

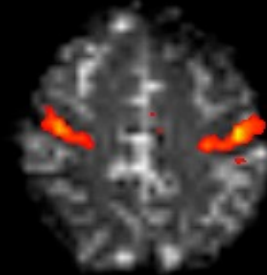
# The Spatial, Temporal and Interpretive Limits of Functional MRI

Peter A. Bandettini, Ph.D

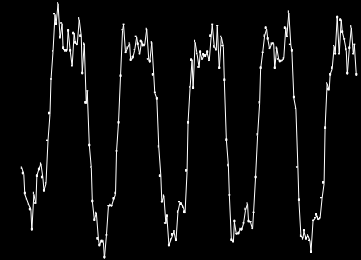
Unit on Functional Imaging Methods  
Laboratory of Brain and Cognition  
National Institute of Mental Health

# Categories of Questions Asked with fMRI

Where?



When?



How much?

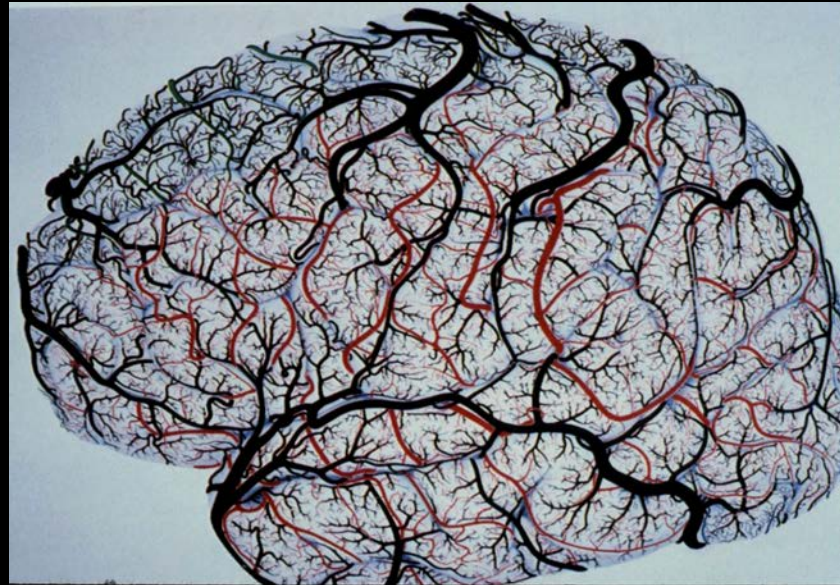
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How to get the brain to do what we want it to  
do in the context of an fMRI experiment?

*(limitations: time, motion, acoustic noise....)*

# A Primary Challenge:

...to make progressively more precise inferences using fMRI without making too many assumptions about non-neuronal physiologic factors.



# Contrast in Functional MRI

- **Blood Volume**

- Contrast agent injection and time series collection of T2\* or T2 - weighted images

- **BOLD**

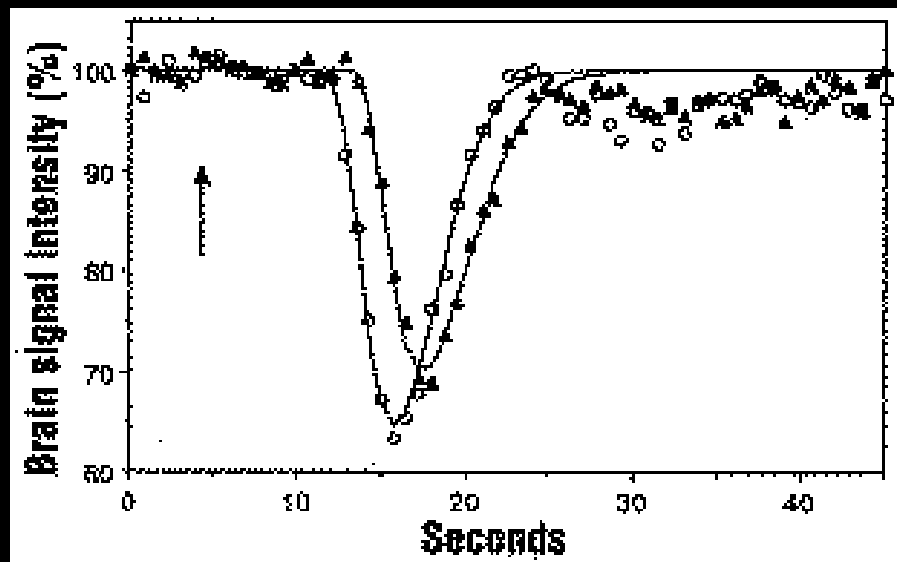
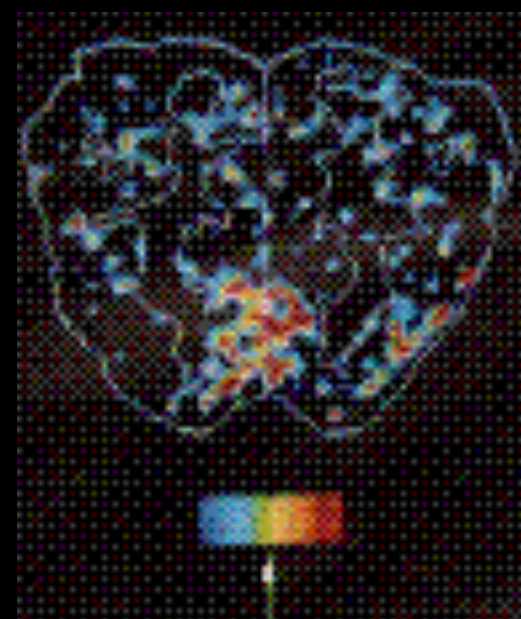
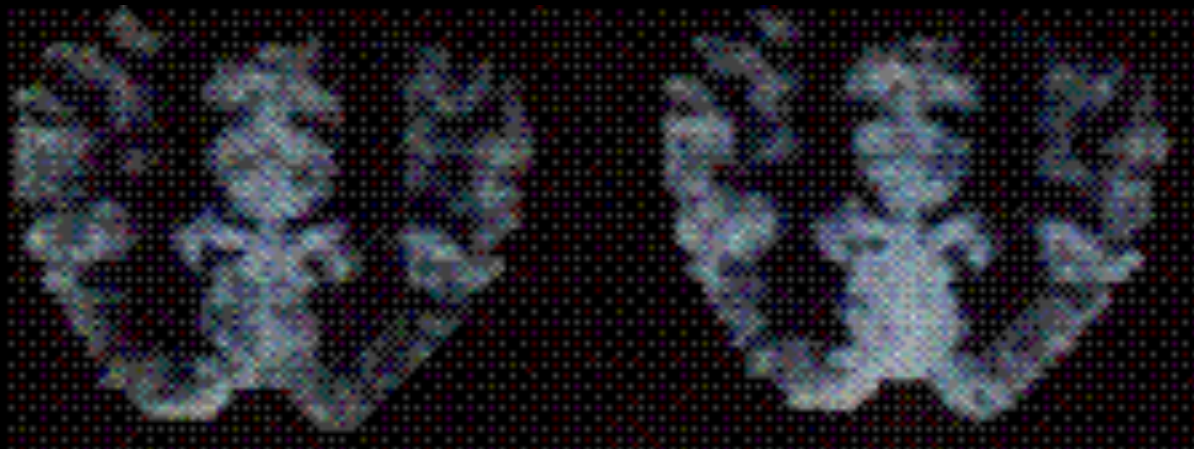
- Time series collection of T2\* or T2 - weighted images

- **Perfusion**

- T1 weighting
- Arterial spin labeling

# Resting

# Active

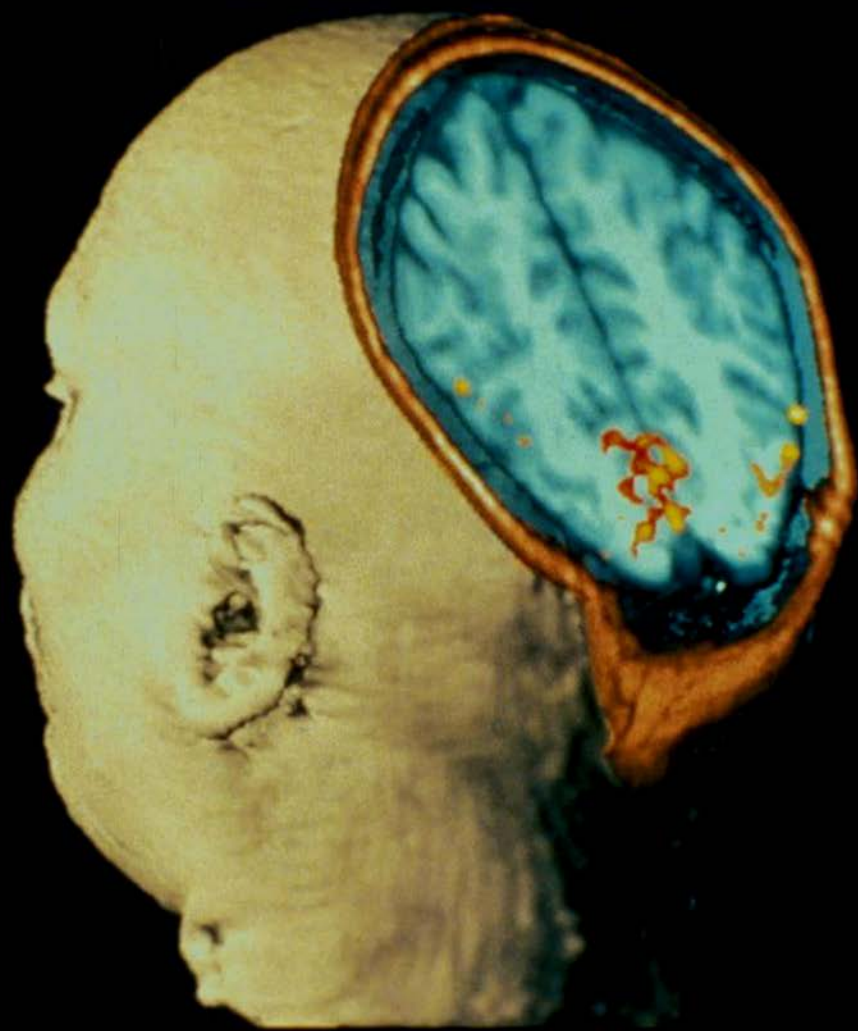


# Photic Stimulation

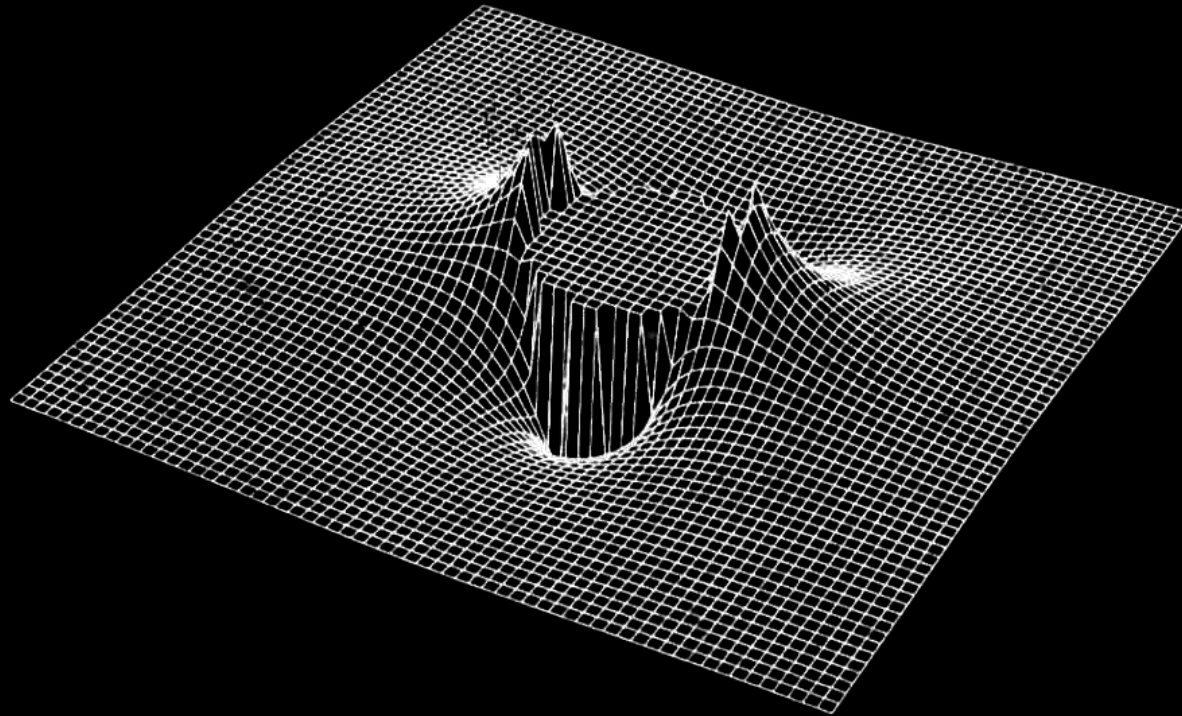
MRI Image showing  
activation of the  
Visual Cortex

From Belliveau, et al.  
Science Nov 1991

MSC - perfusion



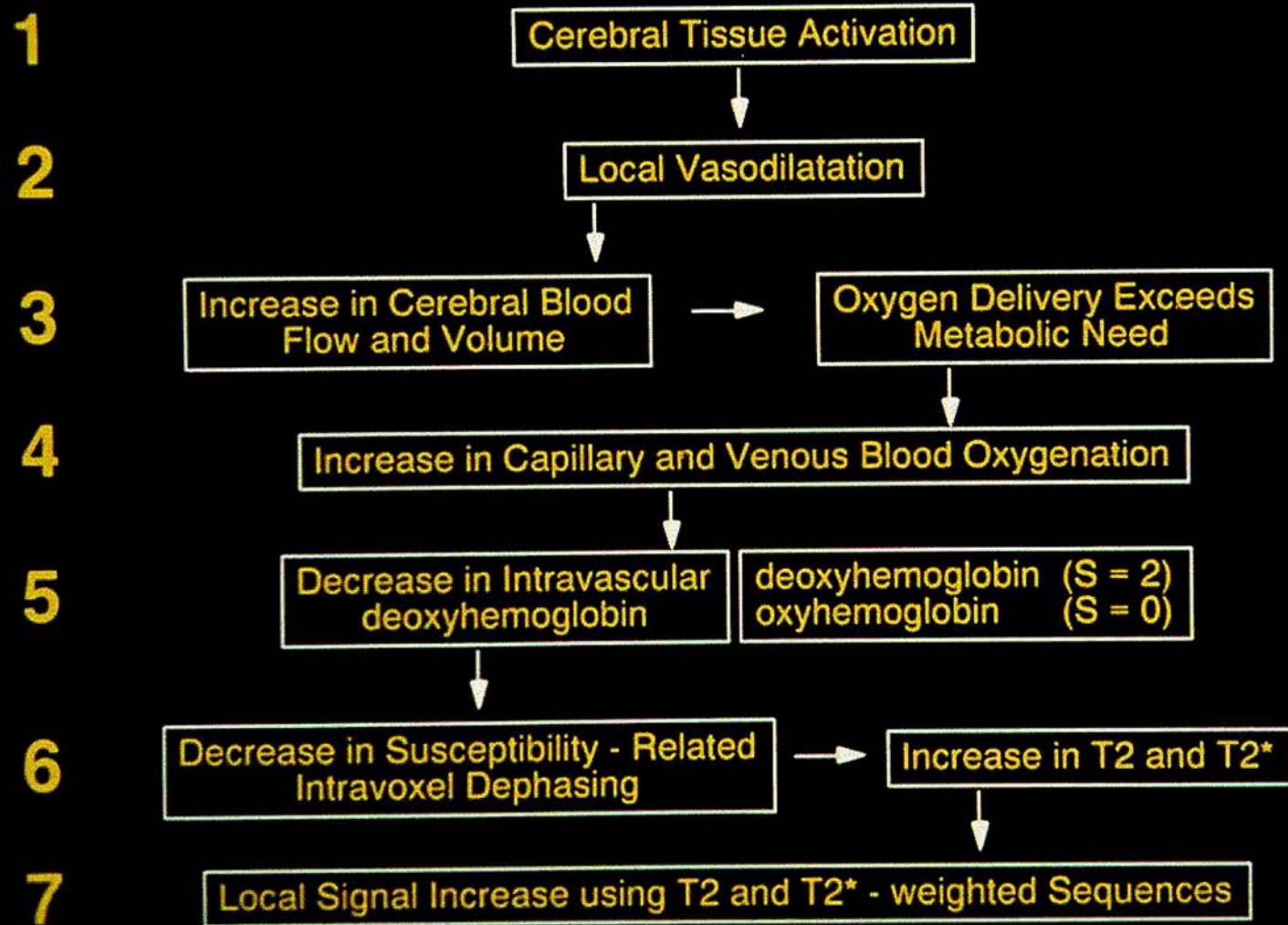
Susceptibility-Induced Field Distortion in the  
Vicinity of a Microvessel  $\perp$  to  $B_0$ .



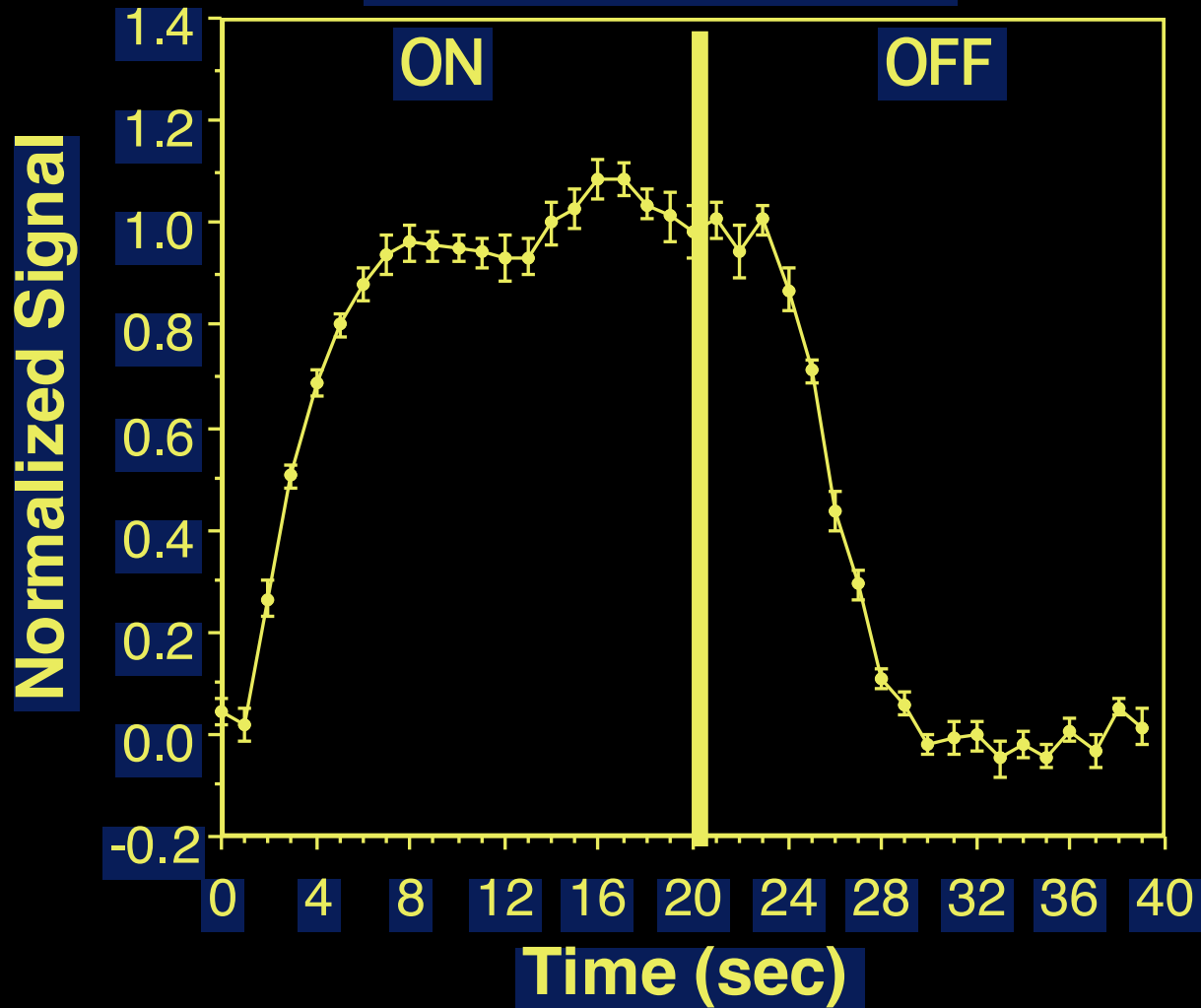




## *BOLD Contrast in the Detection of Neuronal Activity*



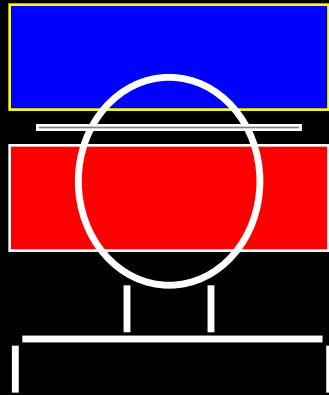
# Primary Motor Cortex: Gradient-Echo EPI



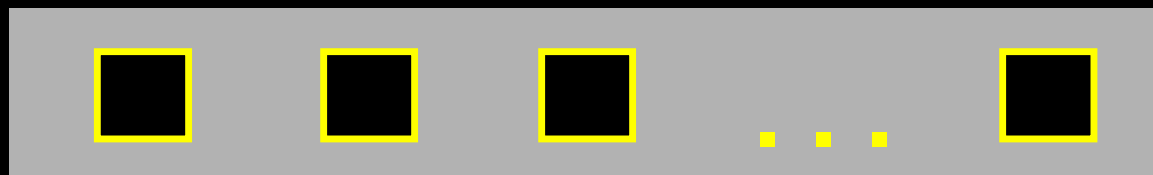
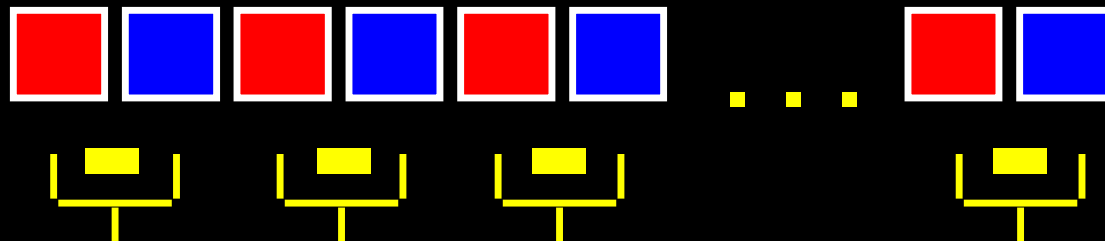
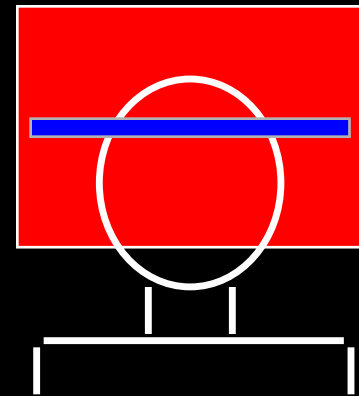


# Perfusion / Flow Imaging

**EPISTAR**



**FAIR**



**Perfusion  
Time Series**

TI (ms)

**FAIR**

**EPISTAR**

**200**

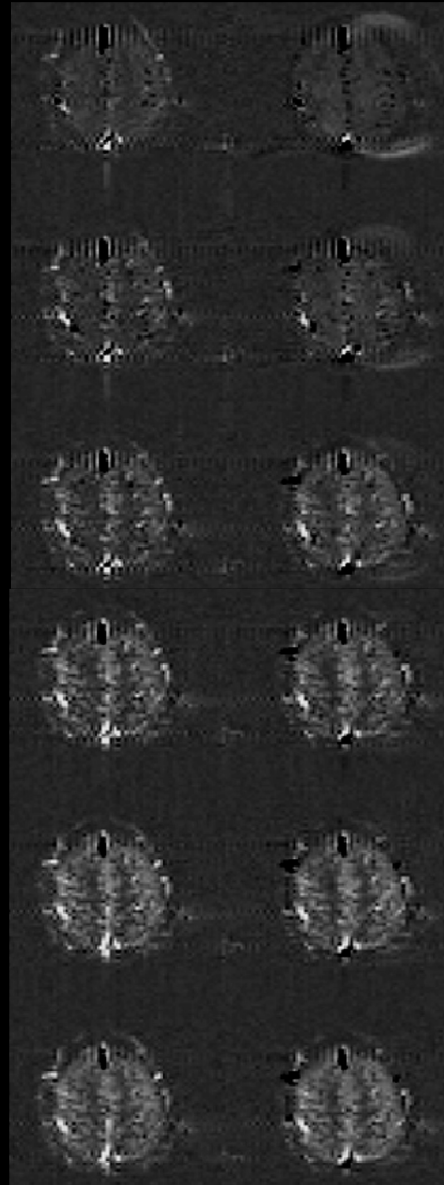
**400**

**600**

**800**

**1000**

**1200**



+

-

## Volume

- unique information
- baseline information
- multislice trivial

- invasive
- low C / N for func.

## BOLD

- highest C / N
- easy to implement
- multislice trivial
- non invasive
- highest temp. res.

- complicated signal
- no baseline info.

## Perfusion

- unique information
- control over ves. size
- baseline information
- non invasive

- multislice non trivial
- lower temp. res.
- low C / N

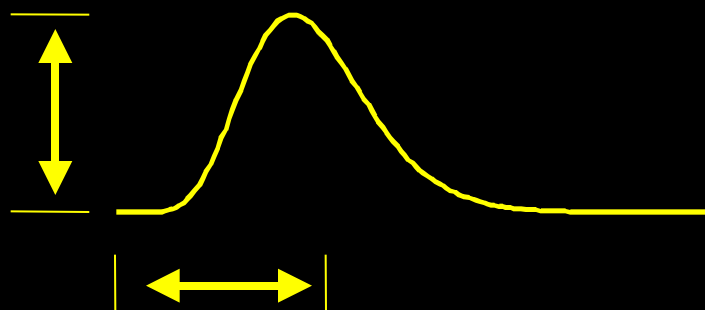
Neuronal  
Activation

?

Hemodynamics

?

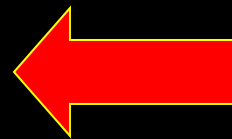
Measured  
fMRI  
Signal



Physiologic Factors

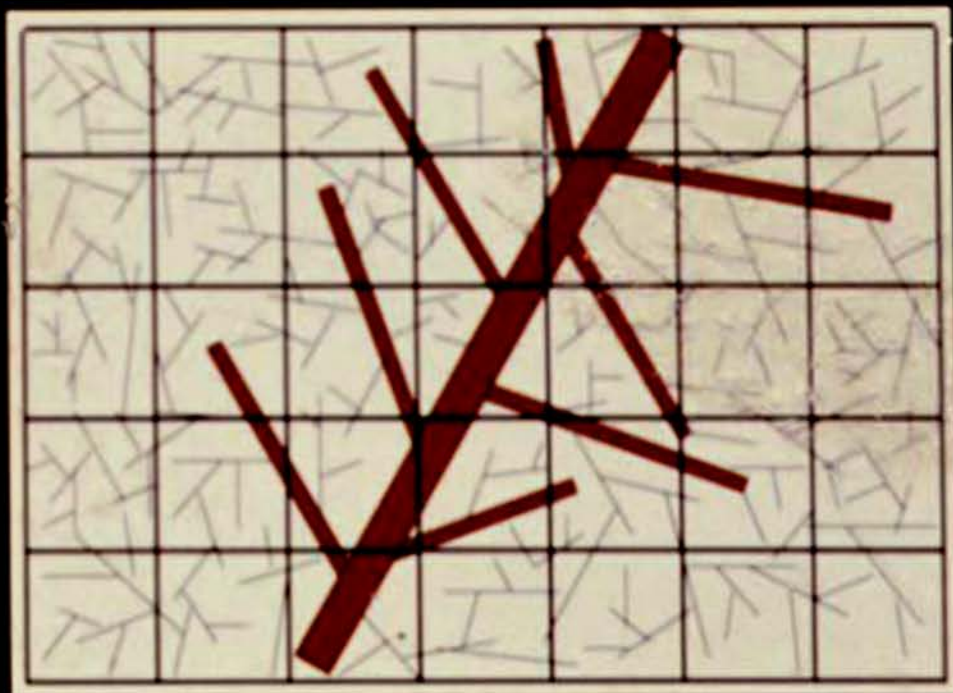
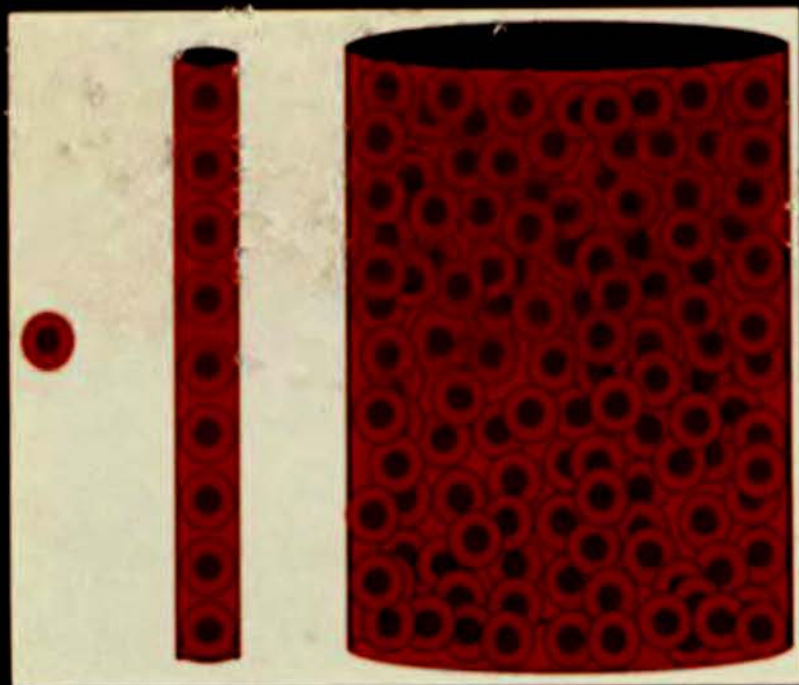
# Physiologic Factors that Influence BOLD Contrast

- Blood oxygenation
- Blood volume
- Blood pressure
- Hematocrit
- Vessel size



**Coupling:  
Flow & CMRO<sub>2</sub>**



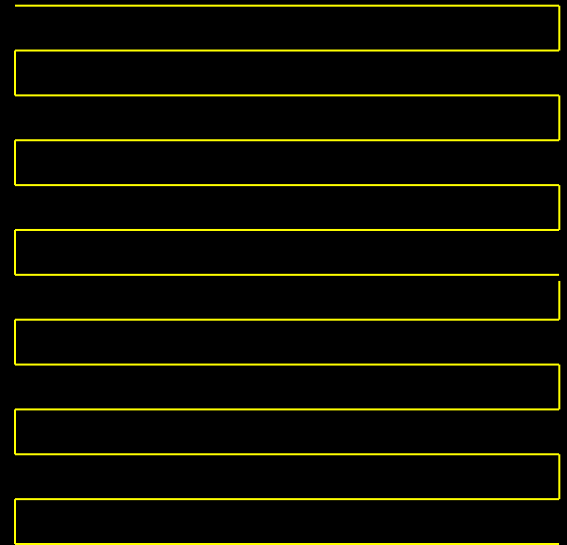
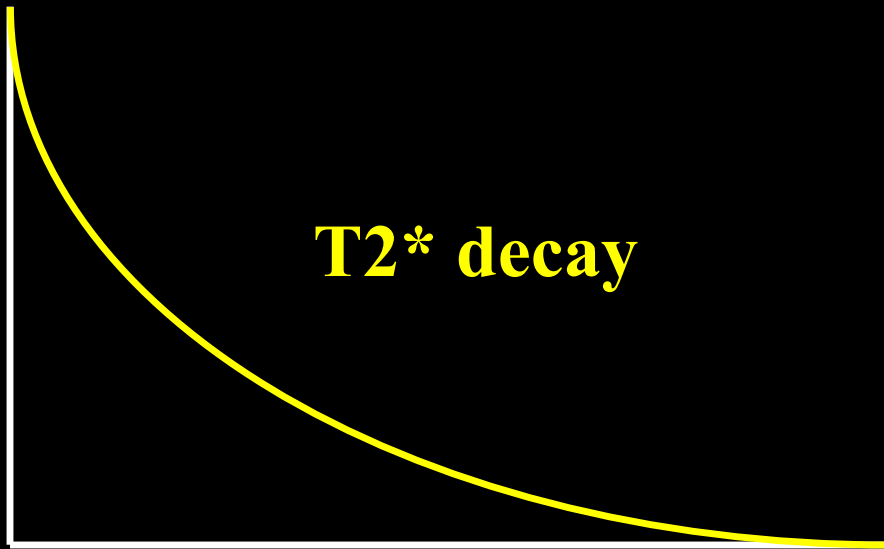


# Where and When?

**The resolution is determined by the cerebral hemodynamics.**

- **Know the vasculature at which you are looking.**
- (or)**
- **Normalize to the spatial variation in the vasculature.**
- (or)**
- **Make several assumptions.**

# Single Shot Imaging



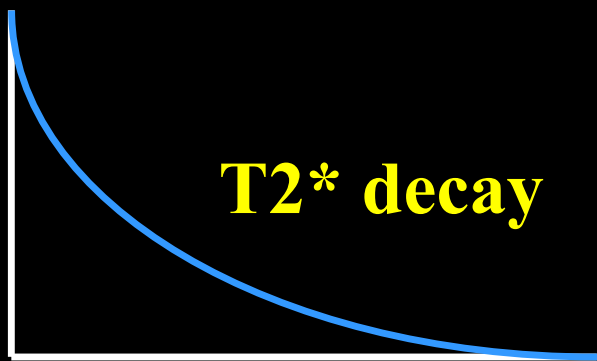
**EPI Readout Window**

**≈ 20 to 40 ms**

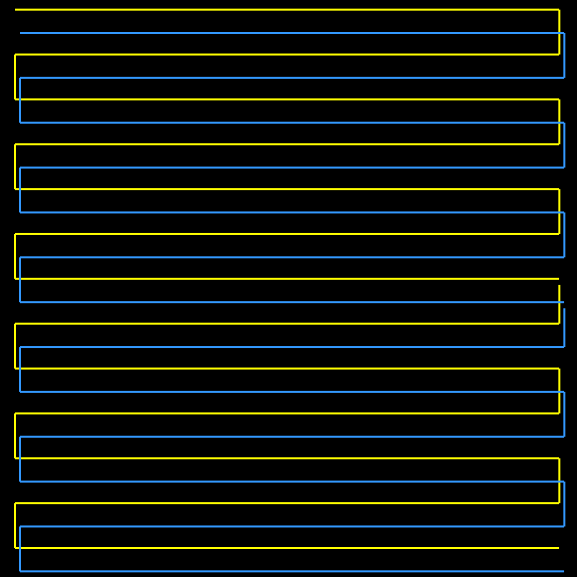
# Multishot Imaging



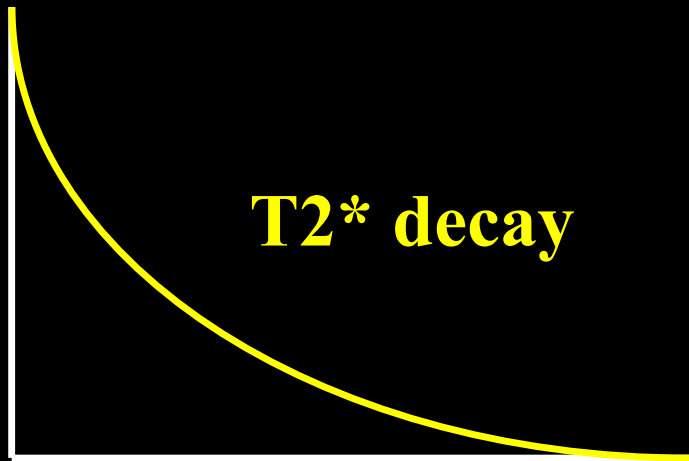
**EPI Window 1**



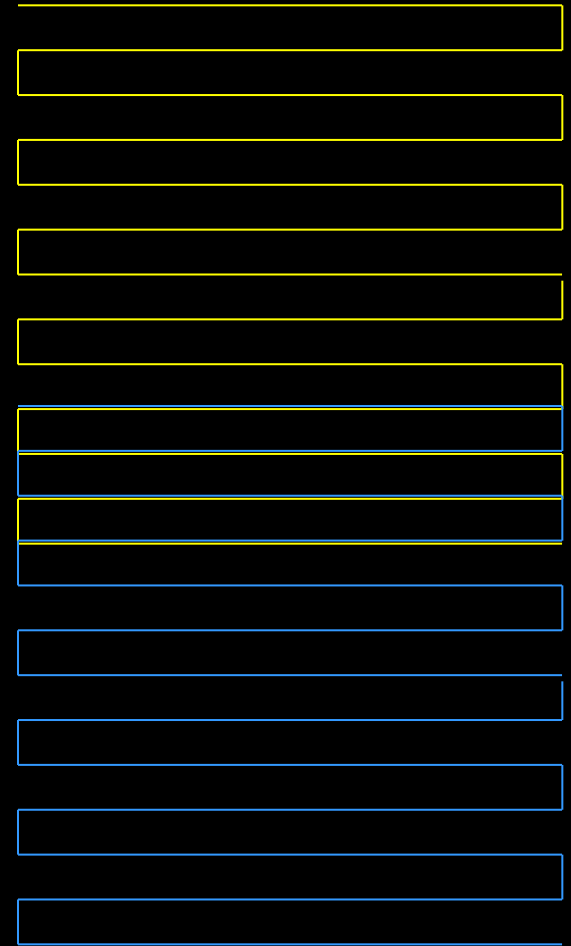
**EPI Window 2**



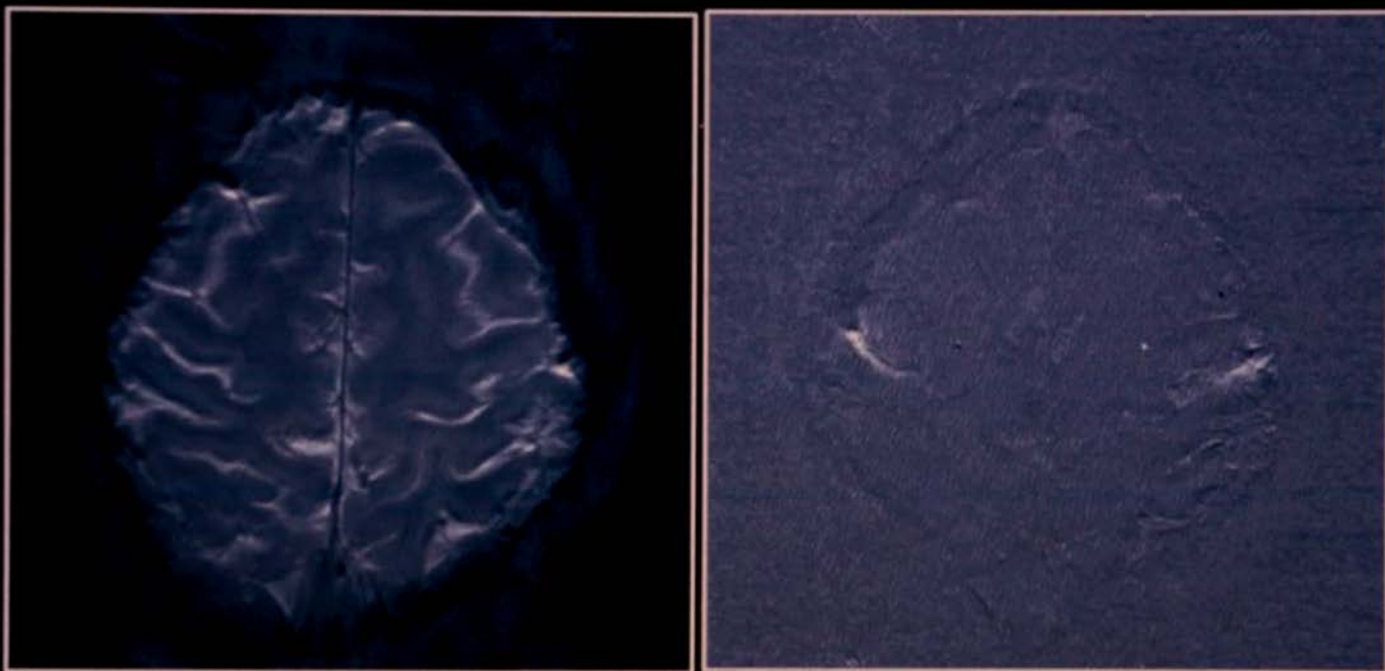
# Partial k-space imaging



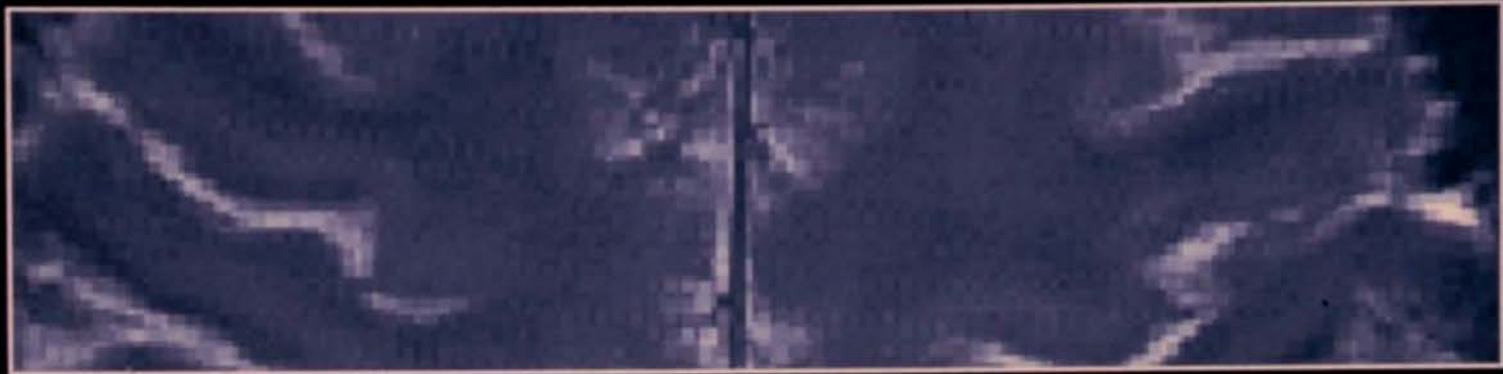
**EPI Window**

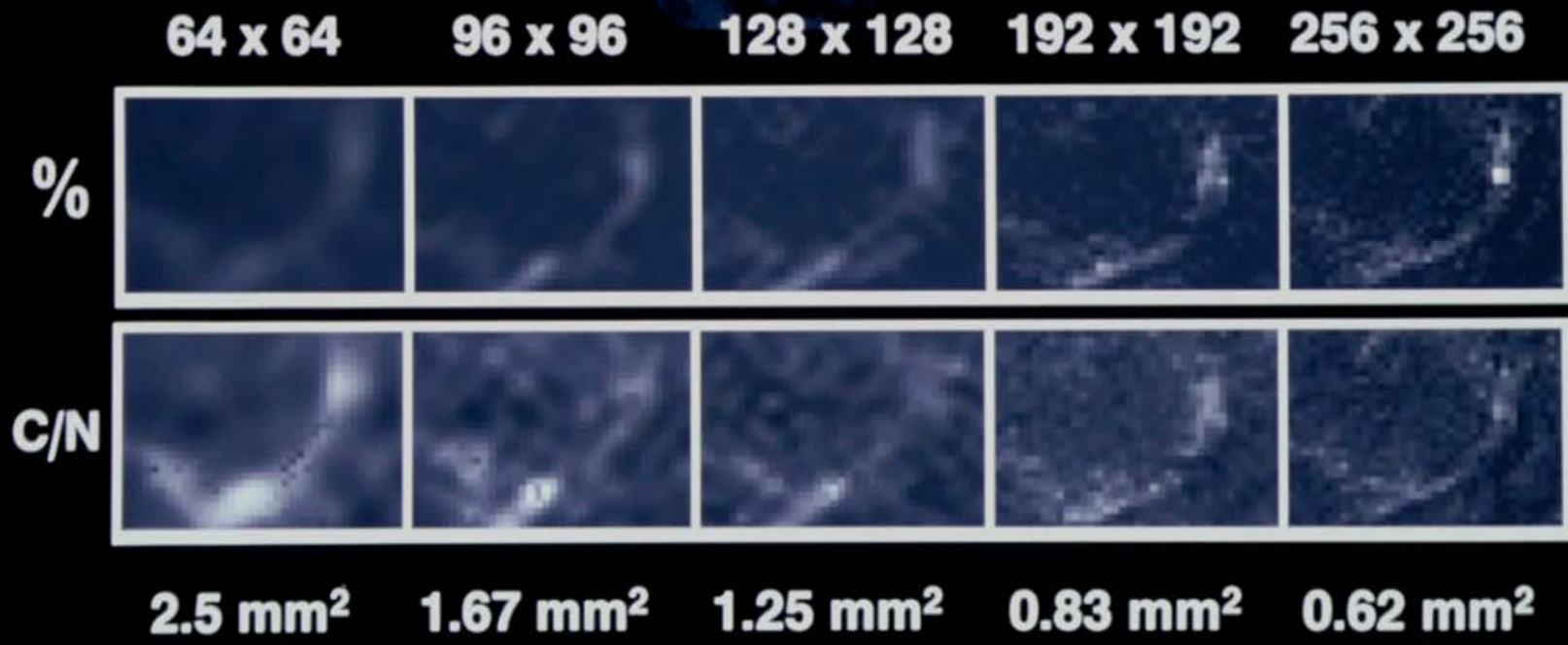


**Single - Shot EPI at 3T:  
Half NEX, 256 x 256, 16 cm FOV**



**Single - Shot EPI at 3T:  
Half NEX 256 x 256, 16 cm FOV**



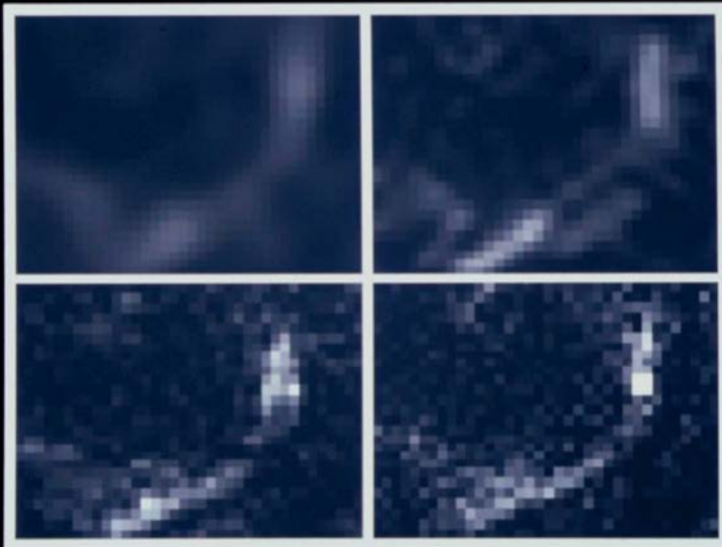




## Fractional Signal Change

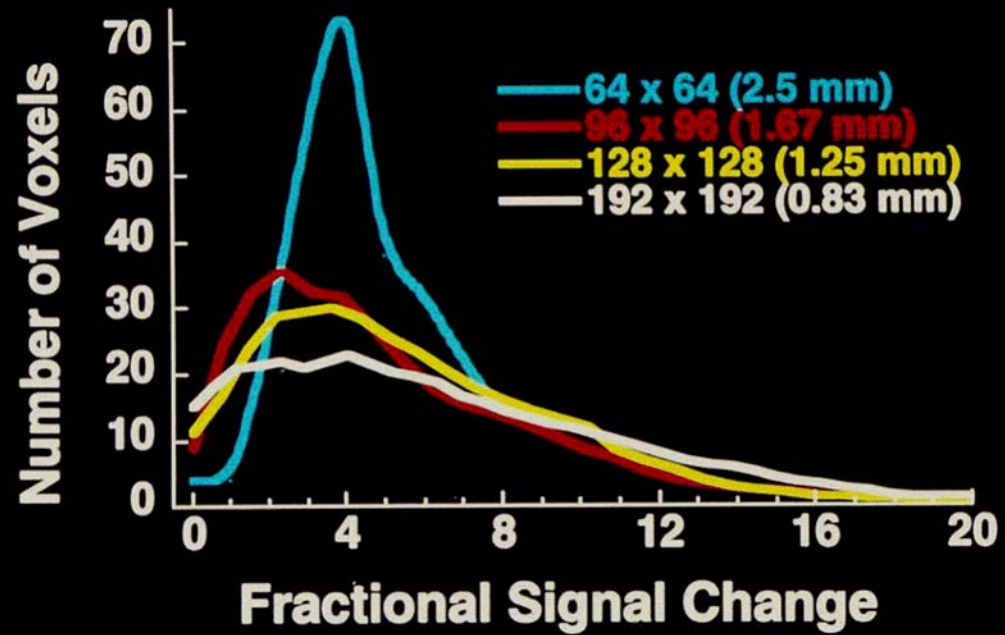
2.5 mm<sup>2</sup>

1.25 mm<sup>2</sup>



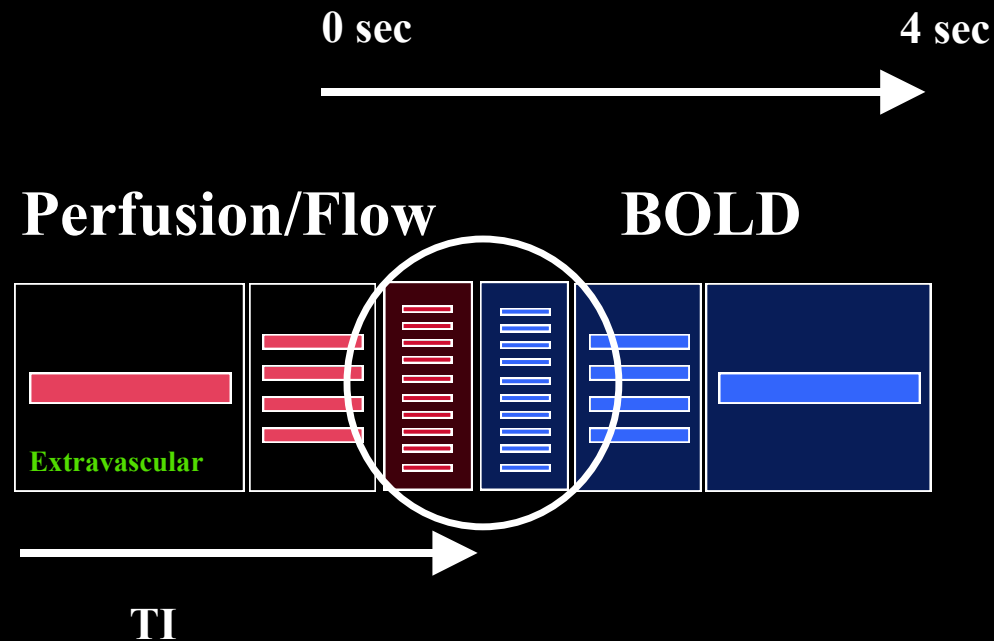
0.83 mm<sup>2</sup>

0.62 mm<sup>2</sup>



# Pulse sequence based methods for increasing spatial and temporal resolution

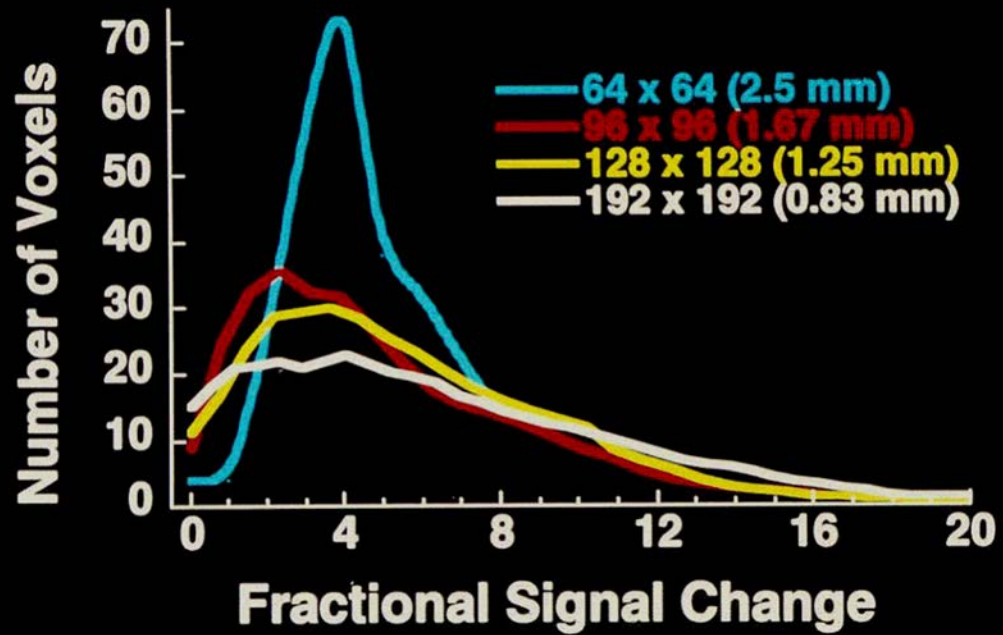
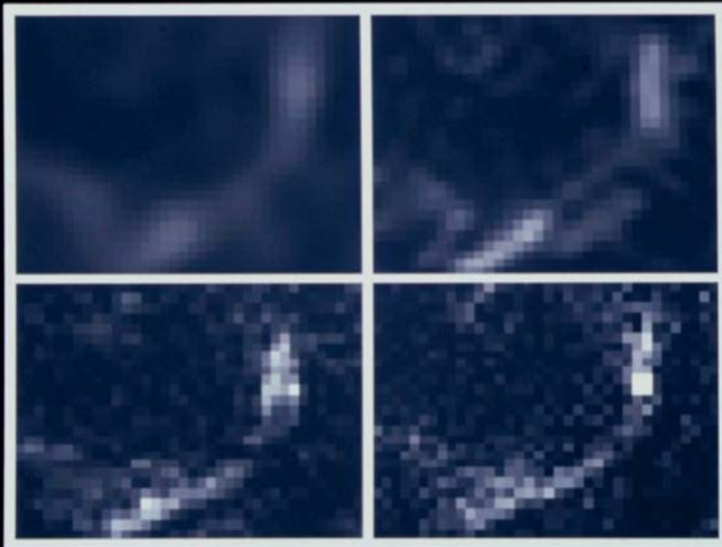
- Spin-echo
- ASL
- Diffusion weighting
- Threshold based on magnitude



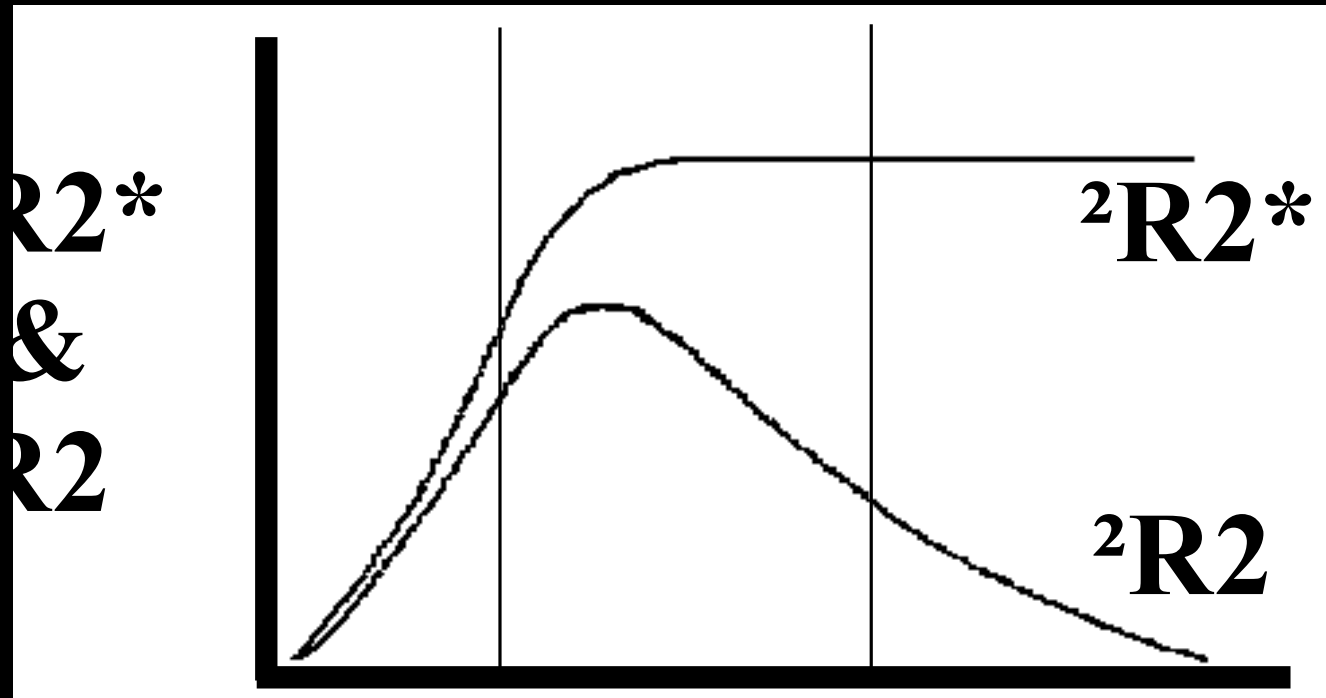
## Fractional Signal Change

2.5 mm<sup>2</sup>

1.25 mm<sup>2</sup>



# Spin echo vs. Gradient echo



compartment  
radius:

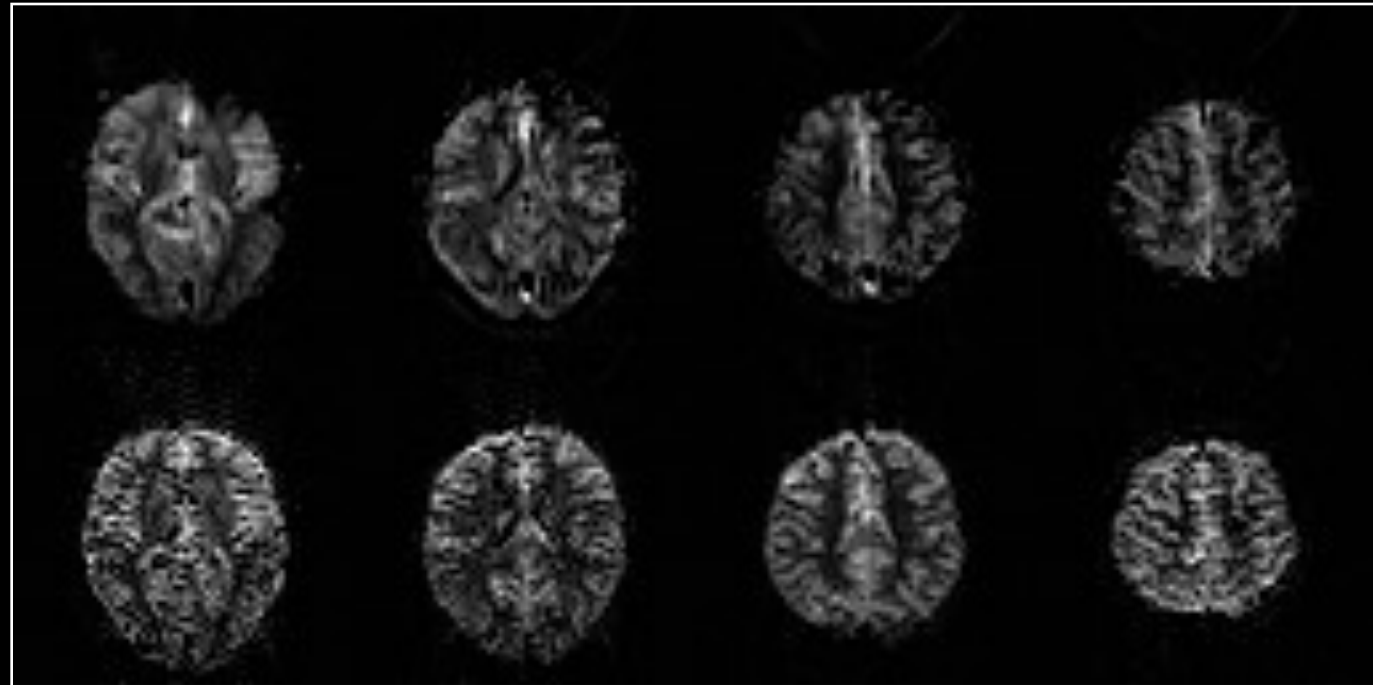
$< 3 \mu\text{m}$

3 to 15  $\mu\text{m}$

$> 15 \mu\text{m}$

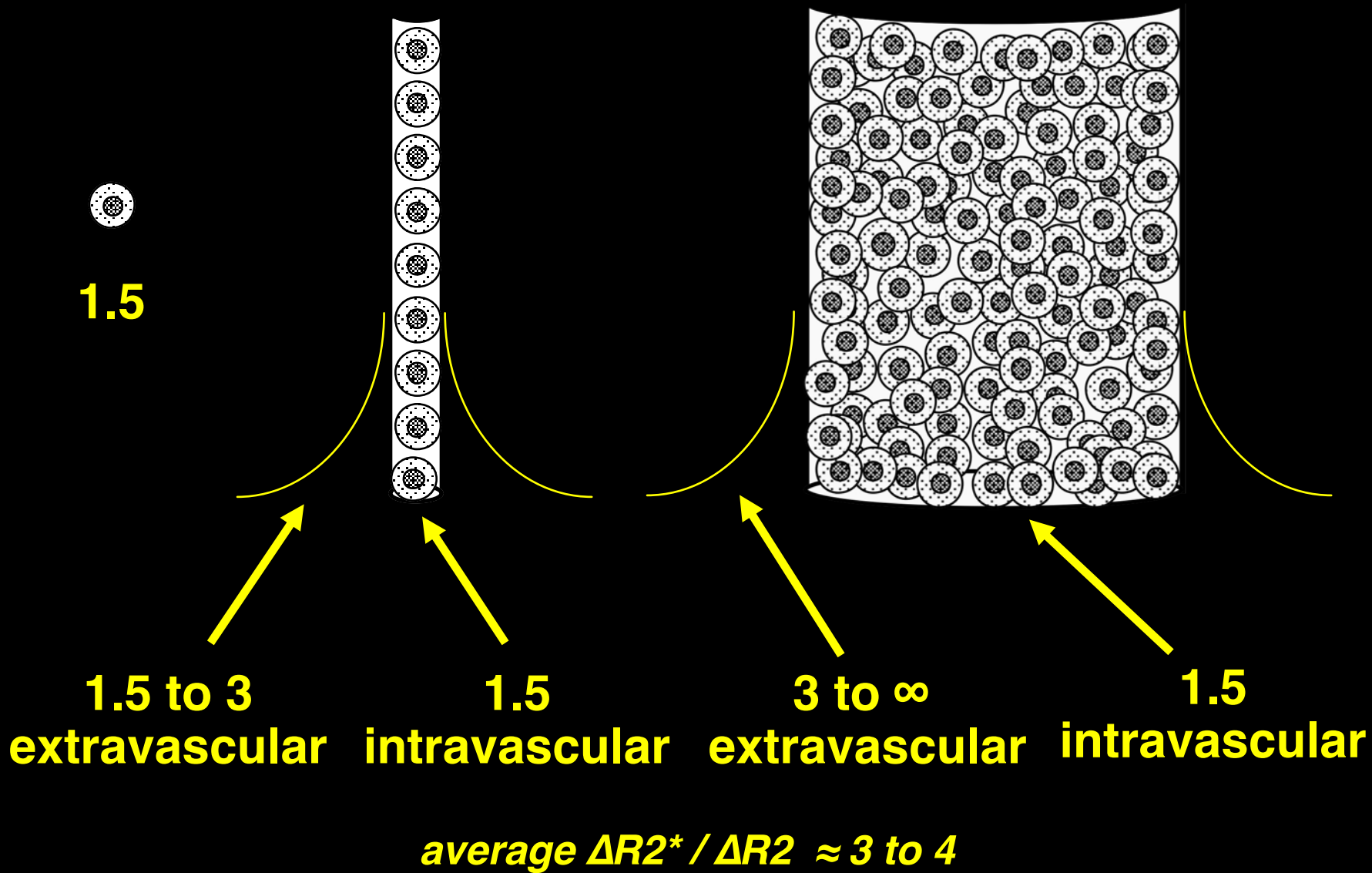
**GE**  
**TE = 30 ms**

**SE**  
**TE = 110 ms**



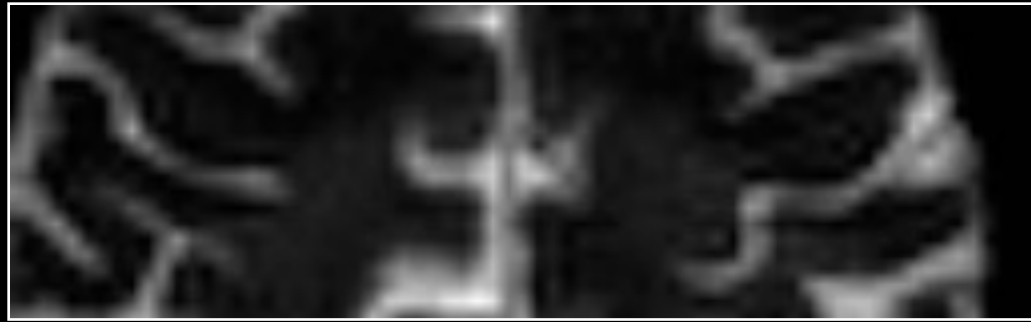
Spin-echo??

$\Delta R2^* / \Delta R2$



3T

Spin-Echo  
TE = 105 ms  
TR =  $\infty$



Gradient-Echo  
TE = 50 ms



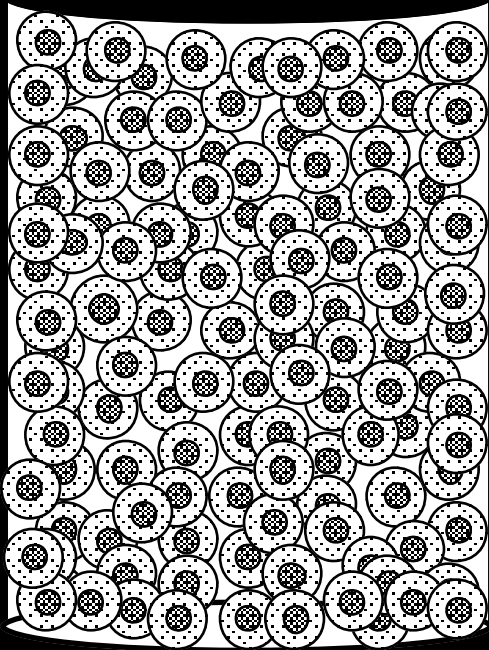
Gradient-Echo  
functional  
TE = 50 ms



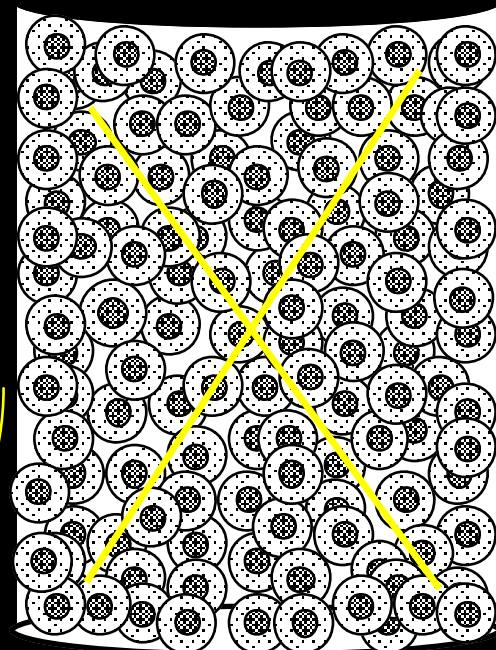
Spin-Echo  
functional  
TE = 105 ms



**no diffusion weighting**



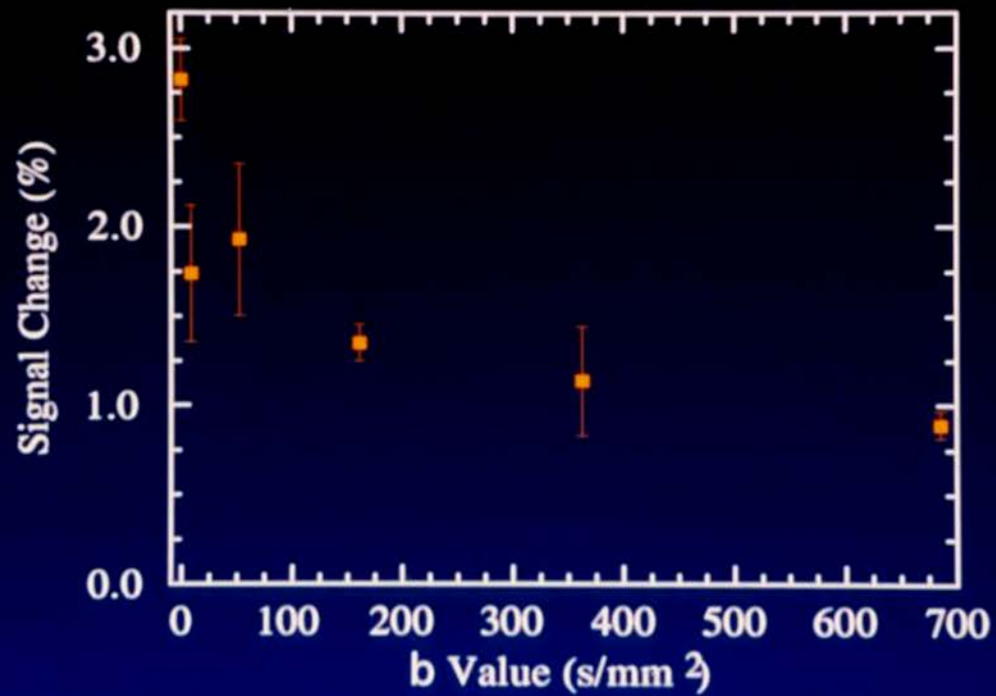
**diffusion weighting**



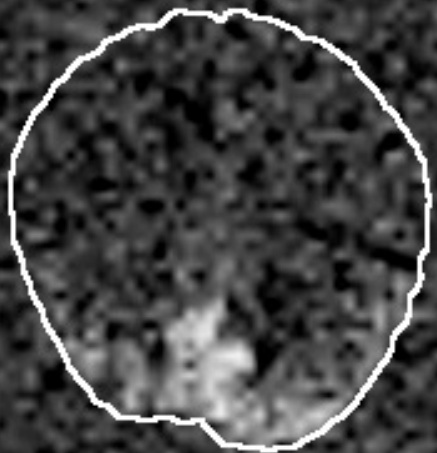


## Summary of Diffusion-Weighted fMRI Data

---



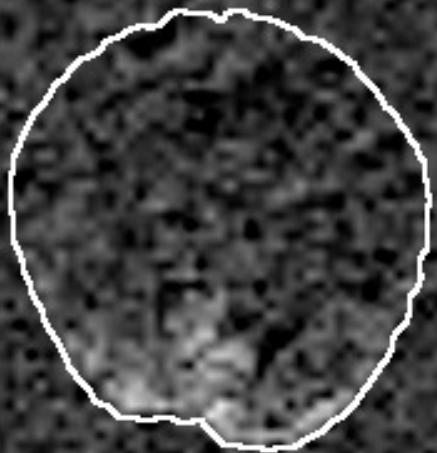
**b = 0**



**b = 10**



**b = 50**



**b = 160**

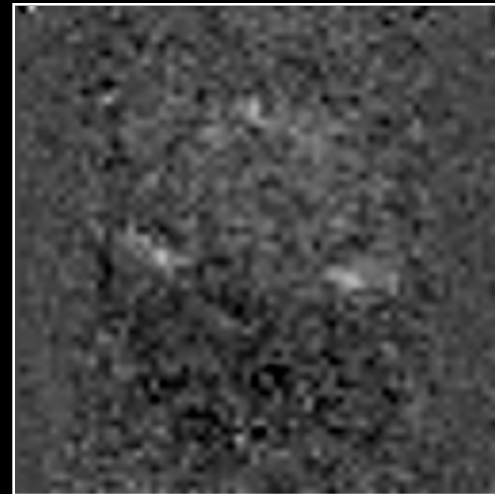
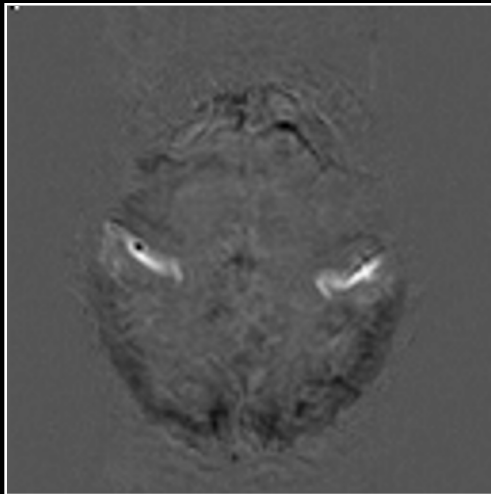
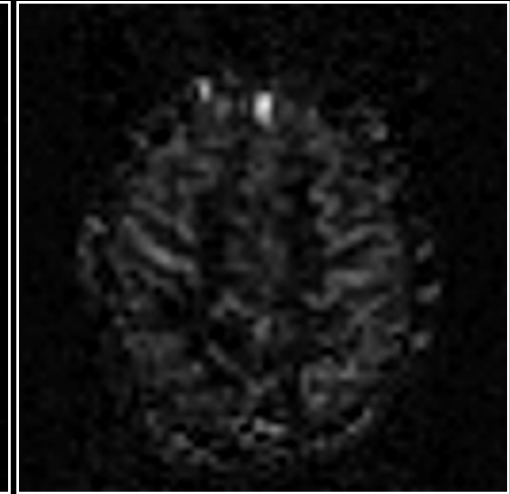
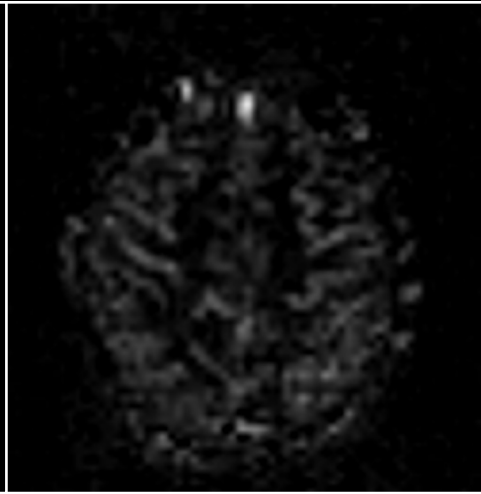
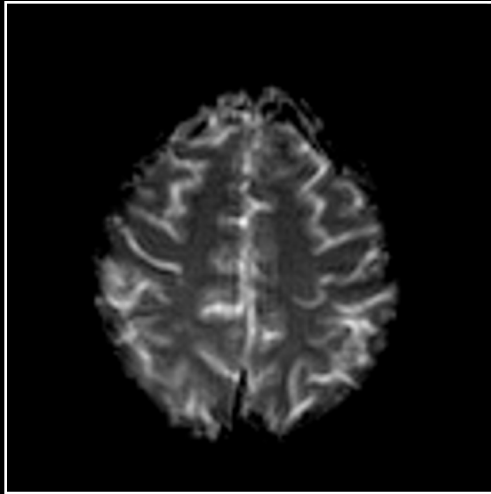


# Perfusion

**BOLD**

*Rest*

*Activation*



**Anatomy**



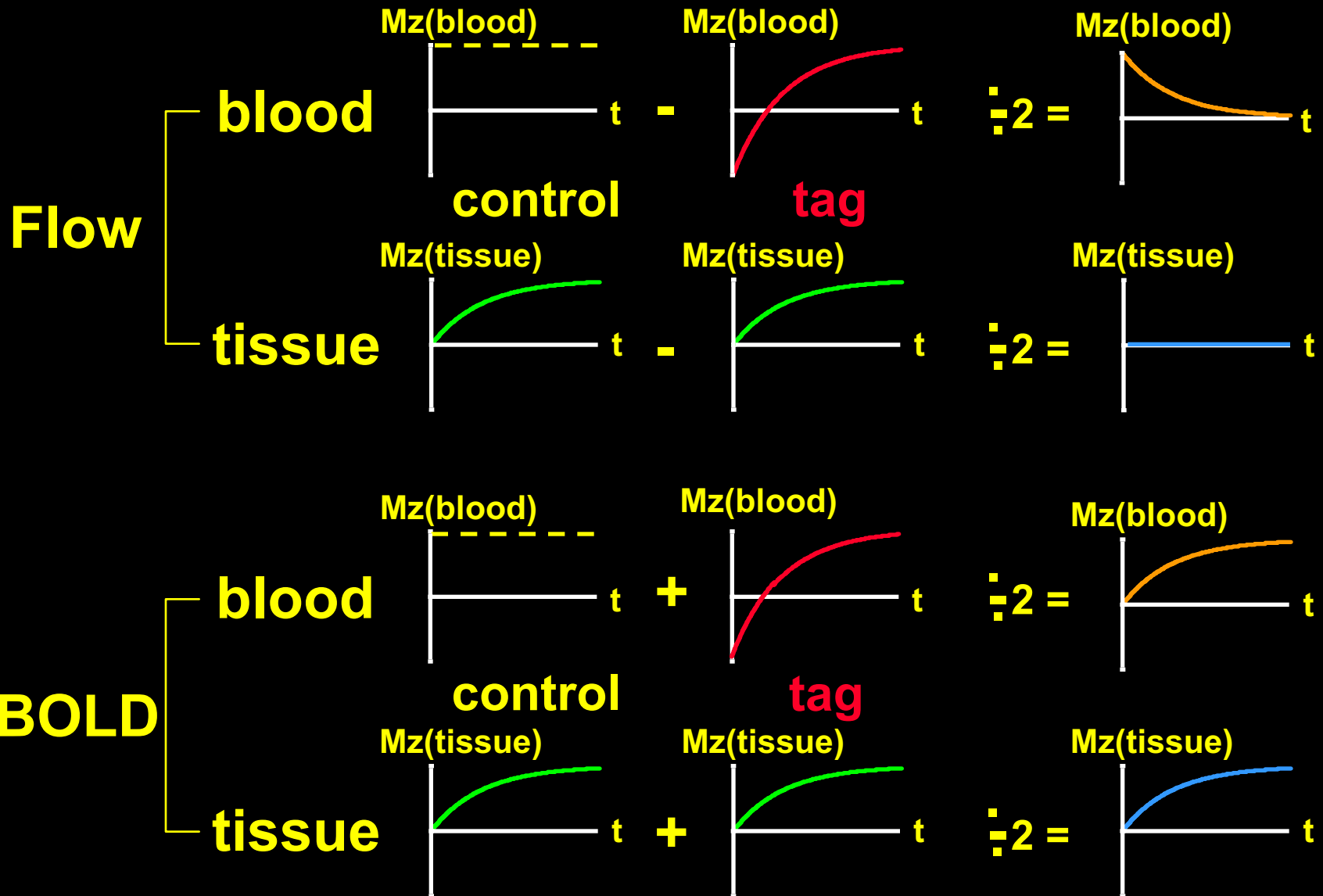
**BOLD**



**Perfusion**



# Simultaneous Flow and BOLD



# Simultaneous BOLD and Perfusion



**BOLD**



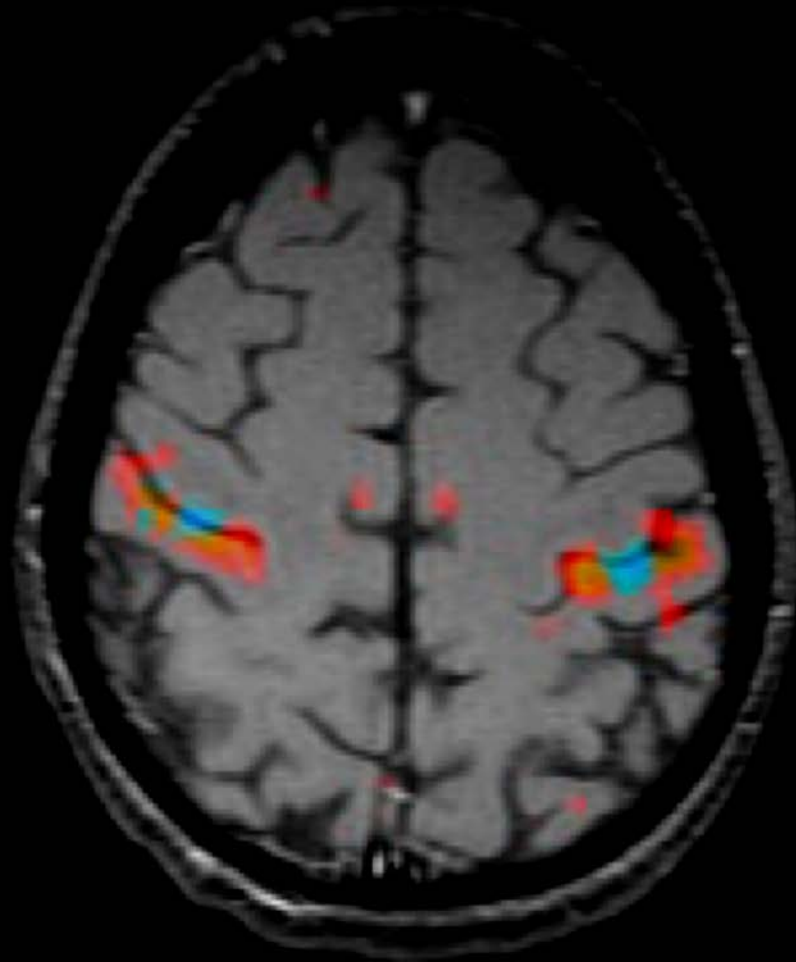
**Perfusion**



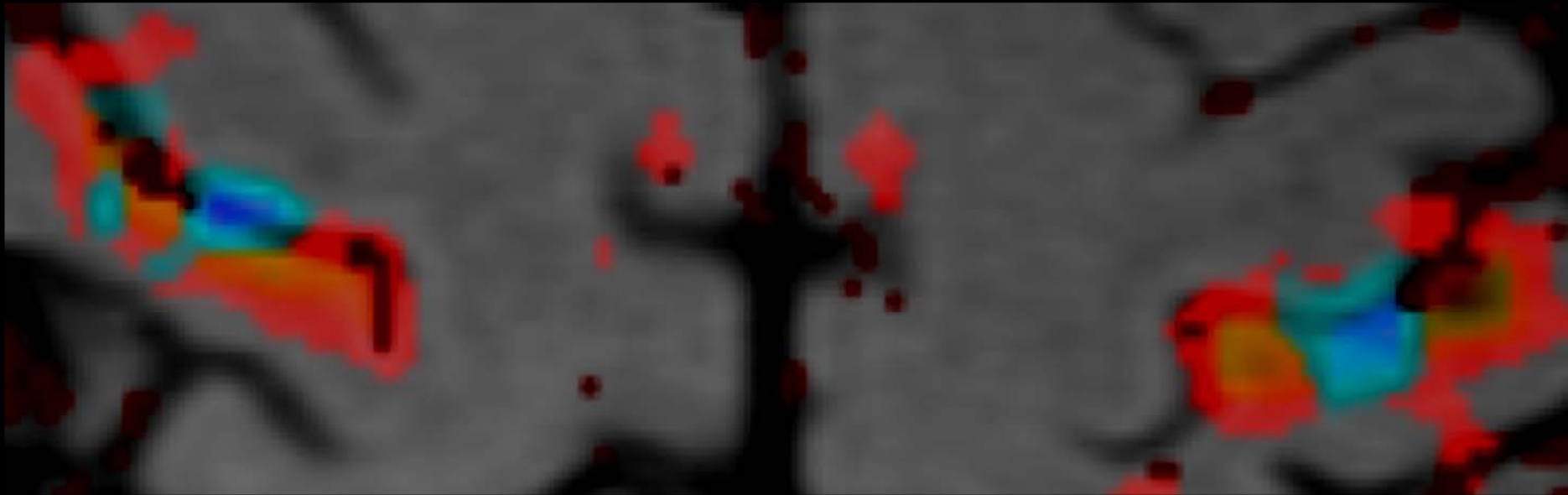
# Simultaneous BOLD and Perfusion

perfusion

BOLD

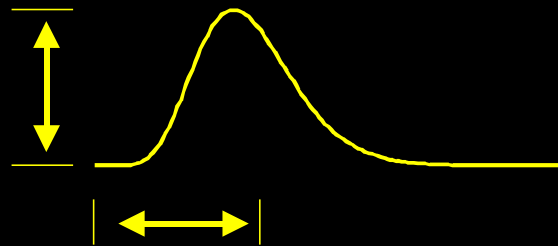
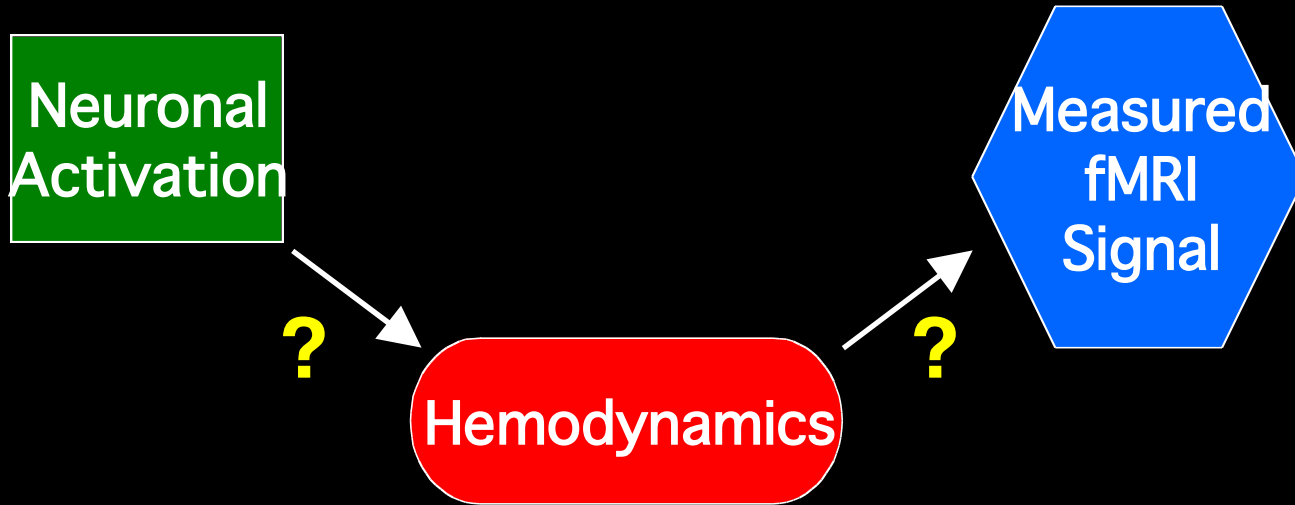


**Angiogram**  
**Perfusion**  
**BOLD**





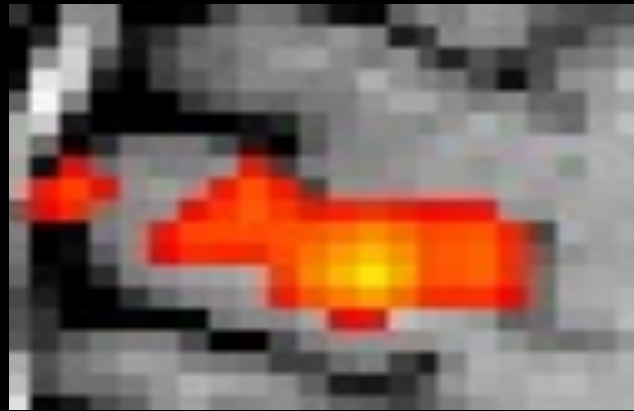
# Spatial Normalization



Physiologic Factors

**Hypercapnia**

**T1 - weighted**



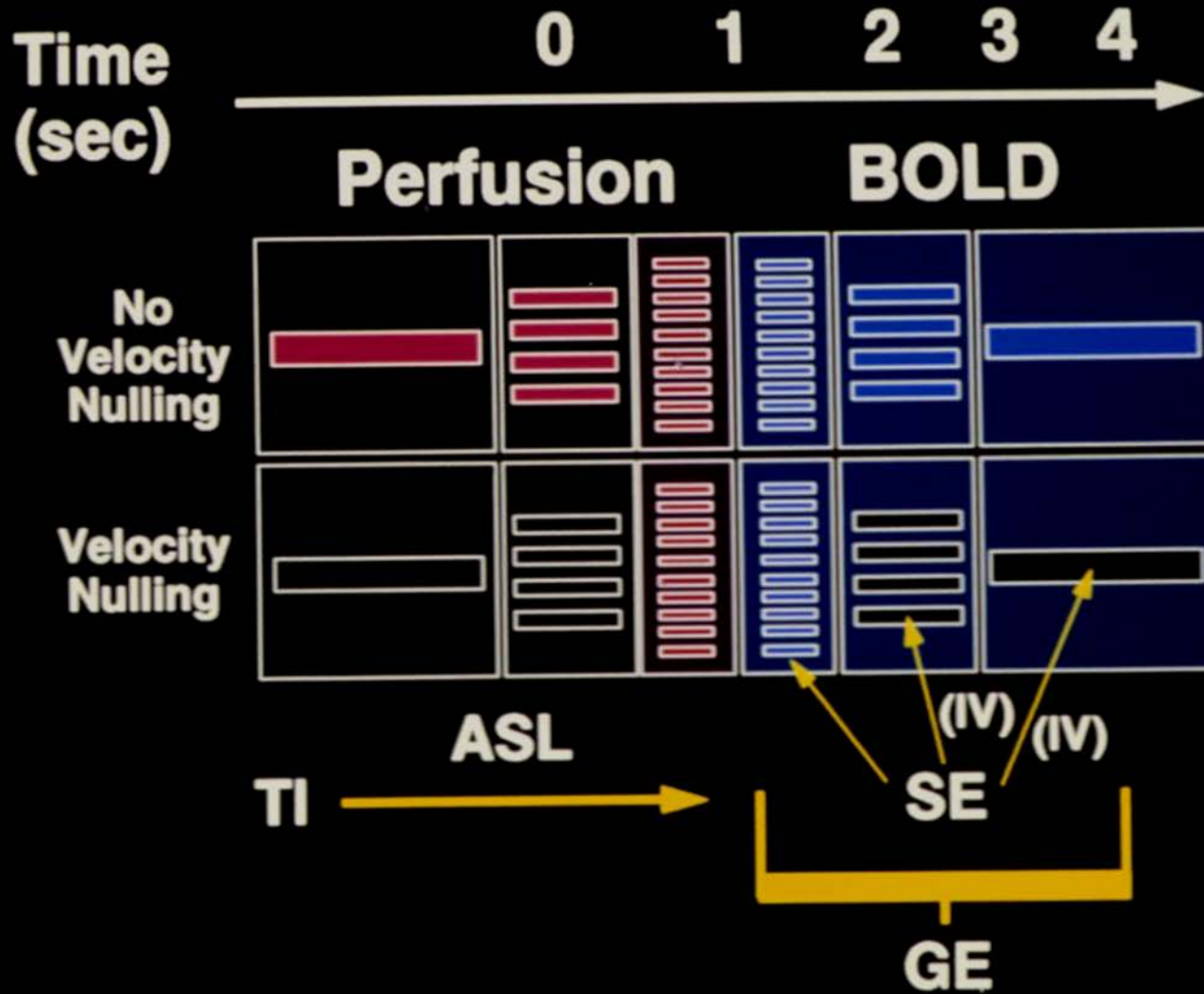
**T2\* weighted**



**T1 and T2\*  
weighted**

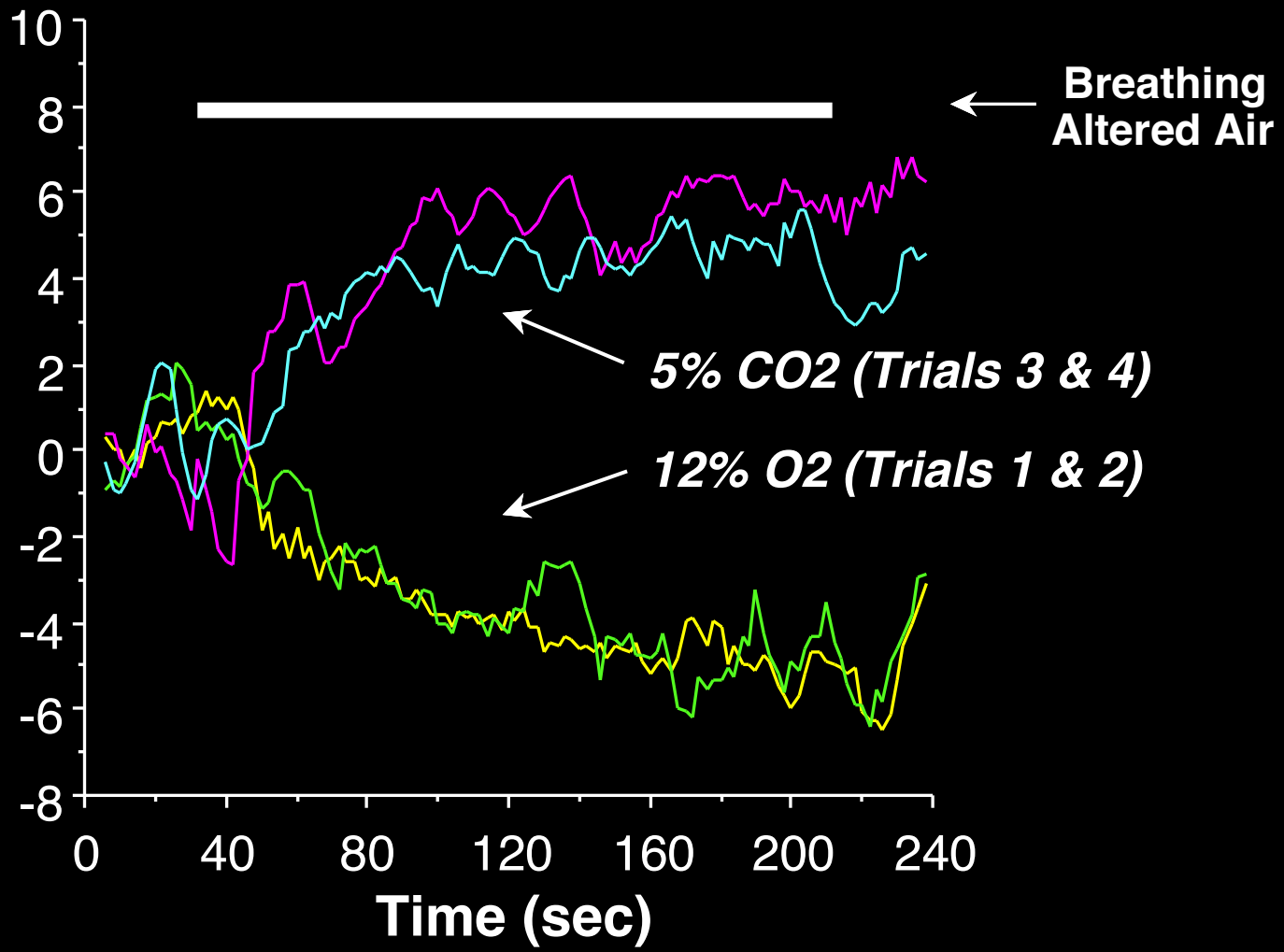


# Vascular Sensitization



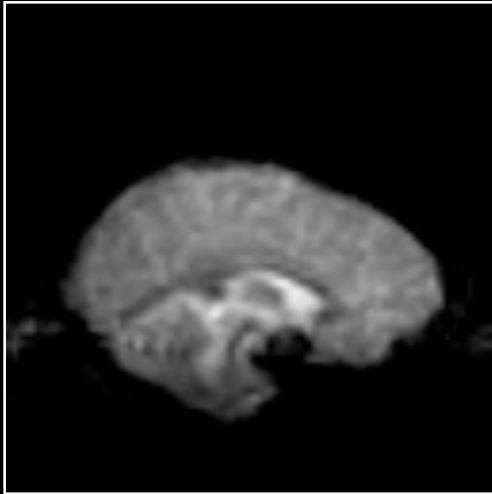
# Problems with pulse sequence - based methods for increasing resolution

- Spin-echo (sensitivity, specificity)
- Arterial spin-labeling (sensitivity, time, range)
- Diffusion weighting (sensitivity, specificity)
- Threshold based on magnitude (sensitivity, specificity)

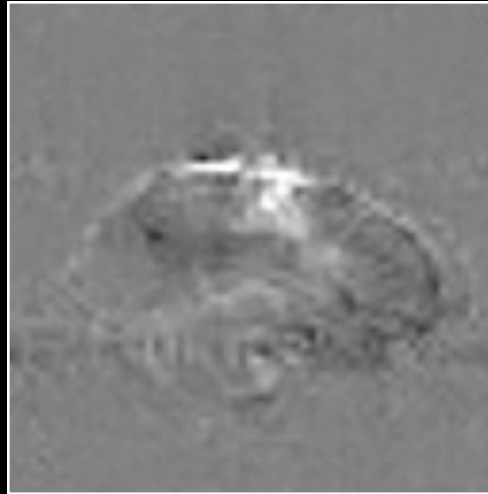


,

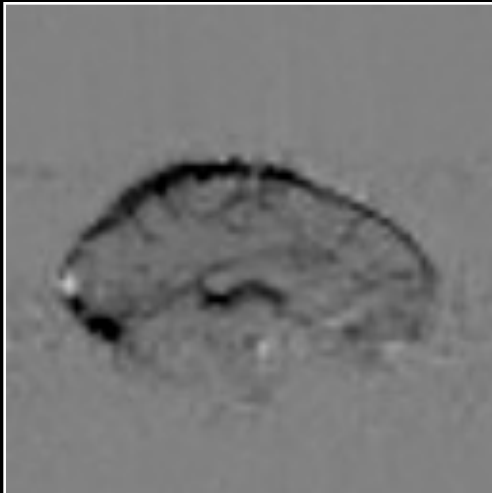
**Anatomical**



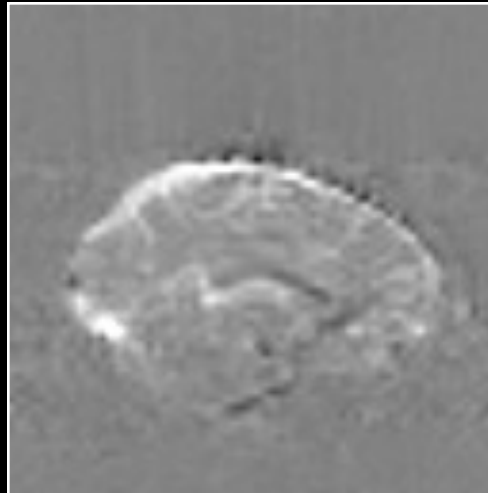
**Finger  
Movement**



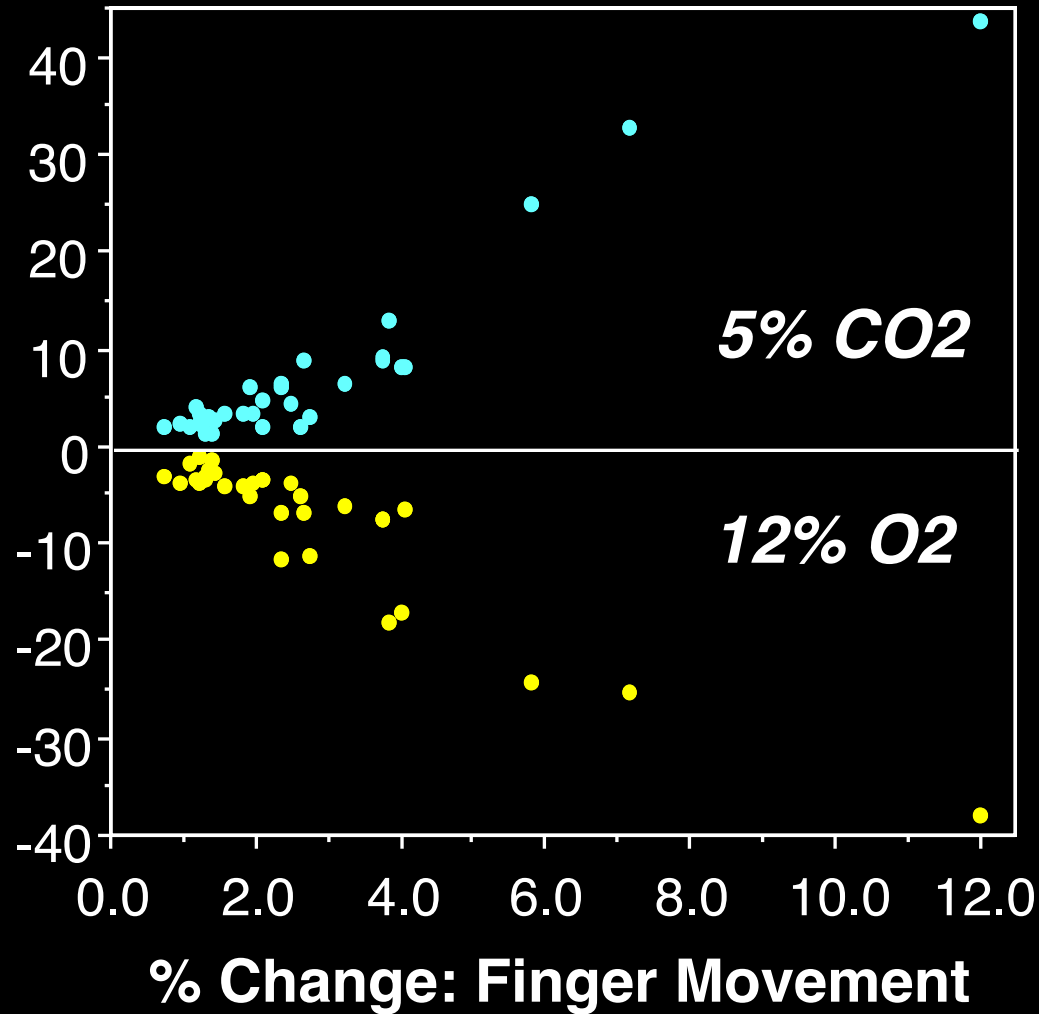
**12% O2**

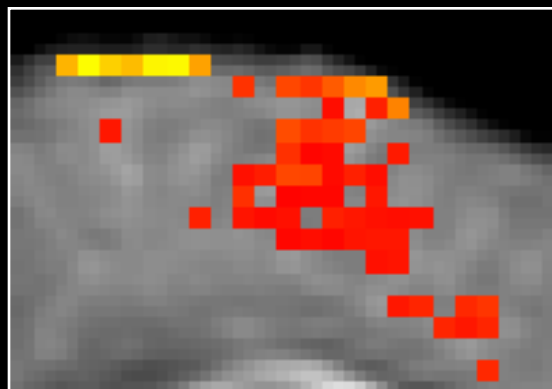
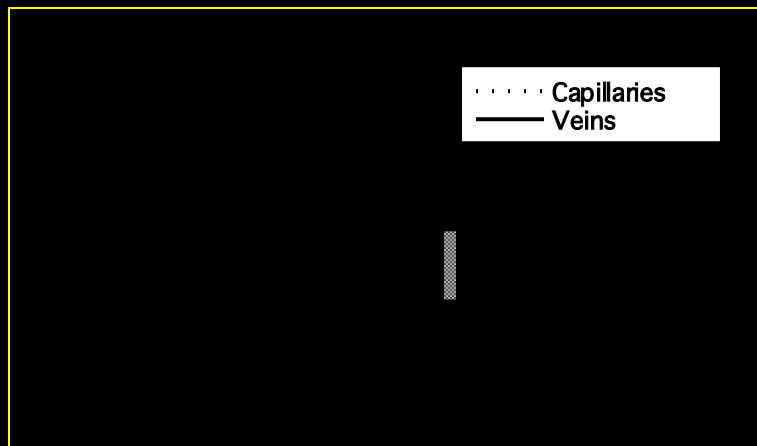


**5% CO2**

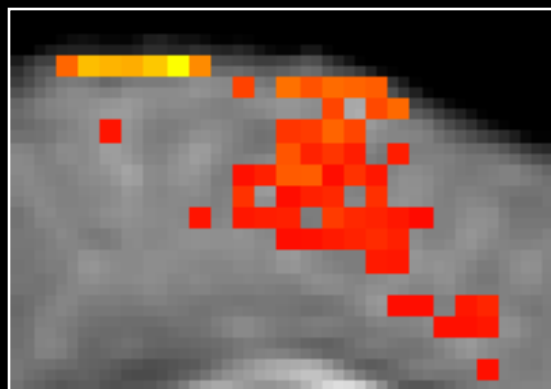


# Resting State Blood Volume Weighting

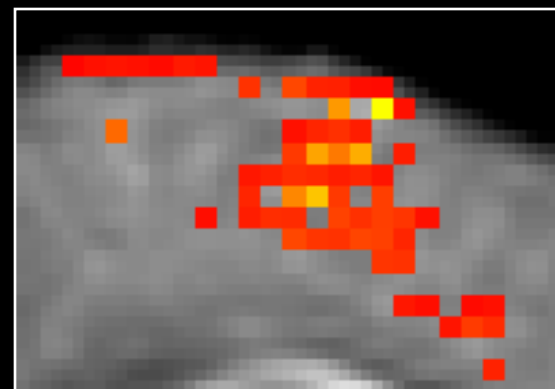




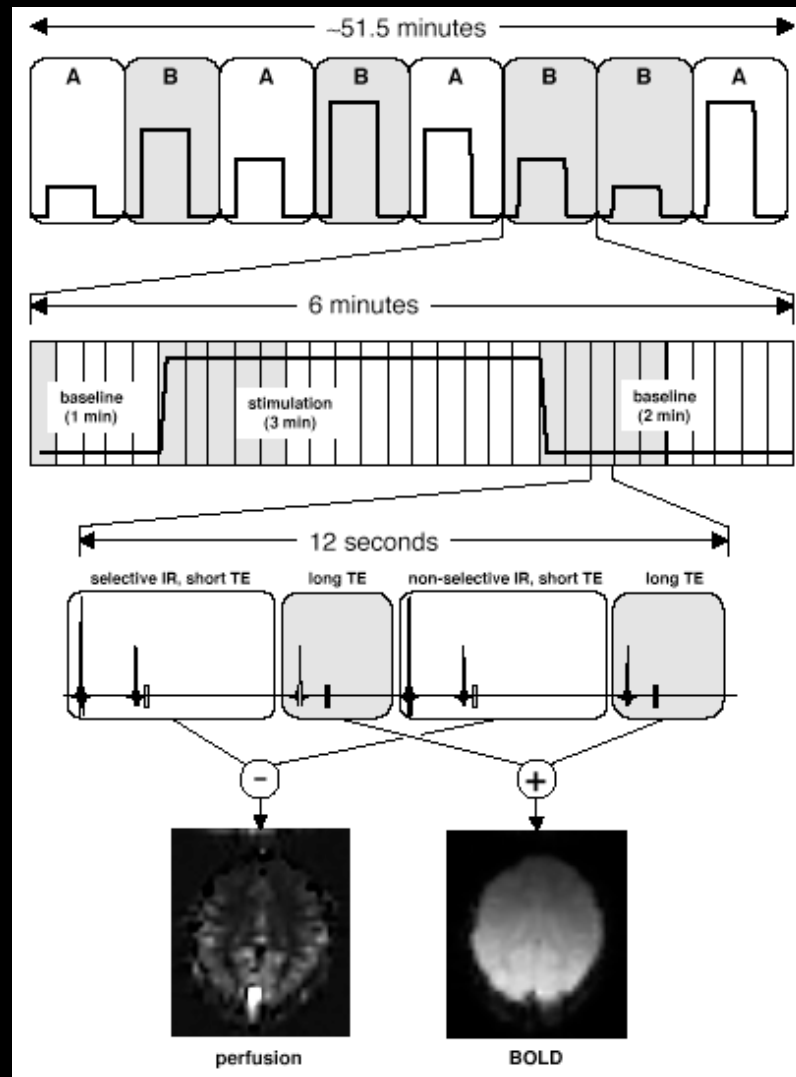
%



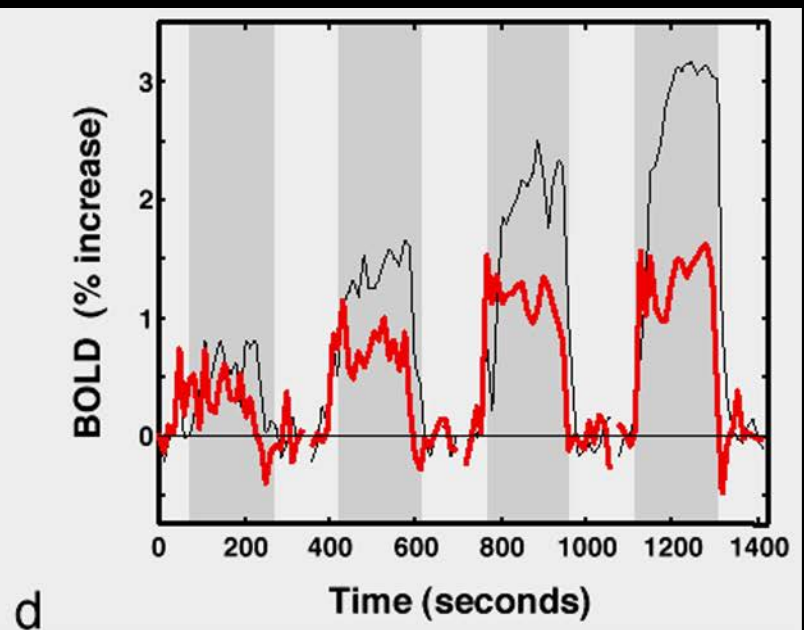
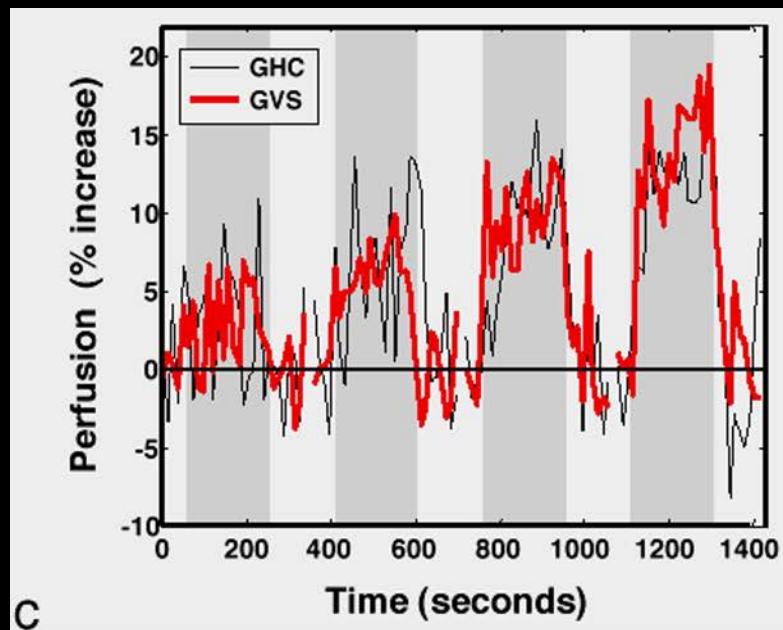
=





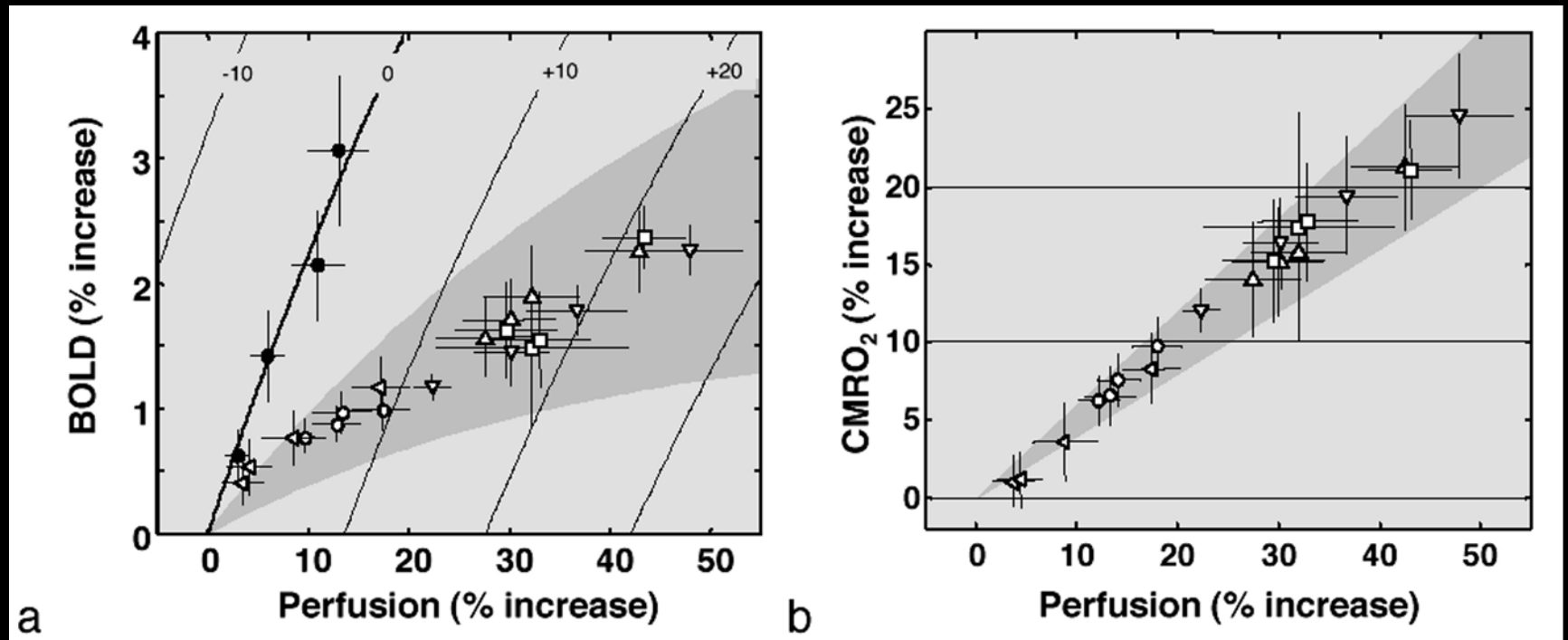


**Hoge et al**



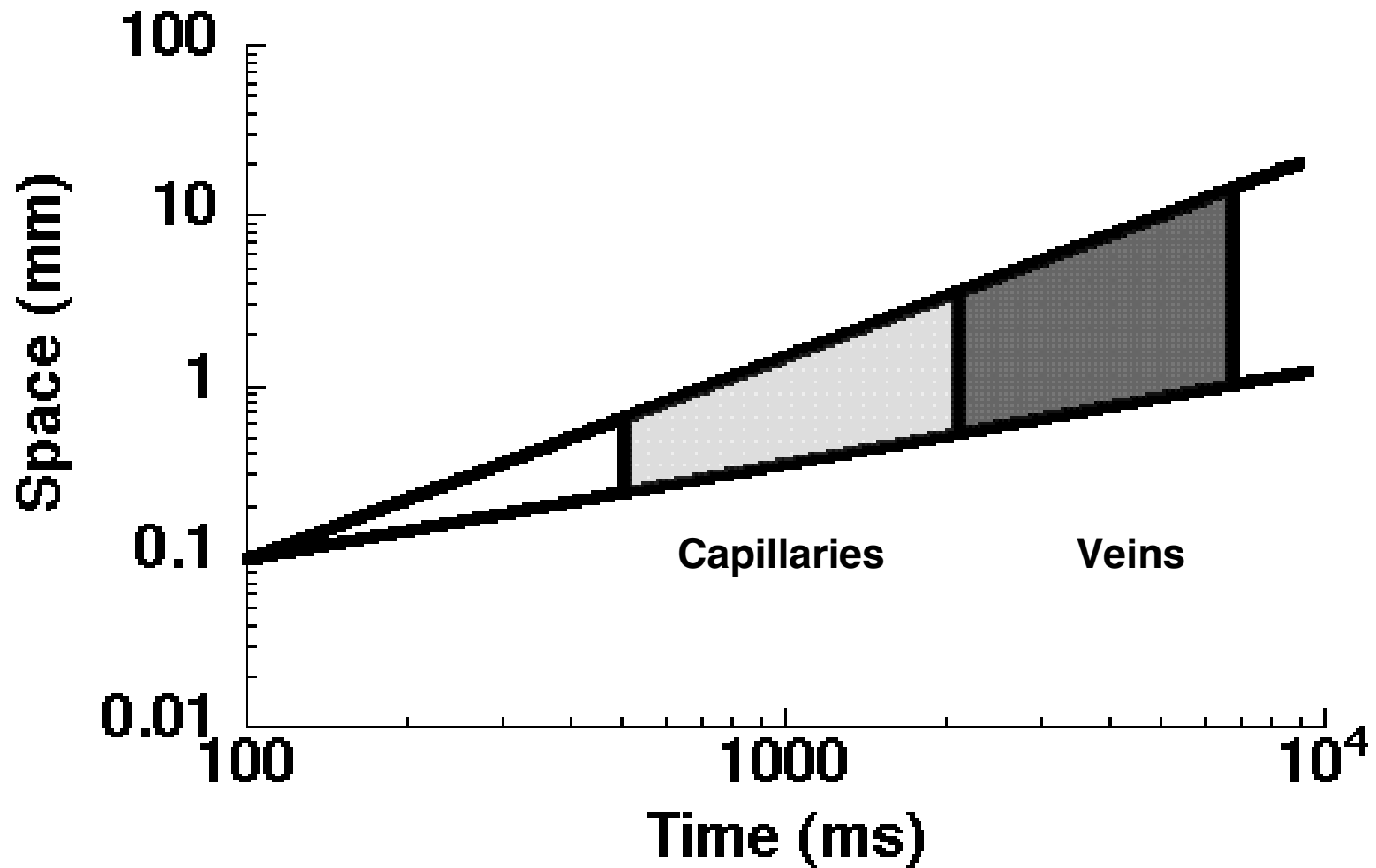
**Hoge et al**

# Mapping CMRO<sub>2</sub> using CO<sub>2</sub> Calibration



Hoge et al

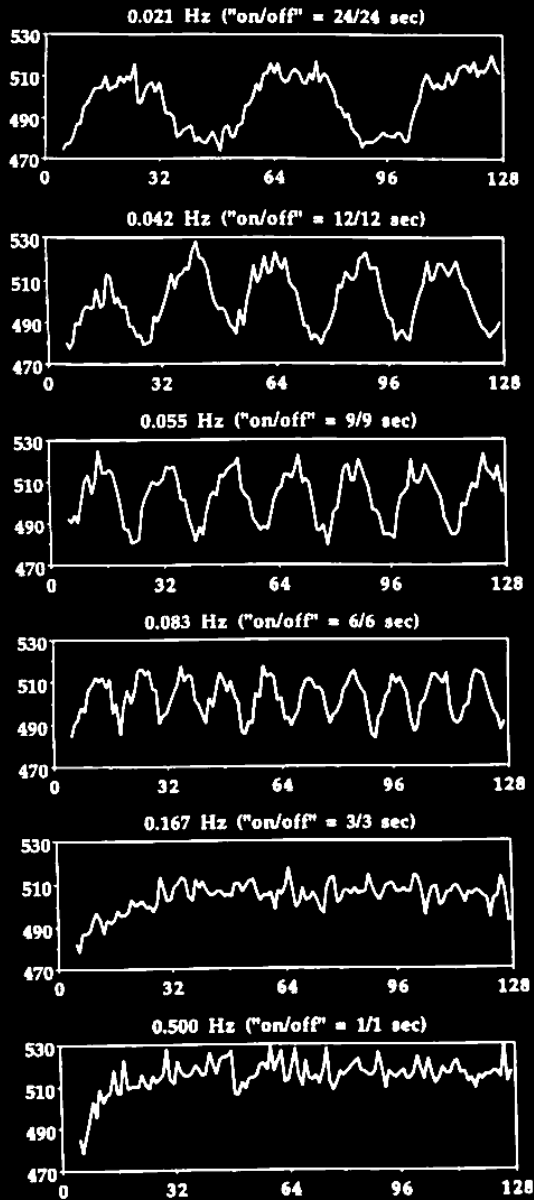
# Hemodynamic Latency and Variability Following Neuronal Activation



# Types of Temporal Resolution

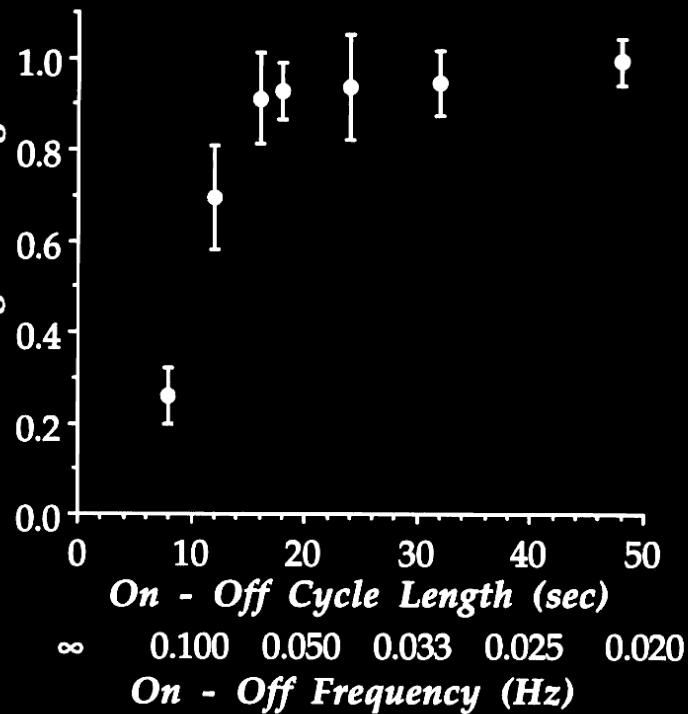
1. **Maximum on-off switching rate.**
2. **Minimum detectable activation duration.**
3. **Minimum detectable difference in activation duration or onset in same region.**
4. **Minimum detectable activation interval across separate brain regions.**
5. **Maximum image acquisition rate.**

MRI Signal



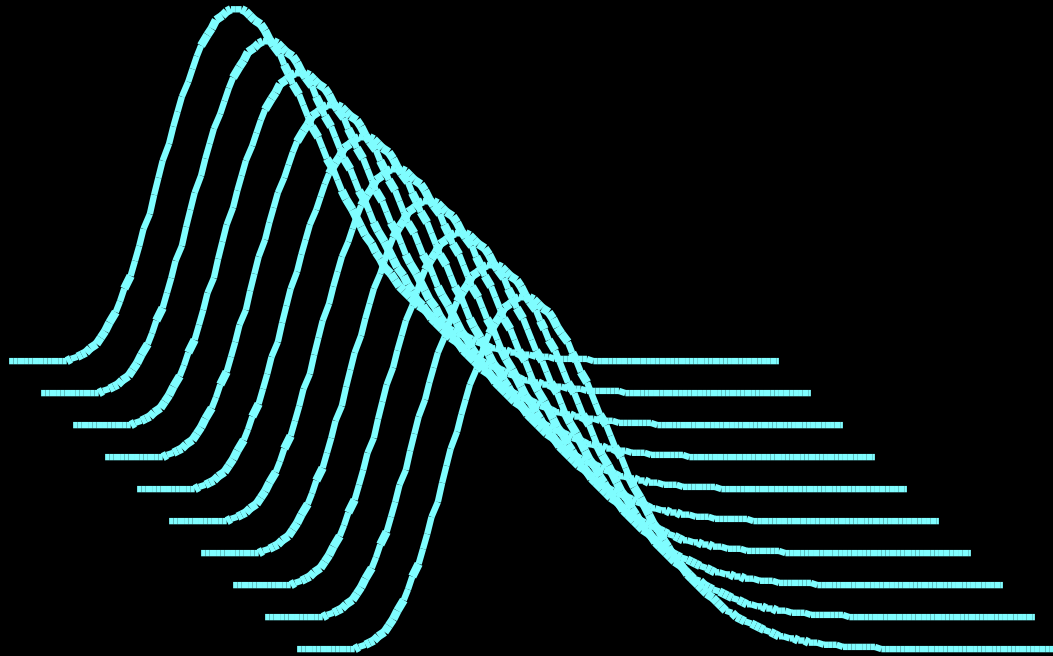
Time (seconds)

Relative Activation - Induced  
MR Signal Change

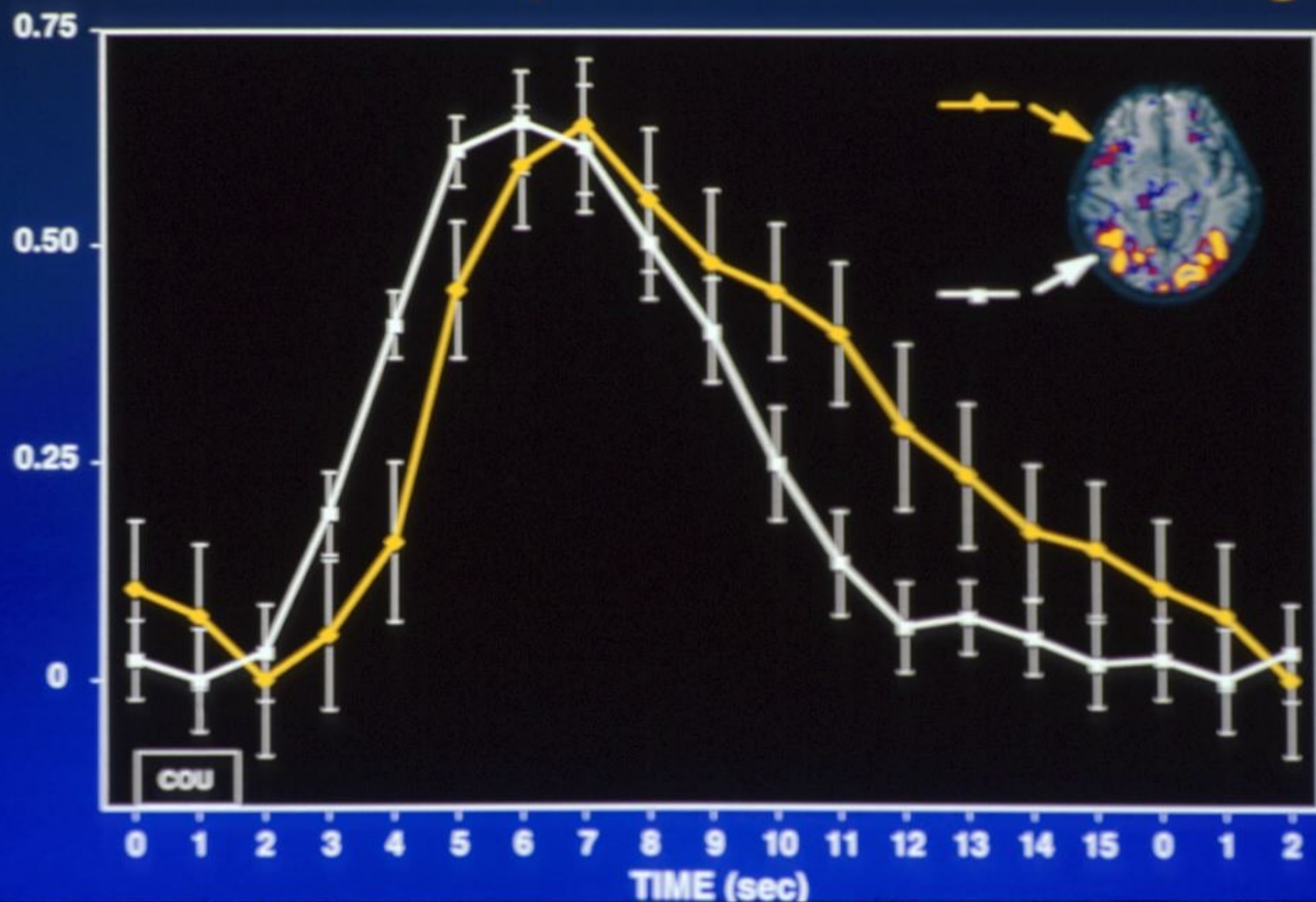


$$S = k t^{8.6} e^{-t/0.547}$$

Cohen, Neuroimage 6, 93-103 (1997)



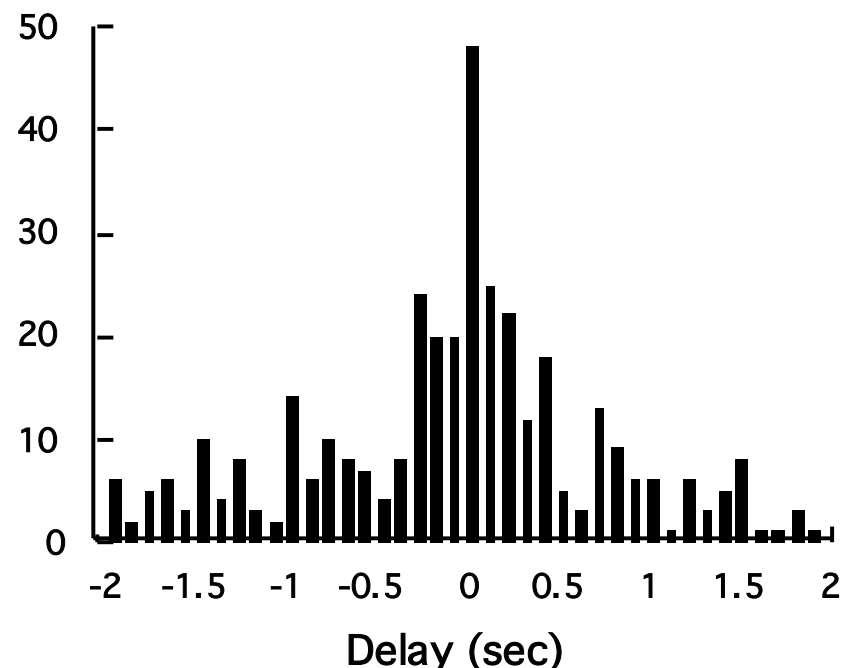
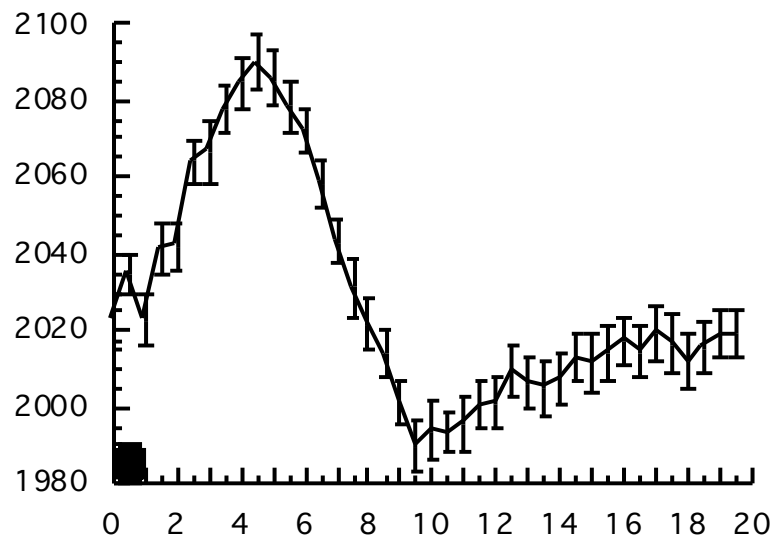
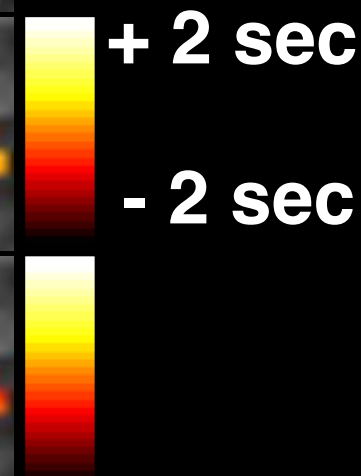
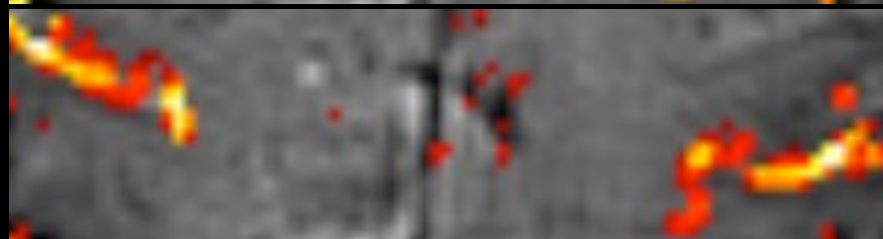
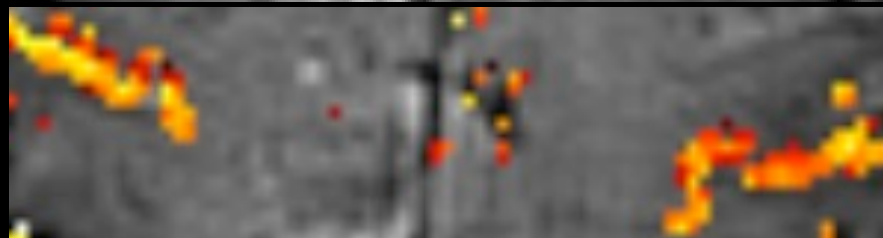
# Time Course Comparison Across Brain Regions





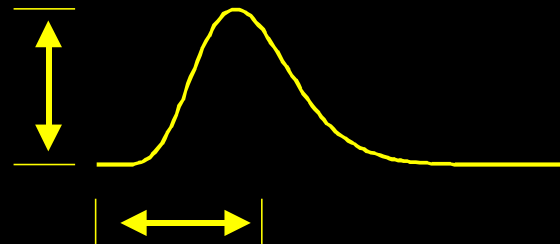
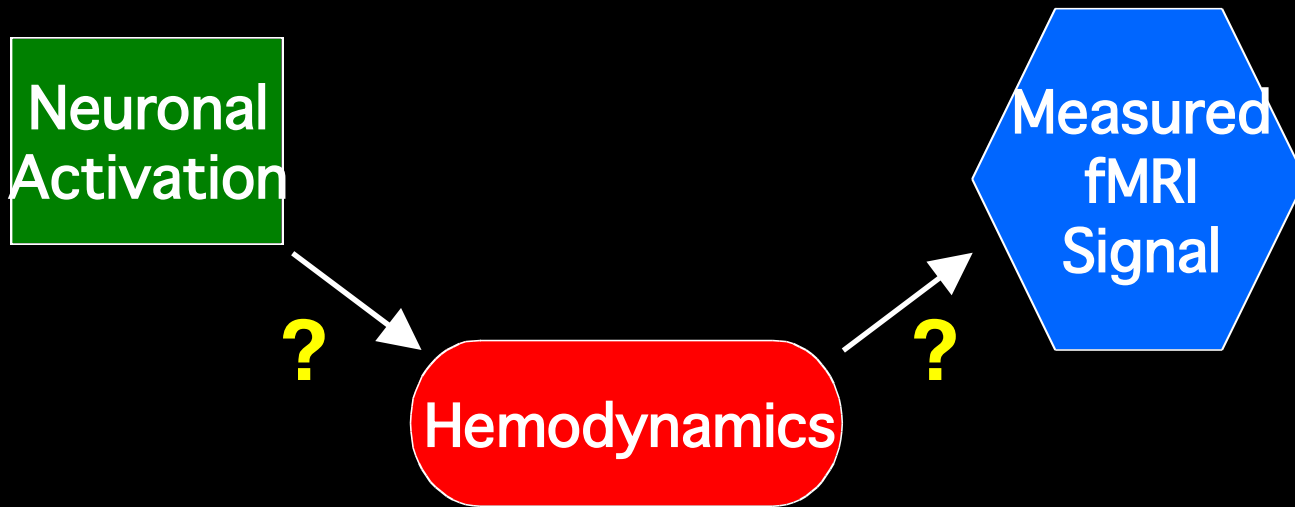
**Latency**

**Magnitude**



# Temporal Normalization

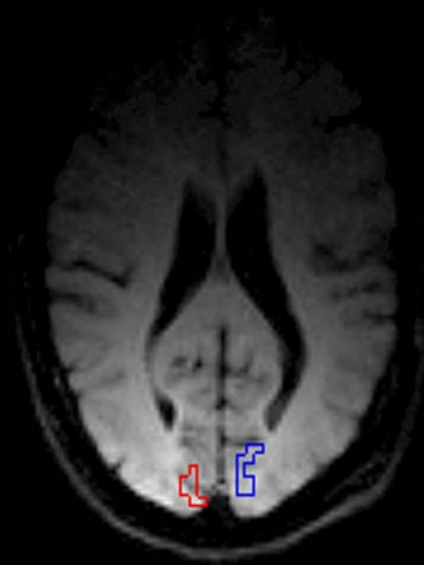
## Relative Timing



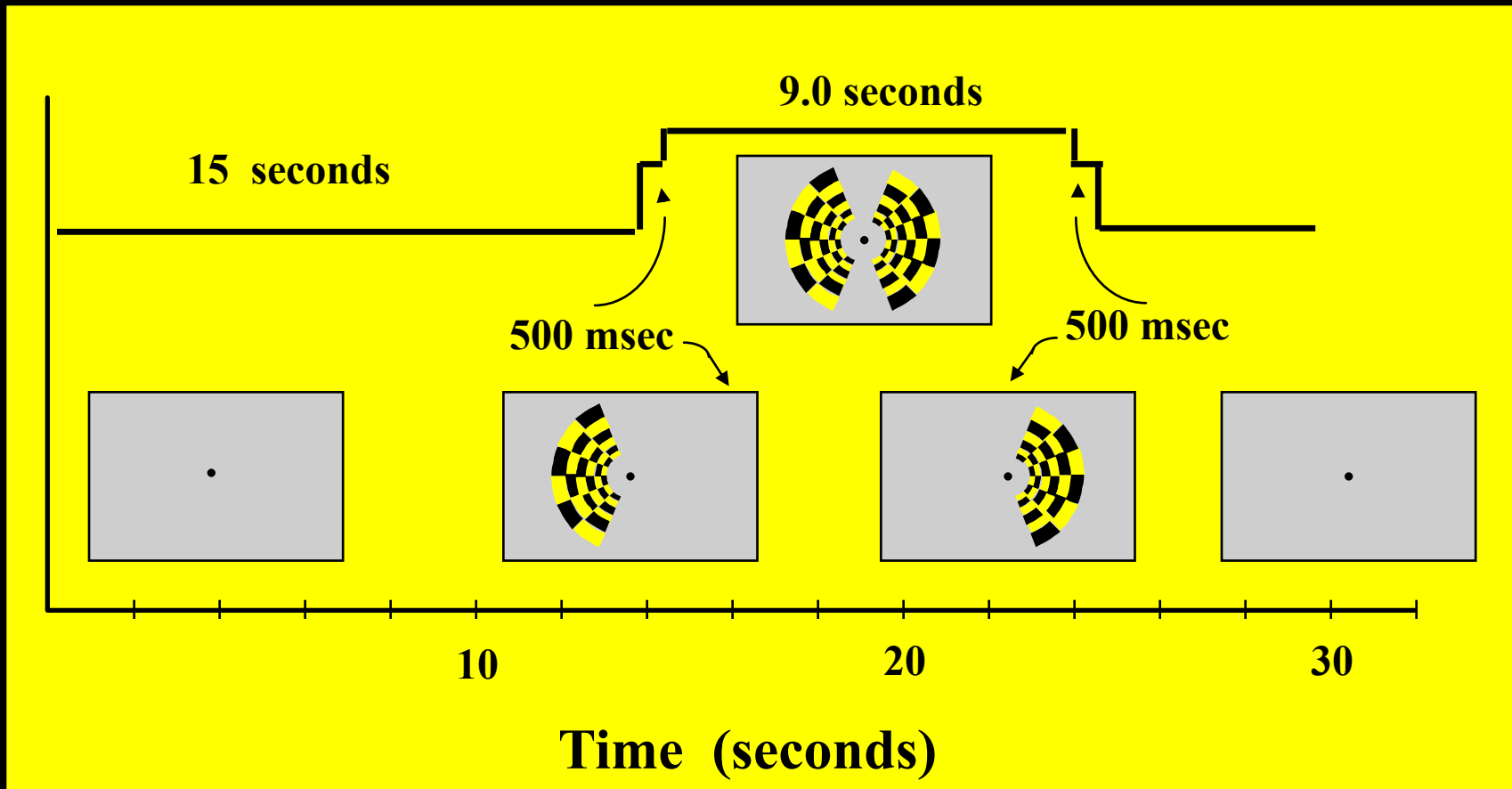
Physiologic Factors

# Regions of Interest Used for Hemi-Field Experiment

**Right  
Hemisphere**

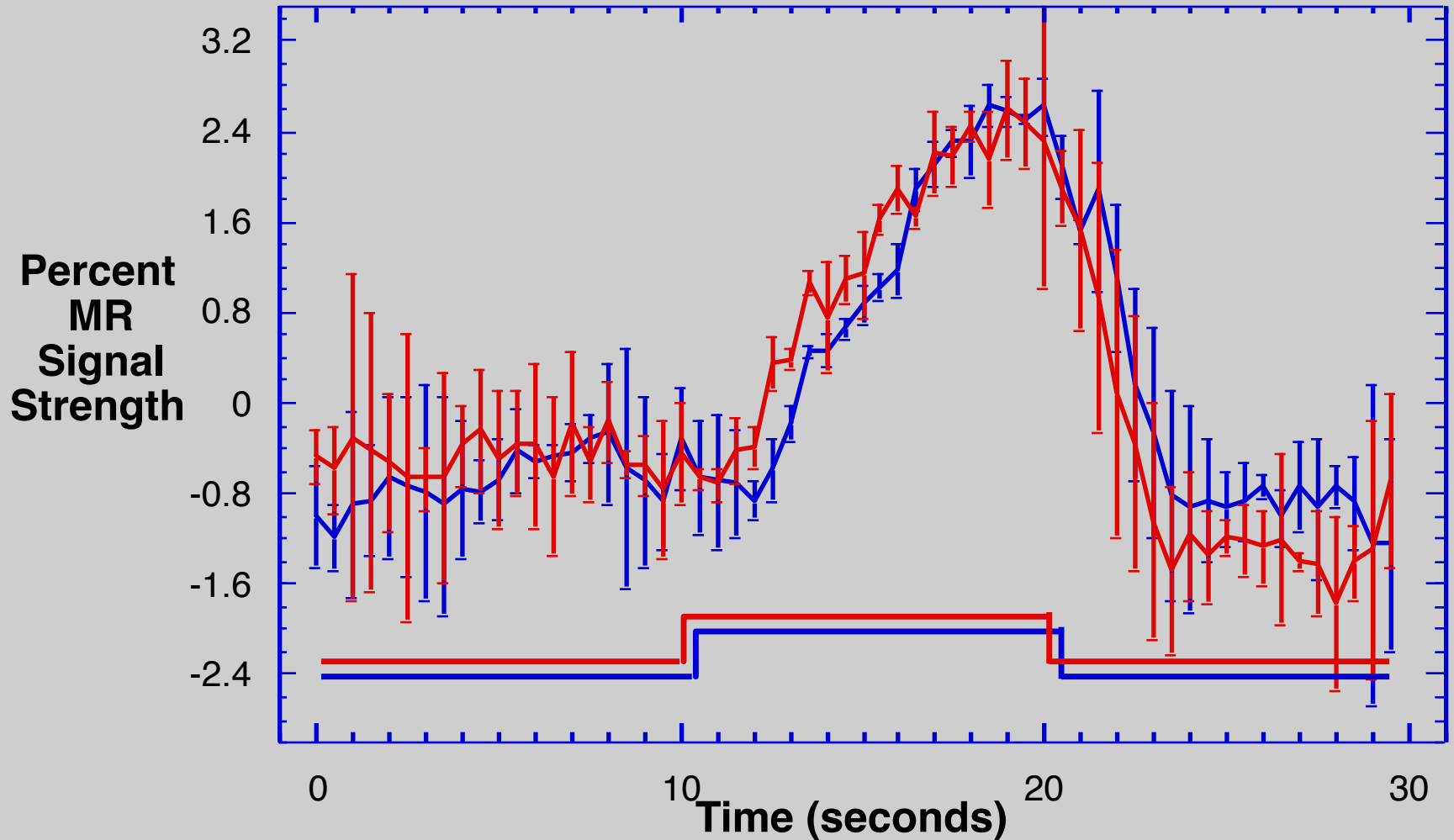


**Left  
Hemisphere**

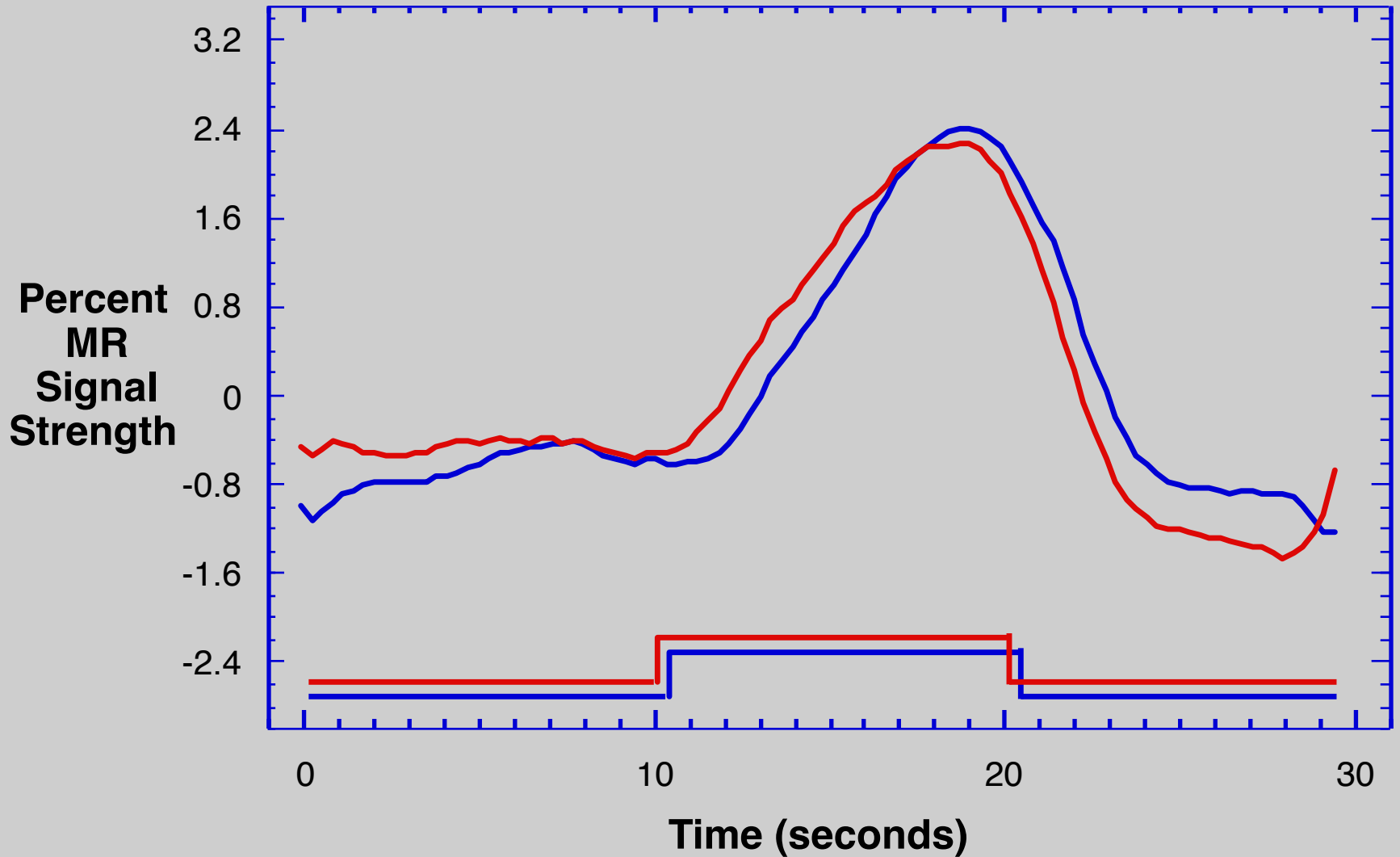


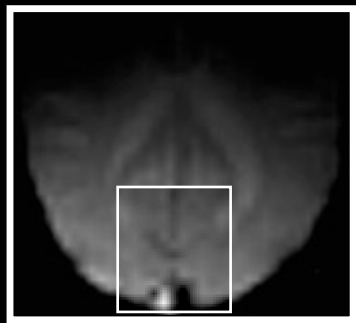
# Hemi-field with 500 msec asynchrony

Average of 6 runs    Standard Deviations Shown



# Average of 6 runs    Smoothed Data





500 ms



500 ms



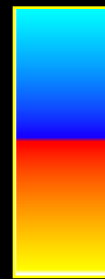
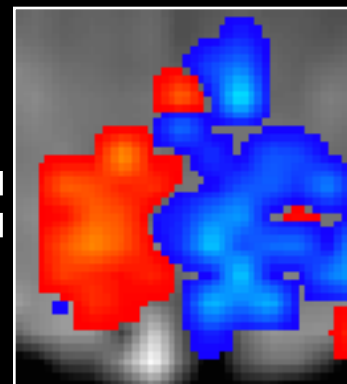
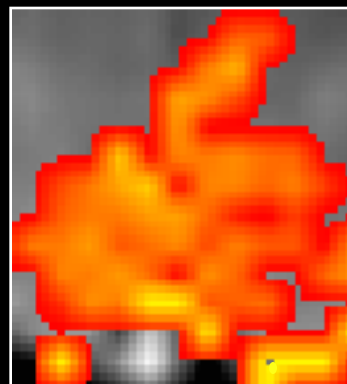
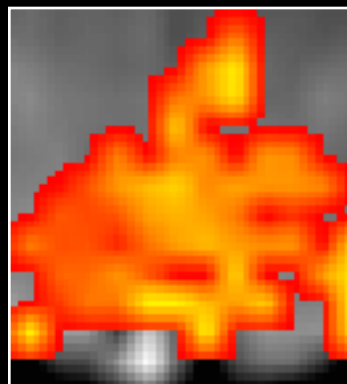
Right Hemifield

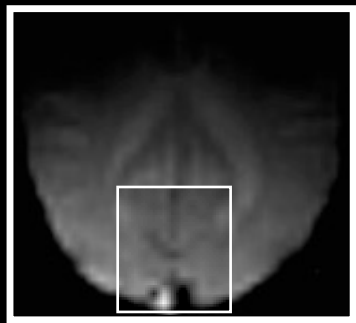
Left Hemifield

+ 2.5 s

0 s

- 2.5 s





250 ms



250 ms



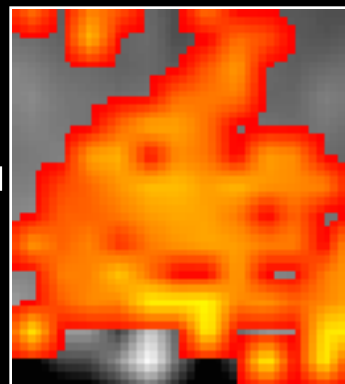
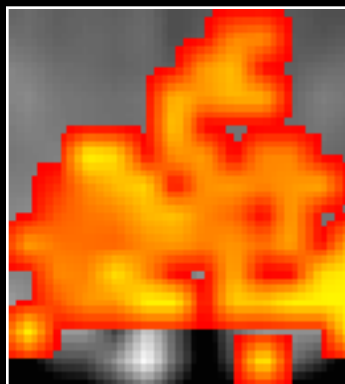
Right Hemifield

Left Hemifield

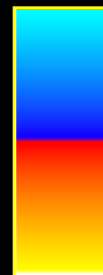
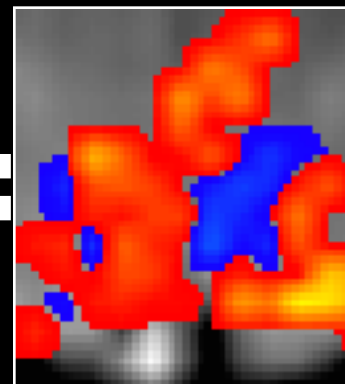
+ 2.5 s

0 s

- 2.5 s



=





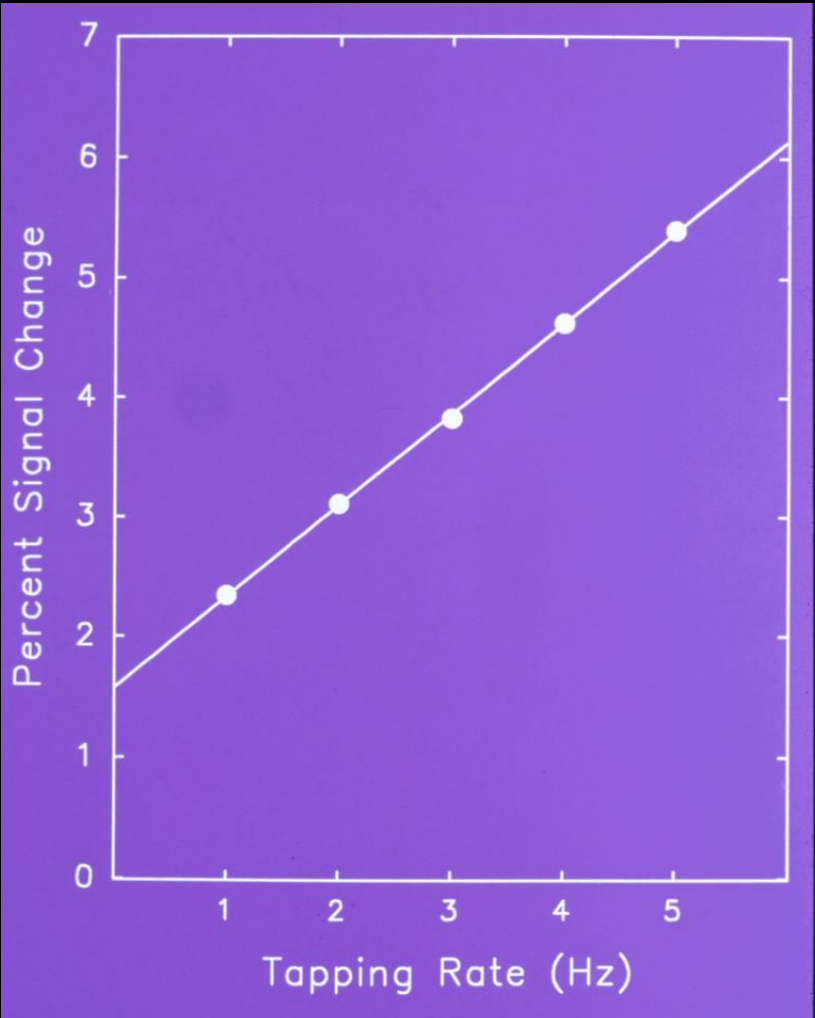
# How Much?

## Central Issue:

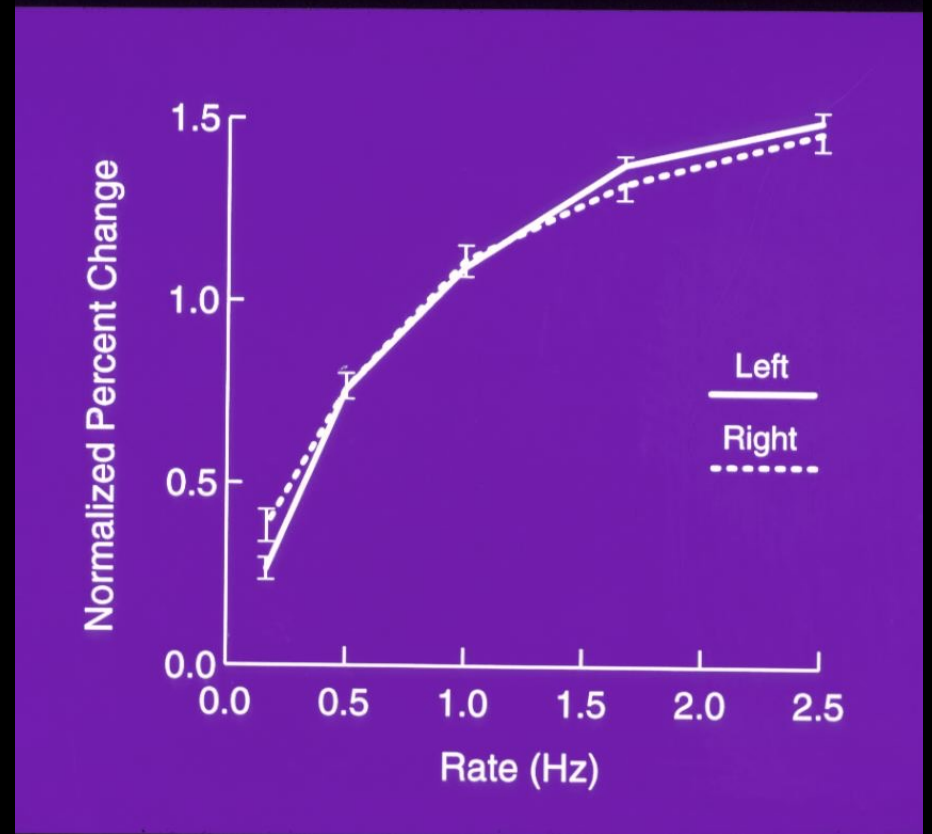
**Spatial and temporal neuronal firing integration  
to create an fMRI signal change.**

- is the hemodynamic response a linear system?*
- what is the dynamic range?*

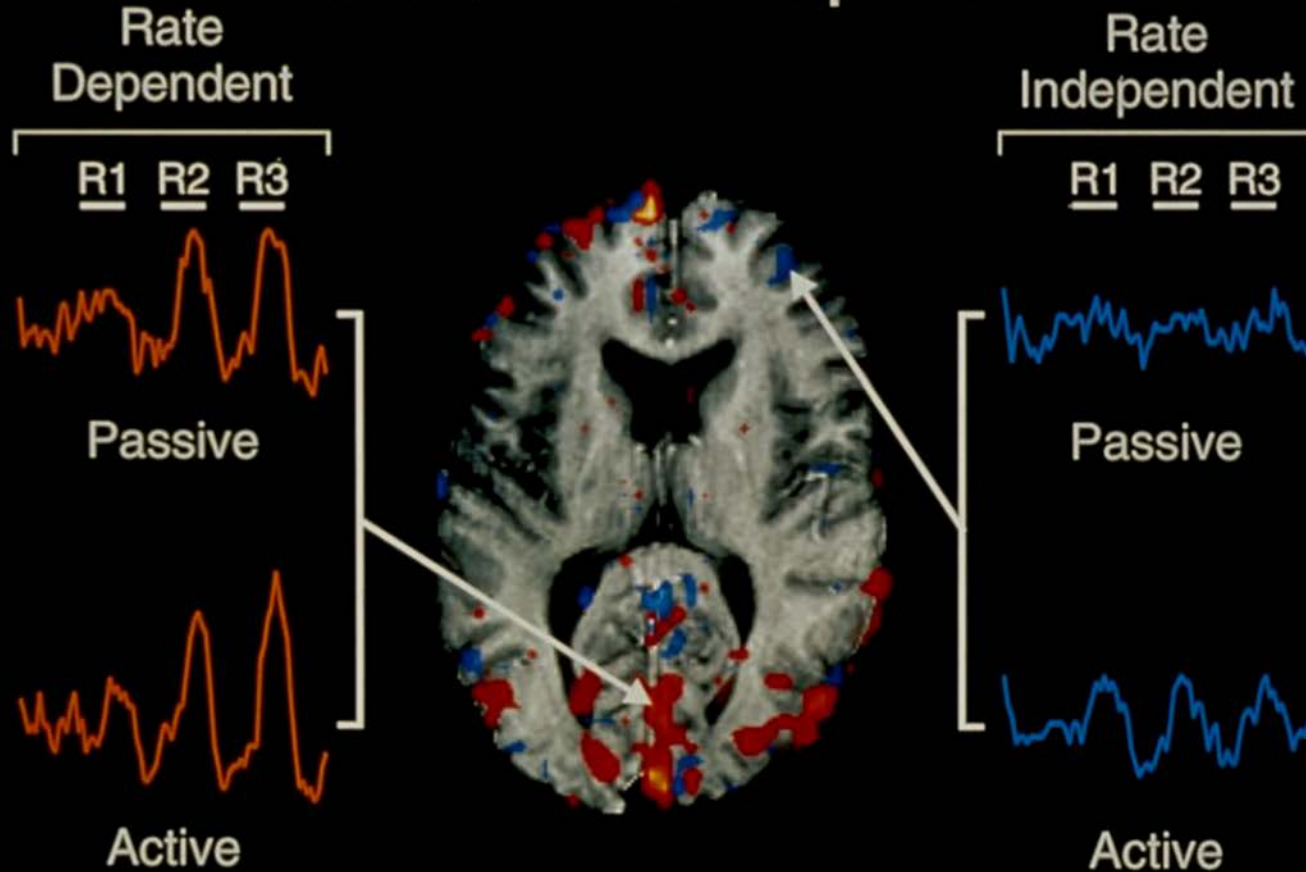
# Motor Cortex



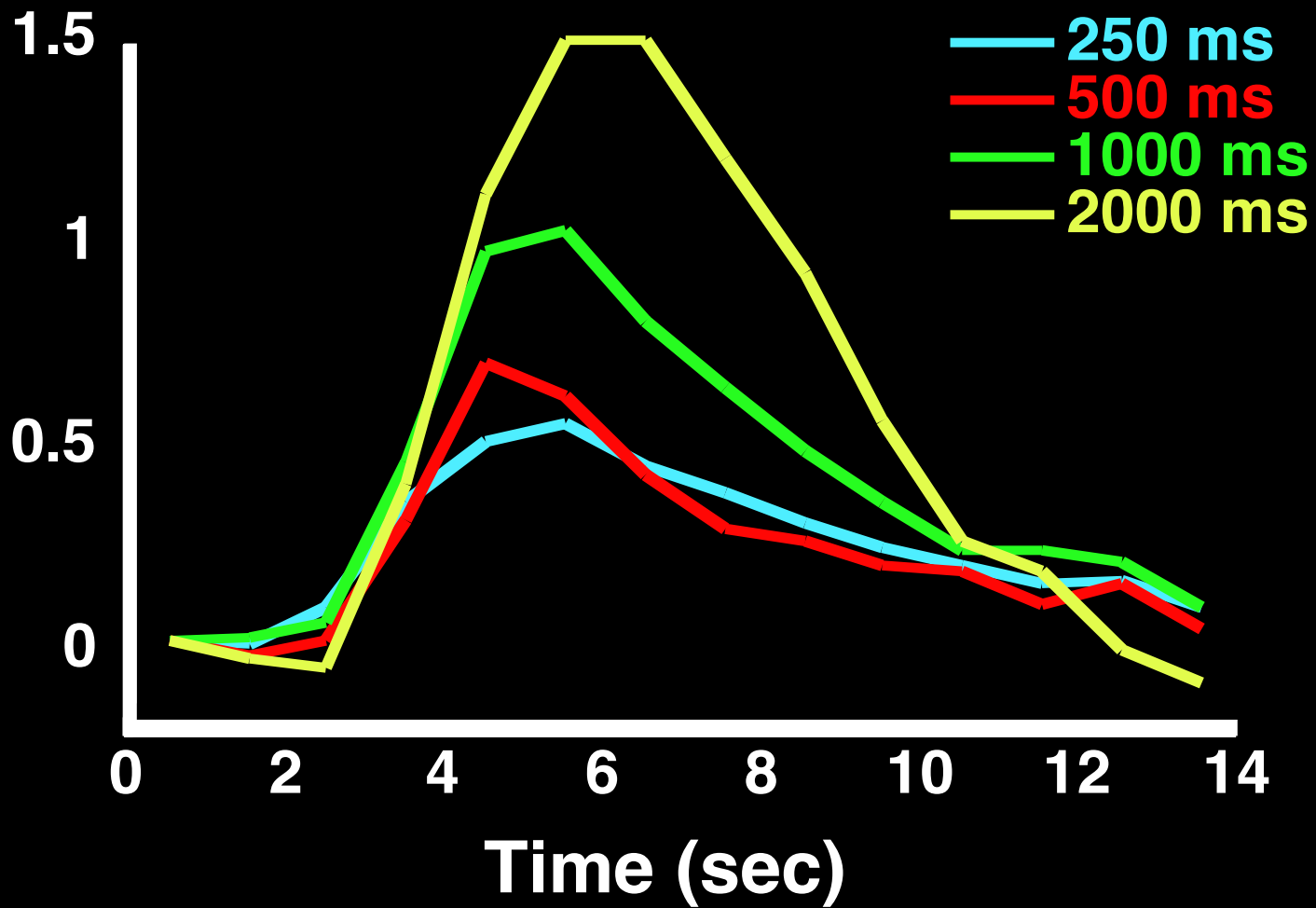
# Auditory Cortex

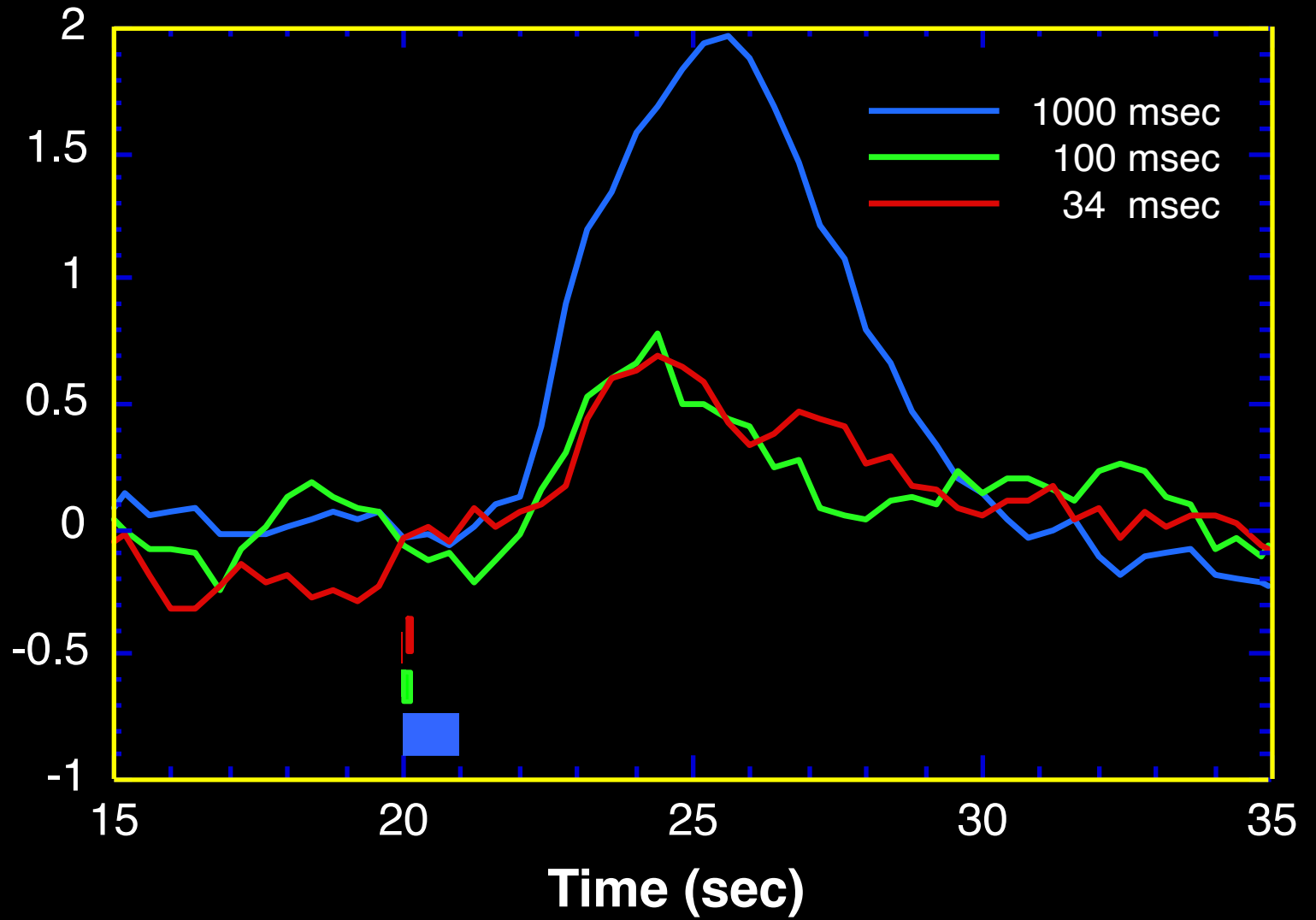


# Both the Task and Presentation Rate Affect the fMRI Response

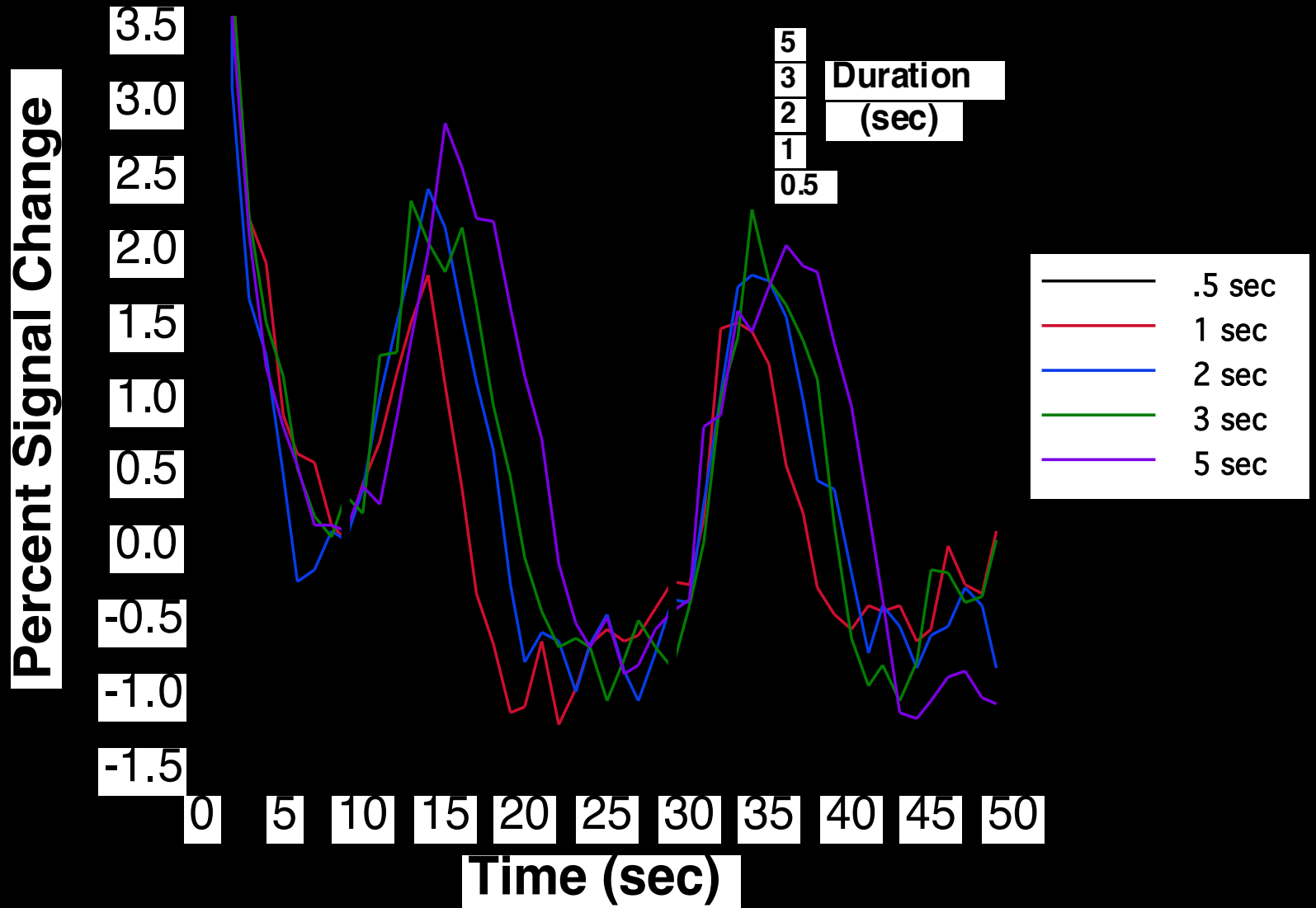


DeYoe et al.

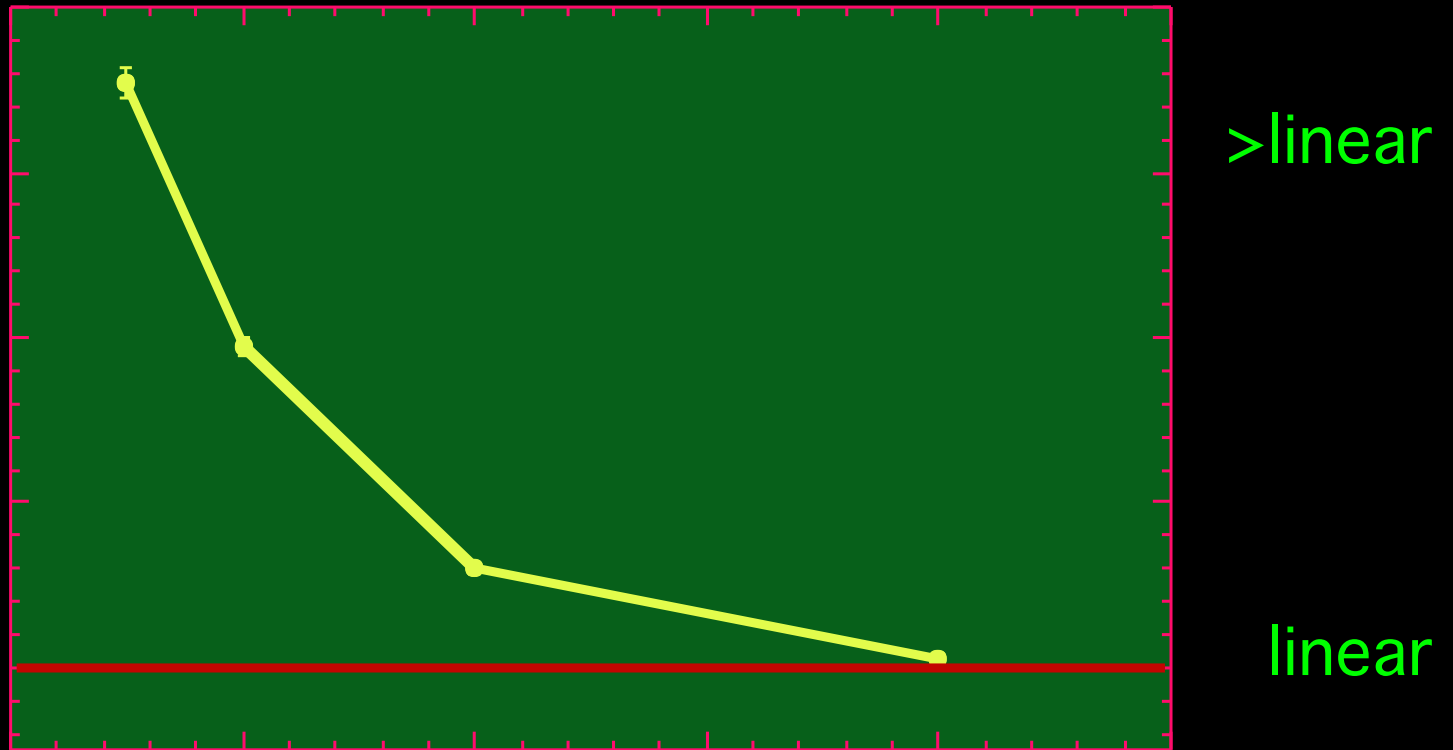




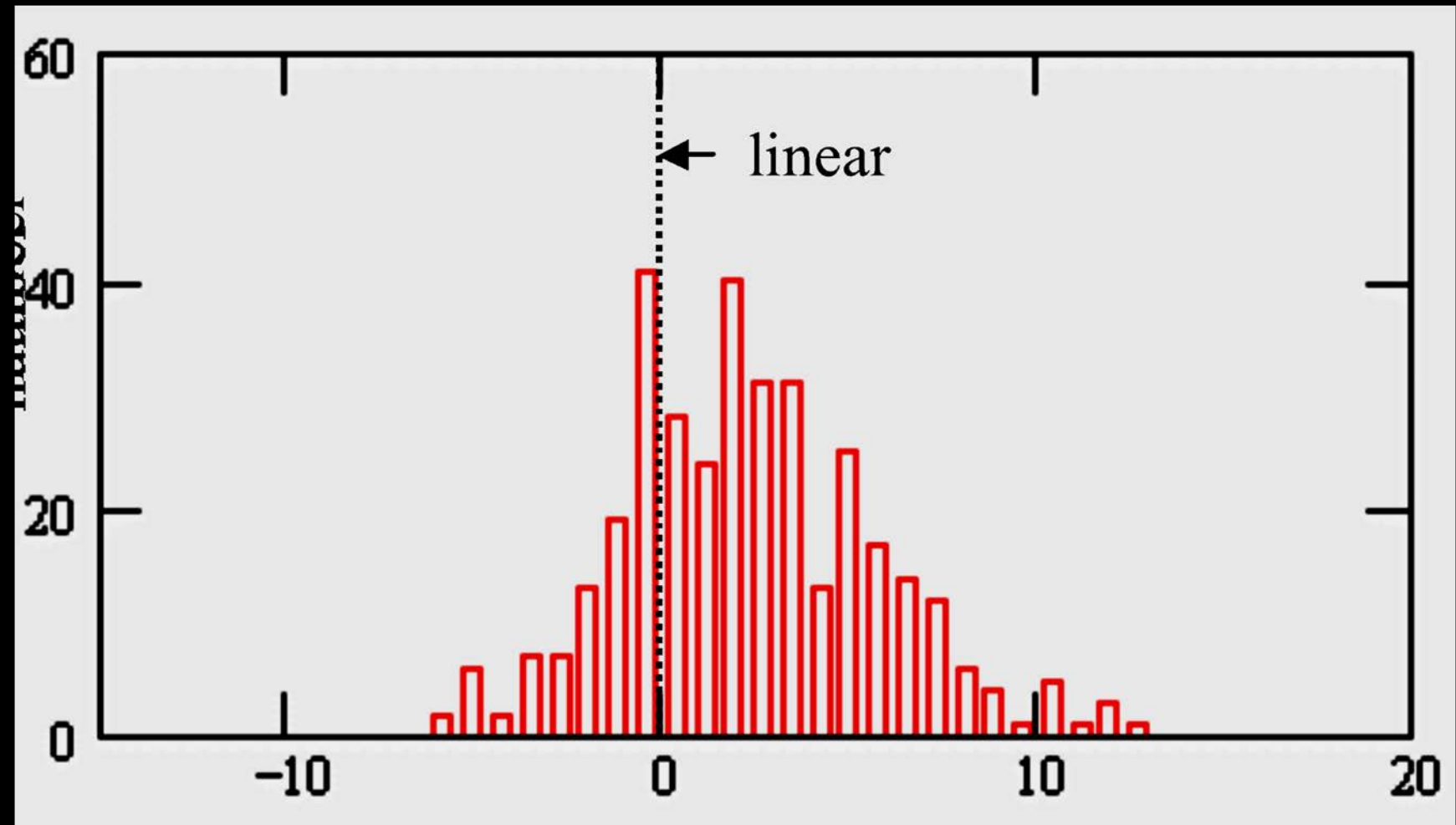
# Motor Cortex



# Stimulus - Duration Dependent Deviation from Linearity of the fMRI Response (Hemodynamic or Neuronal?)



# Spatial Distribution of the Hemodynamic Response Linearity

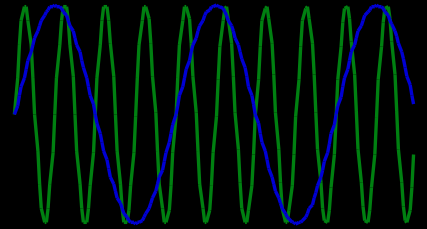




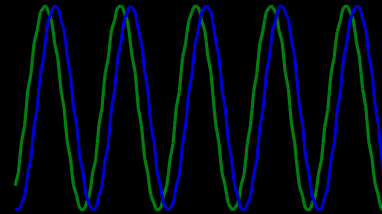
# Neuronal Activation Input Strategies

1. Block Design

2. Frequency Encoding

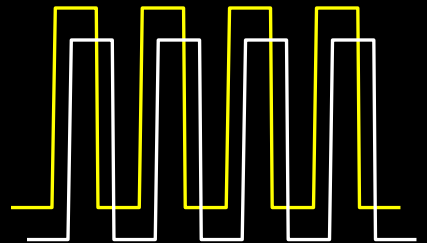


3. Phase Encoding



4. Single Event

5. Orthogonal Block Design



6. Free behavior Design.

## Ultimate Limits?

Spatial: 0.5 mm

Temporal: 100 ms

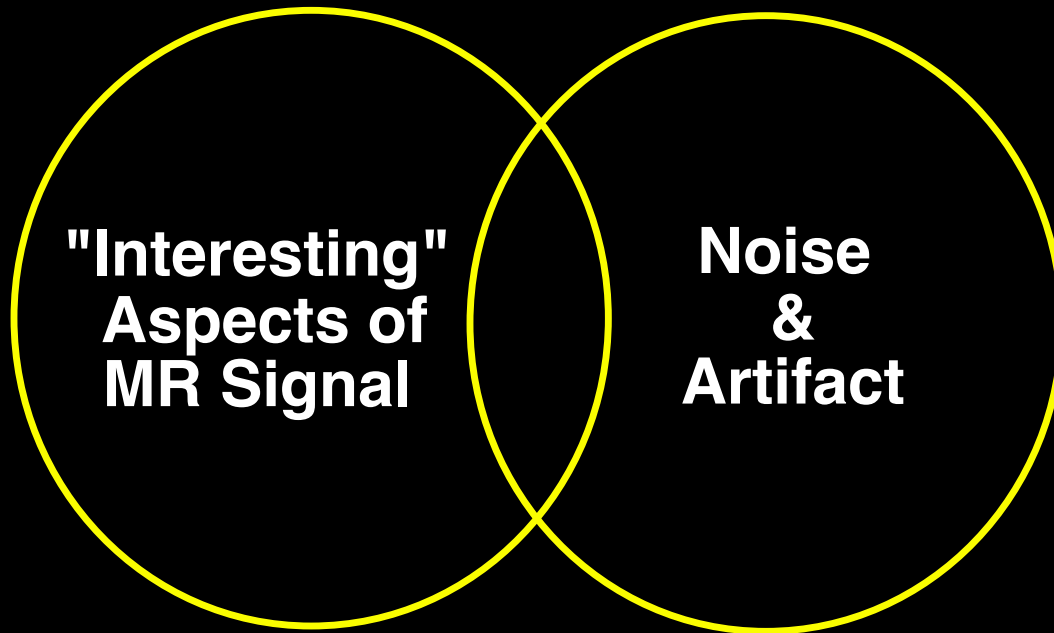
Interpretability...too early to tell, but hopeful

# Neuronal Input Strategies

Peter A. Bandettini, Ph.D

Unit on Functional Imaging Methods  
Laboratory of Brain and Cognition  
National Institute of Mental Health

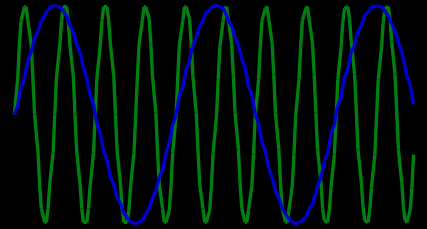
# How to get the brain to do what we want it to do in the context of an fMRI experiment?



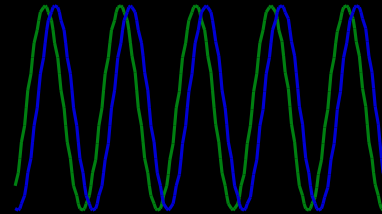
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1. Block Design

2. Frequency Encoding

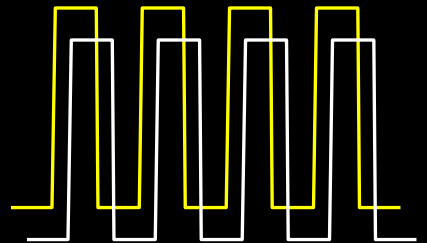


3. Phase Encoding



4. Single Event

5. Orthogonal Block Design

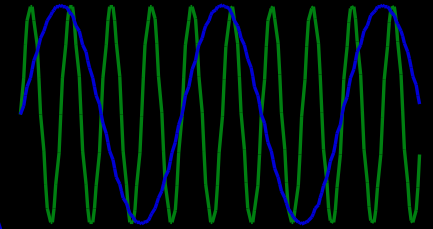


6. Free behavior Design.

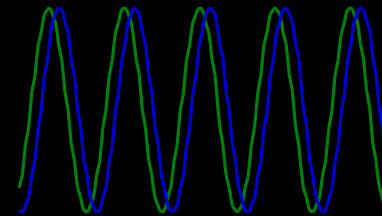
# Neuronal Activation Input Strategies

## 1. Block Design

## 2. Frequency Encoding

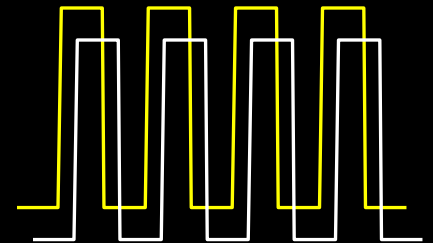


## 3. Phase Encoding



## 4. Single Event

## 5. Orthogonal Block Design

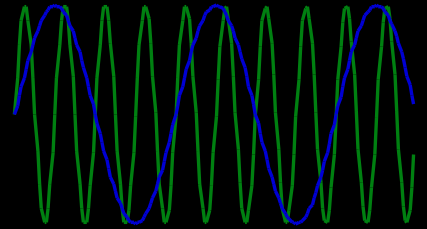


## 6. Free behavior Design.

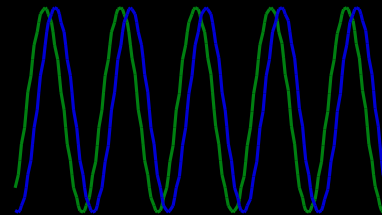
# Neuronal Activation Input Strategies

1. Block Design

2. Frequency Encoding

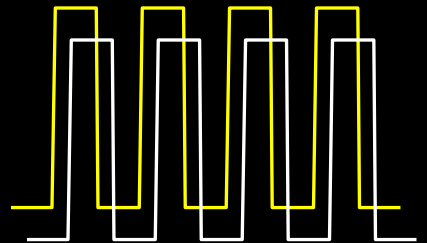


3. Phase Encoding

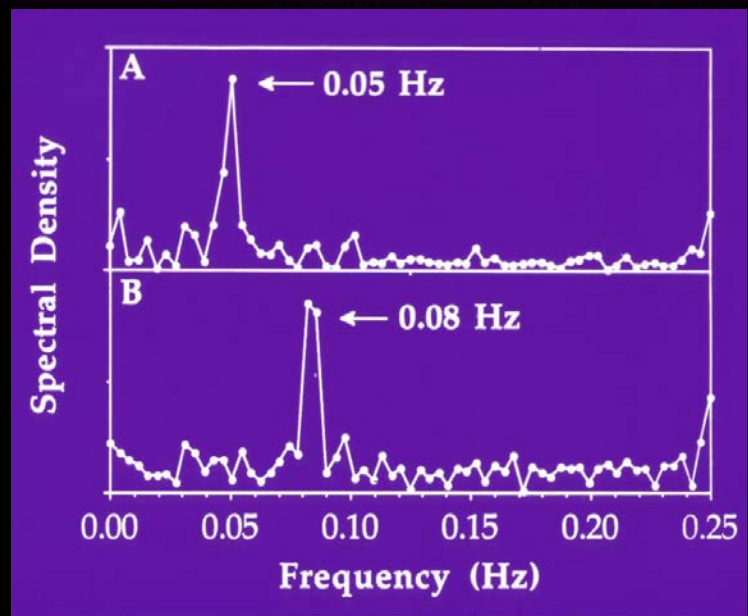
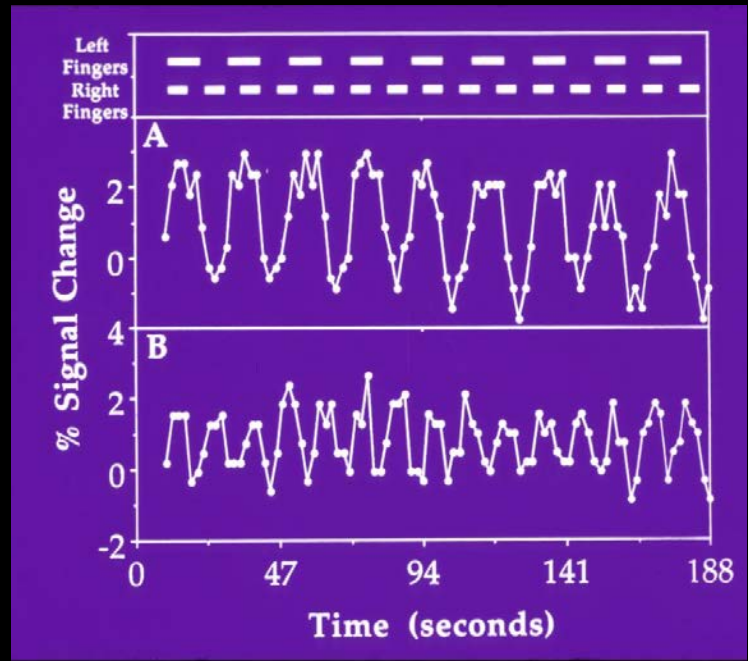
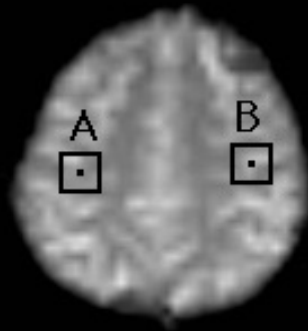


4. Single Event

5. Orthogonal Block Design



6. Free behavior Design.

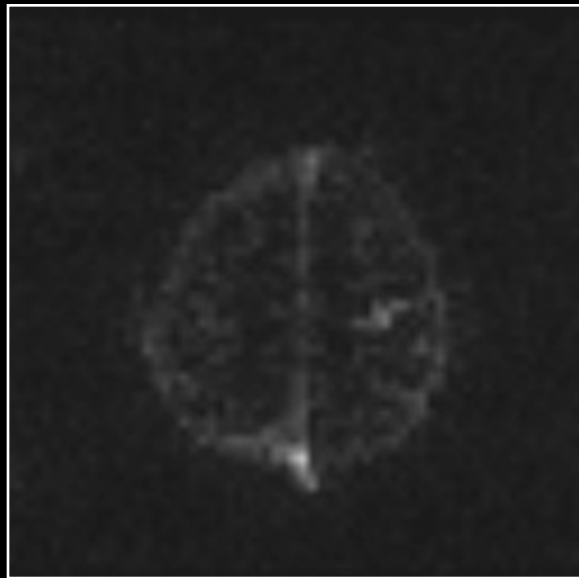




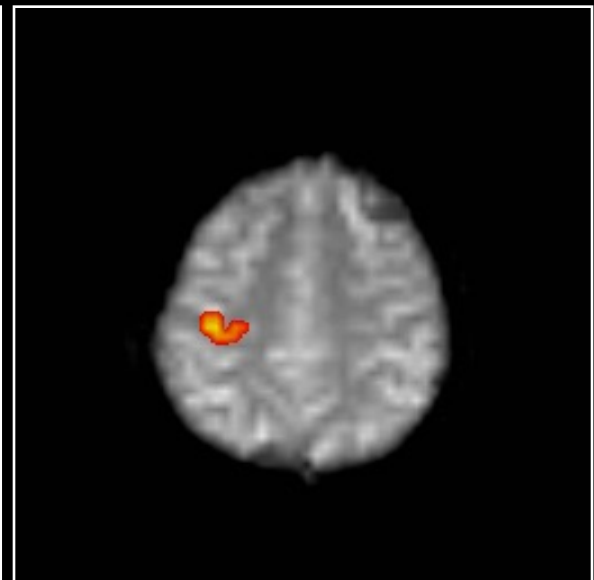
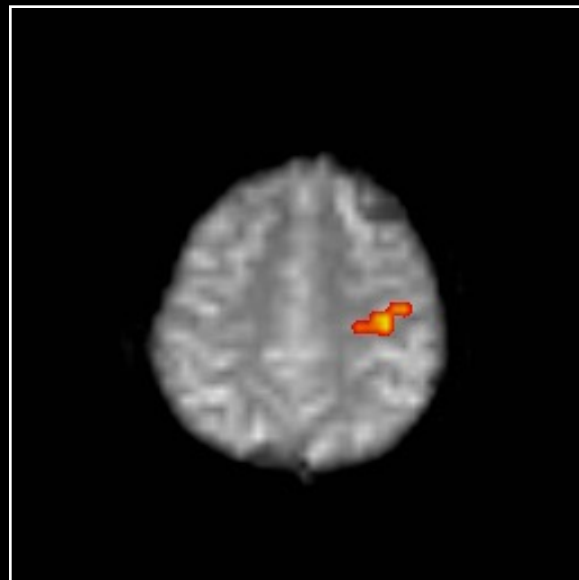
**0.08 Hz**

**0.05 Hz**

**spectral  
density**



**c.c. > 0.5  
with spectra**



# Neuronal Activation Input Strategies

1. Block Design

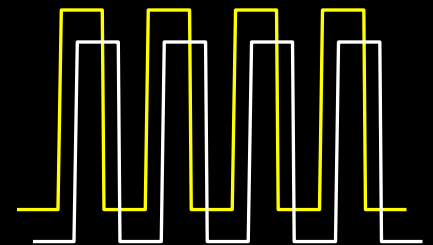
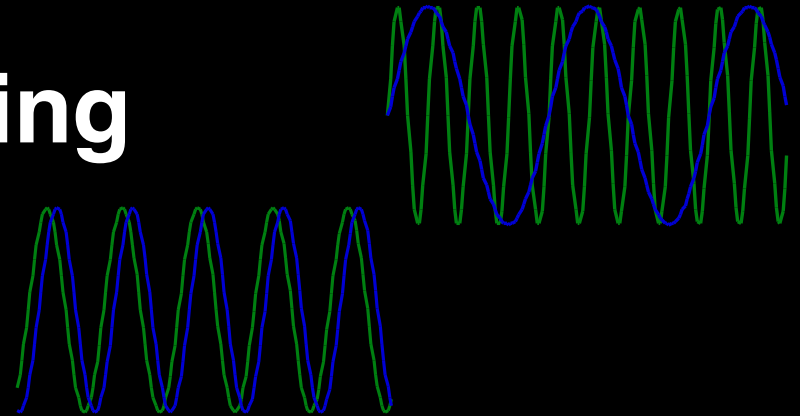
2. Frequency Encoding

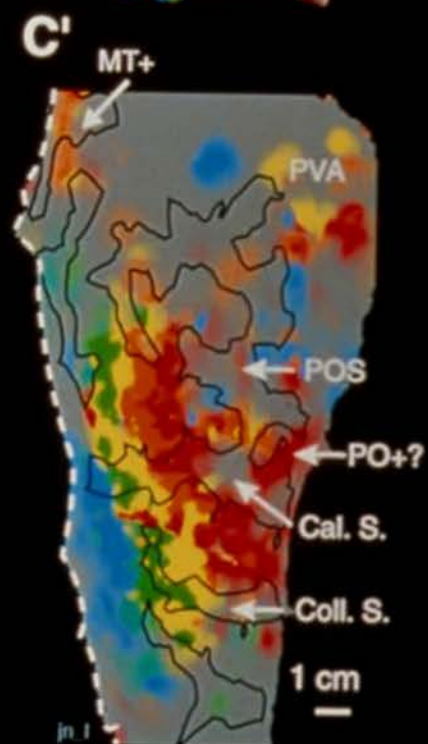
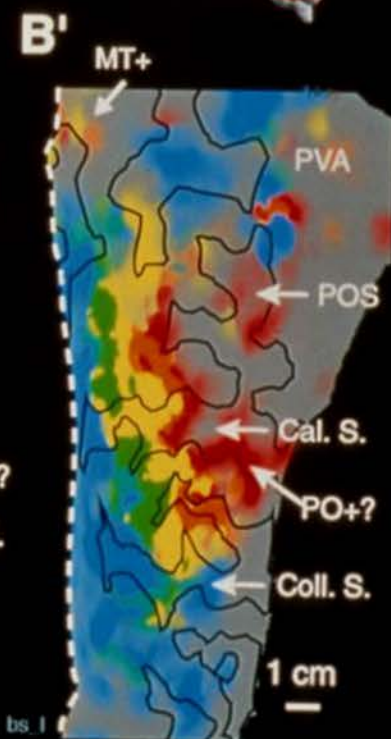
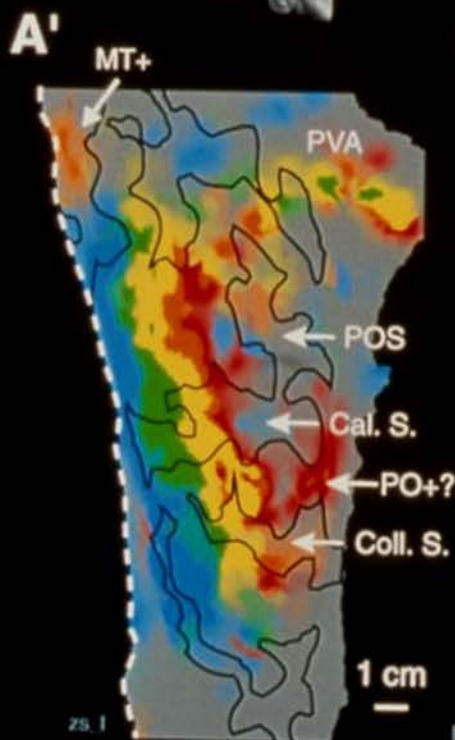
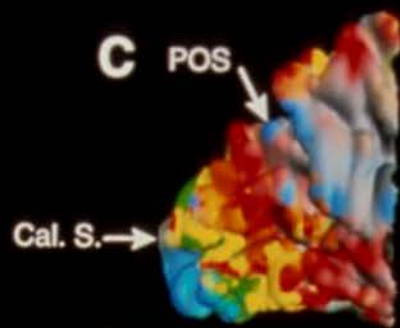
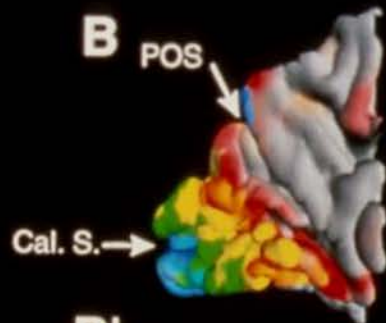
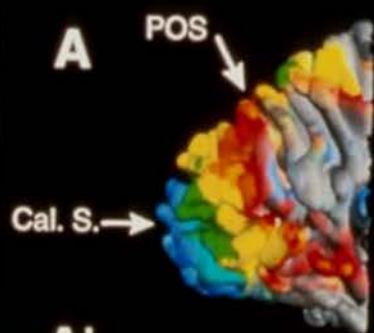
3. Phase Encoding

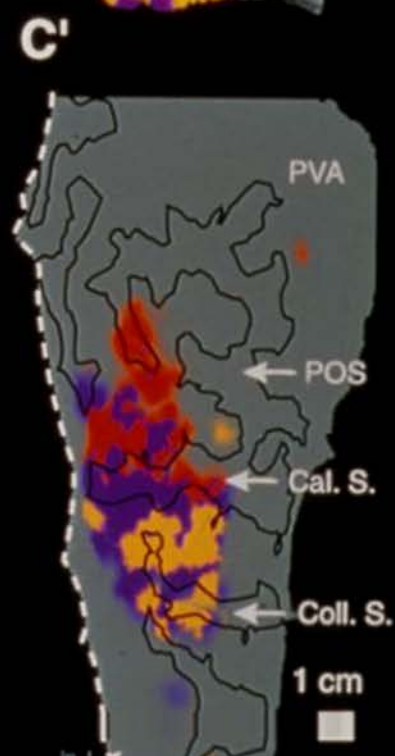
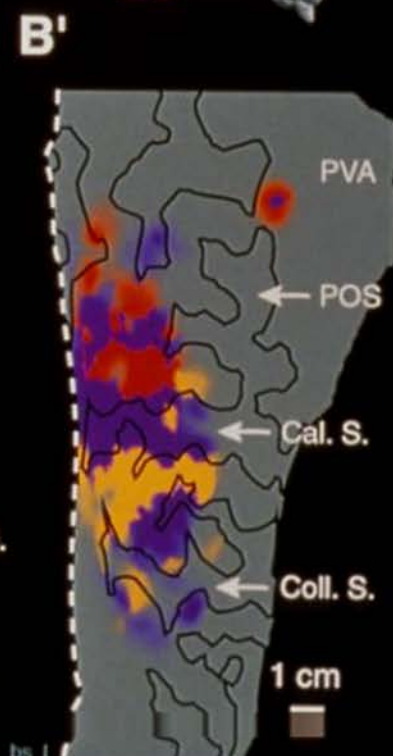
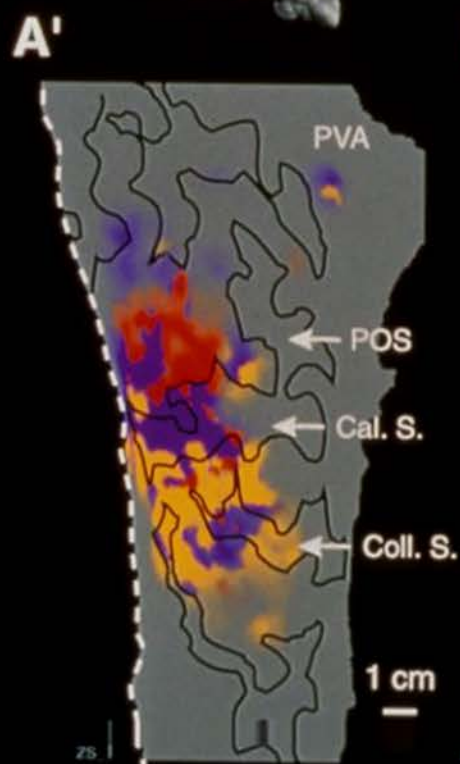
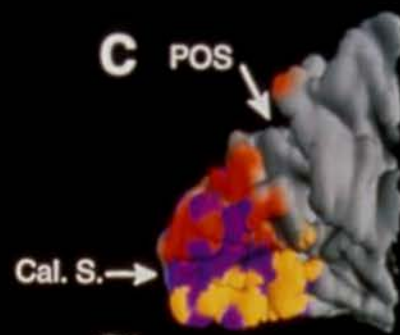
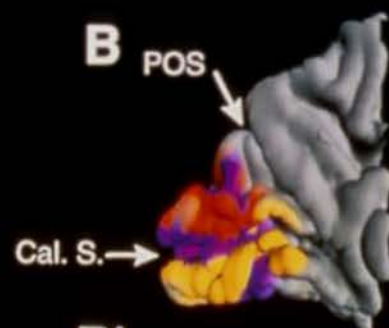
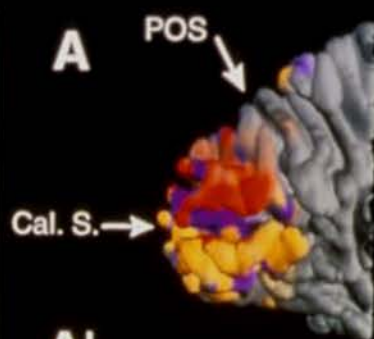
4. Single Event

5. Orthogonal Block Design

6. Free behavior Design.



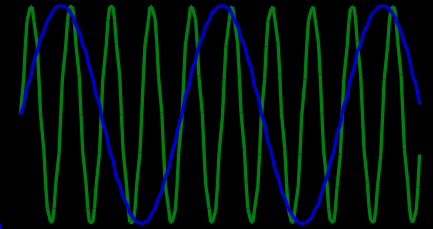




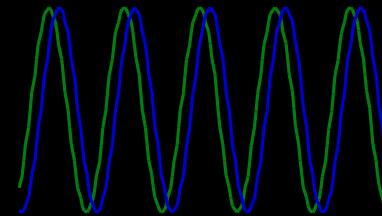
# Neuronal Activation Input Strategies

1. Block Design

2. Frequency Encoding

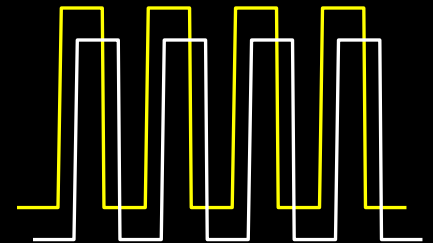


3. Phase Encoding



4. Single Event

5. Orthogonal Block Design

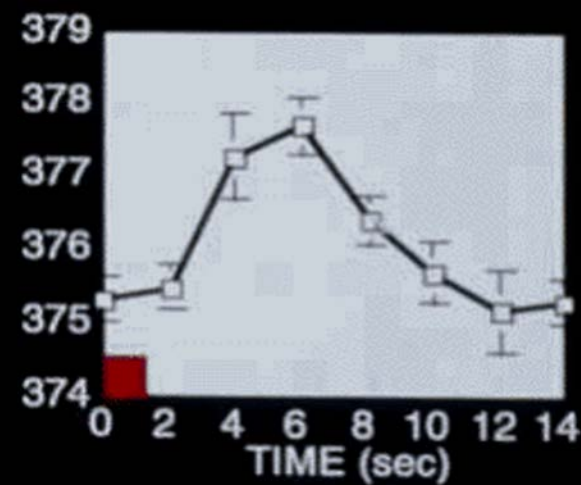
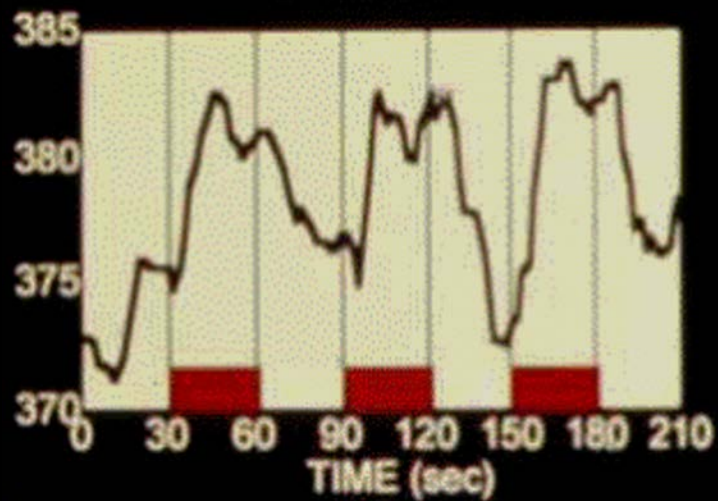
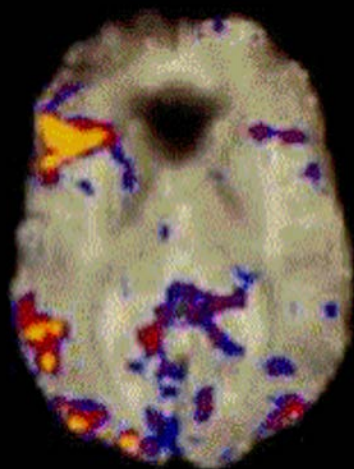


6. Free behavior Design.

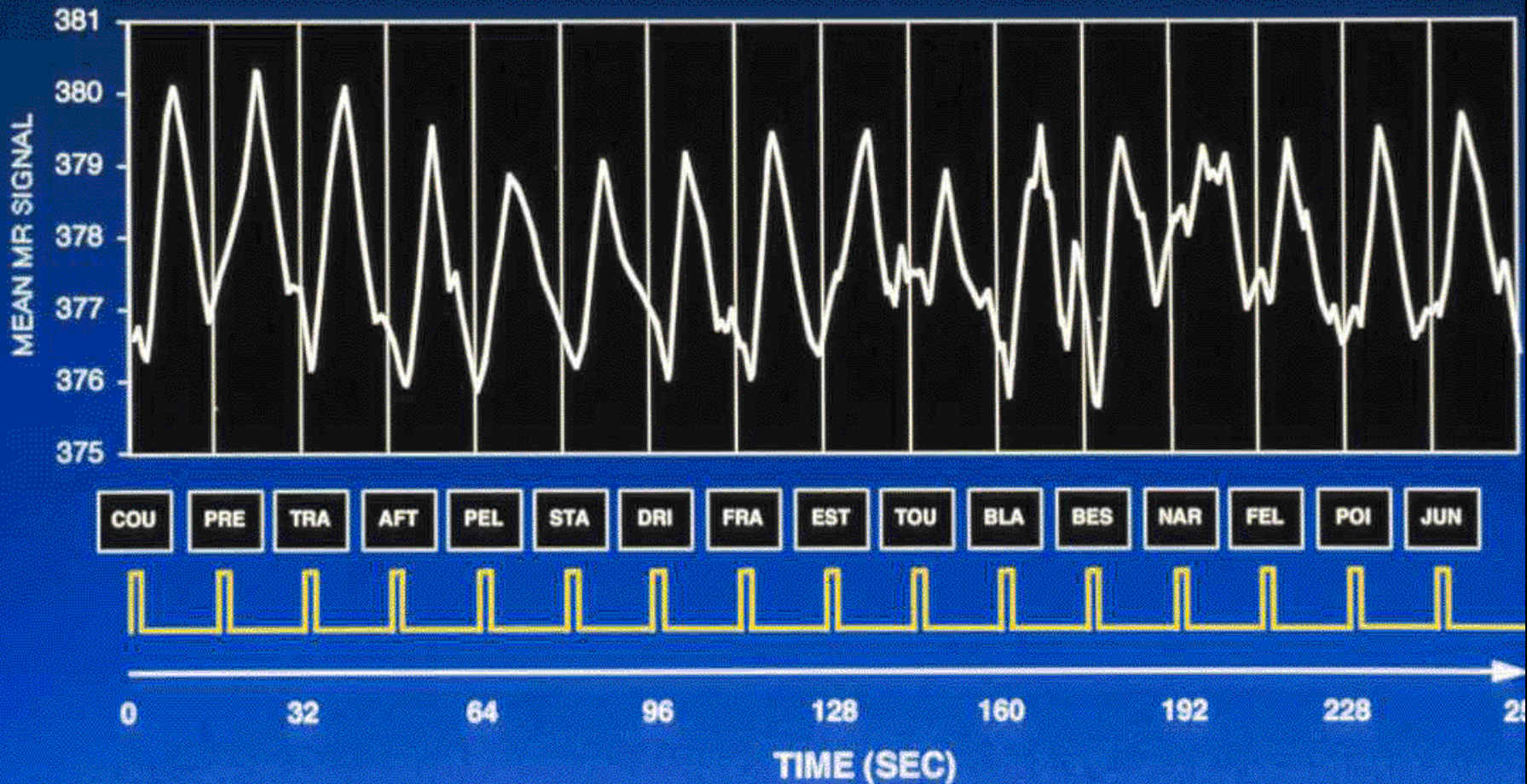
**BLOCKED:**



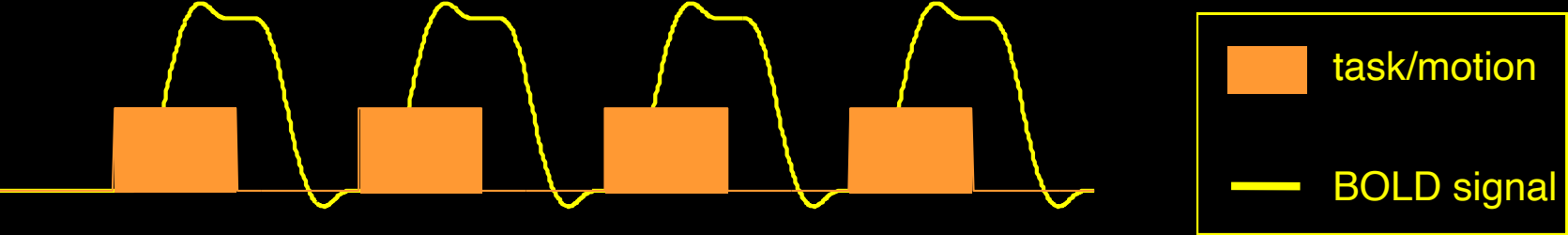
**SINGLE TRIAL:**



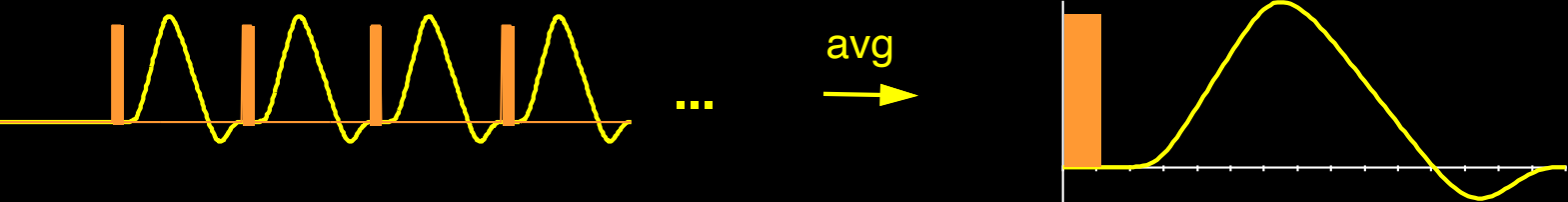
# "Single-Trial" Response Across an Averaged Data Set



Block-trial

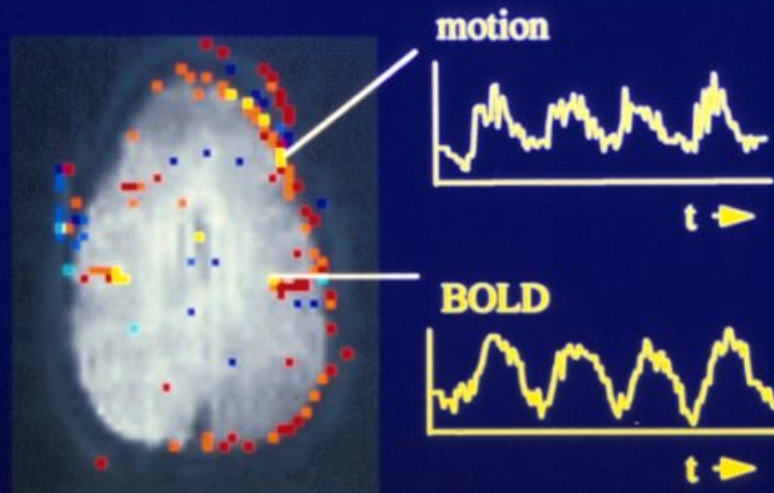


Single-trial (brief stimulus)



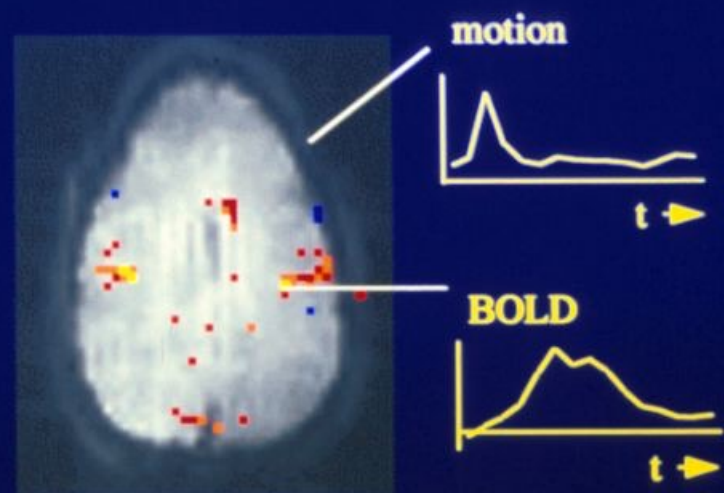


## Motion-Decoupled fMRI: Functional MRI during of overt word production



### “block-trial” paradigm

Motion induced signal changes resemble functional (BOLD) signal changes

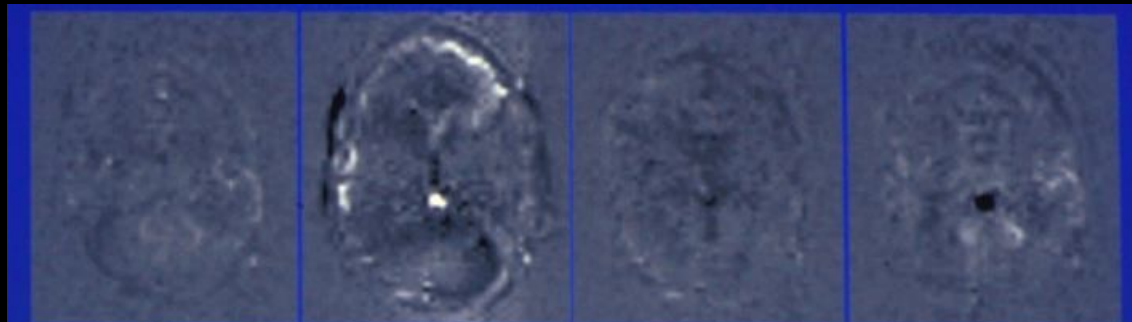


### “single-trial” paradigm

Motion induced and BOLD signal changes are separated in time

*R.M. Birn, et al.*

# Overt Word Production



2

3

4

5



6

7

8

9



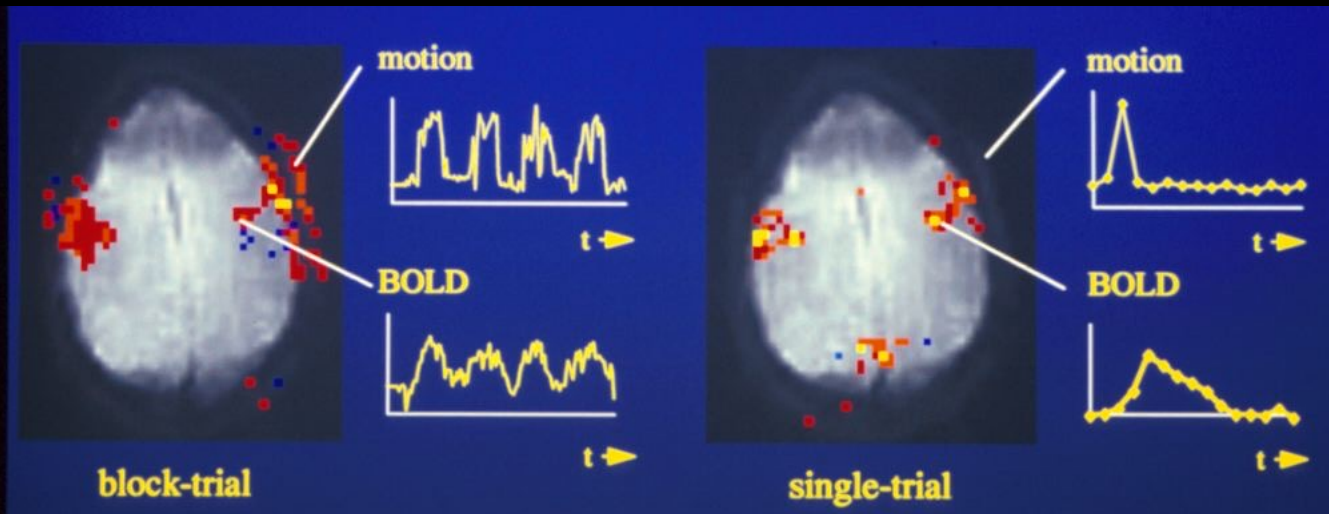
10

11

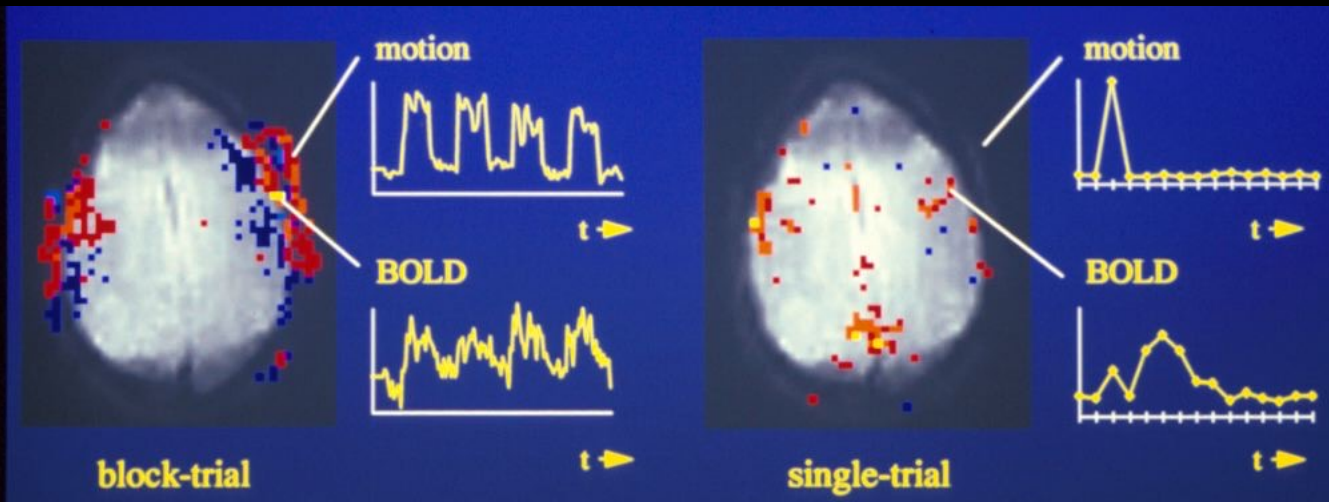
12

13

# Tongue Movement



# Jaw Clenching



# Event-Related fMRI Questions:

**1. What is the optimal ISI?**

**2. How does functional contrast compare with “blocked” timing?**

*(Is the hemodynamic response a linear system?)*

# Contrast in Event Related fMRI

## Dependency on:

- **Inter-stimulus Interval (ISI)**
- **Stimulus Duration (SD)**

## Comparison with:

- **Blocked strategies**
- **Synthesized responses created using convolution**

# Issues:

## 1. ISI Issue

- Shorter ISI provides more trials per unit time.
- Shorter ISI causes overlap in hemodynamic response, reducing dynamic range.

## 2. Contrast Issue

- Does signal behave like a linear system with brief SD?

# Experimental Methods

- Two imaging planes containing motor and visual cortex.
- EPI, 3.75 x 3.75 x 7 mm, TE = 40 ms, TR = 1 sec.
- Time series duration = 360 images (6 minutes).
- 10 series compared:
  - Single Trial: SD = 2, ISI = 24, 20, 16, 12, 10, 8, 6, 4, 2.
  - Blocked: SD = 20, ISI = 20.
- Subjects instructed to tap fingers when GRASS goggles were on.

# Visual Cortex



**ISI, SD**

**ISI, SD**

**20, 20**

**8, 2**

**12, 2**

**6, 2**

**10, 2**

**4, 2**

**2, 2**



# Motor Cortex



**ISI, SD**

**ISI, SD**

**20, 20**

**8, 2**

**12, 2**

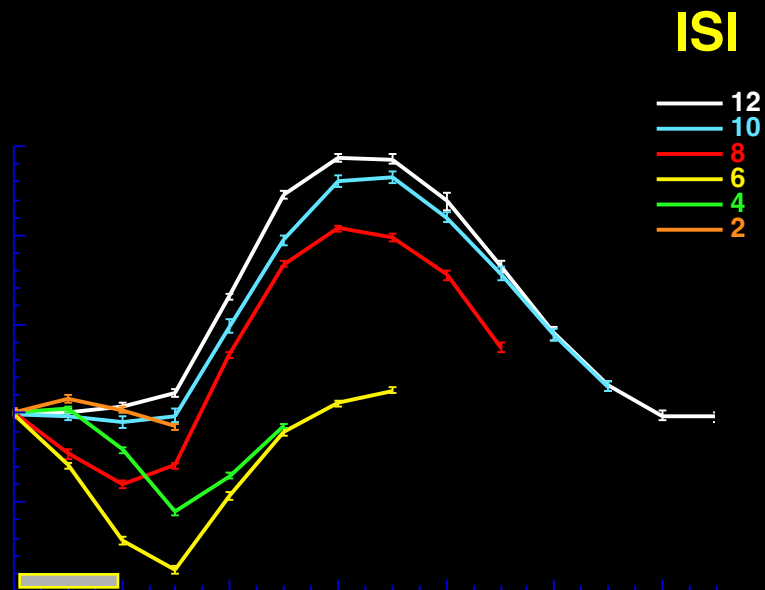
**6, 2**

**10, 2**

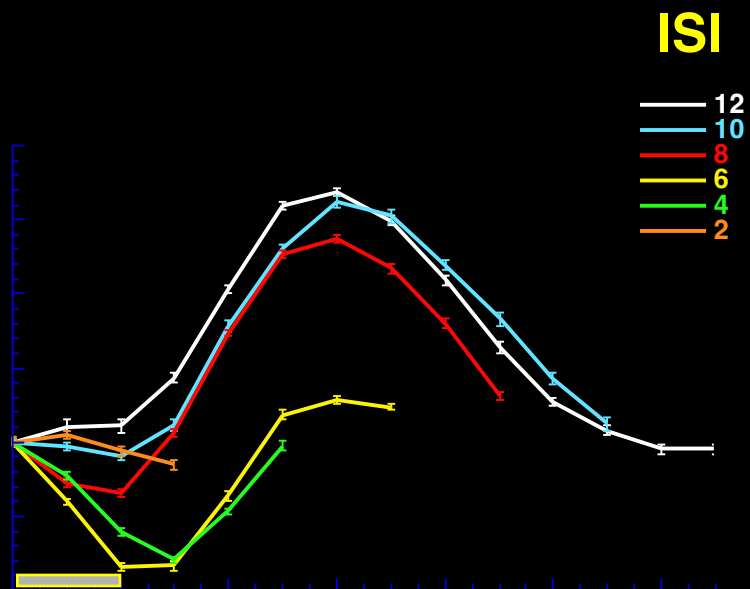
**4, 2**

**2, 2**

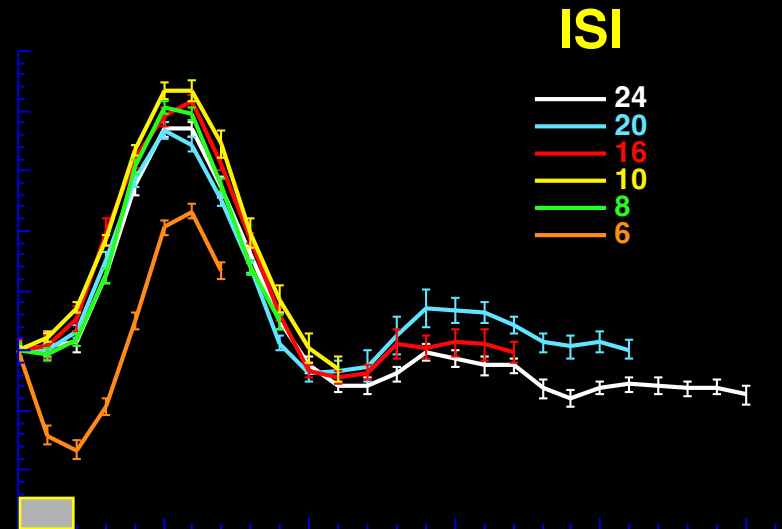
# Motor Cortex



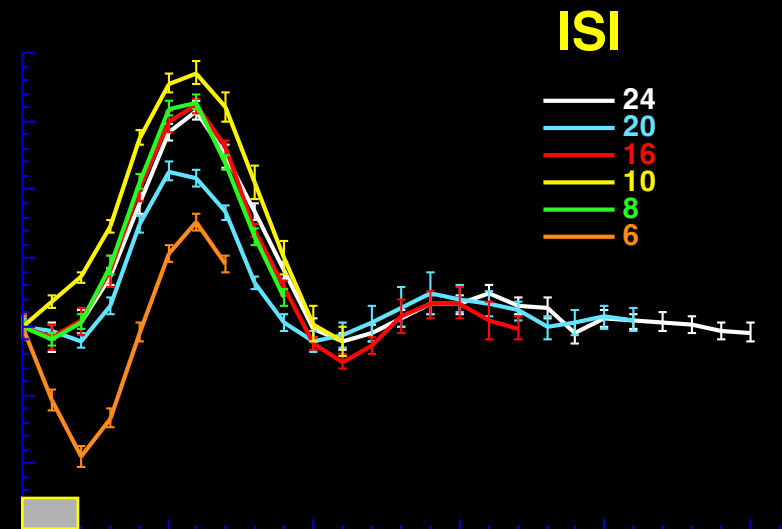
# Visual Cortex



# Motor Cortex



# Visual Cortex



# Contrast to Noise Images

( ISI, SD )

20, 20

12, 2

10, 2

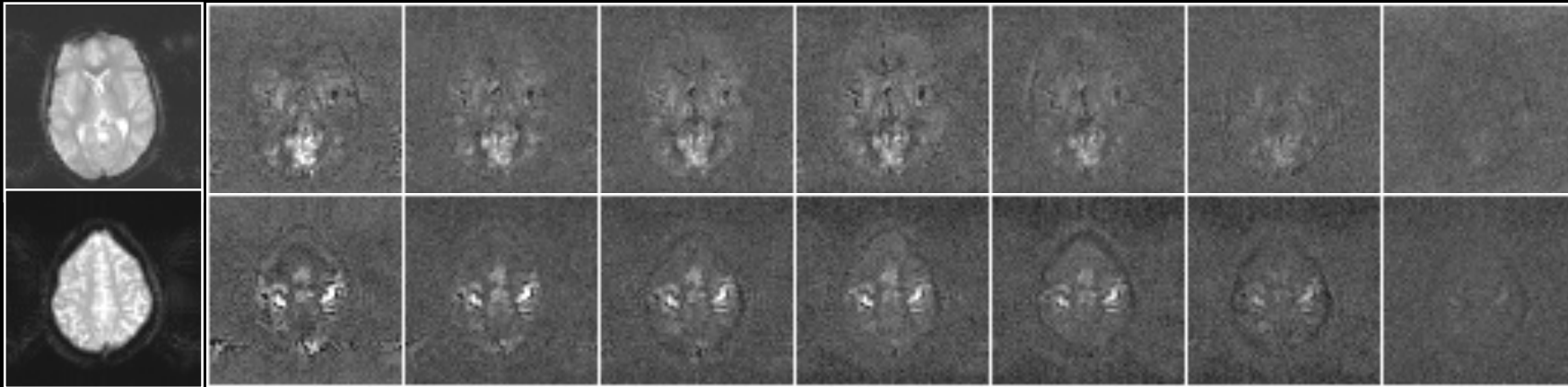
8, 2

6, 2

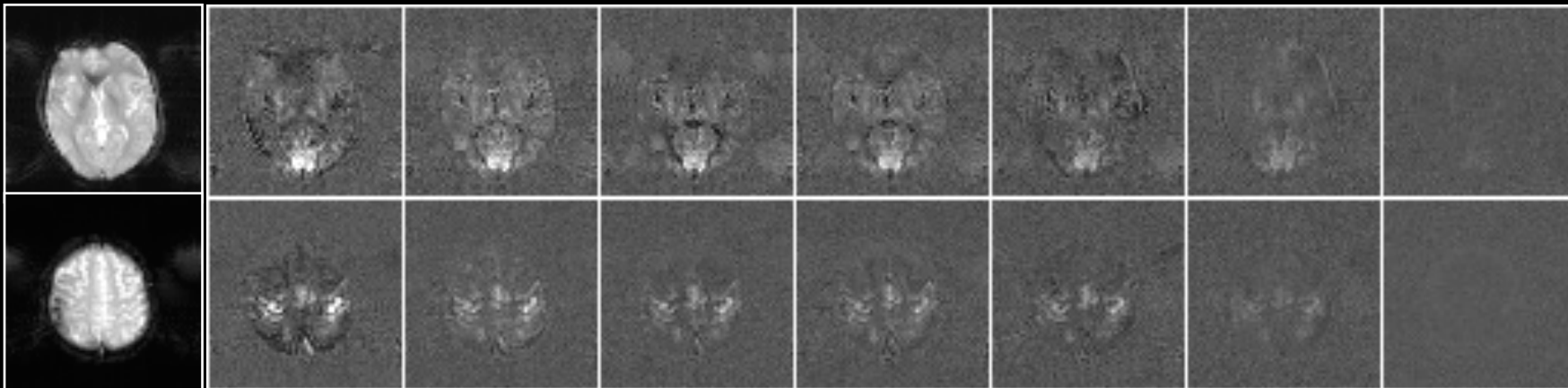
4, 2

2, 2

S1



S2



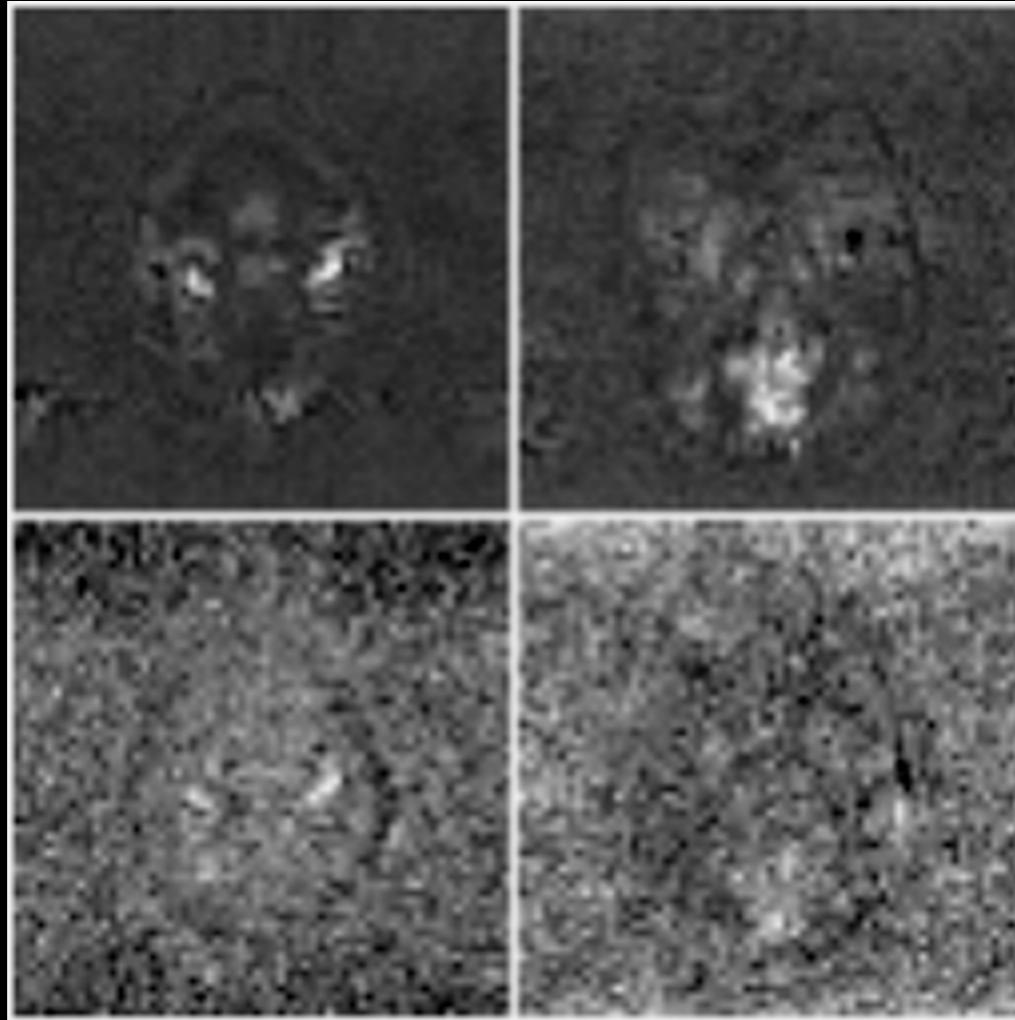
# Motor

# Visual

( ISI, SD )

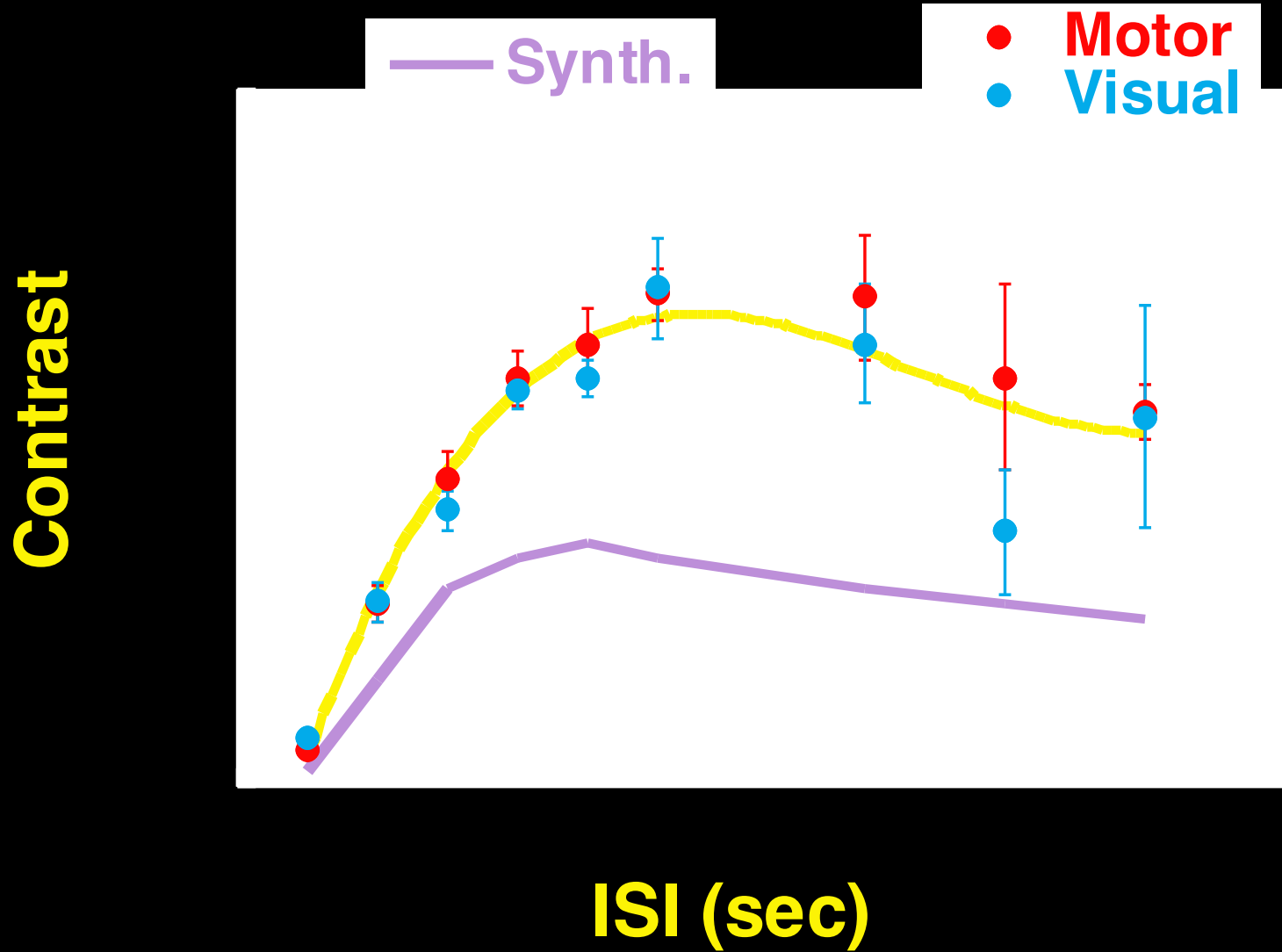
20, 20

2, 2



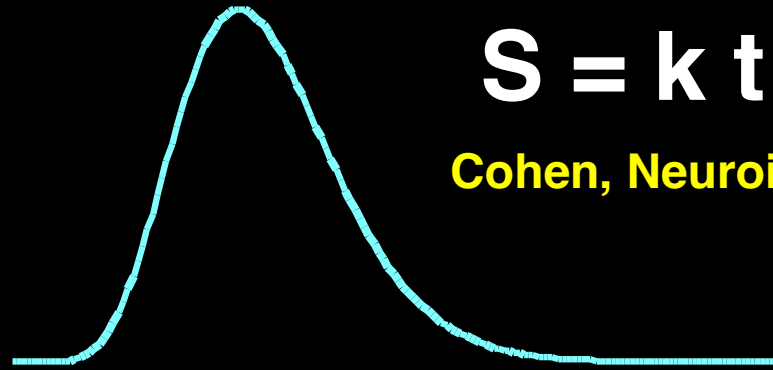
Relative differences in activation intensities may reflect spatial differences in hemodynamic responsivity. (draining veins vs. capillaries).

# Functional Contrast



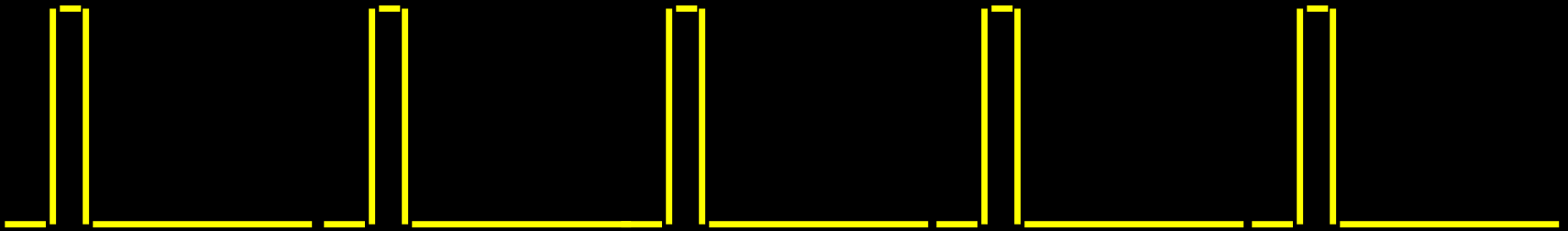
( Block design = 1 )

# Response Synthesis



$$S = k t^{8.6} e^{-t/0.547}$$

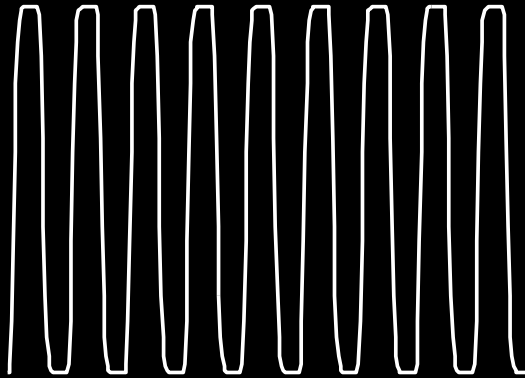
Cohen, Neuroimage 6, 93-103 (1997)



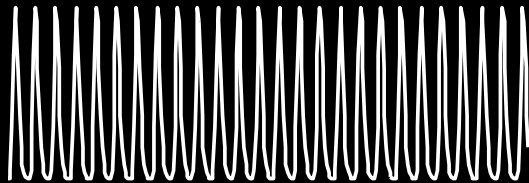
# Synthesized Responses

ISI, Dur

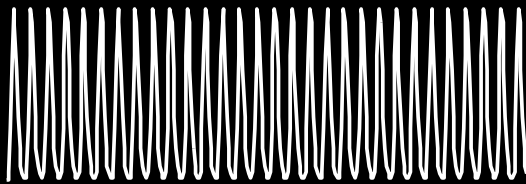
20, 20



12, 2

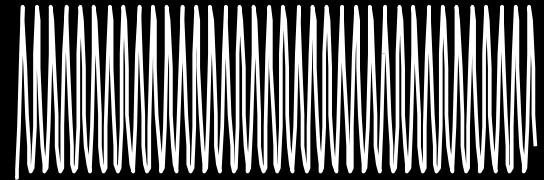


10, 2

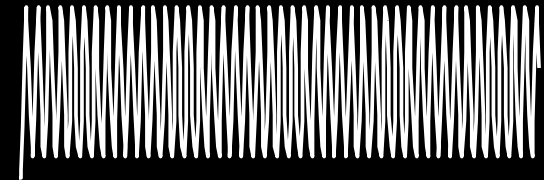


ISI, Dur

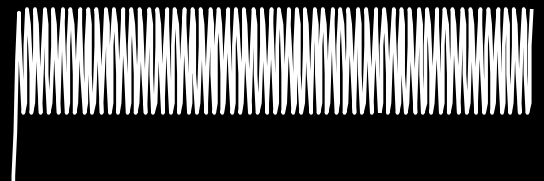
8, 2



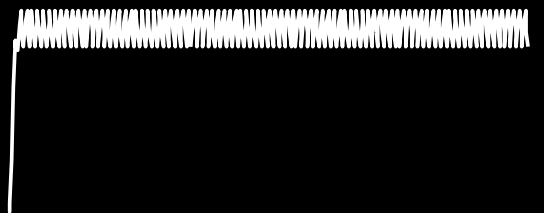
6, 2



4, 2



2, 2

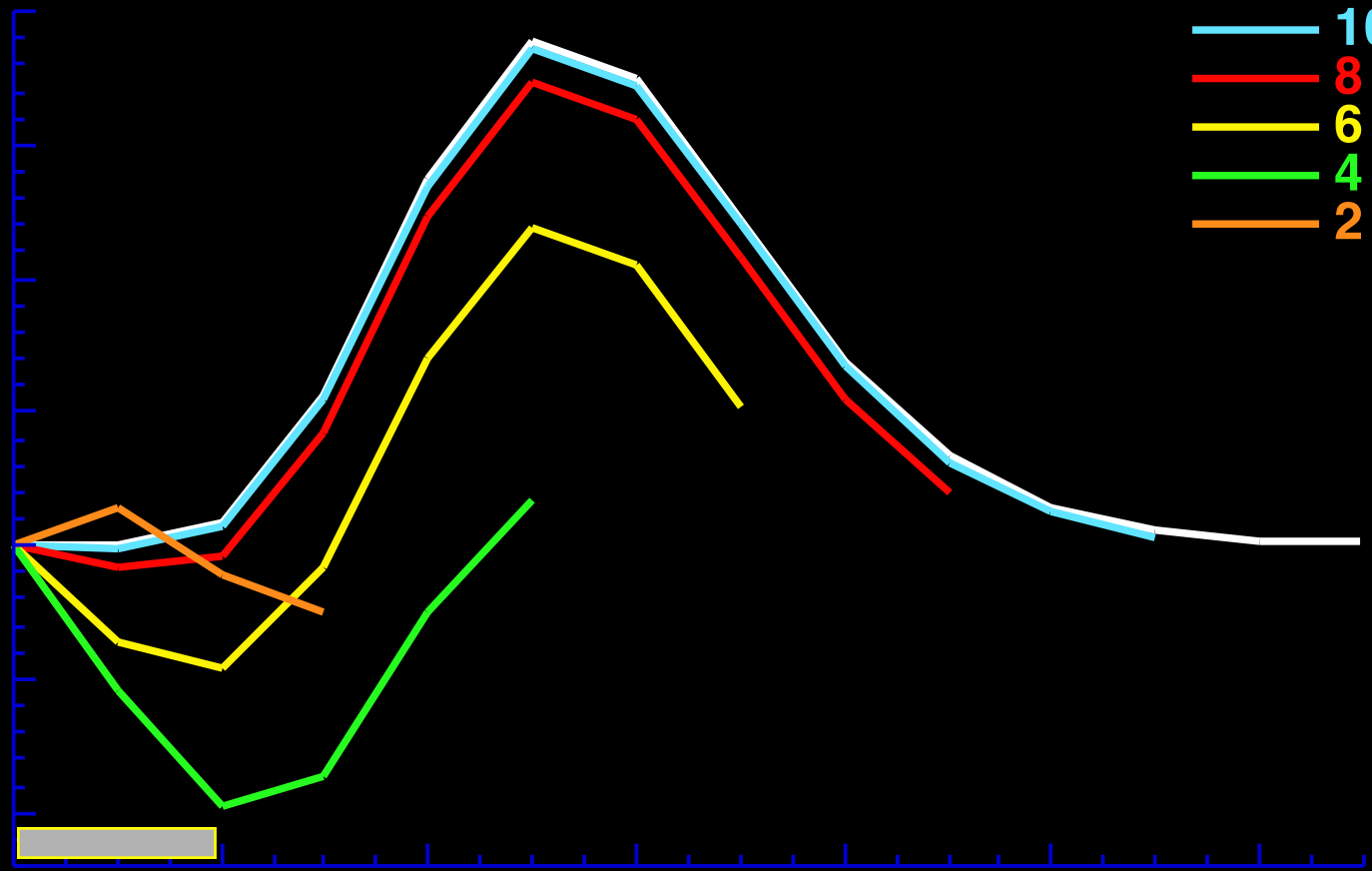




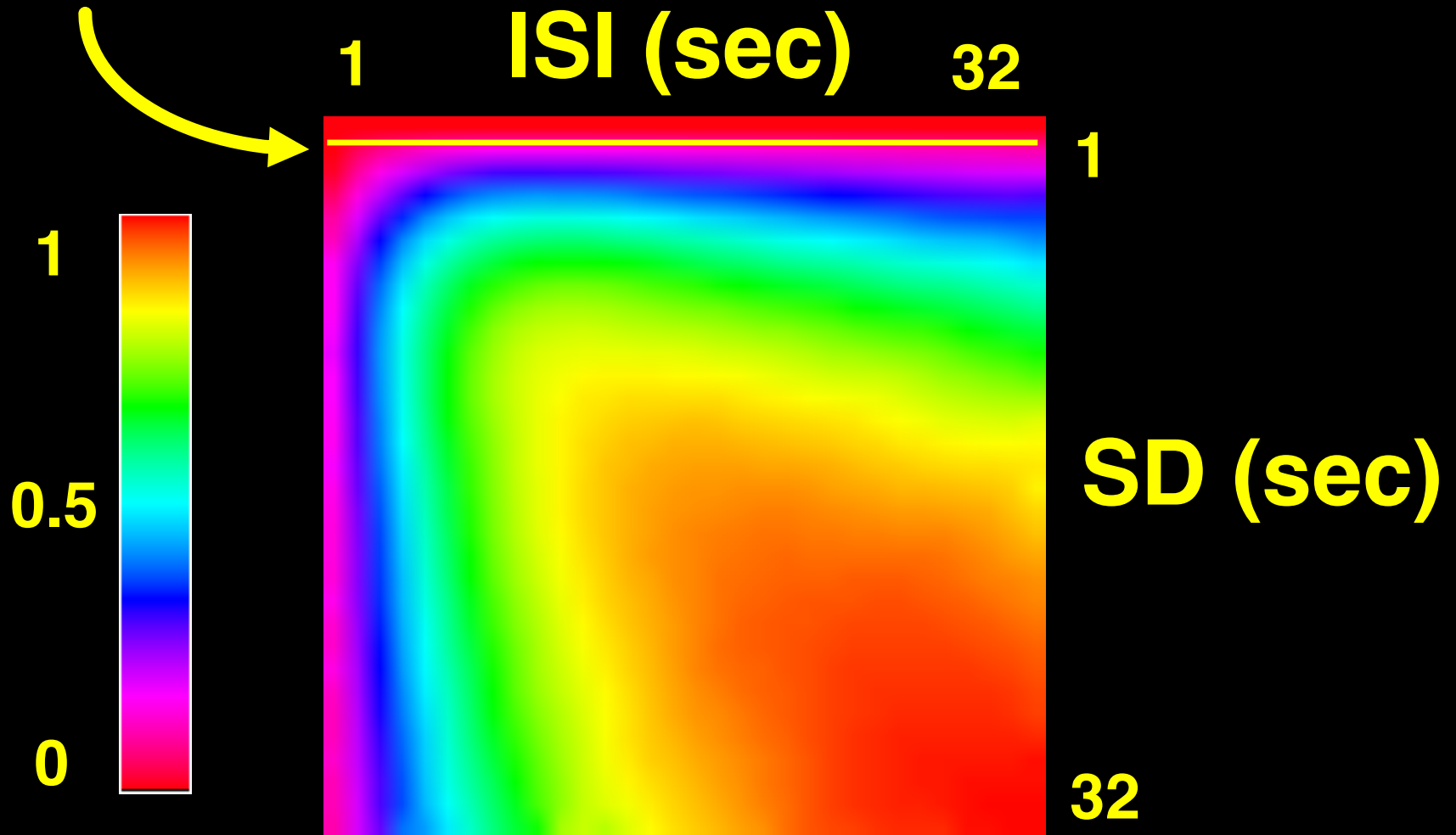
# Convolution

ISI

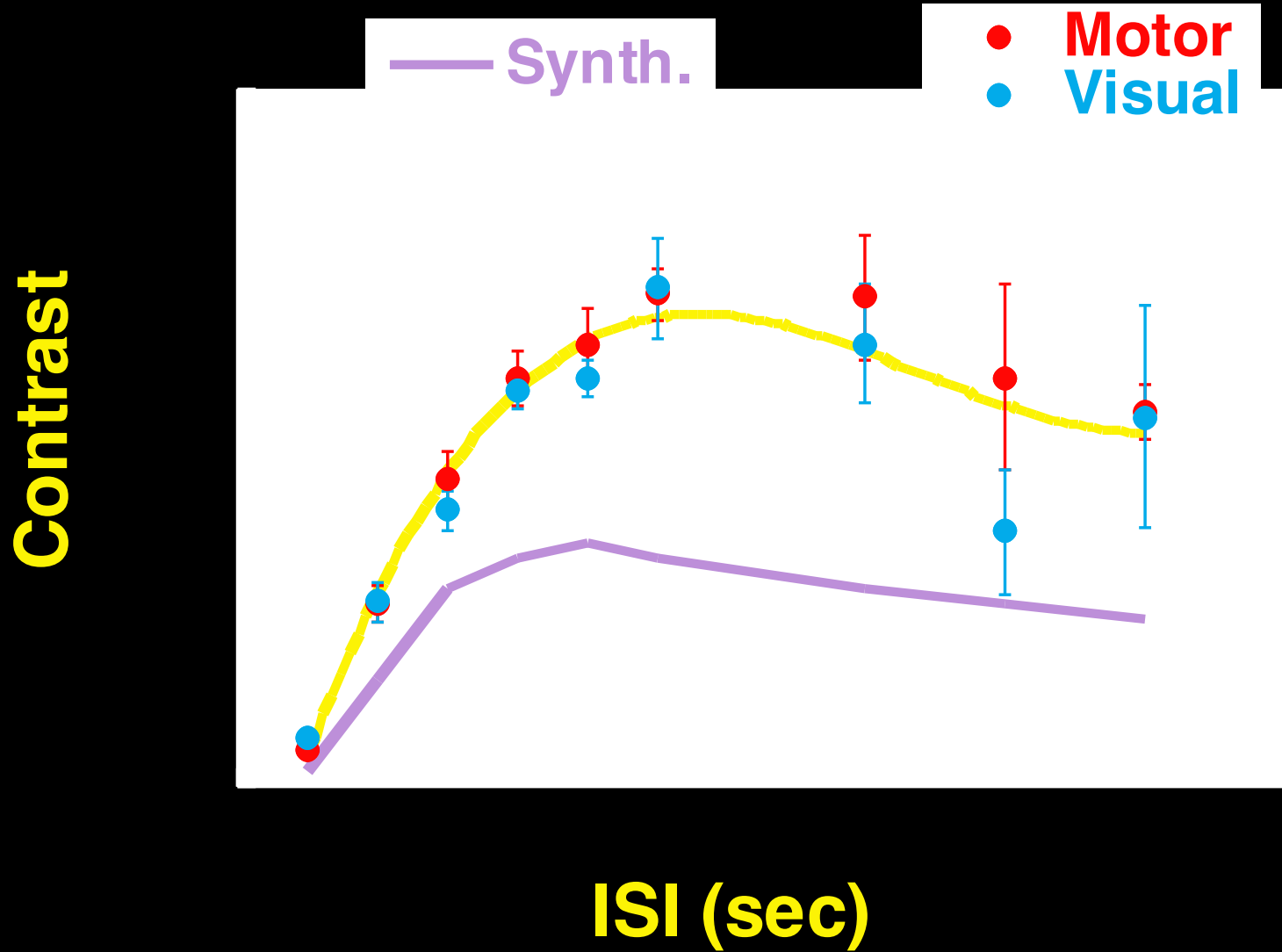
- 12
- 10
- 8
- 6
- 4
- 2



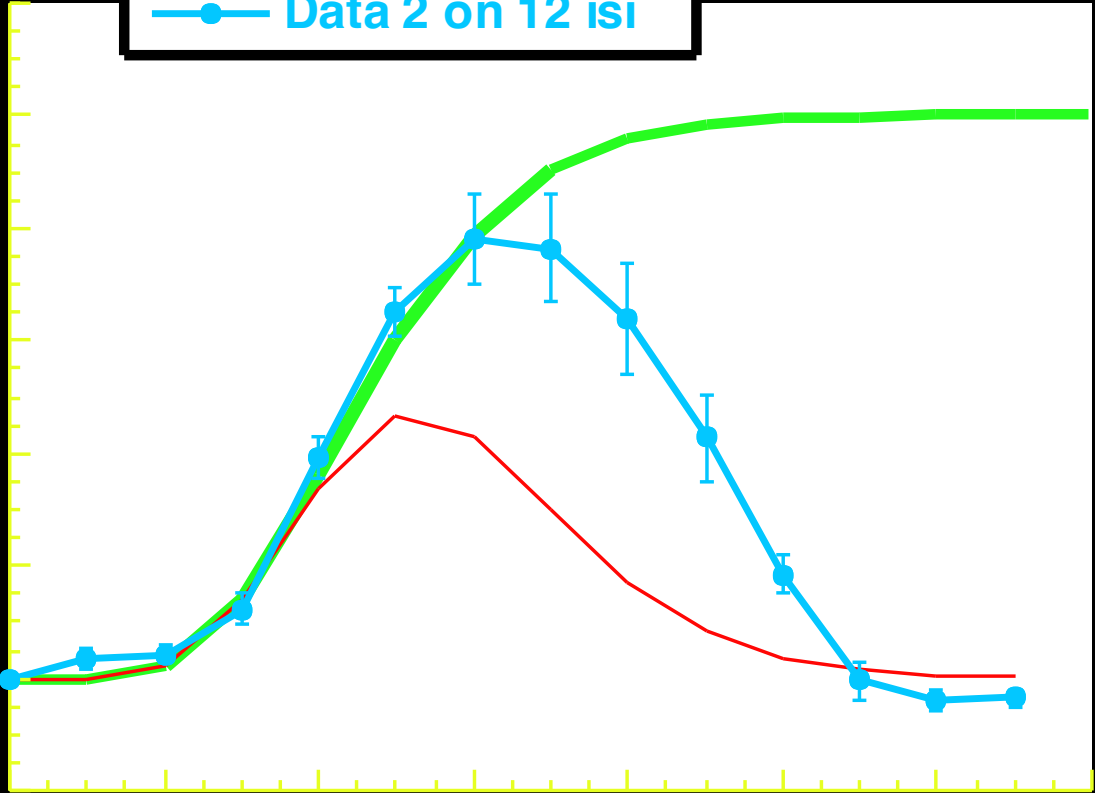
# Functional Contrast



# Functional Contrast



( Block design = 1 )



# Conclusions

- **Experimental:**

For SD = 2 sec, Optimal ISI  $\approx$  12 sec.  
Contrast = 0.65 x blocked contrast

- **Simulation using convolution:**

For SD = 2 sec, Optimal ISI  $\approx$  10 sec.  
Contrast = 0.35 x blocked contrast

**Possible reasons for greater than linear response.**

**Neuronal:**

“Bursting” during first 100 ms.

**Hemodynamic/Metabolic:**

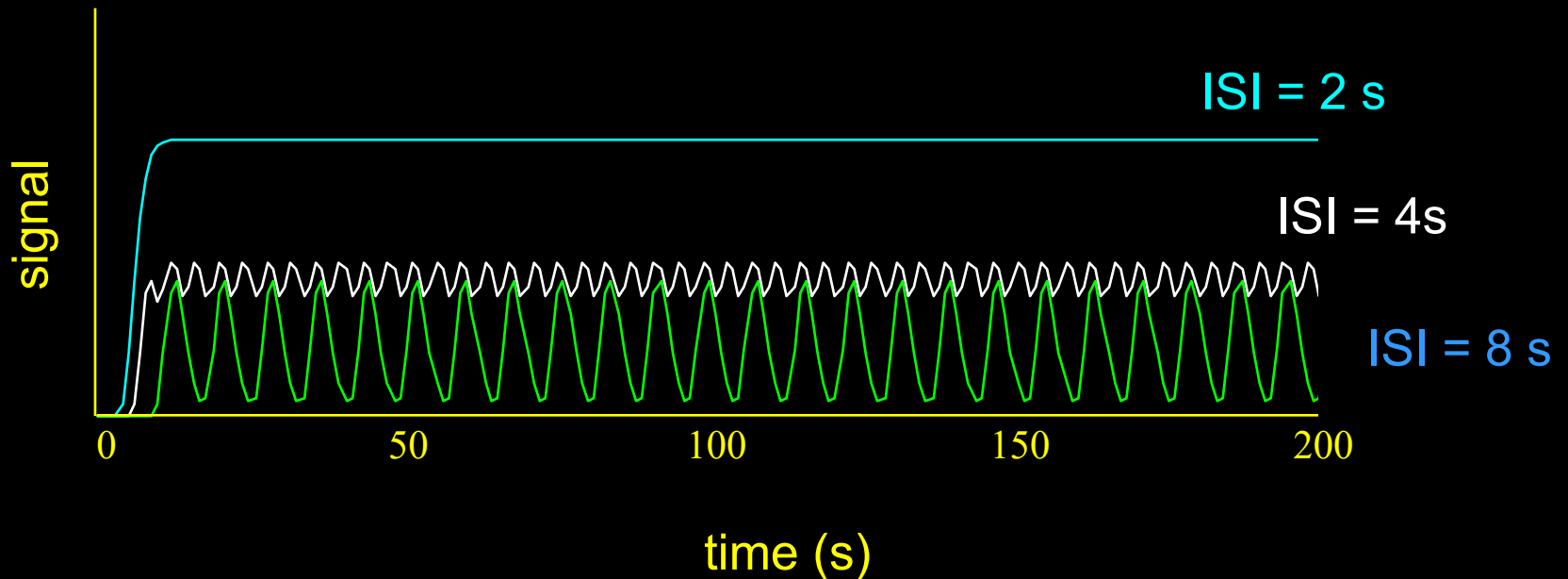
$\Delta$ BV and/or  $\Delta$ CMRO<sub>2</sub> time constants  
slower than  $\Delta$ Flow during initial seconds  
of activation.

Possible implications for interpretation of event-related  
data using short, randomized ISI w/ deconvolution.

Dale AM, Buckner RL (1997), Human Brain Mapping, 5, 329-340.

# BOLD response - constant ISI

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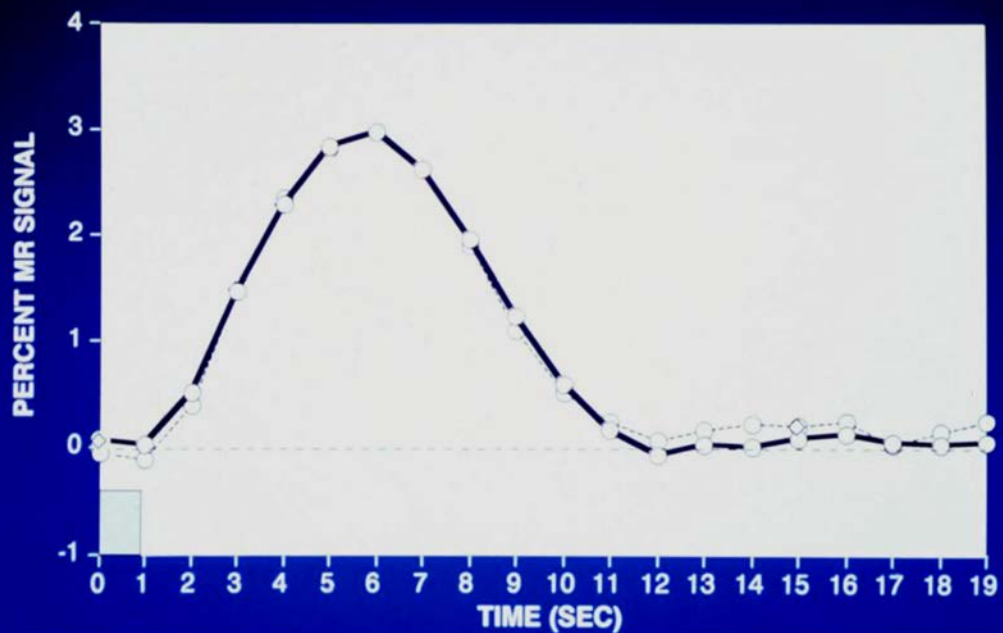
*Tasks can be performed faster by varying the ISI*

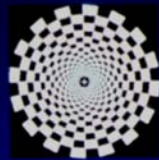


0 sec

20 sec

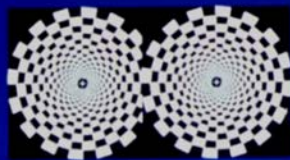
## Response to Averaged Single Trials: Subject JM





0 sec

20 sec

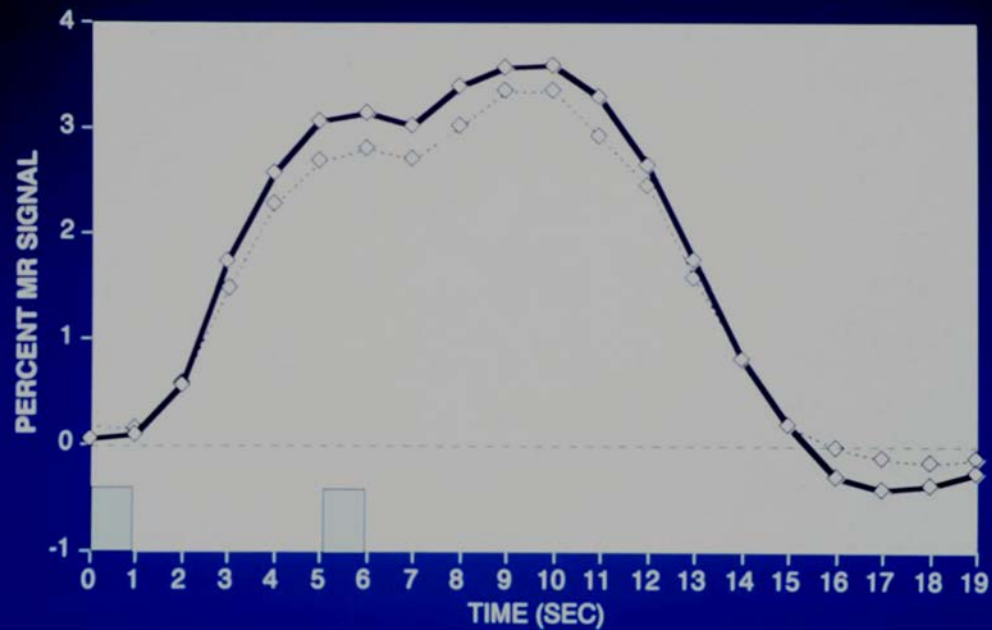


0 sec

5 sec

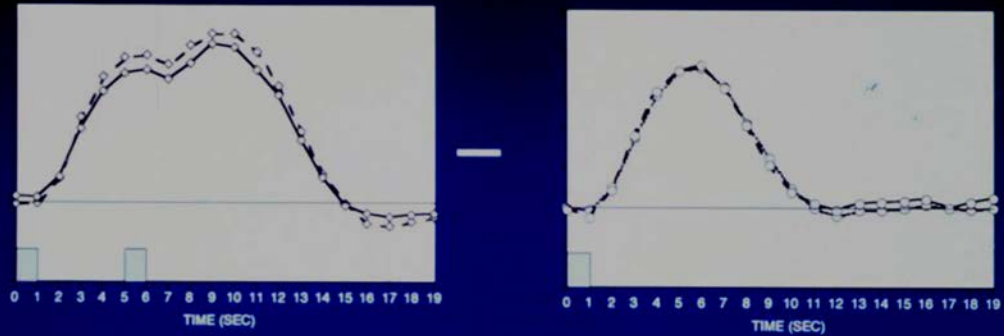
20 sec

## Response to Averaged Double Trials: Subject JM





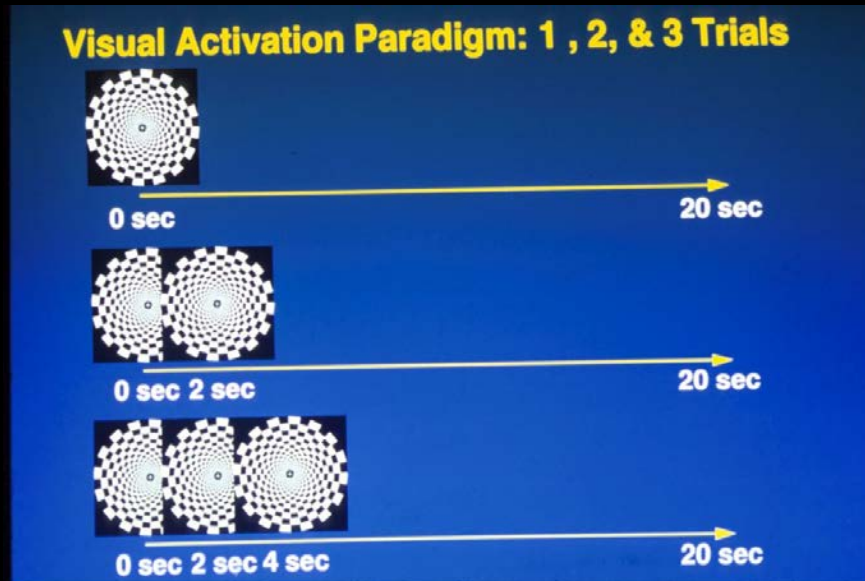
## Response to Averaged Double Trials: Subject JM



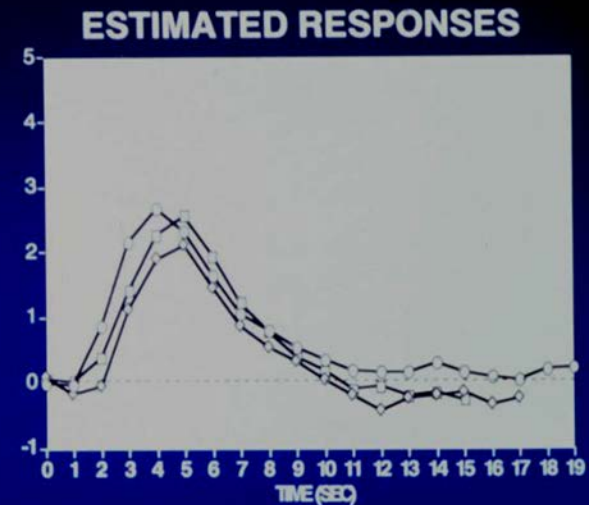
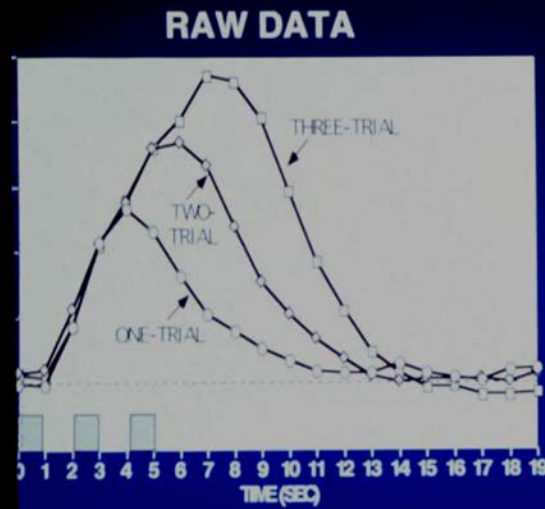
## Separation of Responses: Subject JM



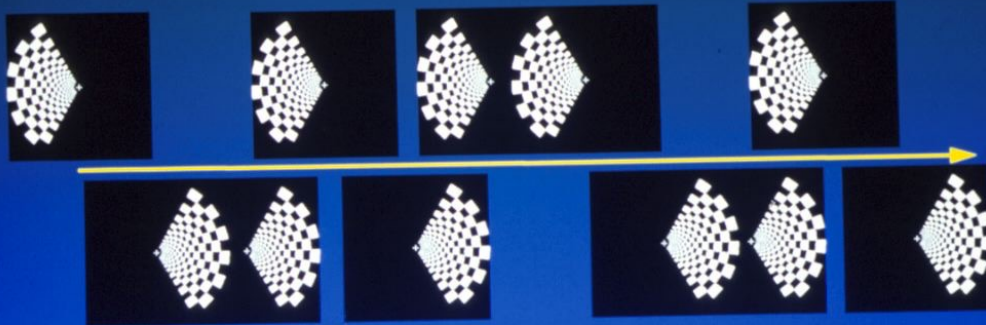
You can go even faster with the assumption of linearity...



### Response to Multiple Trials: Subject RW

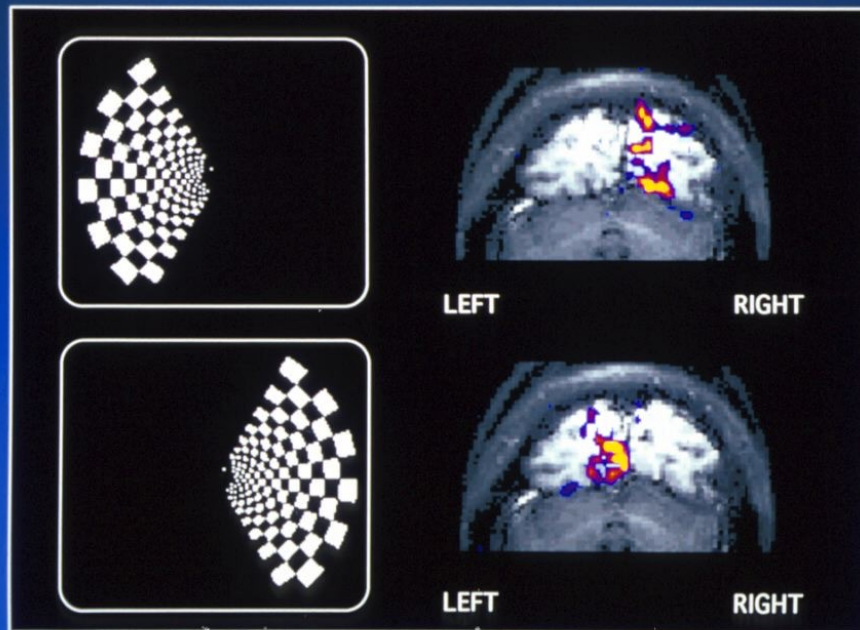


## Rapid-trial Visual Activation Paradigm for Selective Averaging



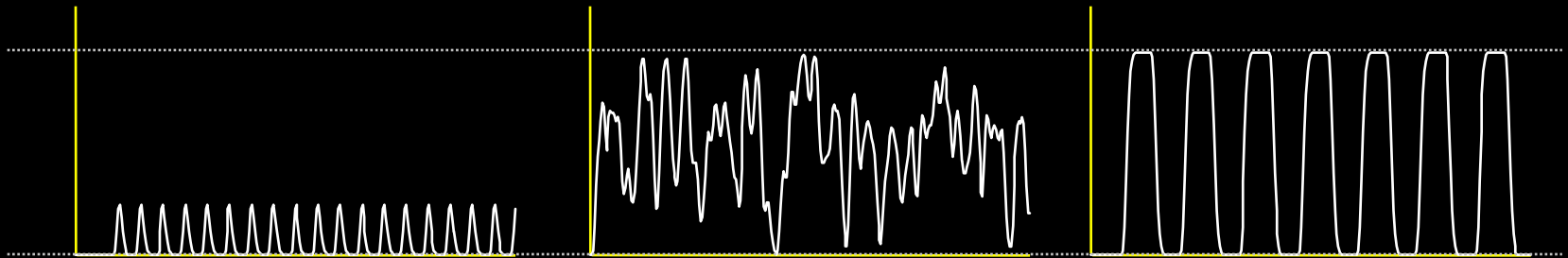
Trials randomly presented 2 sec apart

If ISI is randomized,  
and if ON / OFF distribution  
is 50%, the optimal average  
ISI is as short as you can  
make it.



# BOLD response - varying ISI

## BOLD response



## Stimulus



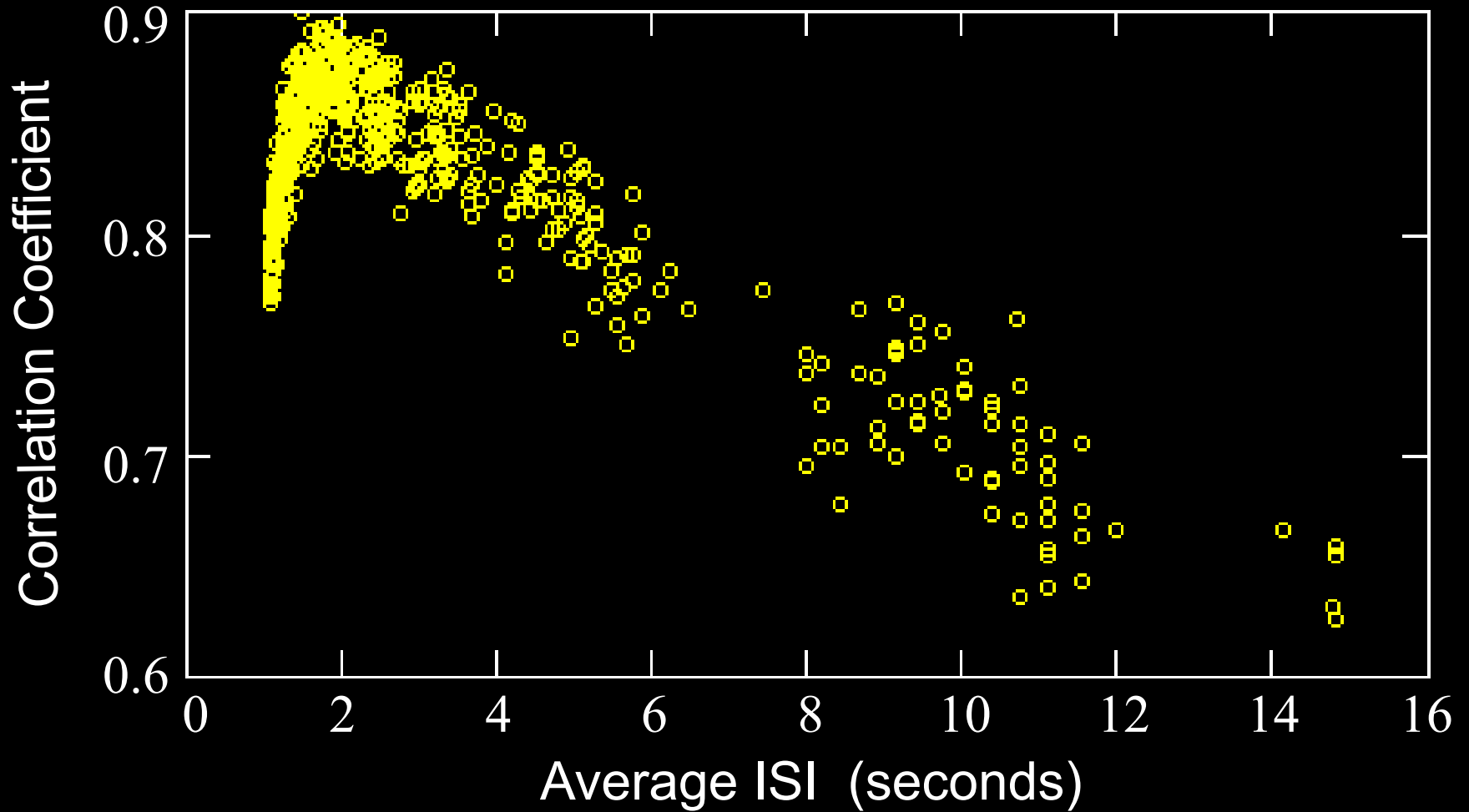
Event-related  
constant ISI

Event-related  
random ISI

Blocked trial

# fCNR vs. Average ISI

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# Conclusions

The fMRI signal is able to be **calibrated**. Physiologic, neuronal, and pulse sequence calibration techniques are just starting to develop to complement pulse sequence advances.

**-spatial resolution** < 0.5 mm

**-temporal resolution** < 100 ms

**-information content:** quantitative flow, CMRO<sub>2</sub>...

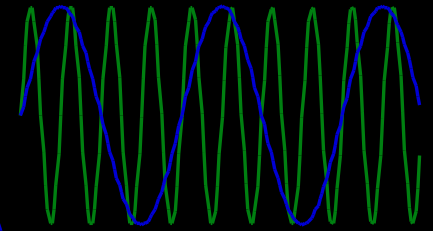
A large amount of additional information exists in the fMRI signal (i.e. fluctuations..).

To aid the development of calibration, more work needs to be done using extremely well understood neuronal activation (across several temporal, spatial, and intensity scales) to better characterize of the fMRI signal.

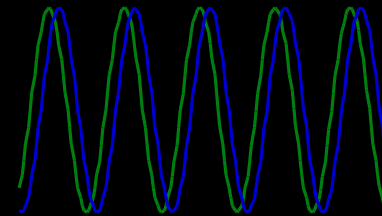
# Neuronal Activation Input Strategies

1. Block Design

2. Frequency Encoding

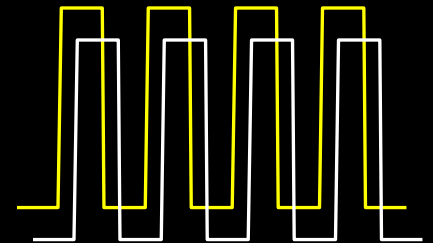


3. Phase Encoding



4. Single Event

5. Orthogonal Block Design

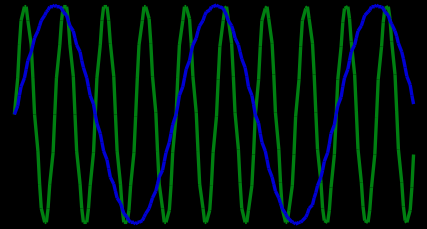


6. Free behavior Design.

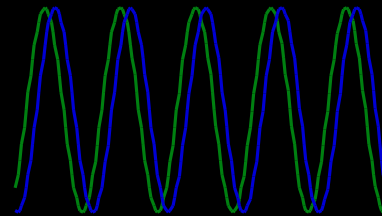
# Neuronal Activation Input Strategies

1. Block Design

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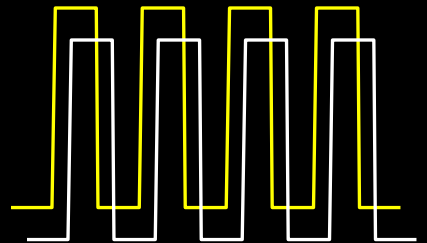


3. Phase Encoding



4. Single Event

5. Orthogonal Block Design



6. Free behavior Design



# Free behavior Design:

Use the following as “reference functions”

- Skin Conductance
- EEG
- Eye tracking
- Task performance
- Heart rate
- Respiration rate

## Pulse sequences

## Processing

## Paradigms

Basic

Shimming

RF coil arrays

Contrast comparisons

Physiologic fluctuations

Embedded contrast

Motion correction

Distortion / dropout correction

Real time fMRI

Perfusion quantitation

<- Multi - modal integration ->

<- Sub - second resolution ->

<- Sub - millimeter resolution ->

<- CMRO<sub>2</sub> mapping ->

Parametric manipulation

Phase and freq. encoding

Orthogonal multi-task encoding

Physiologic manipulations

Event - related fMRI

Effective connectivity mapping



Advanced

**1991-1992**



**1992-1999**



