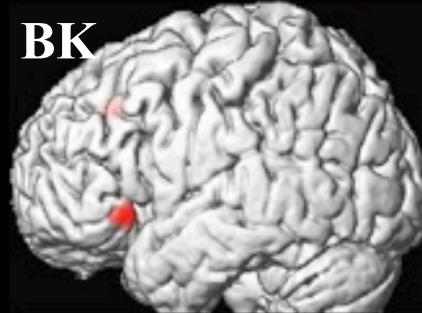
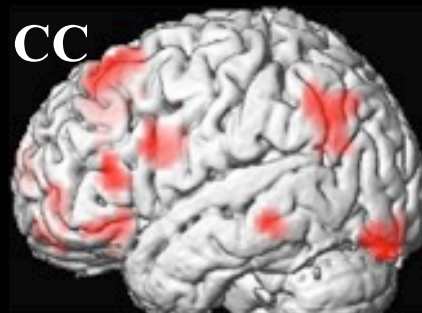
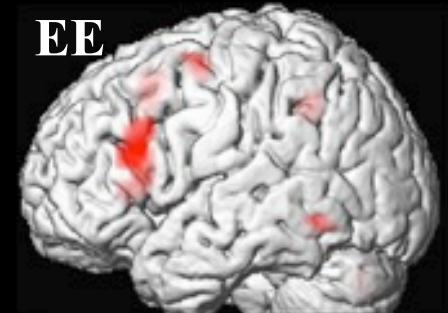
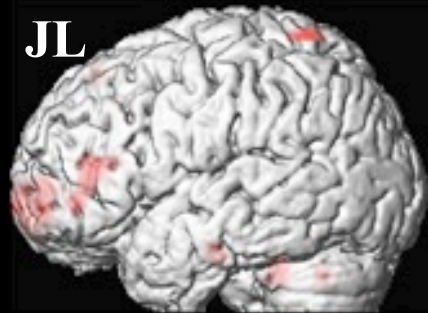
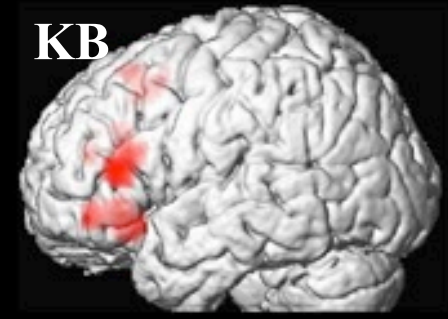
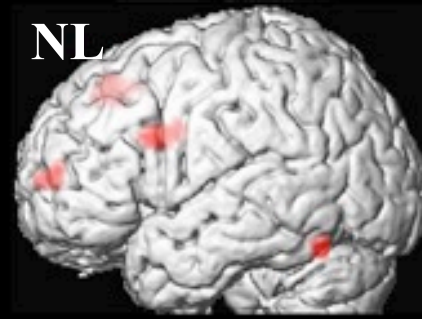
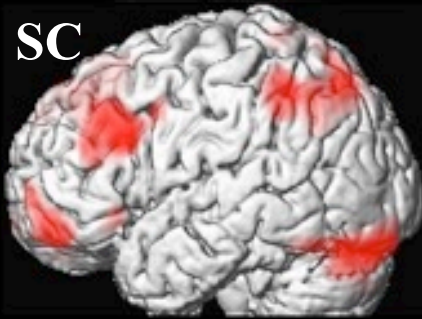
group



# Extensive Individual Differences in Brain Activations During Episodic Retrieval

Miller et al., 2002

Individual activations from the left hemisphere of the 9 subjects



Courtesy, Mike Miler, UC Santa Barbara and Jack Van Horn, fMRI Data Center, Dartmouth University

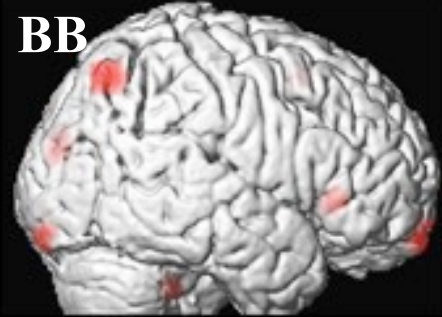
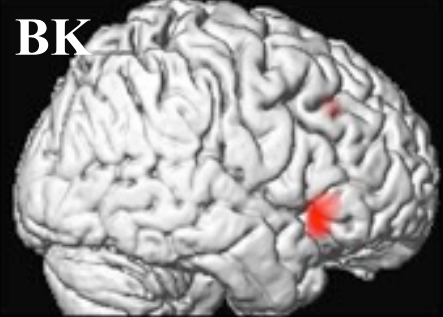
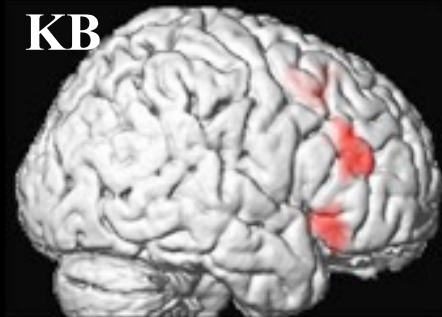
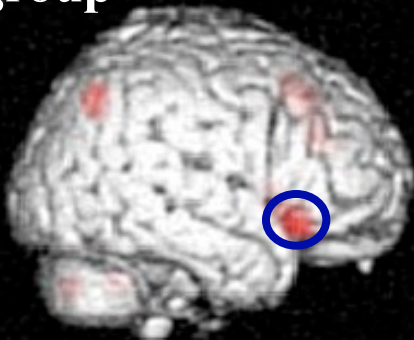


group

# Extensive Individual Differences in Brain Activations During Episodic Retrieval

Miller et al., 2002

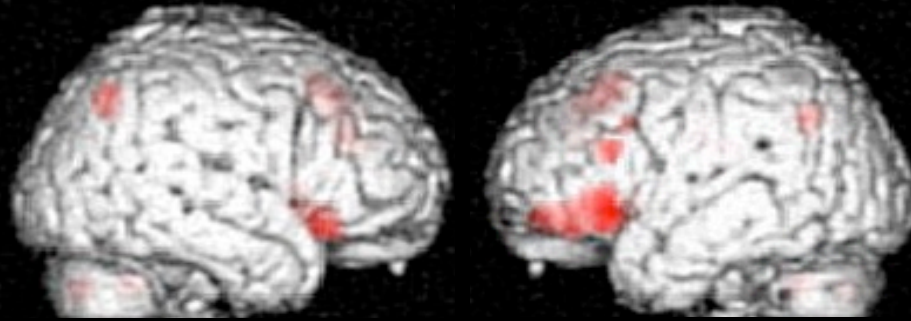
Individual activations from the right hemisphere of the 9 subjects



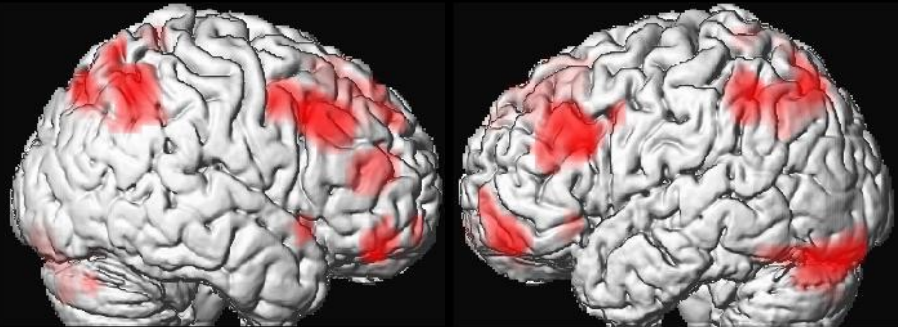
Courtesy, Mike Miler, UC Santa Barbara and Jack Van Horn, fMRI Data Center, Dartmouth University



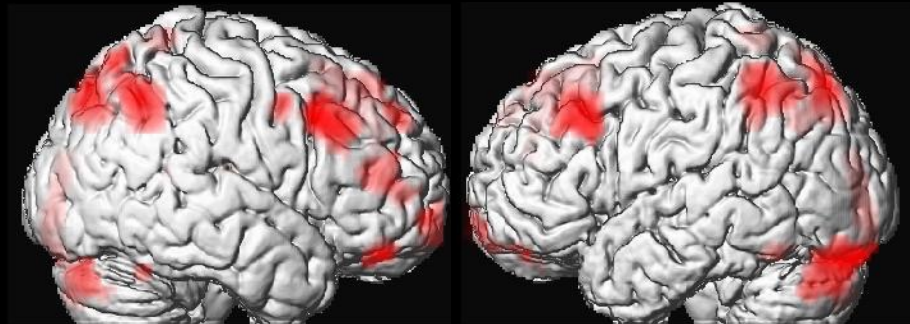
# These individual patterns of activations are stable over time



Group Analysis of Episodic Retrieval



Subject SC

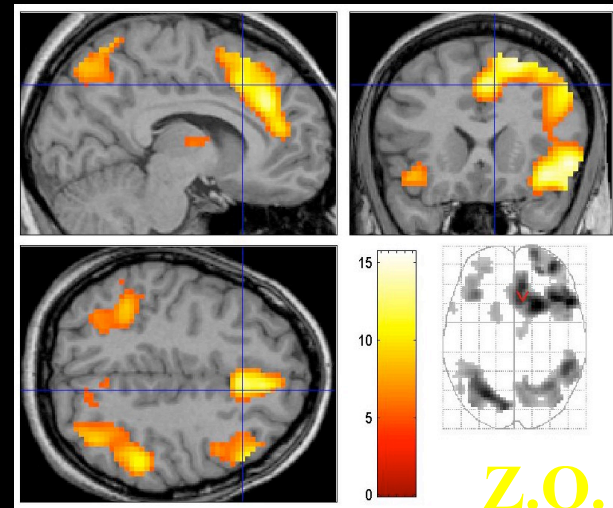
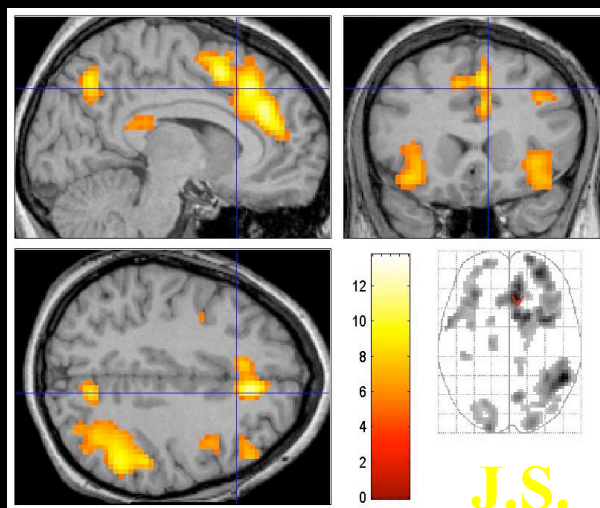
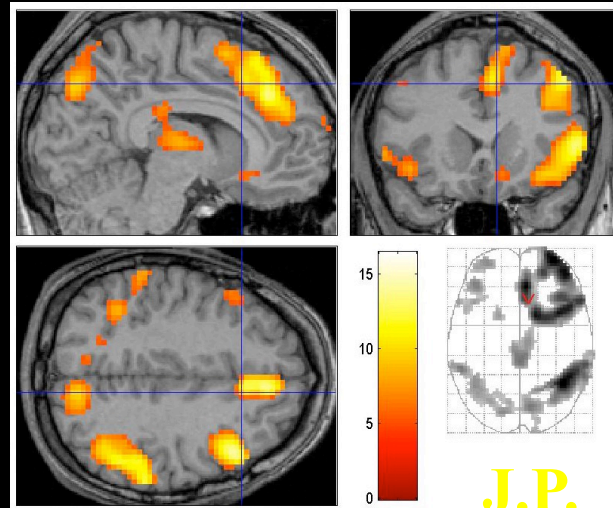
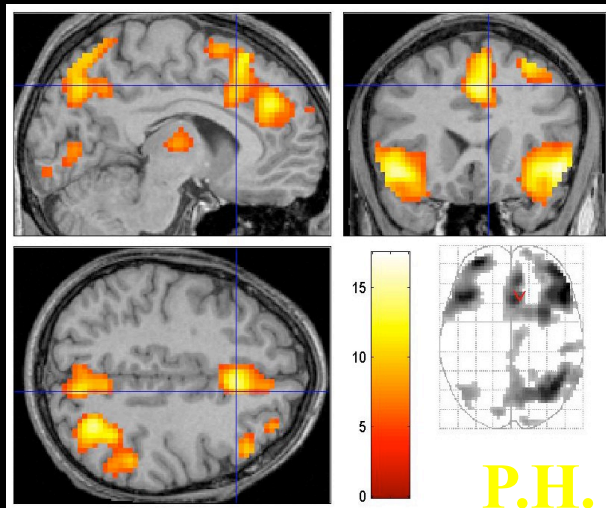
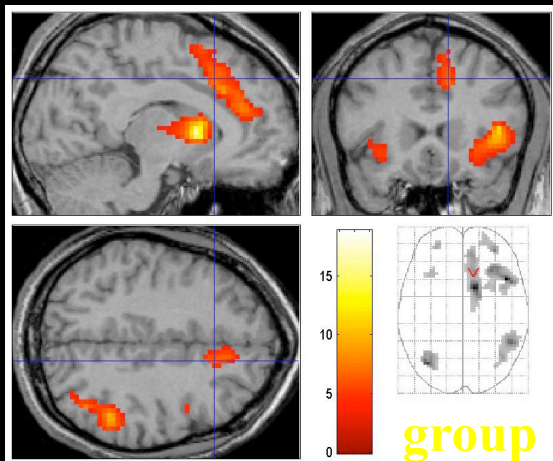


Subject SC 6 months later

Courtesy, Mike Miler, UC Santa Barbara and Jack Van Horn, fMRI Data Center, Dartmouth University

# Individual patterns of activity are much more consistent across subjects for other retrieval tasks.

## spatial working memory



Courtesy, Mike Miler, UC Santa Barbara and Jack Van Horn, fMRI Data Center, Dartmouth University

# Local Pattern Effect Classification and Mapping

Functional magnetic resonance imaging (fMRI) “brain reading”:  
detecting and classifying distributed patterns of fMRI activity  
in human visual cortex

David D. Cox<sup>a,b,\*</sup> and Robert L. Savoy<sup>a,b,c</sup>

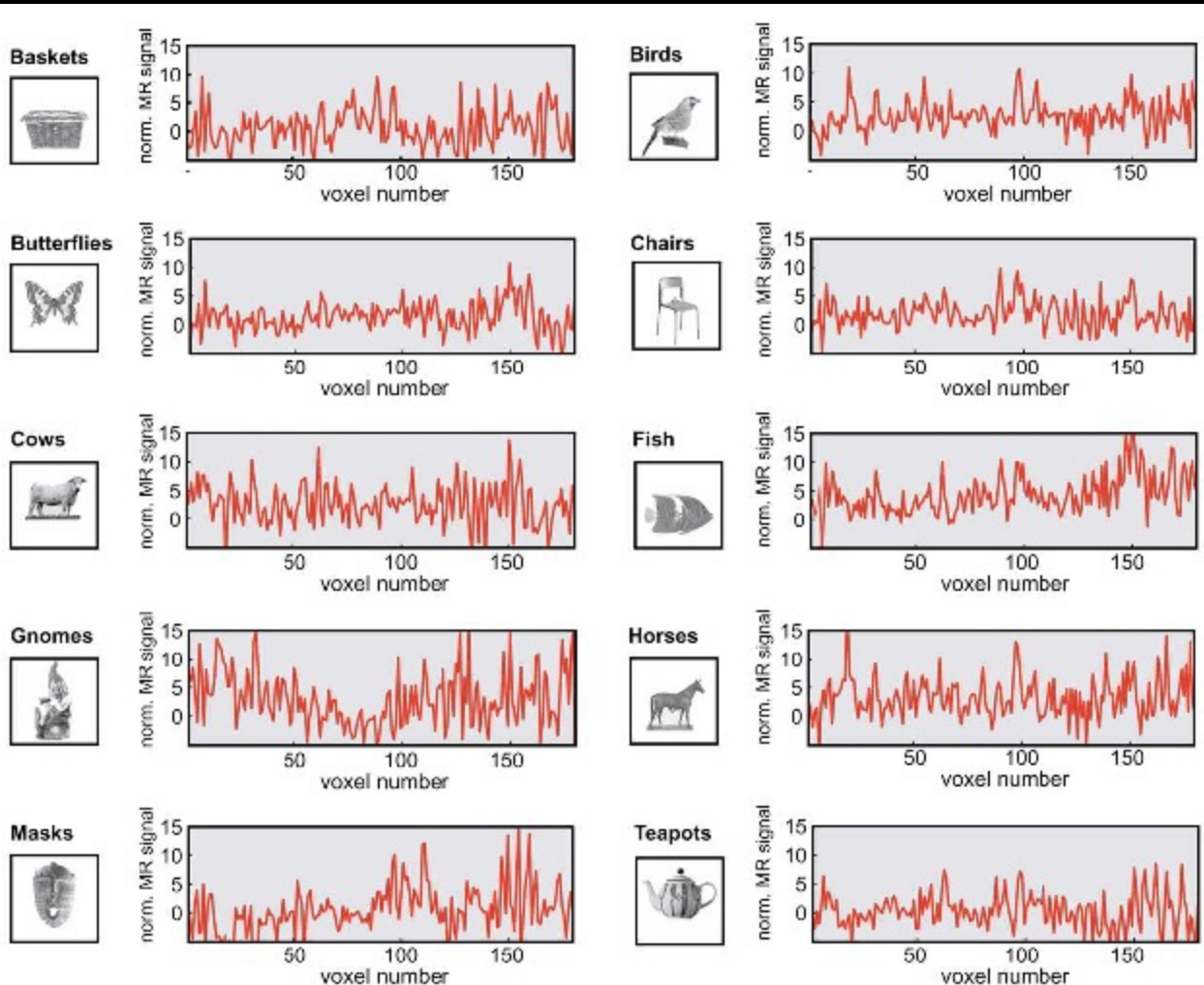
<sup>a</sup> Rowland Institute for Science, Cambridge, MA 02142, USA

<sup>b</sup> Athinoula A. Martinos Center for Structural and Functional Biomedical Imaging, Charlestown, MA 02129, USA

<sup>c</sup> HyperVision, Inc., P.O. Box 158, Lexington, MA 02420, USA

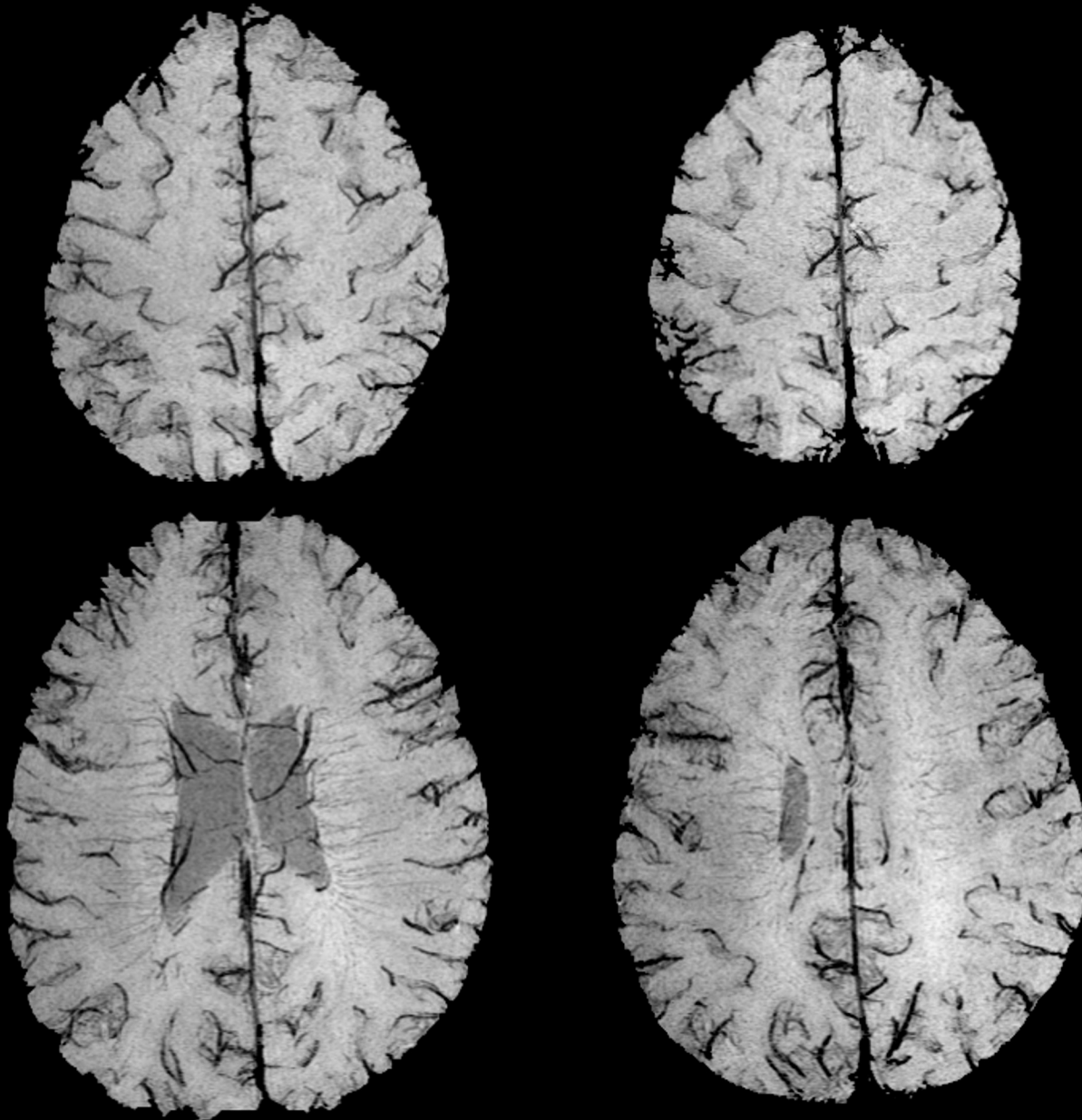
Received 15 July 2002; accepted 10 December 2002

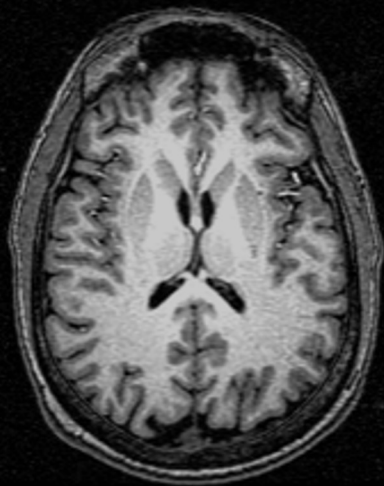
NEUROIMAGE 19 (2): 261-270 Part 1 JUN 2003



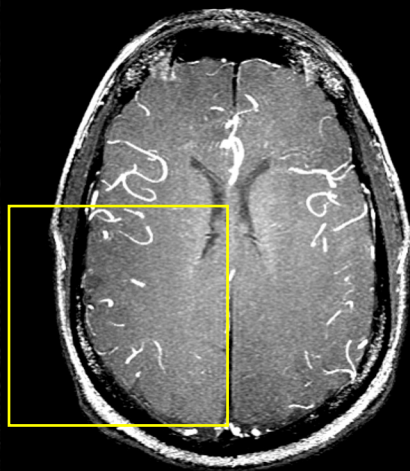


# Baseline susceptibility mapping

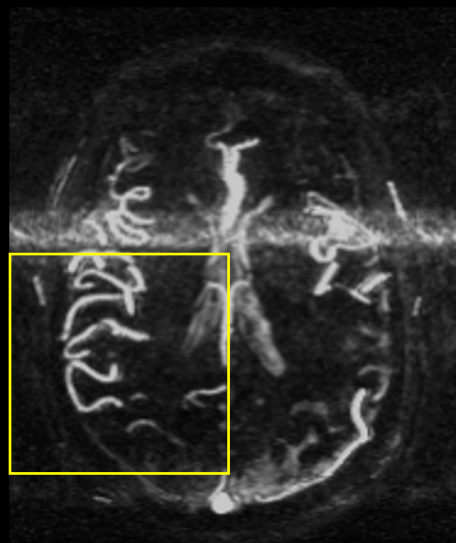




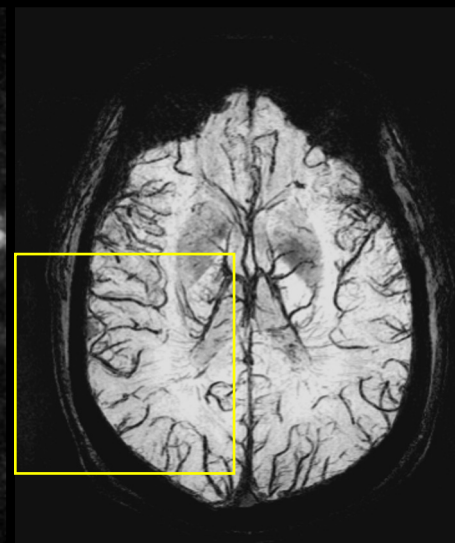
**MP-RAGE**



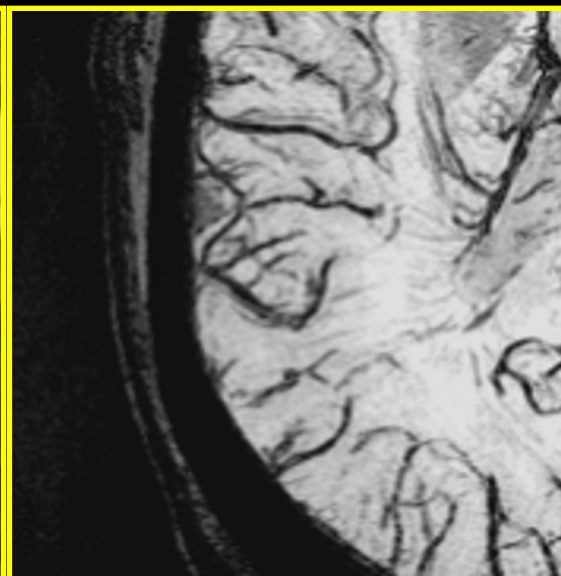
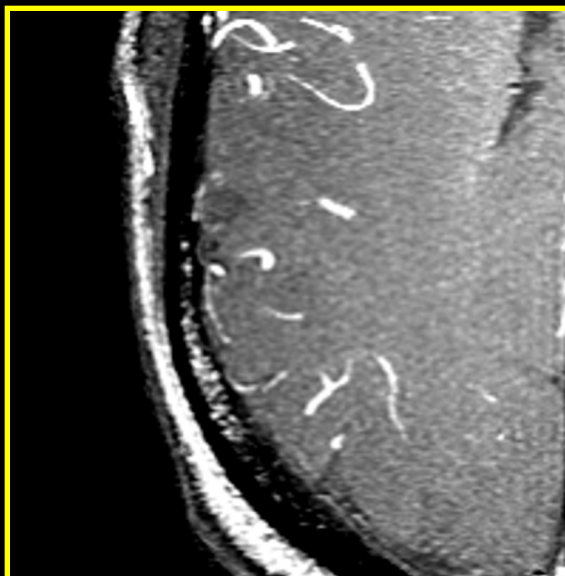
**3D T-O-F MRA**

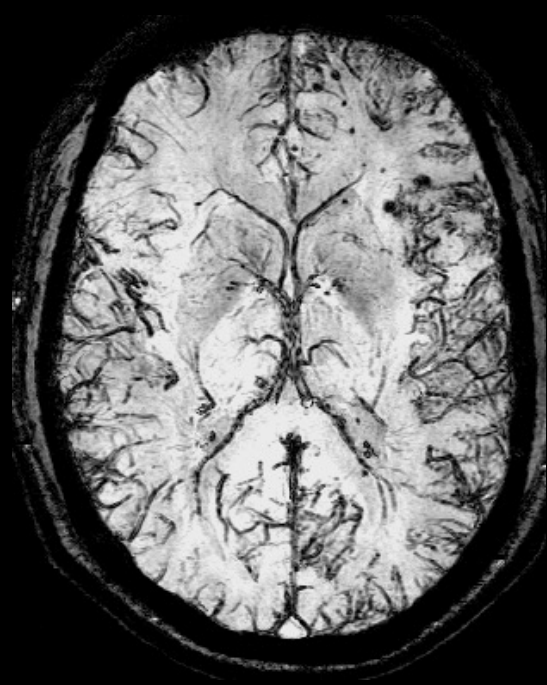
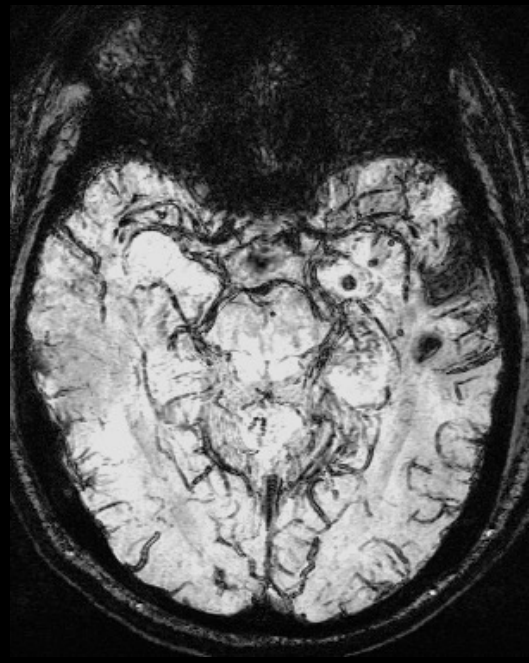


**3D Venous PC**



**MR Venogram**





Direct Neuronal Current Imaging?

# Toward Direct Mapping of Neuronal Activity: MRI Detection of Ultraweak, Transient Magnetic Field Changes

Jerzy Bodurka<sup>1\*</sup> and Peter A. Bandettini<sup>1,2</sup>

- Preliminary models suggest that magnetic field changes on the order of 0.1 to 1 nT are induced (at the voxel scale) in the brain.
- These changes induce about a 0.01 Hz frequency shift or 0.09 deg (@ TE = 30 ms) phase shift.
- Question: Is this detectable?



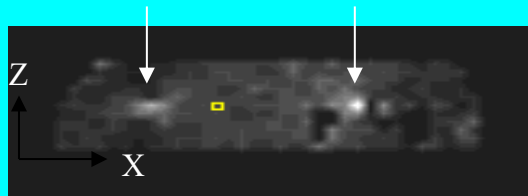
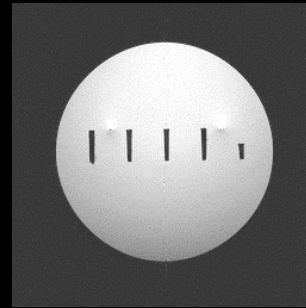
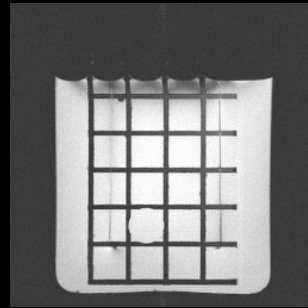
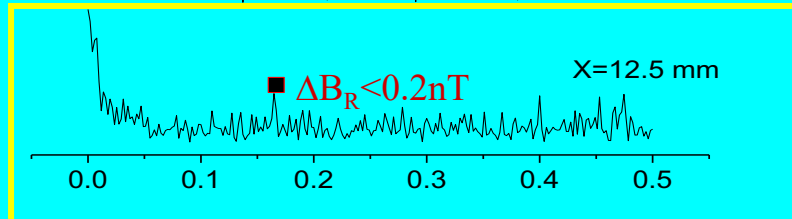
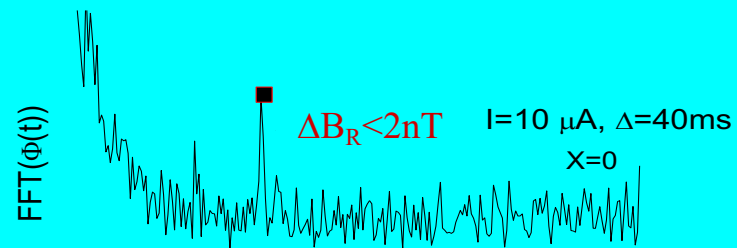
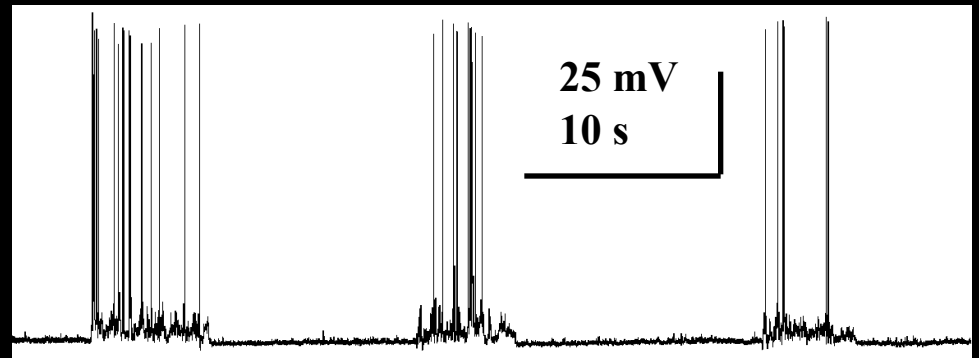
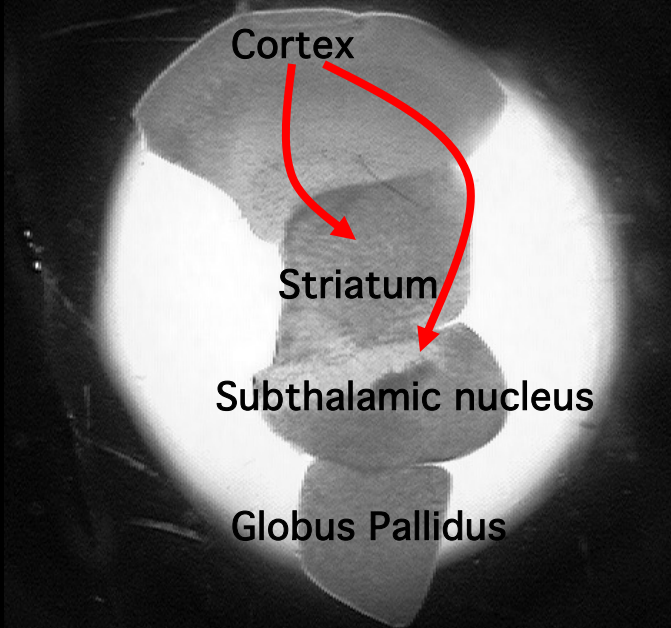


Figure 1

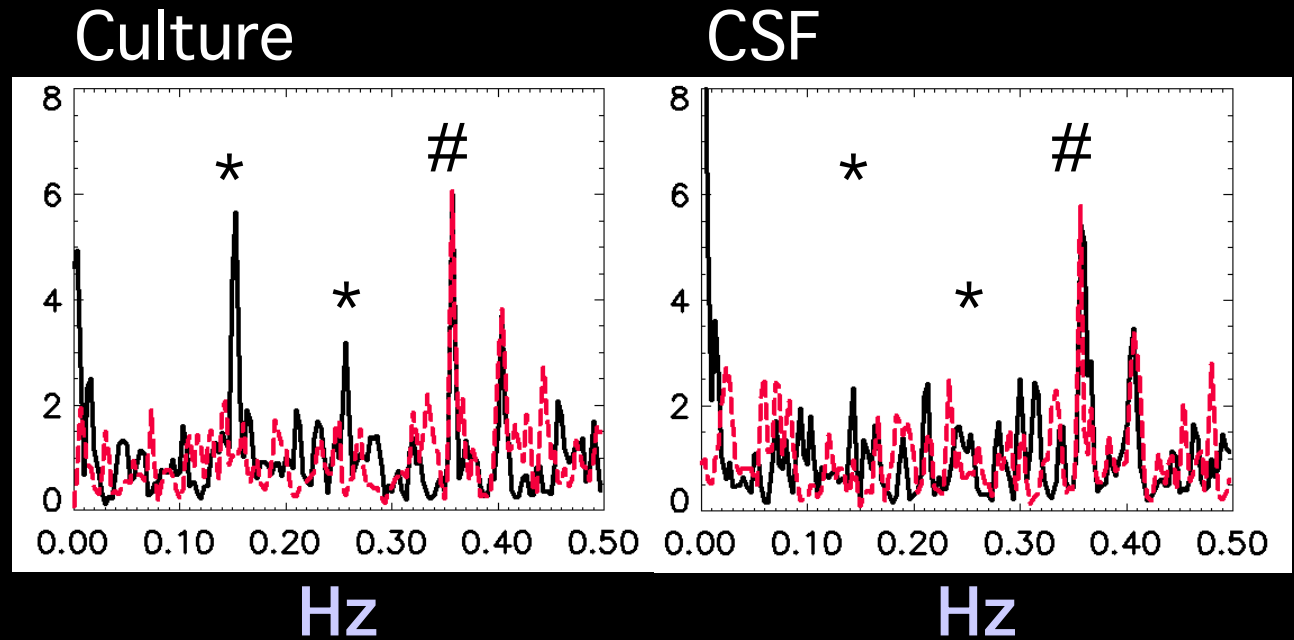


## In Vitro Results

*Newborn rat brains have been found to exhibit spontaneous and synchronous firing at specific frequencies*



# Results



Active state: 10 min, Inactive state: 10 min after TTX admin.

\*: activity

#: scanner pump frequency

Petridou et al.

# What are the biggest unknowns/challenges?

1. Technology

2. Methodology

3. Interpretation

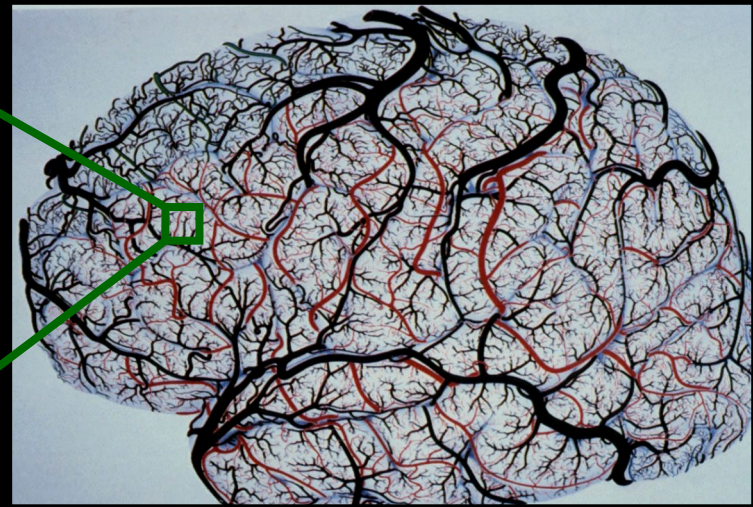
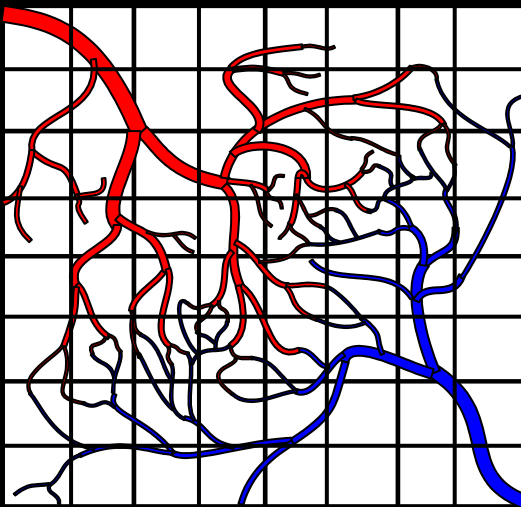
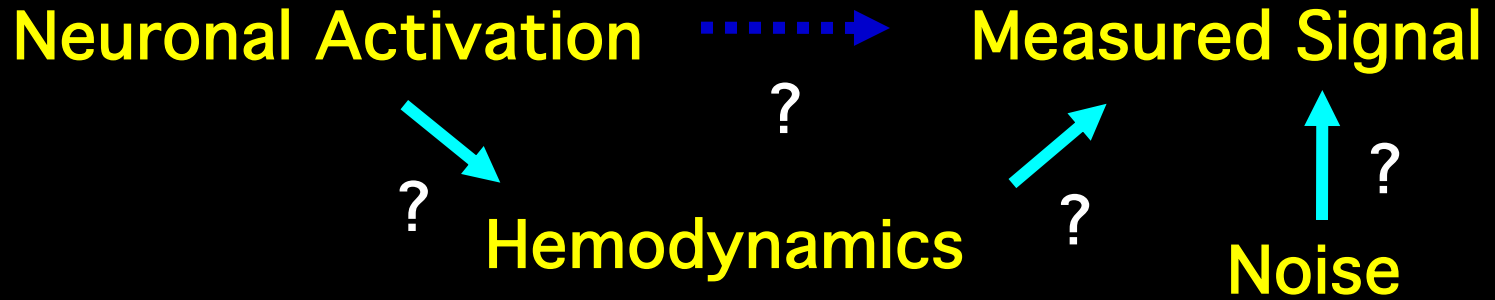
# Interpretation

- Linearity / proportionality
- Hemodynamic vs. Neuronal effects
- Resting state (fluctuations and DC)
- Neuronal inhibition / excitation effects
- Negative signal changes
- HRF latency, magnitude, pre and post undershoot
- T2, T2\*, T1, diffusion, and Mo changes
- Differences across modalities (location, timing)

# Interpretation

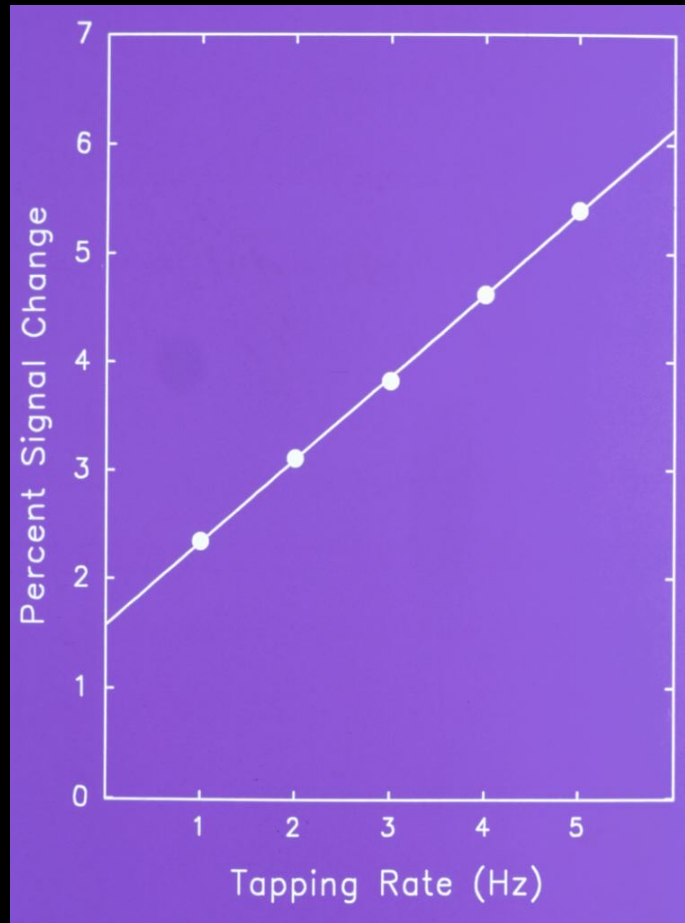
- Linearity / proportionality
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- Neuronal inhibition / excitation effects
- Negative signal changes
- HRF latency, magnitude, pre and post undershoot
- T2, T2\*, T1, diffusion, and Mo changes
- Differences across modalities (location, timing)

# The Problem



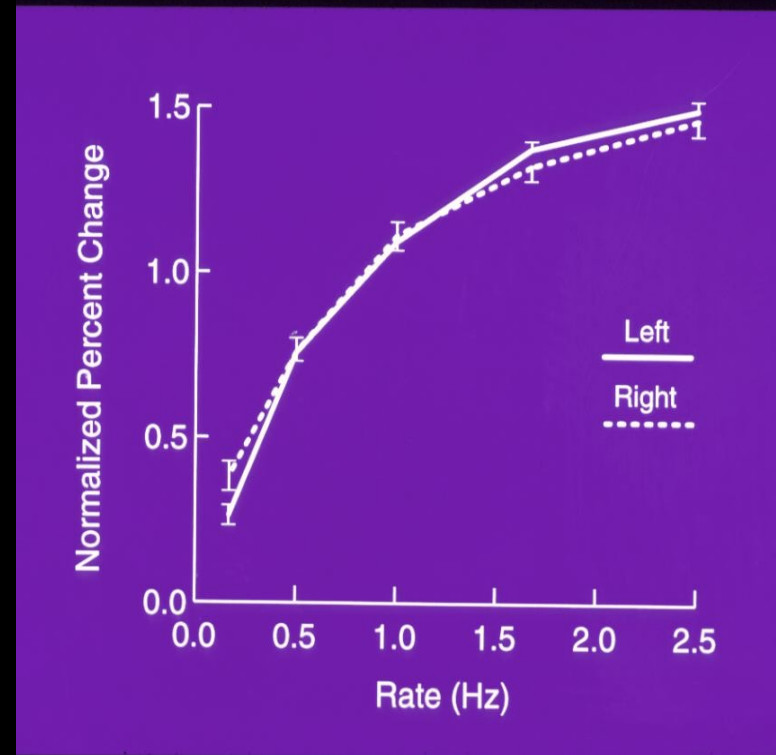
# Linearity / proportionality

## Motor Cortex



S. M. Rao et al, (1996) "Relationship between finger movement rate and functional magnetic resonance signal change in human primary motor cortex." *J. Cereb. Blood Flow and Met.* 16, 1250-1254.

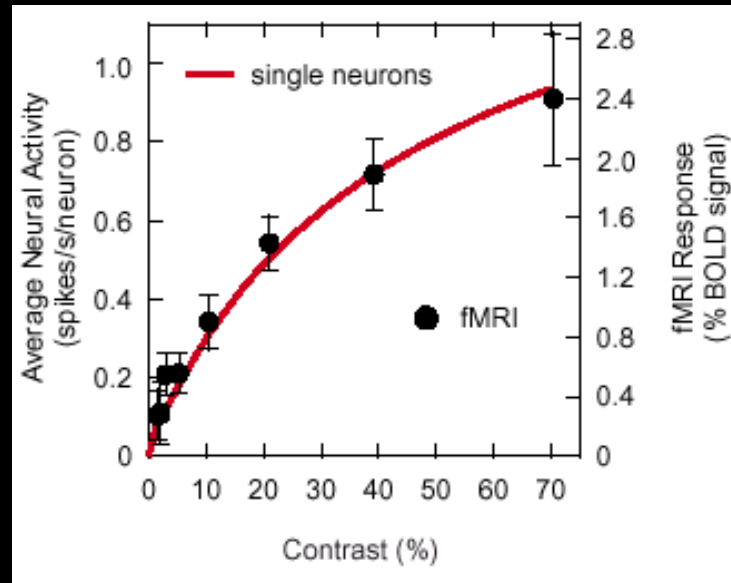
## Auditory Cortex



J. R. Binder, et al, (1994). "Effects of stimulus rate on signal response during functional magnetic resonance imaging of auditory cortex." *Cogn. Brain Res.* 2, 31-38



# fMRI responses in human V1 are proportional to average firing rates in monkey V1



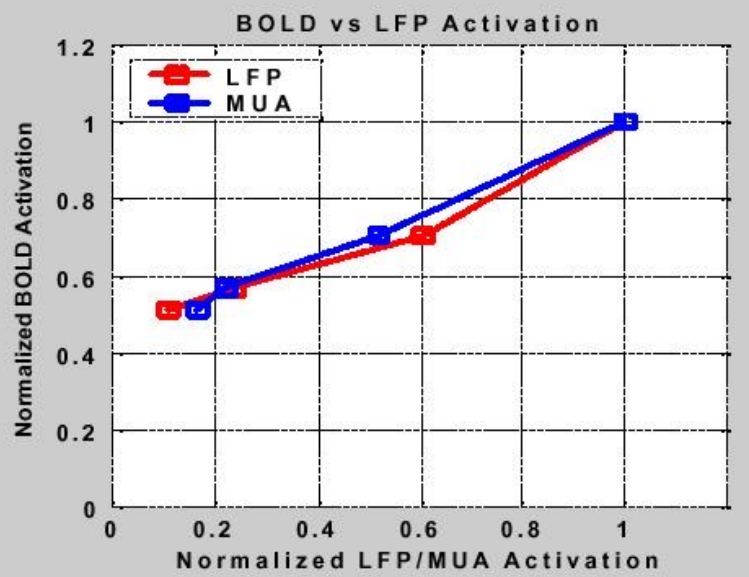
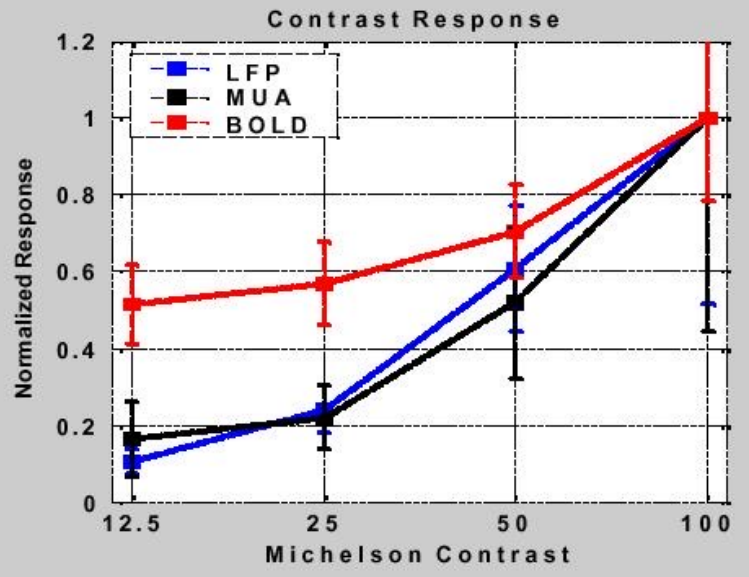
Heeger, D. J., Huk, A. C., Geisler, W. S., and Albrecht, D. G. 2000. Spikes versus BOLD: What does neuroimaging tell us about neuronal activity? *Nat. Neurosci.* 3: 631–633.

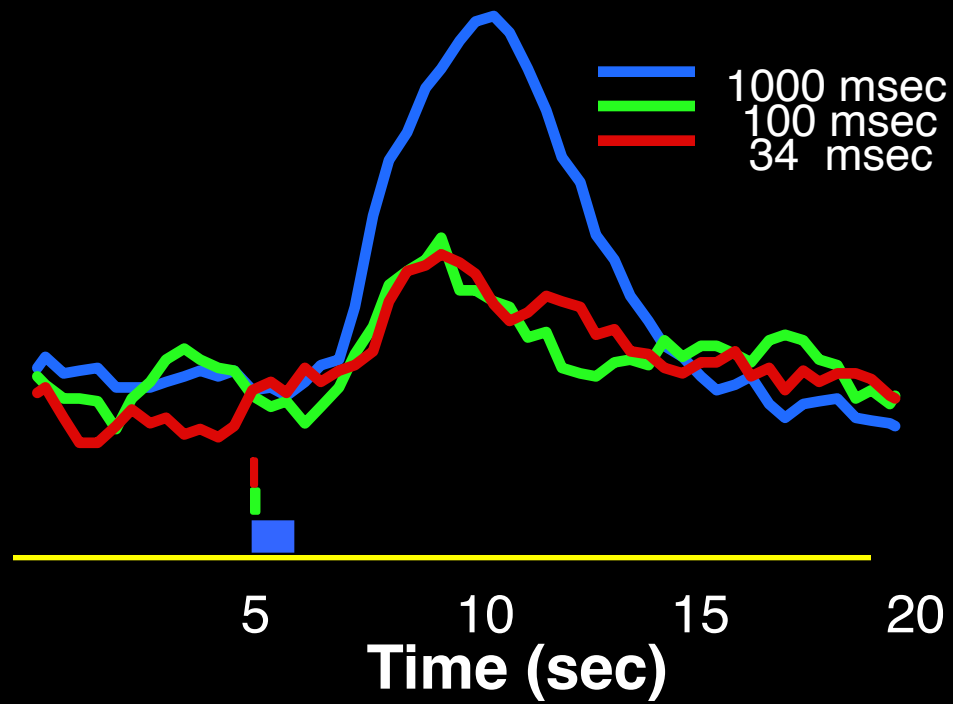
**0.4 spikes/sec -> 1% BOLD**

Rees, G., Friston, K., and Koch, C. 2000. A direct quantitative relationship between the functional properties of human and macaque V5. *Nat. Neurosci.* 3: 716–723.

**9 spikes/sec -> 1% BOLD**

Logothetis et al. (2001) "Neurophysiological investigation of the basis of the fMRI signal" Nature, 412, 150-157

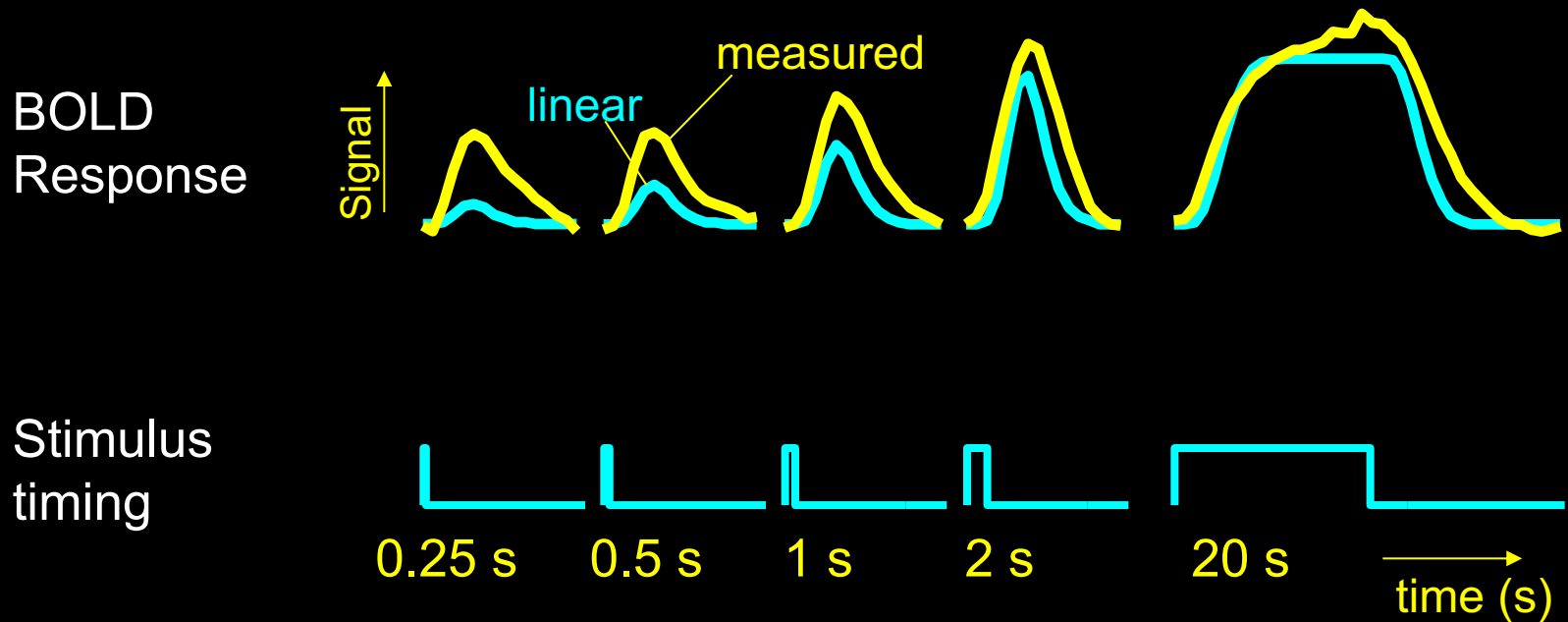




R. L. Savoy, et al., Pushing the temporal resolution of fMRI: studies of very brief visual stimuli, onset variability and asynchrony, and stimulus-correlated changes in noise [oral], 3<sup>rd</sup> Proc. Soc. Magn. Reson., Nice, p. 450. (1995).

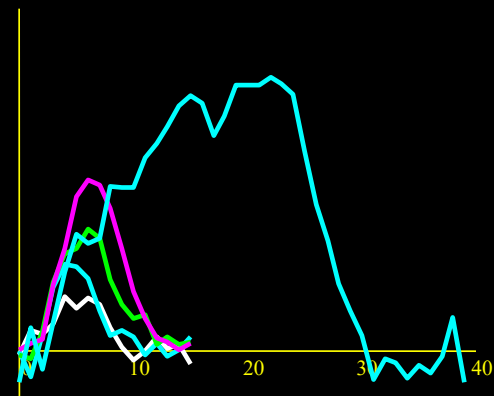
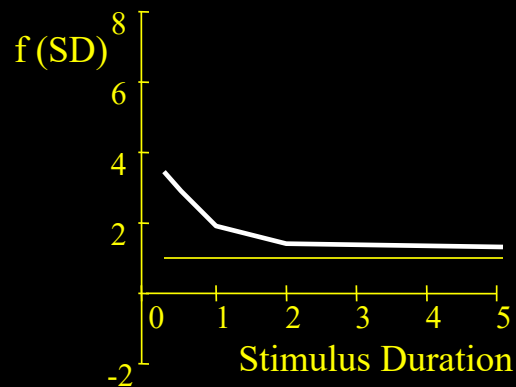
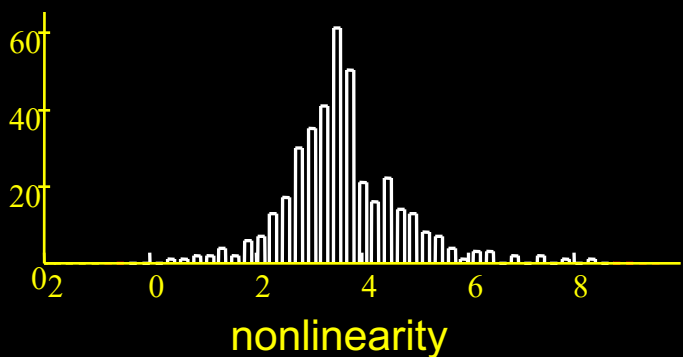
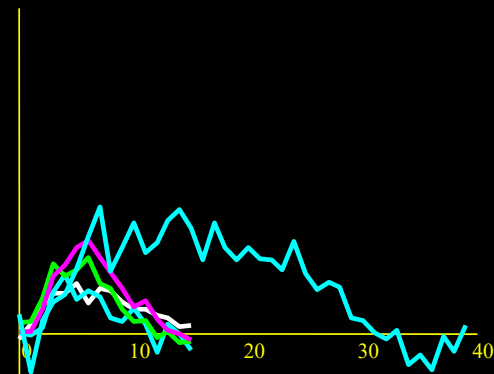
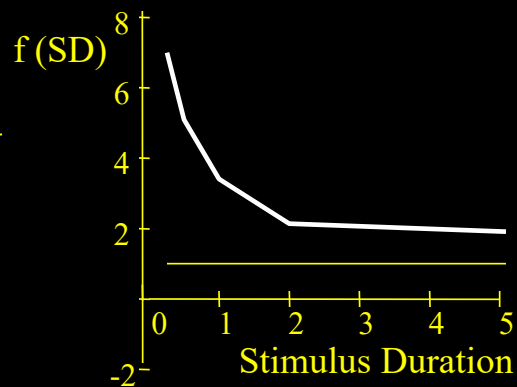
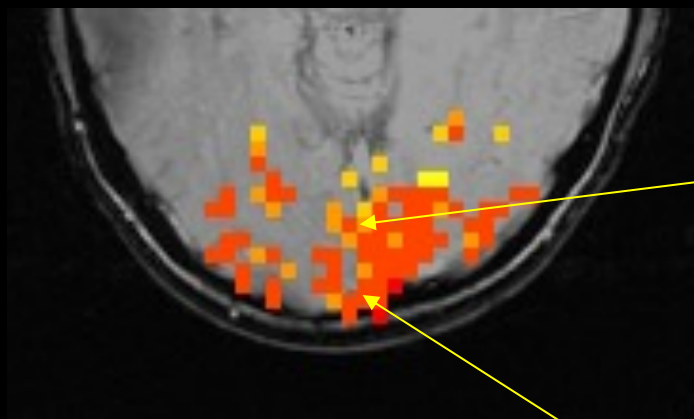
# Dynamic Nonlinearity Assessment

## Different stimulus “ON” periods



*Brief stimuli produce larger responses than expected*

# Spatial Heterogeneity of BOLD Nonlinearity

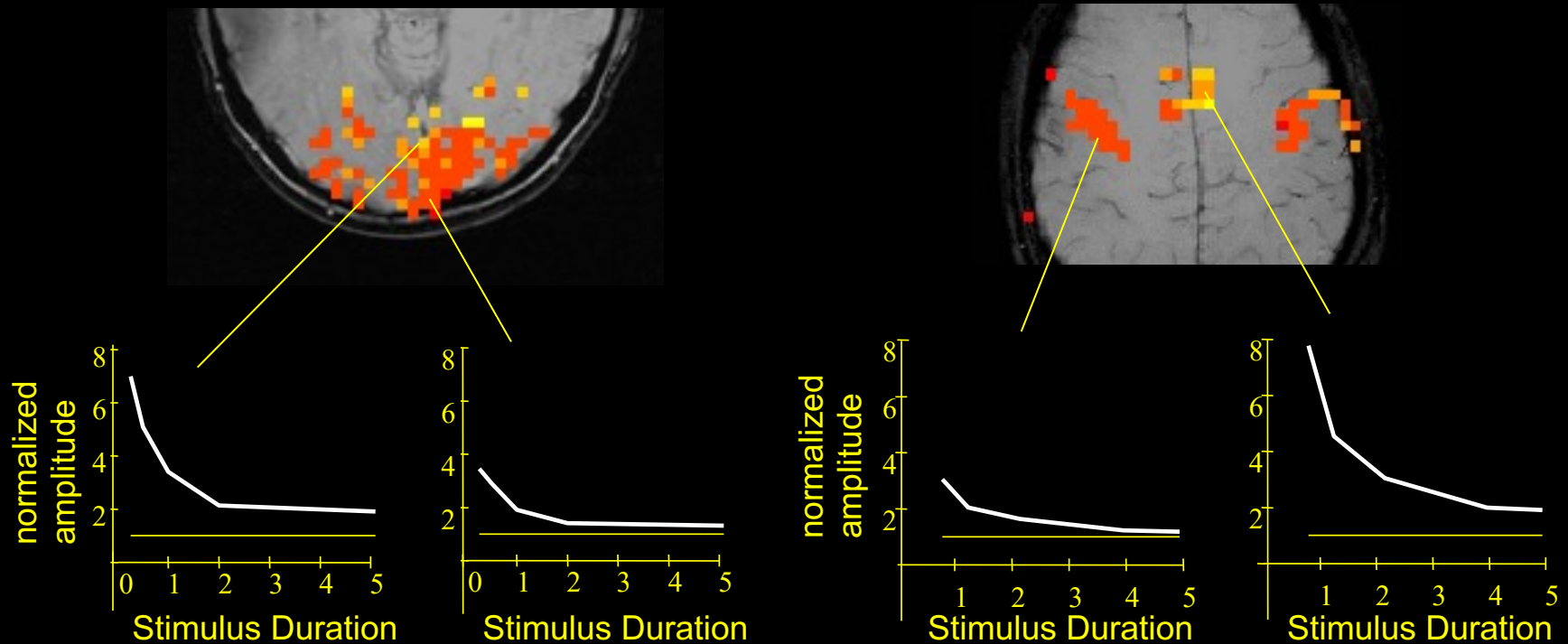


R. M. Birn, Z. Saad, P. A. Bandettini, (2001) "Spatial heterogeneity of the nonlinear dynamics in the fMRI BOLD response." *NeuroImage*, 14: 817-826.

# Spatial variation of linearity

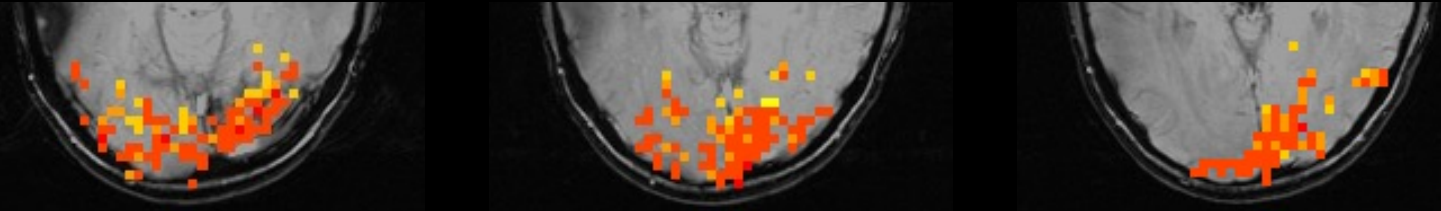
Visual

Motor

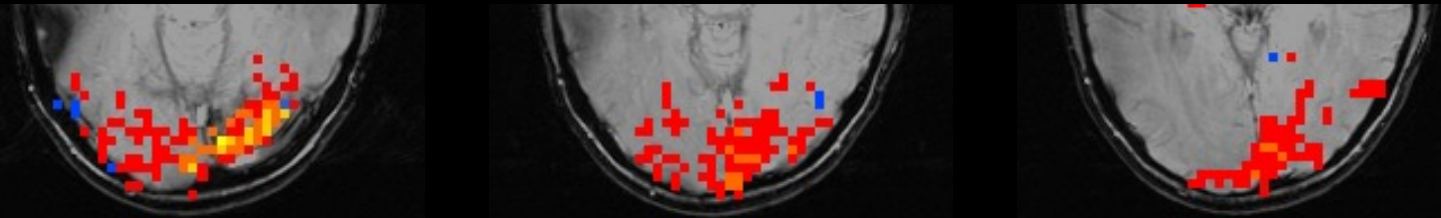


# Results – visual task

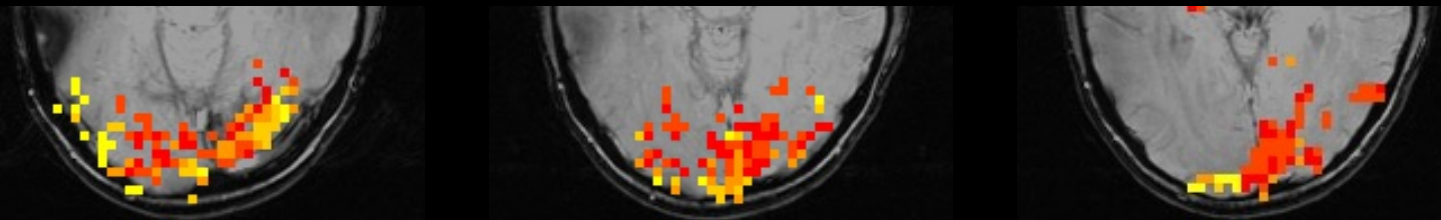
Nonlinearity



Magnitude



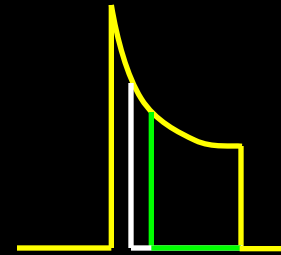
Latency





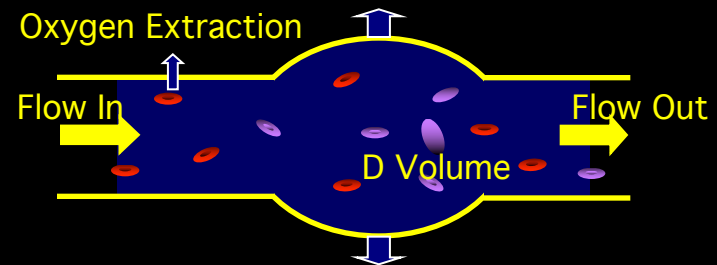
# Sources of this Nonlinearity

- Neuronal



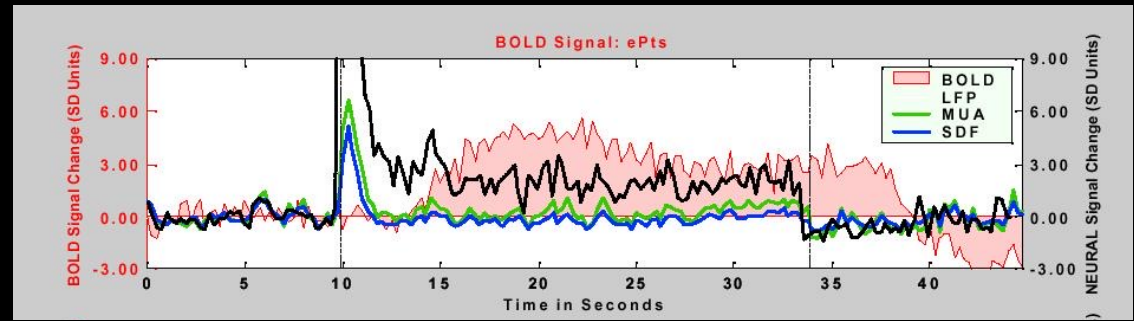
- Hemodynamic

- Oxygen extraction
- Blood volume dynamics

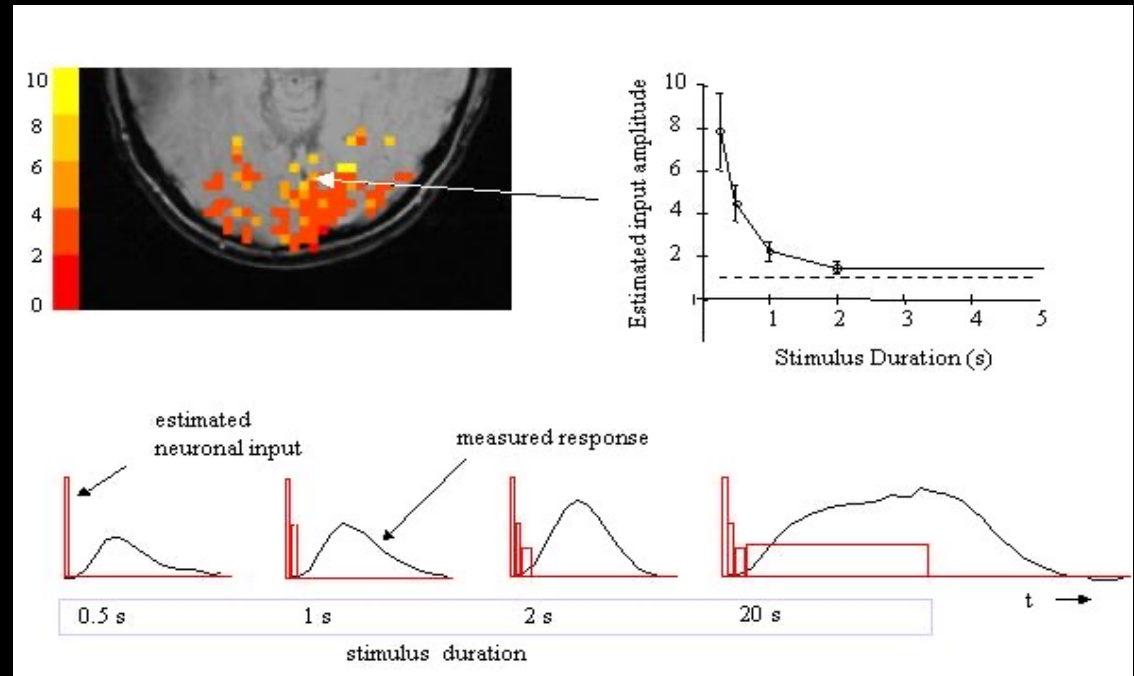


# BOLD Correlation with Neuronal Activity

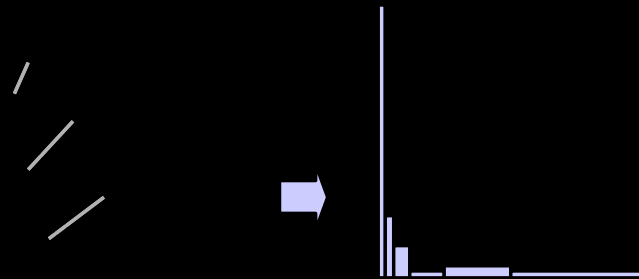
**Logothetis et al. (2001)**  
“Neurophysiological investigation  
of the basis of the fMRI signal”  
*Nature*, 412, 150-157.



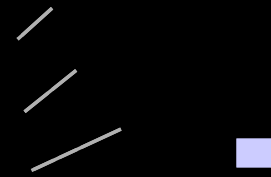
**P. A. Bandettini and L. G. Ungerleider, (2001)** “From neuron  
to BOLD: new connections.”  
*Nature Neuroscience*, 4: 864-866.



Stationary grating



Contrast-reversing checkerboard



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