

Choosing the Optimal Sequences and Strategies for Functional MRI

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Variables to Optimize

- Information Content
- Sensitivity
- Speed
- Resolution
- Image quality

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Information Content

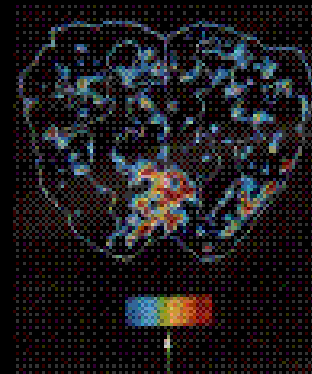
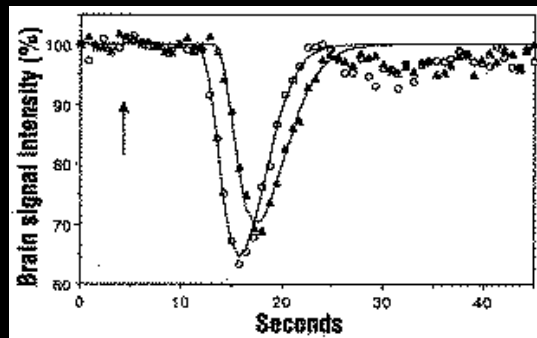
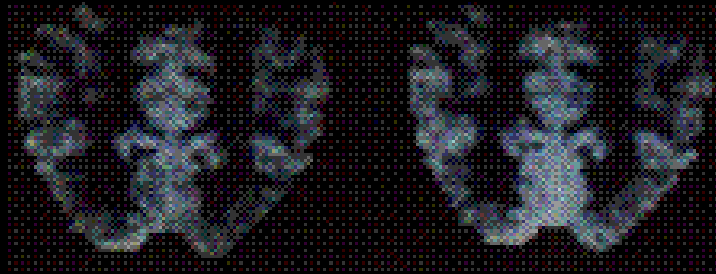
- Blood Volume
- Blood Oxygenation
- Blood Perfusion
- Hemodynamic Specificity
- Mapping of CMRO_2

Blood Volume

Contrast agent injection and time series collection of T2* or T2 - weighted images

Resting

Active

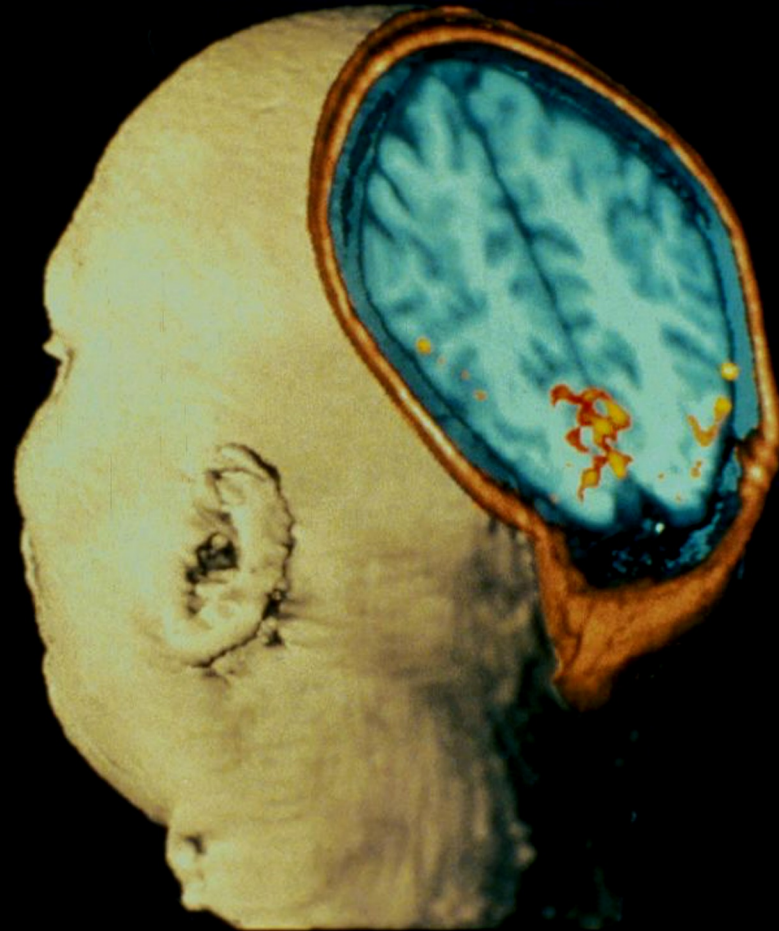


Blood Volume

**Photic
Stimulation**

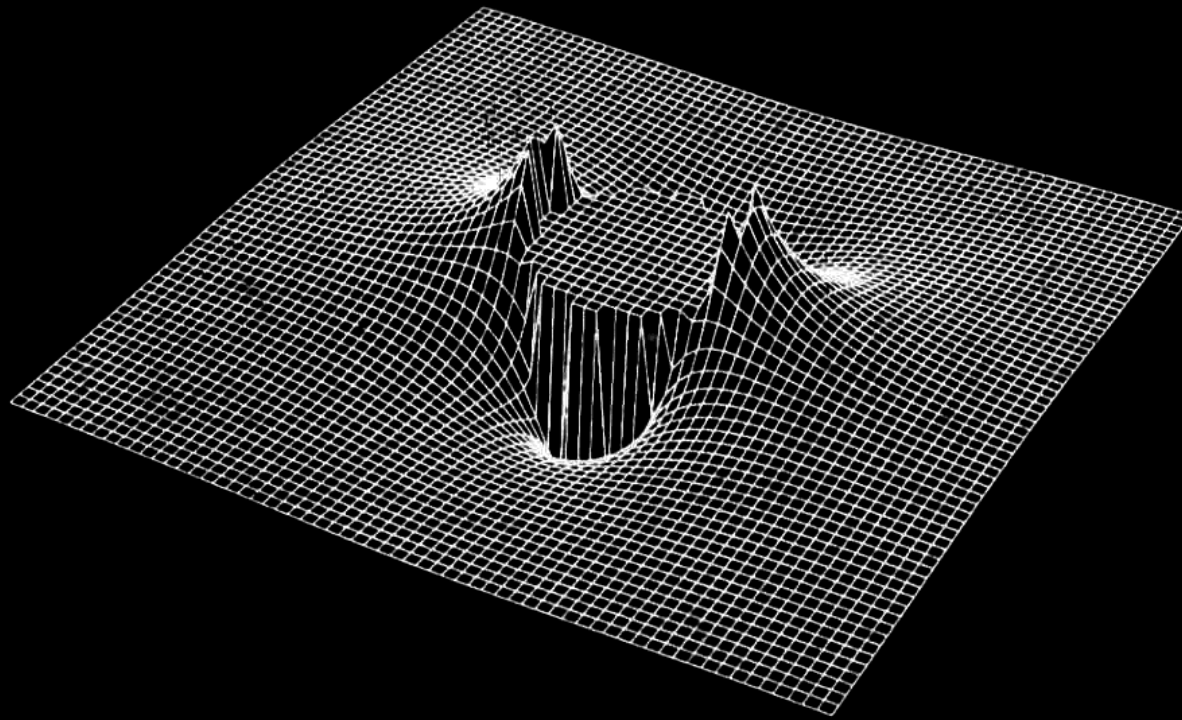
**MRI Image showing
activation of the
Visual Cortex**

**From Belliveau, et al.
Science Nov 1991**



Susceptibility Contrast

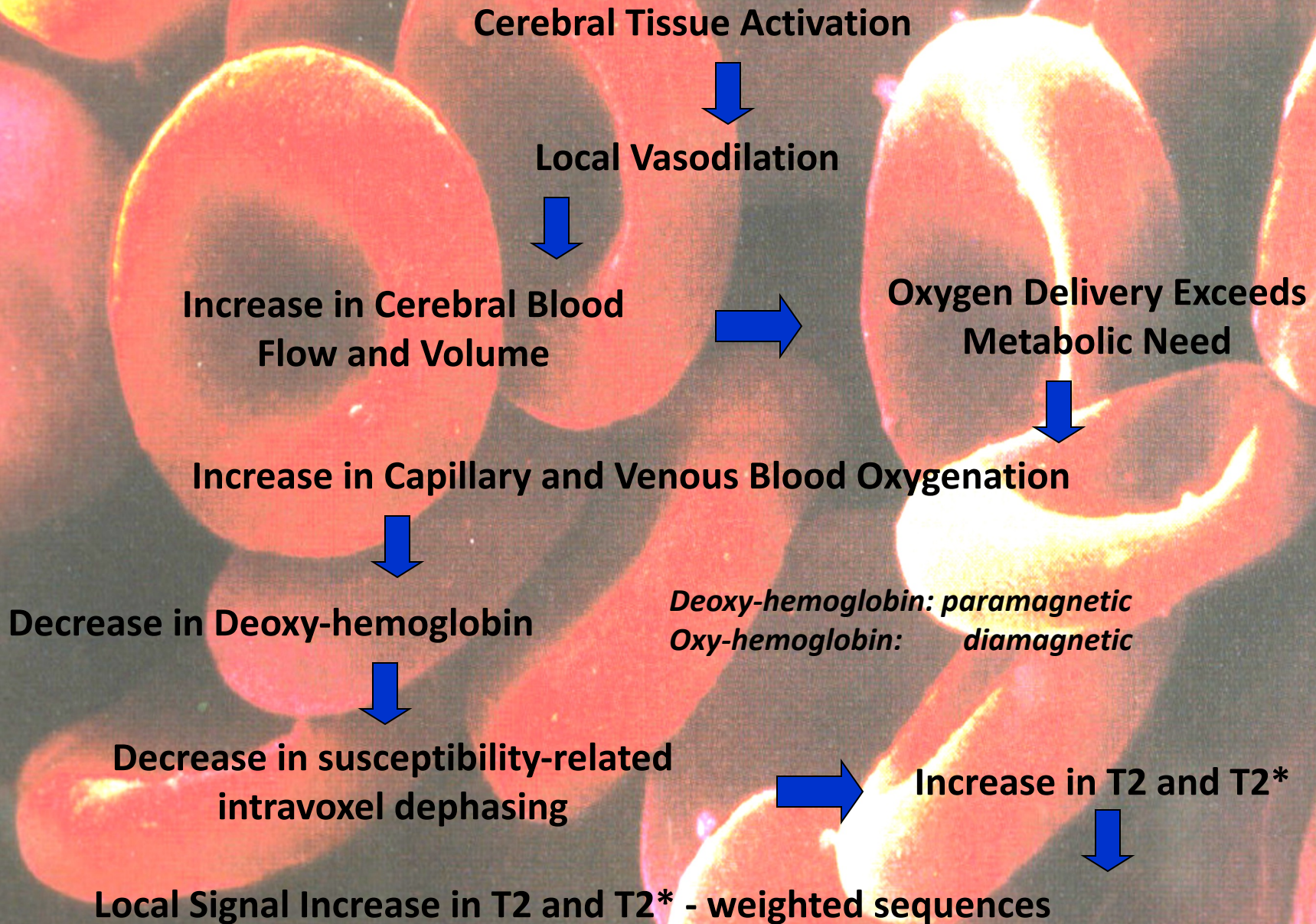
Susceptibility-Induced Field Distortion in the Vicinity of a Microvessel \perp to B_0 .



Blood Oxygenation

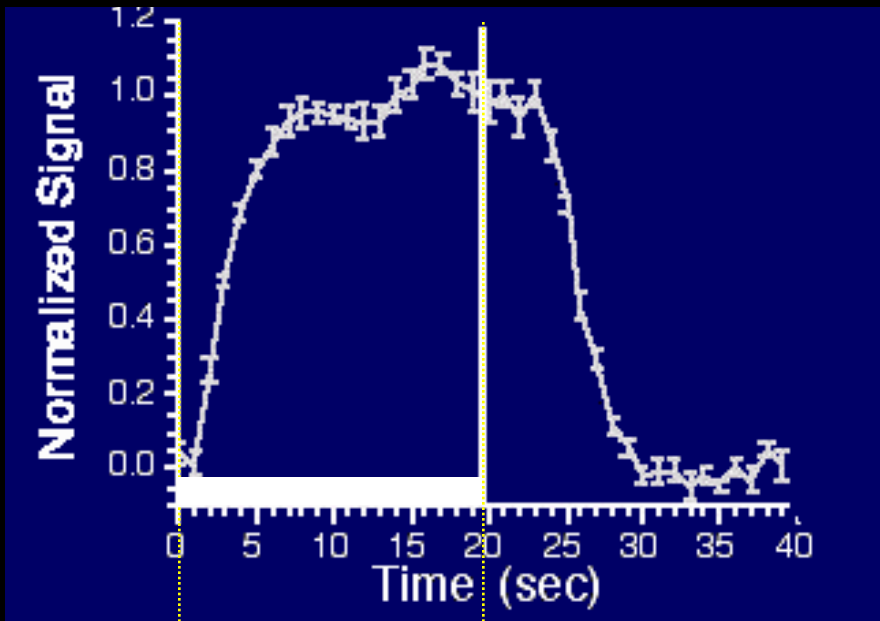


BOLD Contrast in the Detection of Neuronal Activity

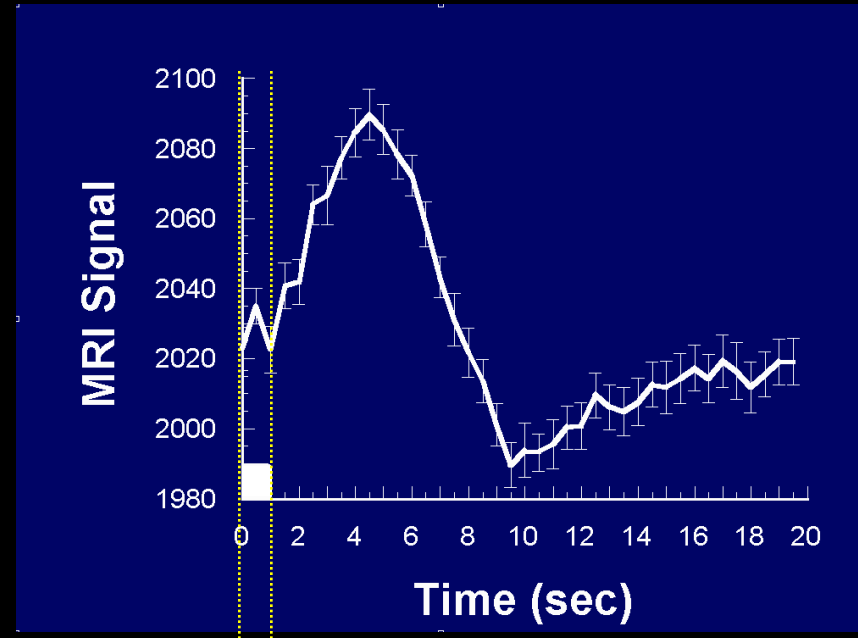


The BOLD Signal

Blood Oxygenation Level Dependent (BOLD) signal changes



task

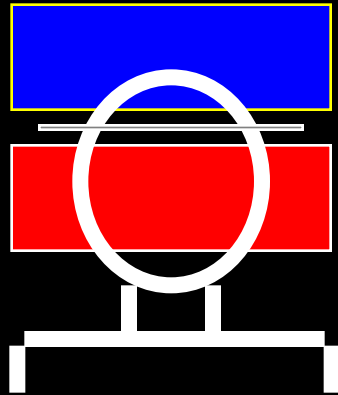


task

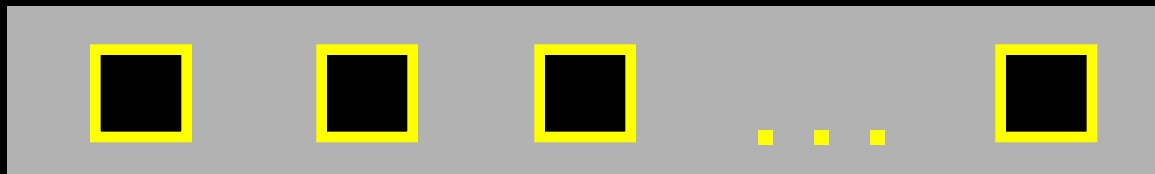
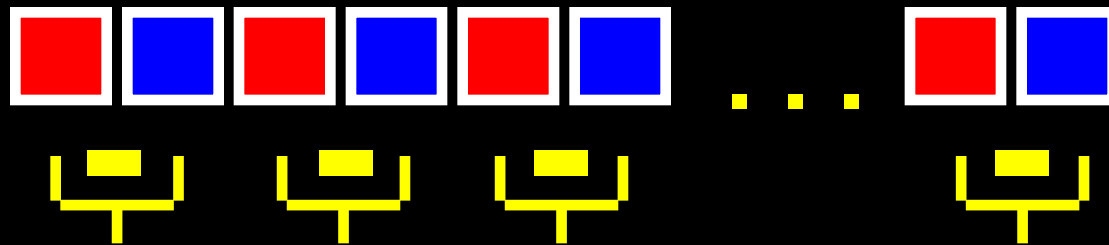
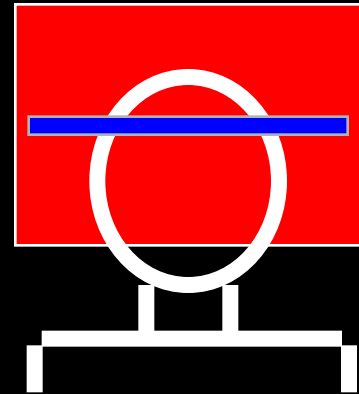


Blood Perfusion

EPISTAR



FAIR



TI (ms)

FAIR

EPISTAR

200

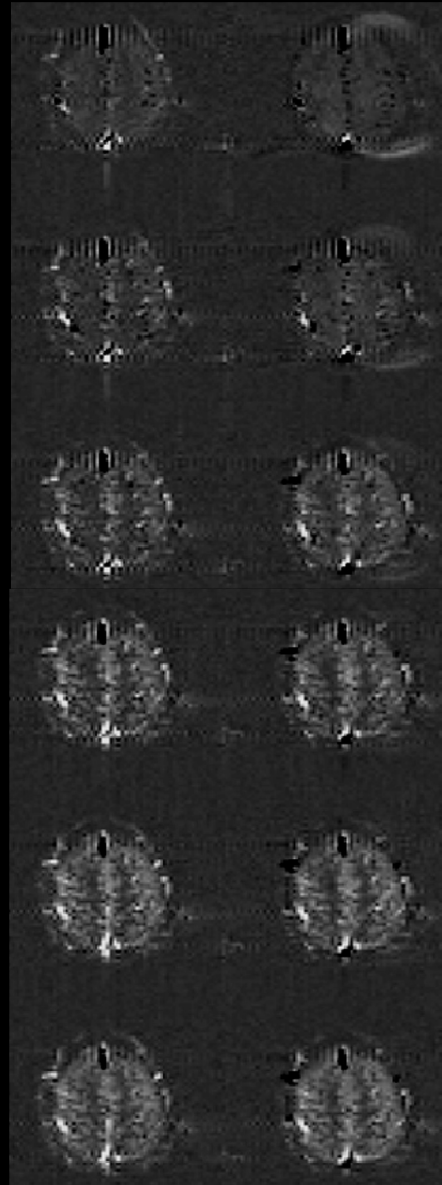
400

600

800

1000

1200

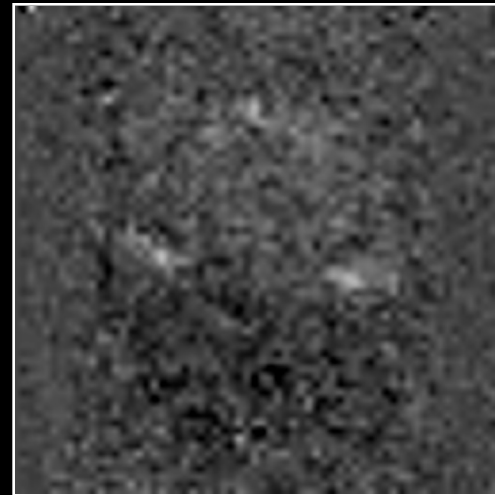
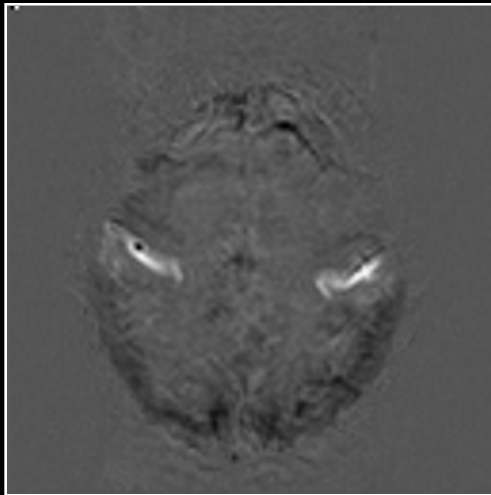
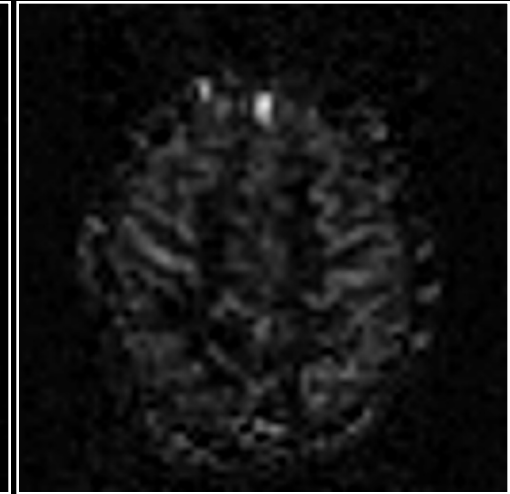
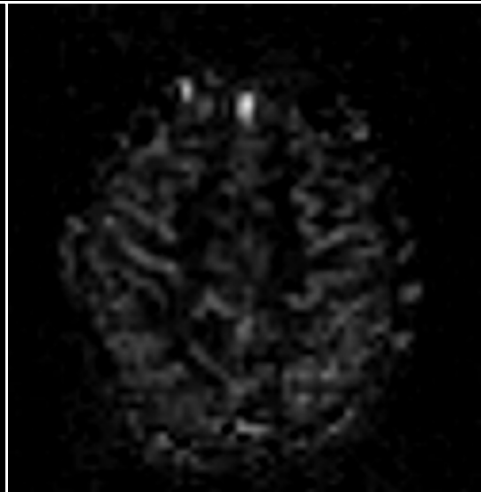
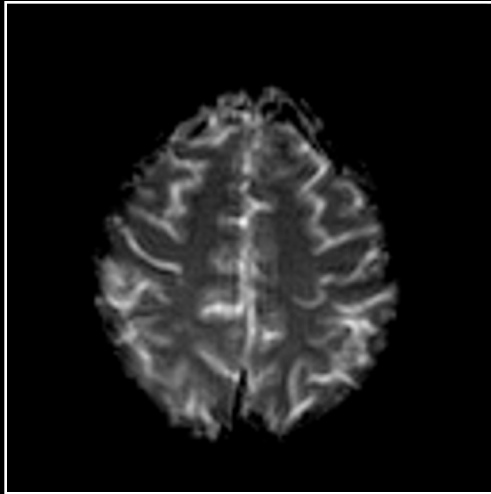


Perfusion

BOLD

Rest

Activation



Anatomy



BOLD



Perfusion



+

-

Volume

- unique information
- baseline information
- multislice trivial

- invasive
- low C / N for func.

BOLD

- highest C / N
- easy to implement
- multislice trivial
- non invasive
- highest temp. res.

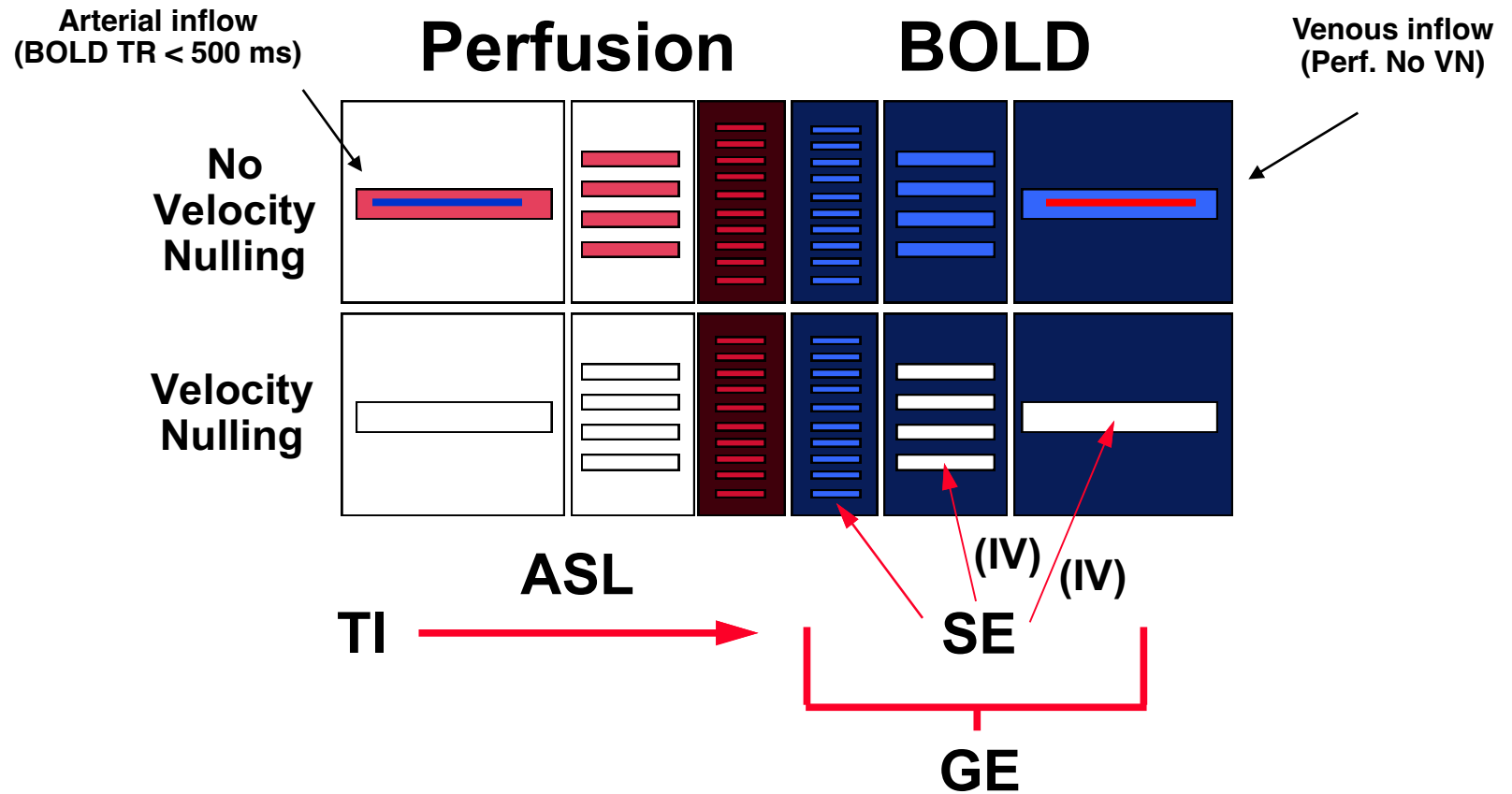
- complicated signal
- no baseline info.

Perfusion

- unique information
- control over ves. size
- baseline information
- non invasive

- multislice non trivial
- lower temp. res.
- low C / N

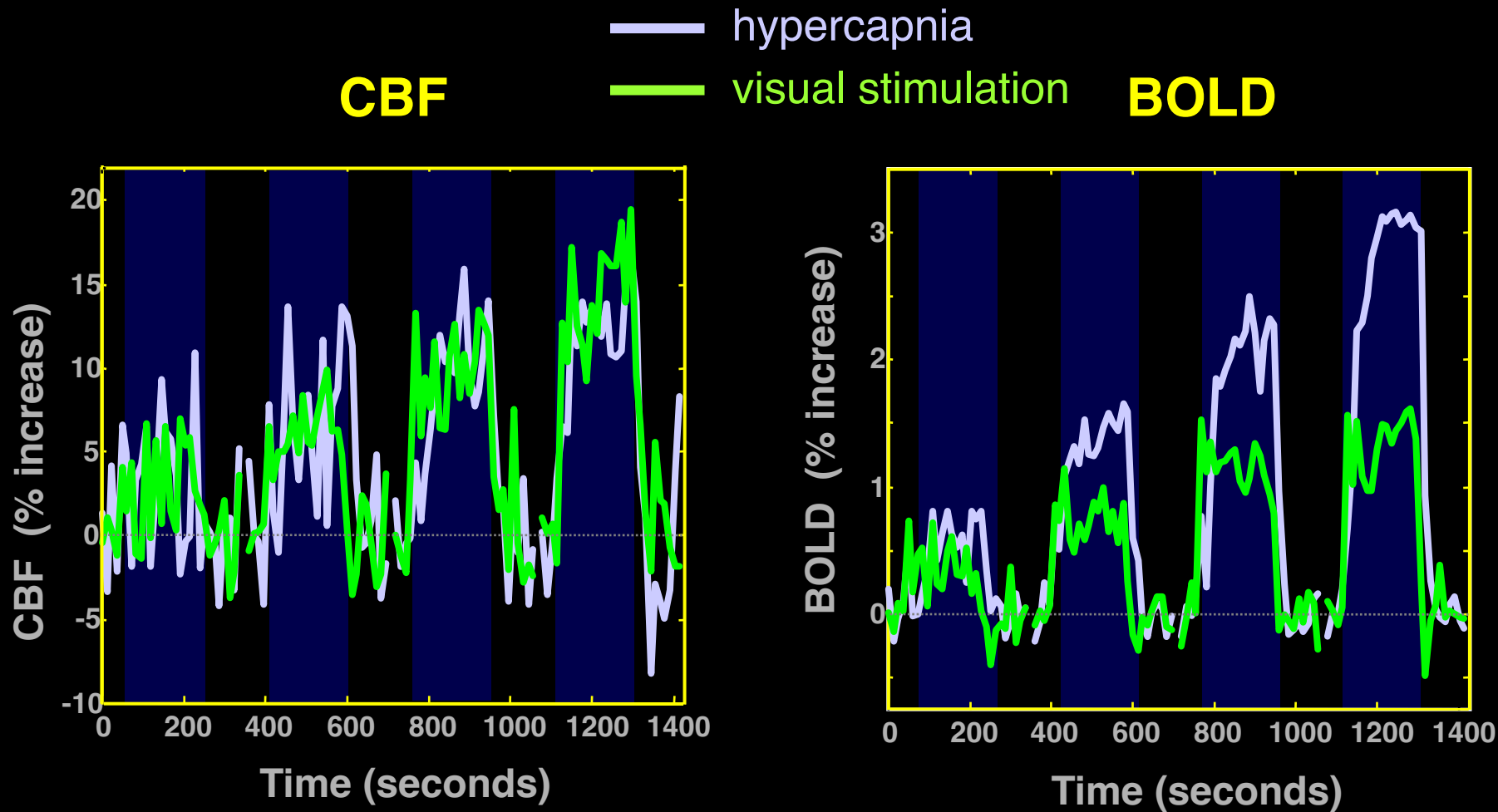
Hemodynamic Specificity



Mapping of CMRO₂

Activation:	Flow	↑↑
	CMRO ₂	↑
	Blood Oxygenation	↑
CO ₂ stress:	Flow	↑↑
	CMRO ₂	→
	Blood Oxygenation	↑↑

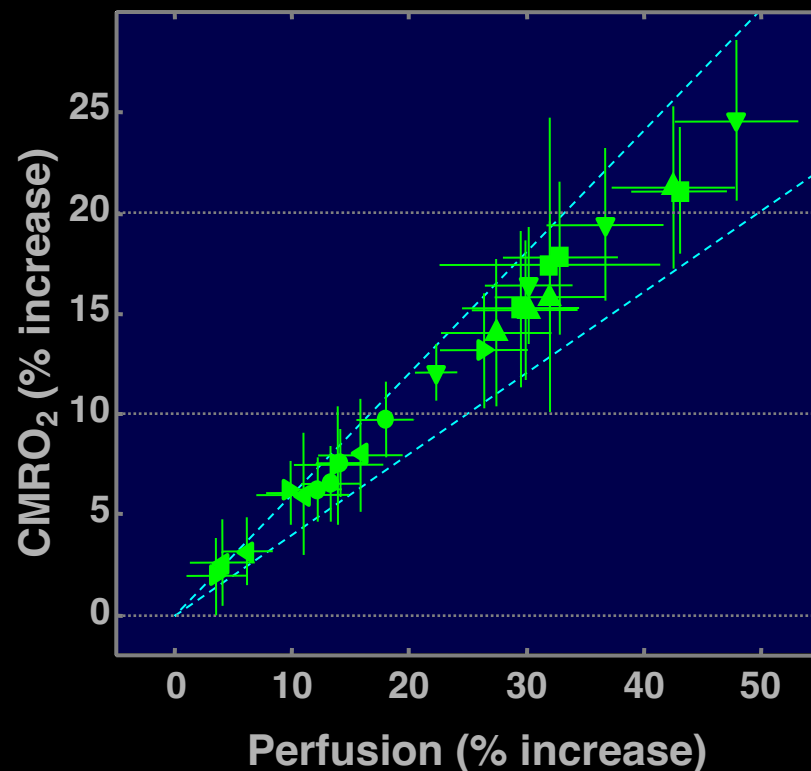
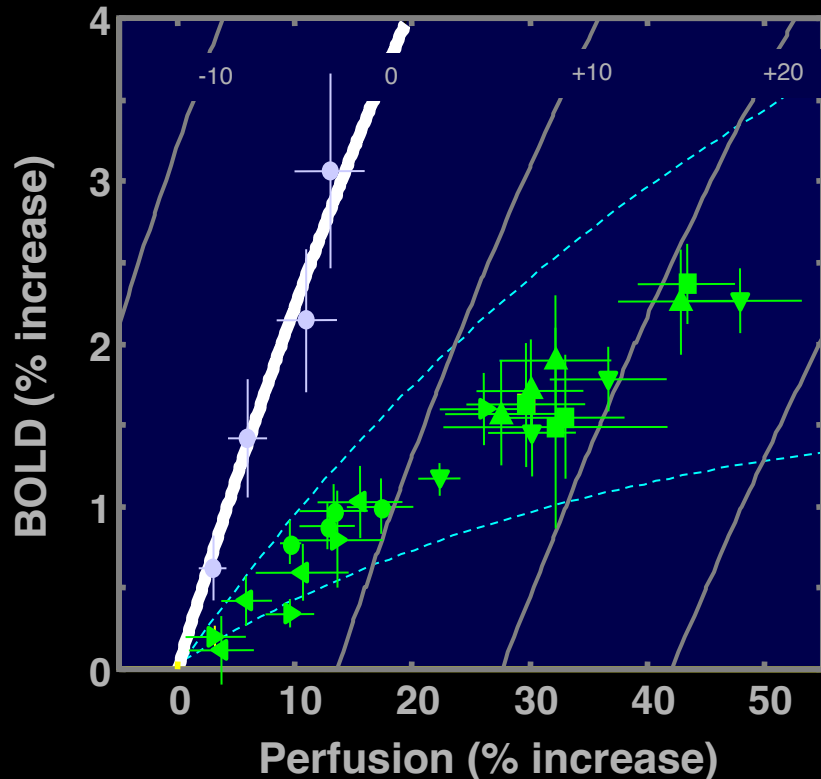
CMRO₂-related BOLD signal deficit:



Simultaneous Perfusion and BOLD imaging during graded visual activation and hypercapnia

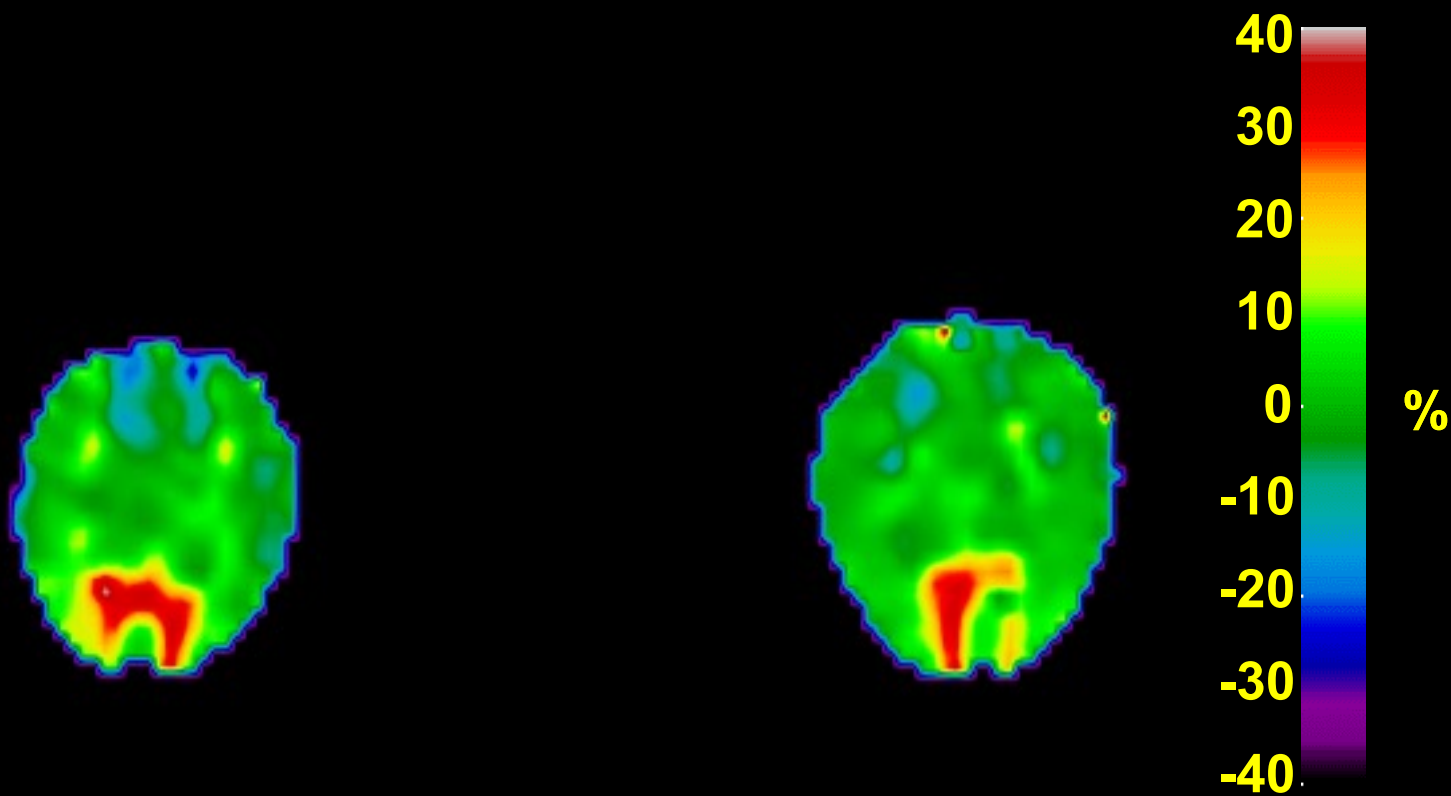
CBF-CMRO₂ coupling

Hoge, et al.



Characterizing Activation-induced CMRO₂ changes using calibration with hypercapnia

Computed CMRO₂ Changes



Subject 1

Subject 2

Variables to Optimize

- Information Content
- Sensitivity
- Speed
- Resolution
- Image quality

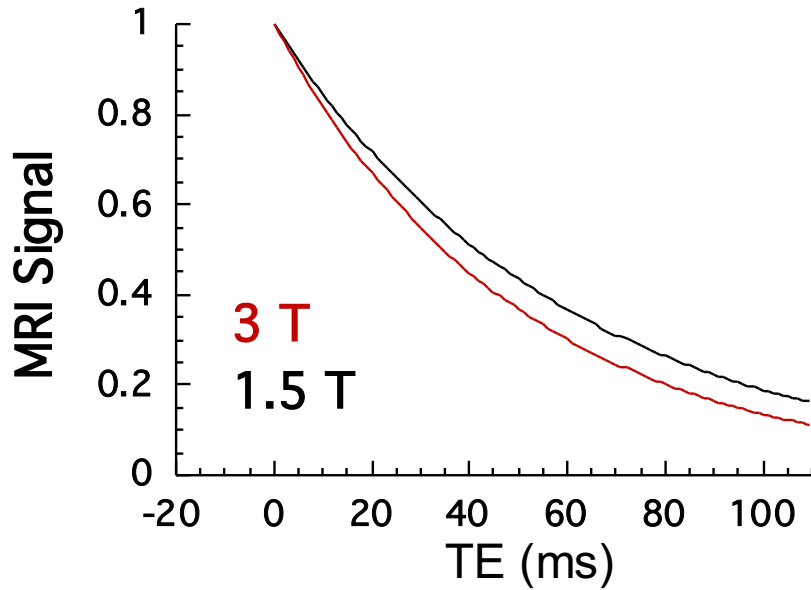
Sensitivity

- **Optimizing fMRI Contrast**
- **Maximizing Signal**
- **Reducing Physiologic Fluctuations**
- **Minimizing Temporal Artifacts**

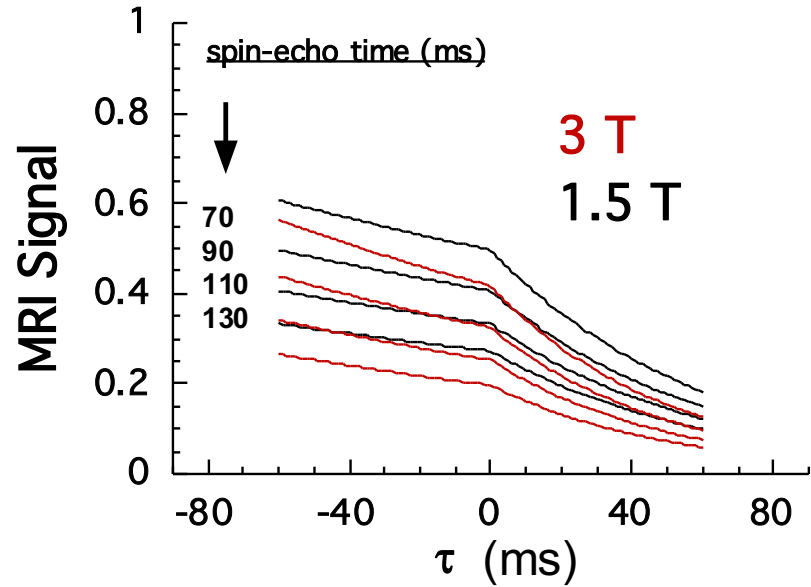
Optimizing fMRI Contrast

- Increase field strength
- Adjust pulse sequence timing ($TE \approx T2^*$)
- Adjust voxel volume (\approx activation volume)

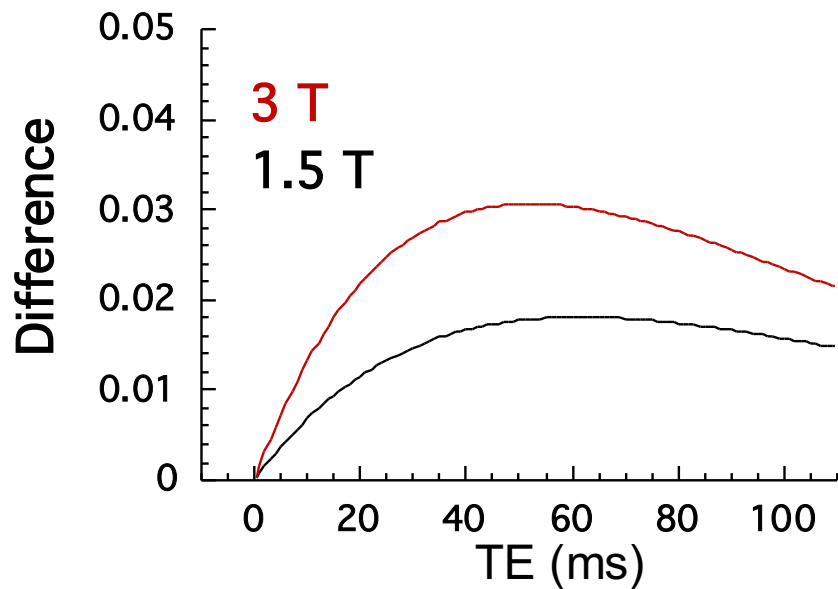
Gradient - Echo



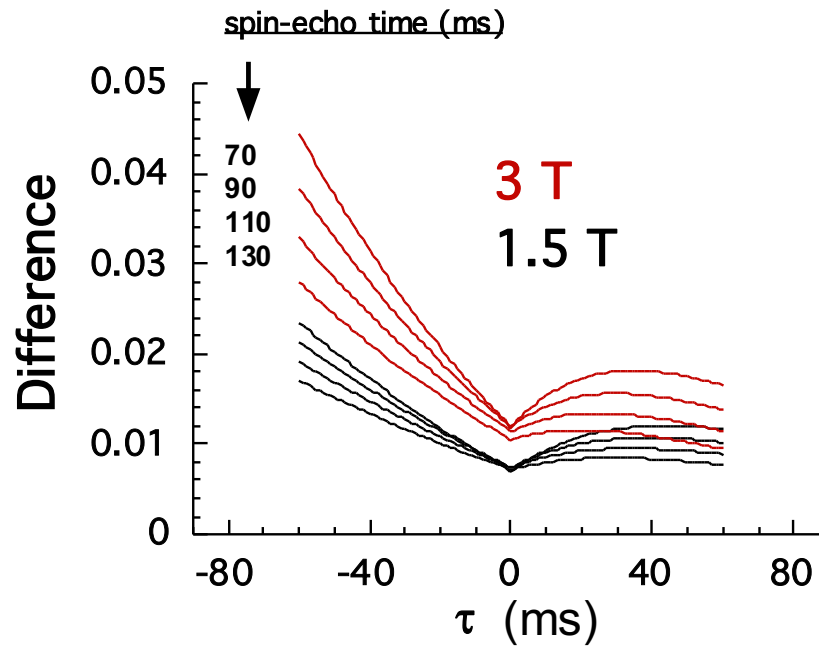
Asymmetric Spin - Echo



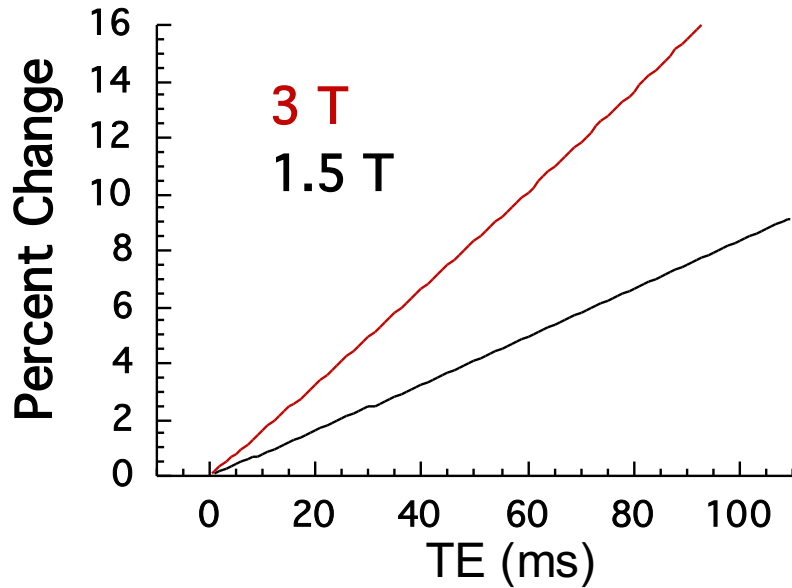
Gradient - Echo



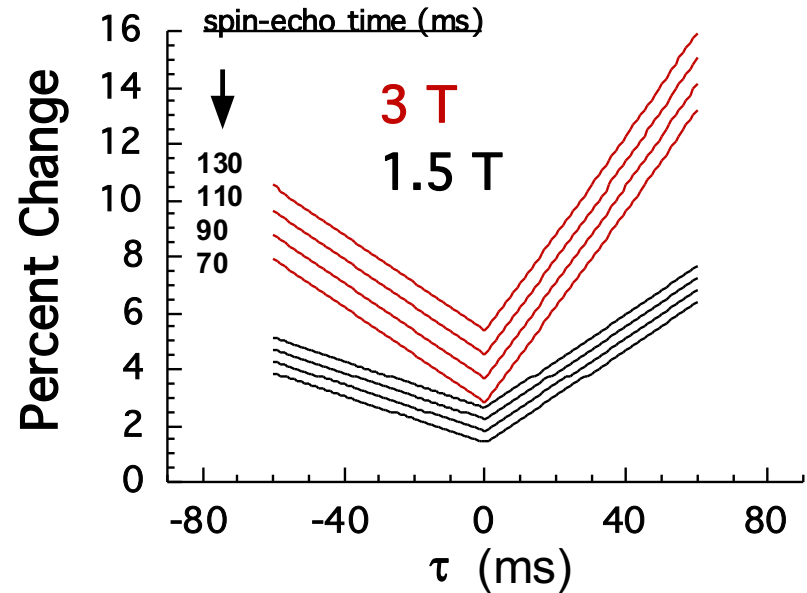
Asymmetric Spin - Echo



Gradient - Echo



Asymmetric Spin - Echo



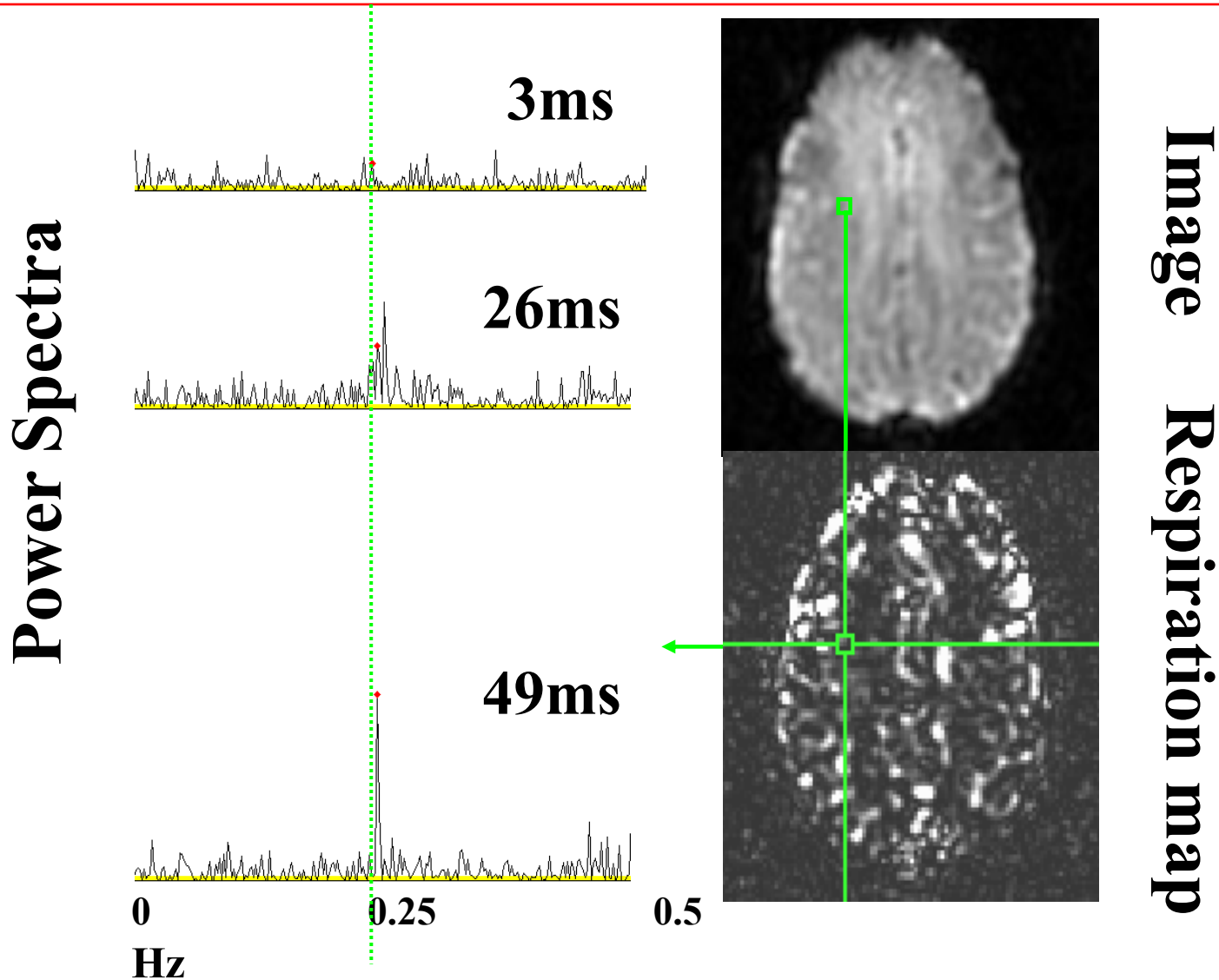
Maximizing Signal

- Higher B_0 Field
- Radio frequency Coils
- Choice of repetition time (TR)
- Voxel volume

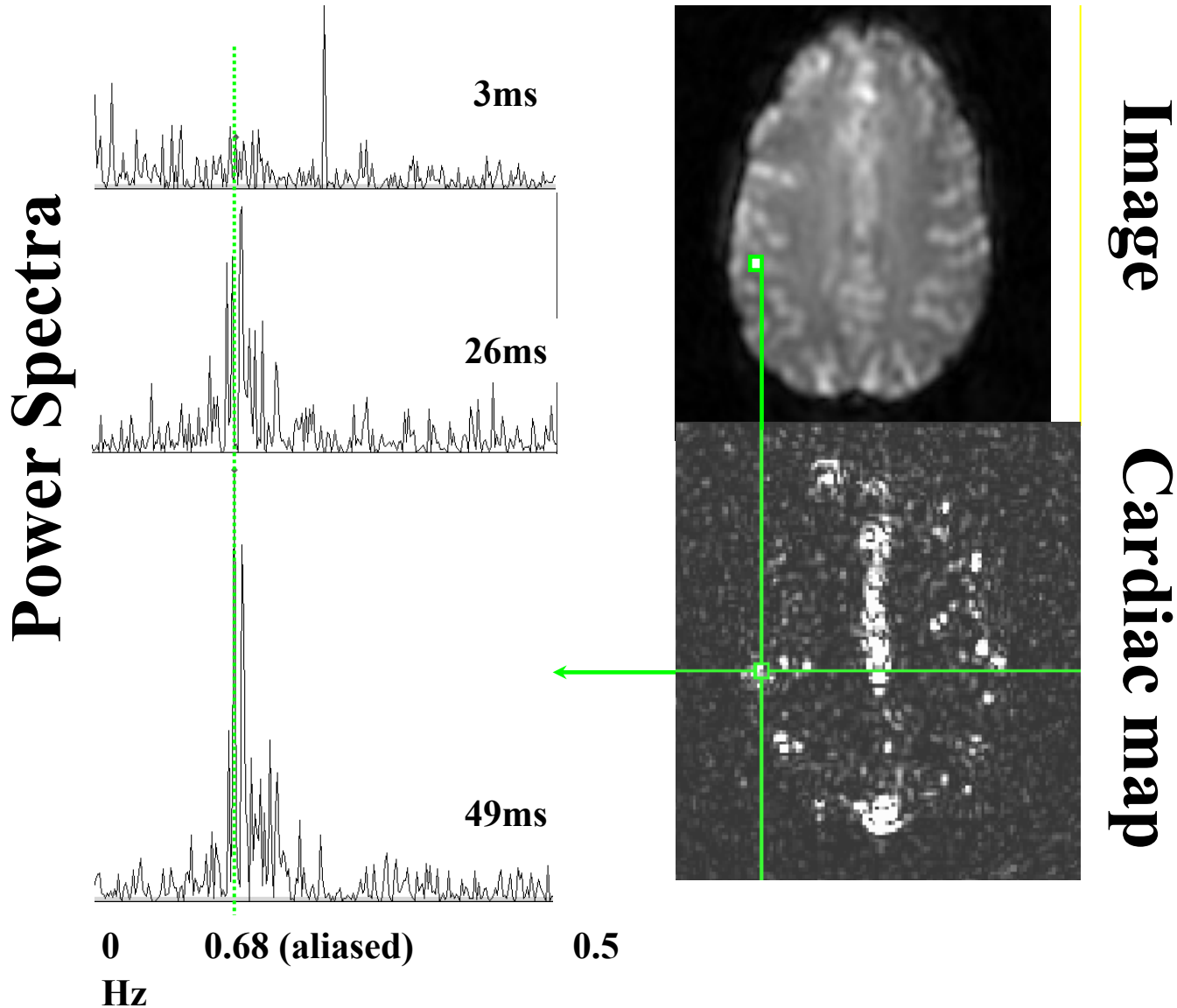
Physiologic Fluctuations

Cardiac	0.6 to 1.2 Hz
Respiratory	0.1 to 0.2 Hz
Low Frequency	0.0 to 0.1 Hz

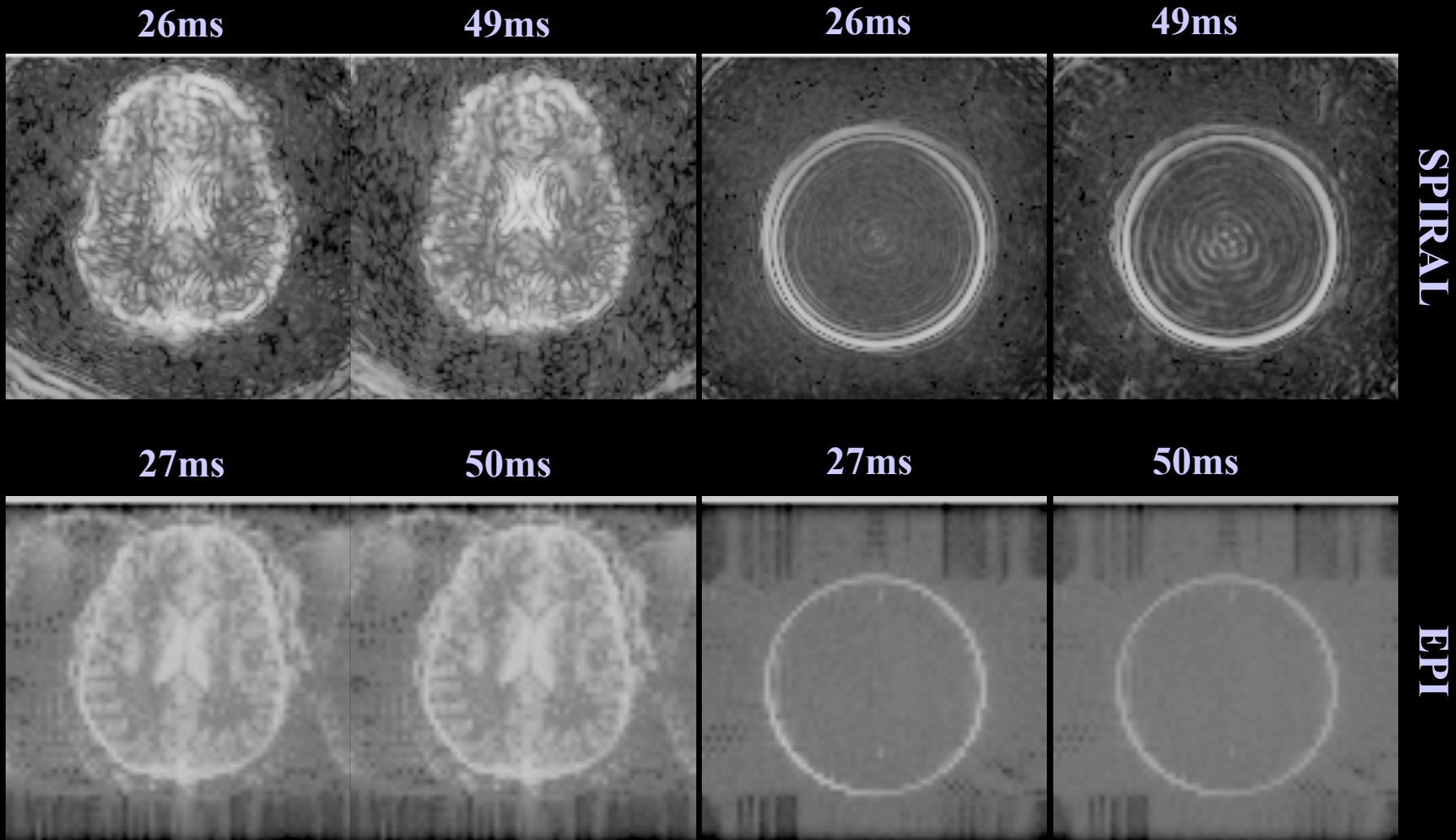
0.25 Hz Breathing at 1.5T



0.68 Hz Cardiac rate at 3T



Temporal vs. Spatial SNR- 3T



Reducing Physiologic Fluctuations

- Filtering
- Pulse sequence
 - single vs. multishot
 - strategies for multishot
- Gating with correction for variable TR

Temporal Artifacts

- System instabilities
- Motion
 - Drift
 - Stimulus correlated
 - Stimulus uncorrelated

Minimizing Temporal Artifacts

Recognize?

- Edge effects
- Shorter signal change latencies
- Unusually high signal changes
- External measuring devices

Correct?

- Image registration algorithms
- Orthogonalize to motion-related function (*cardiac, respiration, movement*)
- Navigator echo for k-space alignment
(*for multishot techniques*)
- Re-do scan

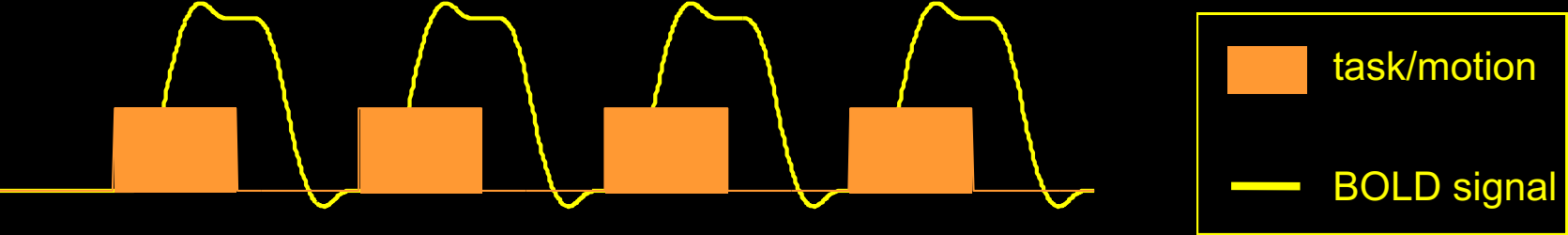
Bypass?

- Paradigm timing strategies..
- Gating (with T1-correction)

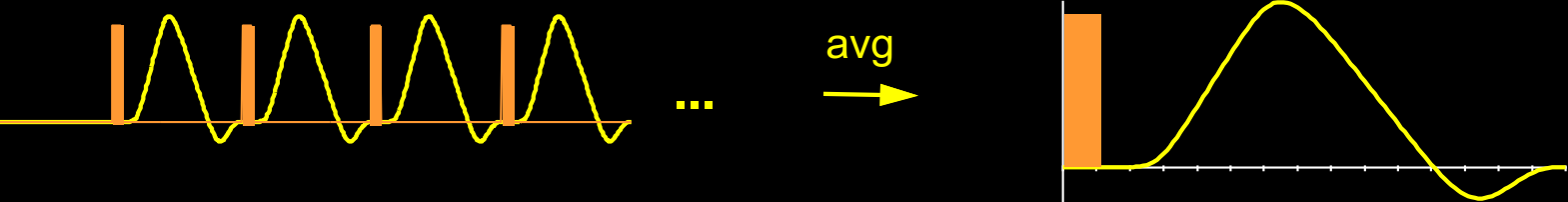
Suppress?

- Flatten image contrast
- Physical restraint
- Averaging, smoothing

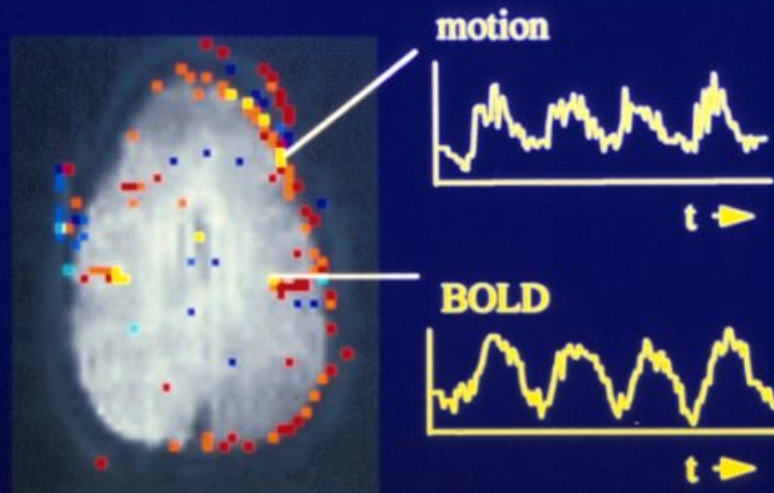
Block-trial



Single-trial (brief stimulus)

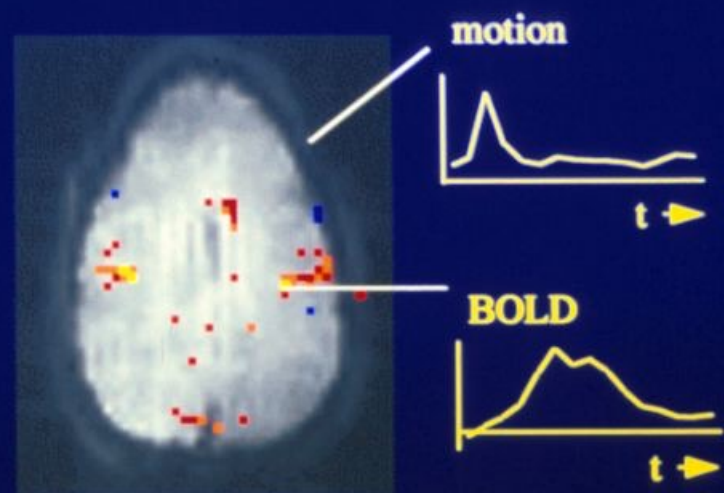


Motion-Decoupled fMRI: Functional MRI during of overt word production



“block-trial” paradigm

Motion induced signal changes resemble functional (BOLD) signal changes

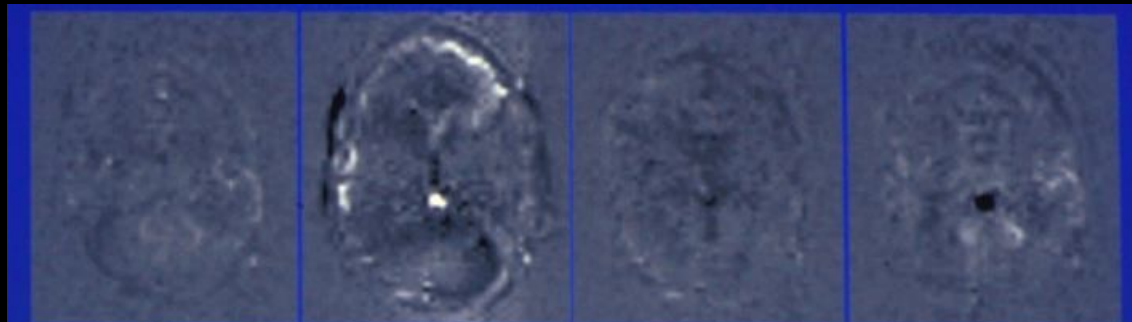


“single-trial” paradigm

Motion induced and BOLD signal changes are separated in time

R.M. Birn, et al.

Overt Word Production



2

3

4

5



6

7

8

9



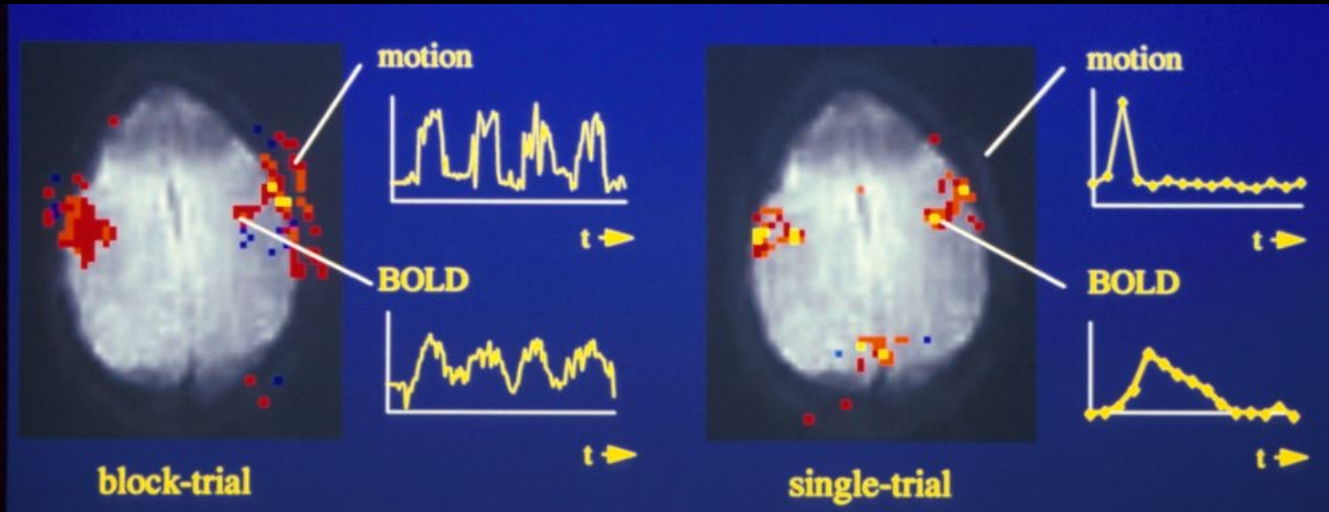
10

11

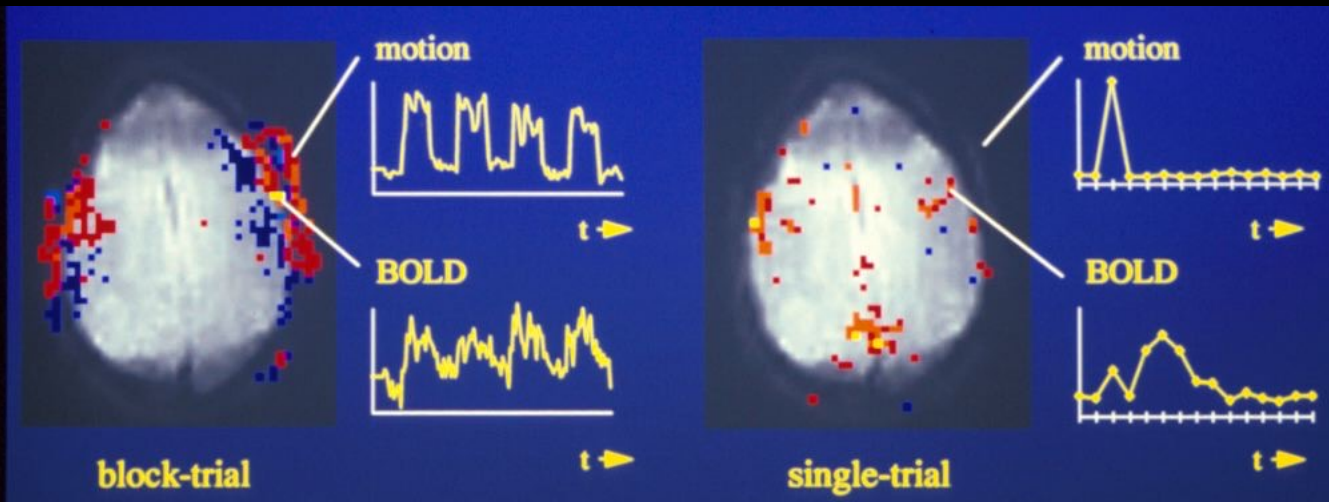
12

13

Tongue Movement



Jaw Clenching



Variables to Optimize

- Information Content
- Sensitivity
- Speed
- Resolution
- Image quality

Speed

- Rapid imaging techniques:

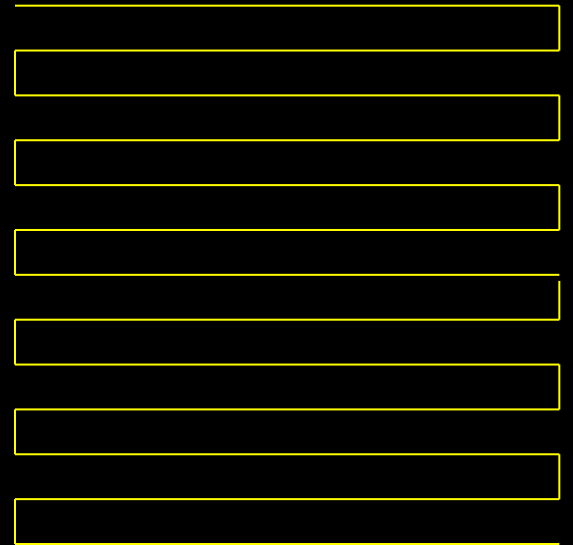
- Single shot imaging
- TR vs. Brain coverage:

$$\text{min TR} = (\text{time/slice}) \times \text{number of slices in volume}$$

- Hemodynamic Issues

- Paradigm timing
- Event related fMRI
- Timing modulation

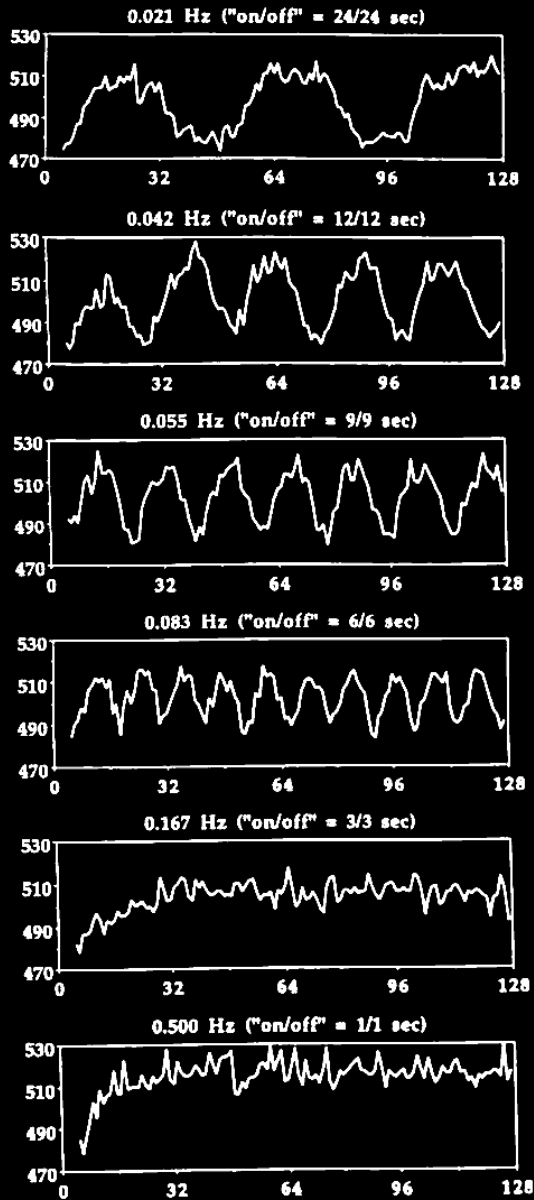
Single Shot Imaging



EPI Readout Window

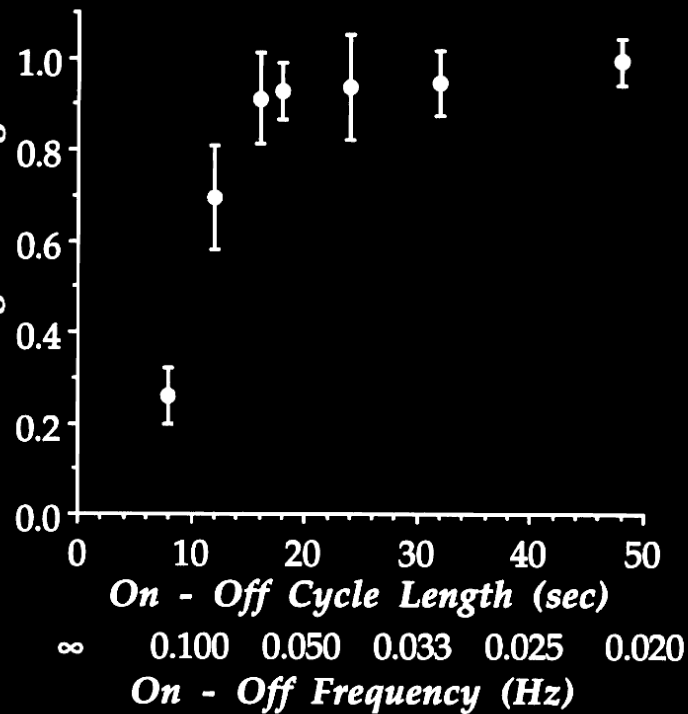
≈ 20 to 40 ms

MRI Signal

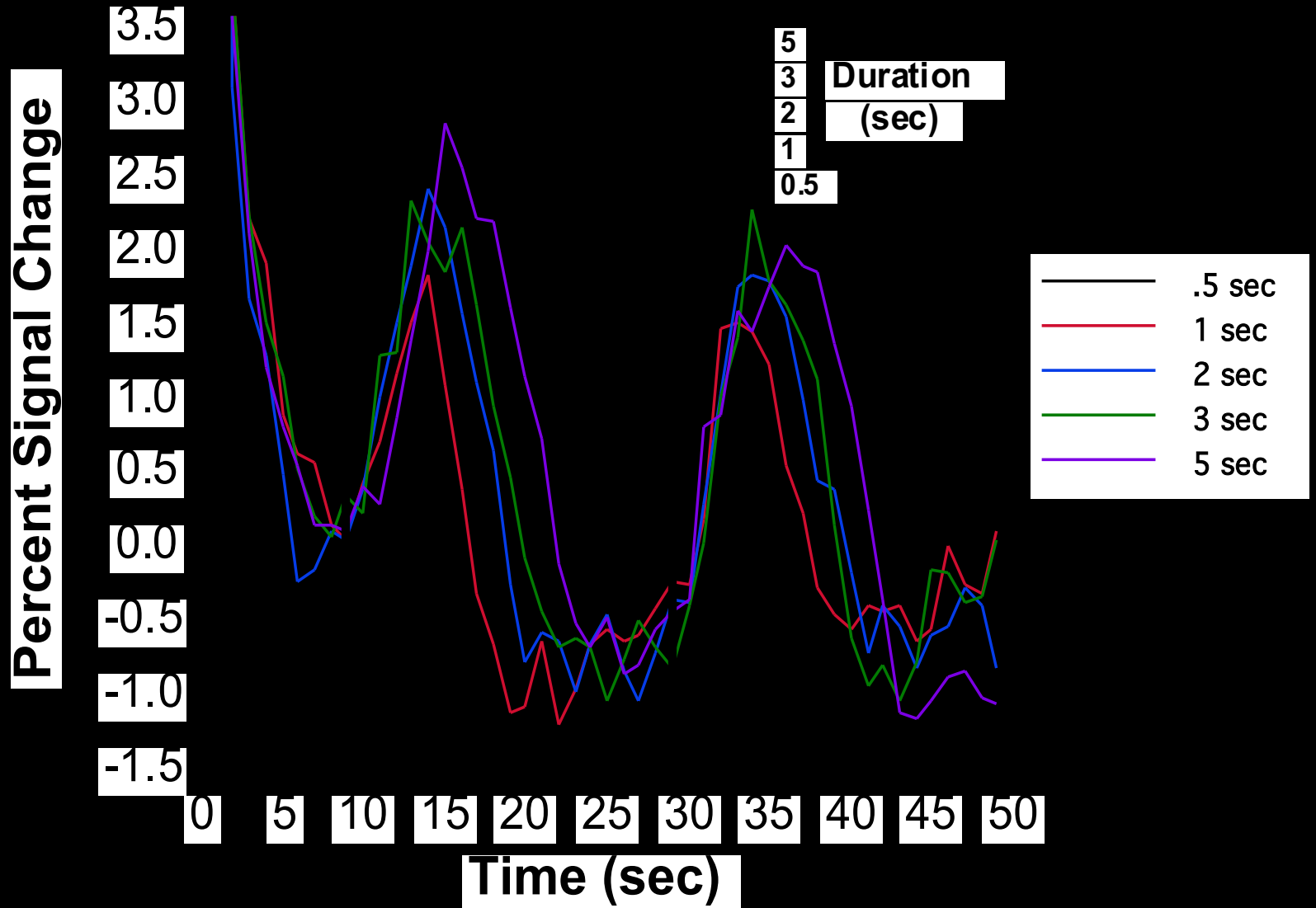


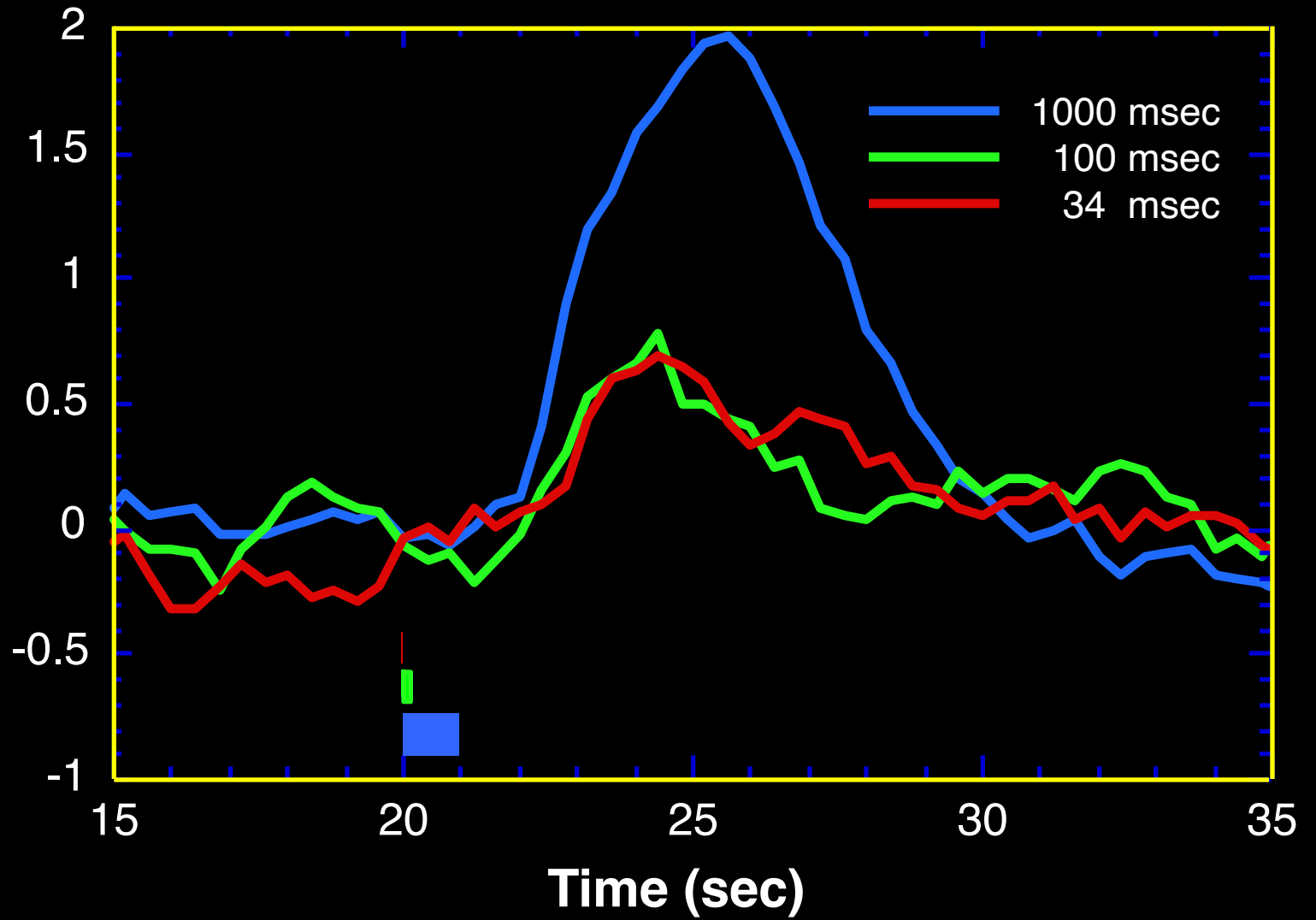
Time (seconds)

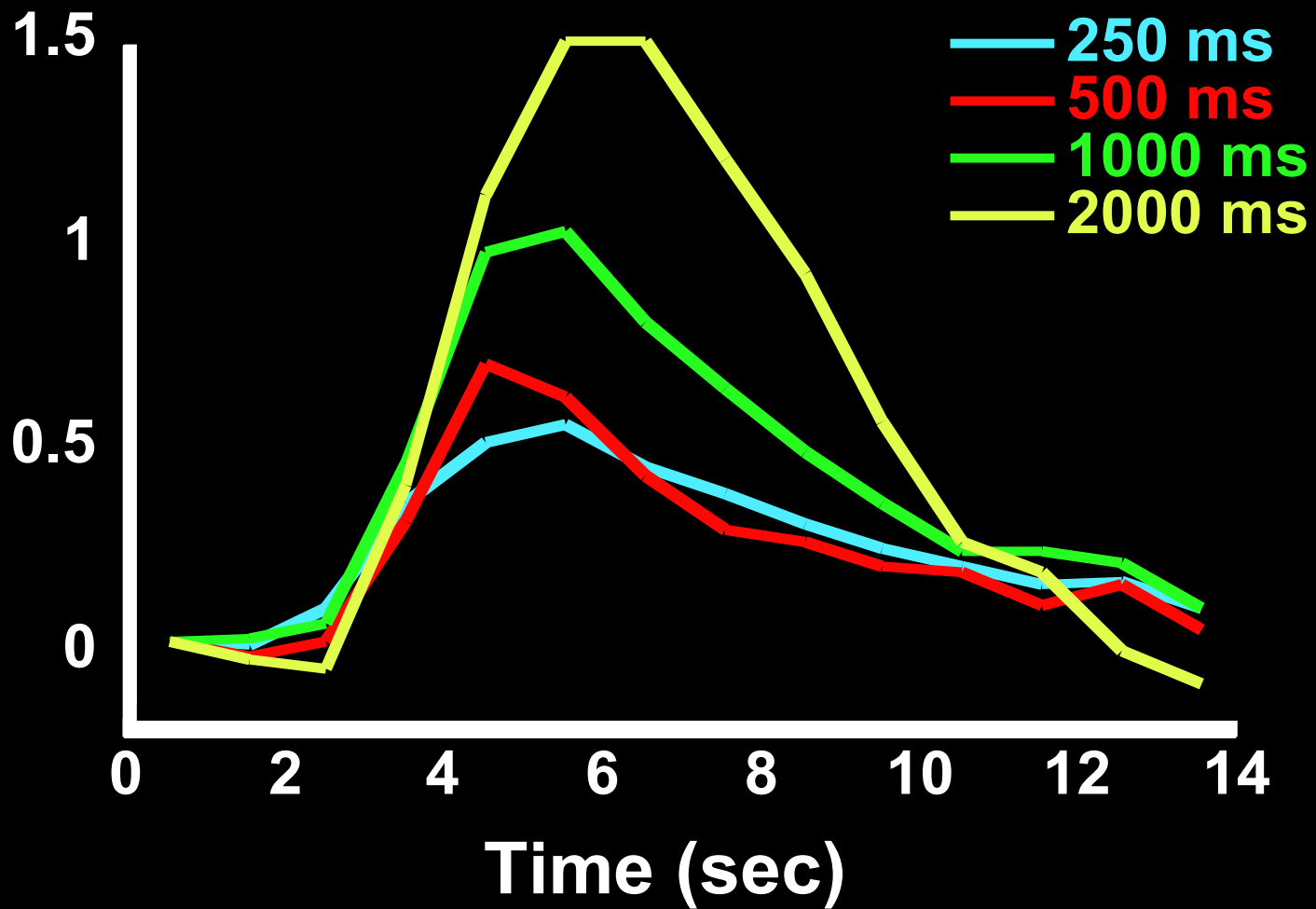
Relative Activation - Induced
MR Signal Change



Motor Cortex

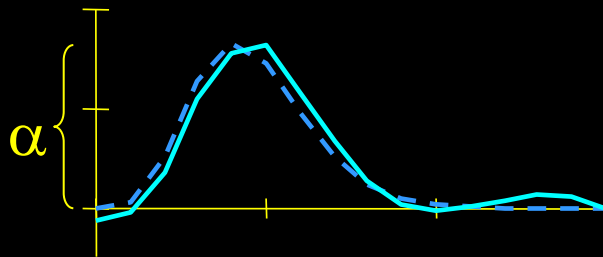






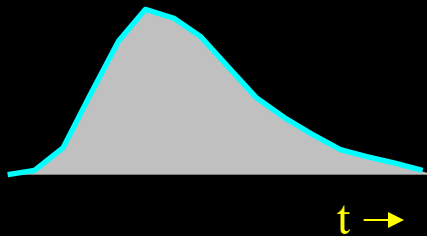
Compute nonlinearity *(for each voxel)*

- Amplitude of Response



Fit ideal (linear) to response

- Area under response / Stimulus Duration



Output Area / Input Area

Nonlinearity

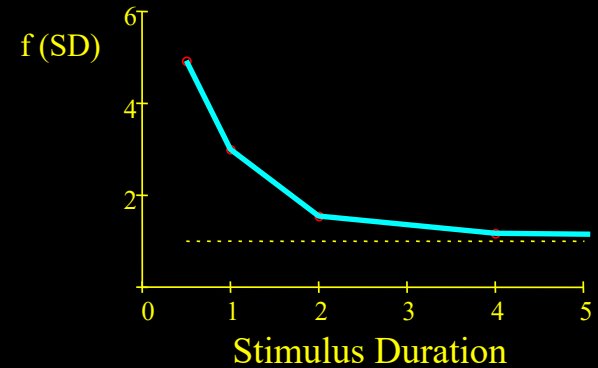
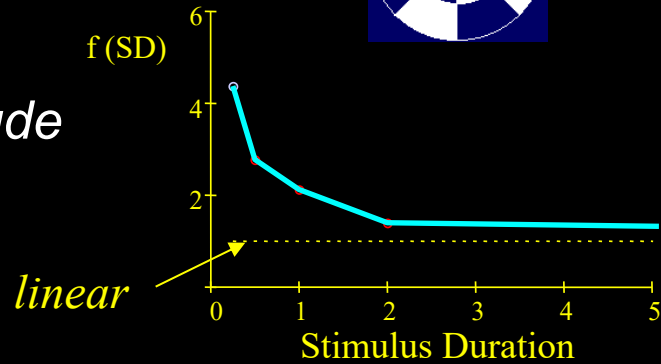
Visual



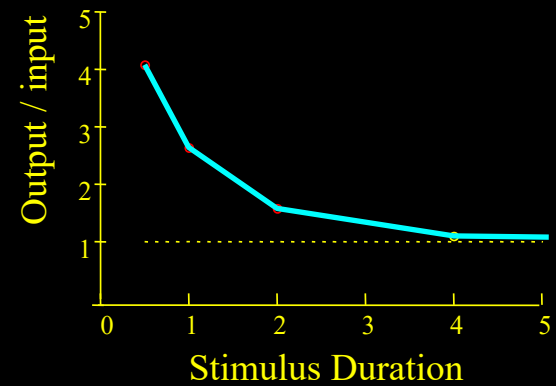
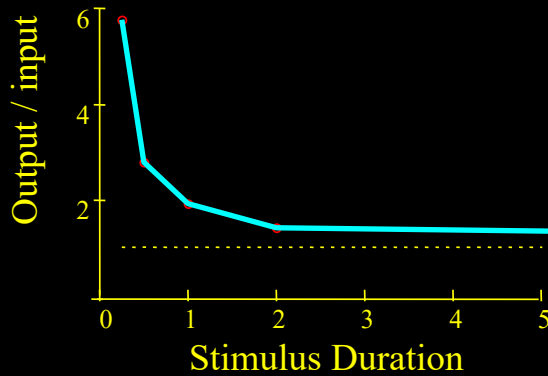
Motor



Magnitude

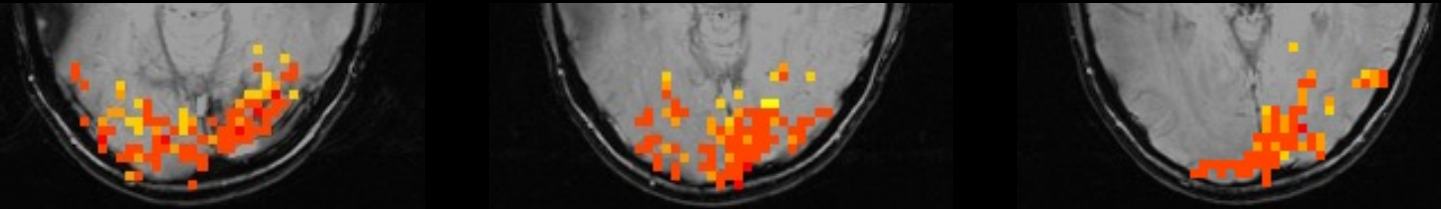


Area

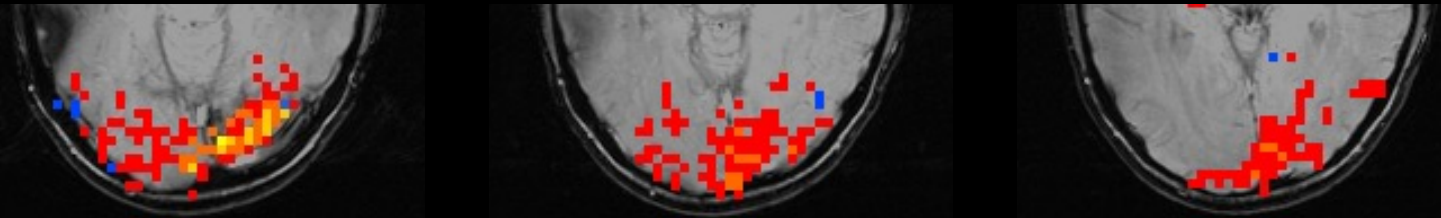


Results – visual task

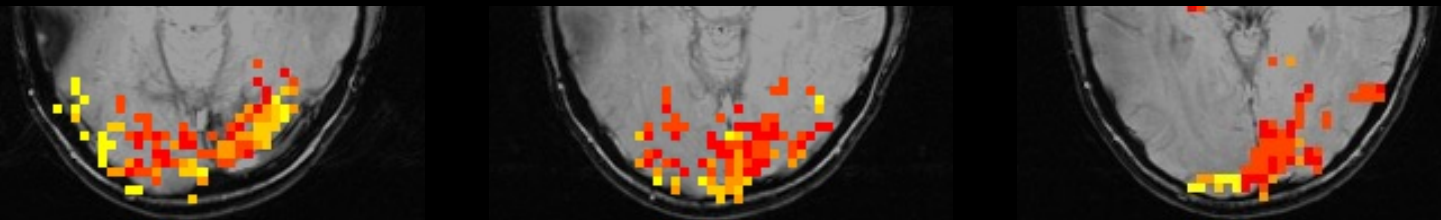
Nonlinearity



Magnitude

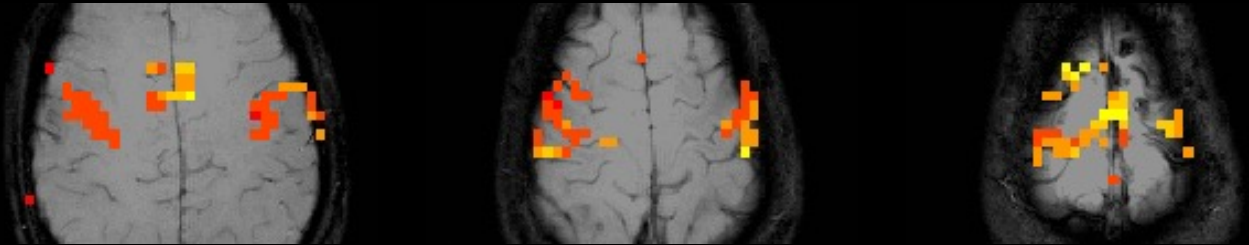


Latency

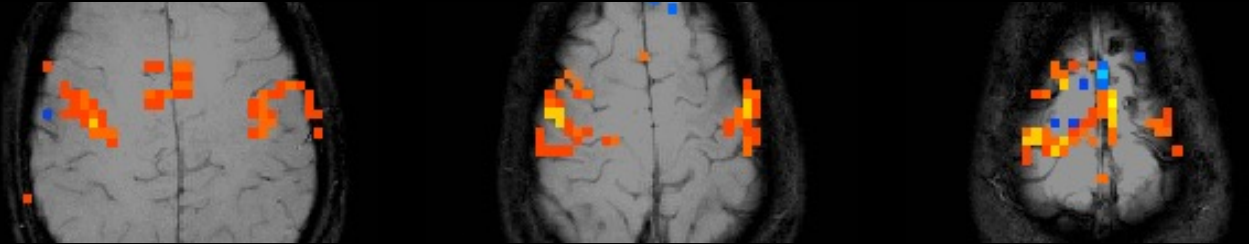


Results – motor task

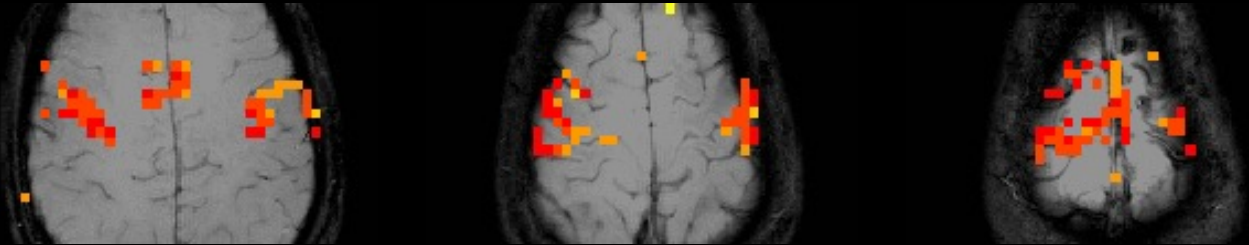
Nonlinearity



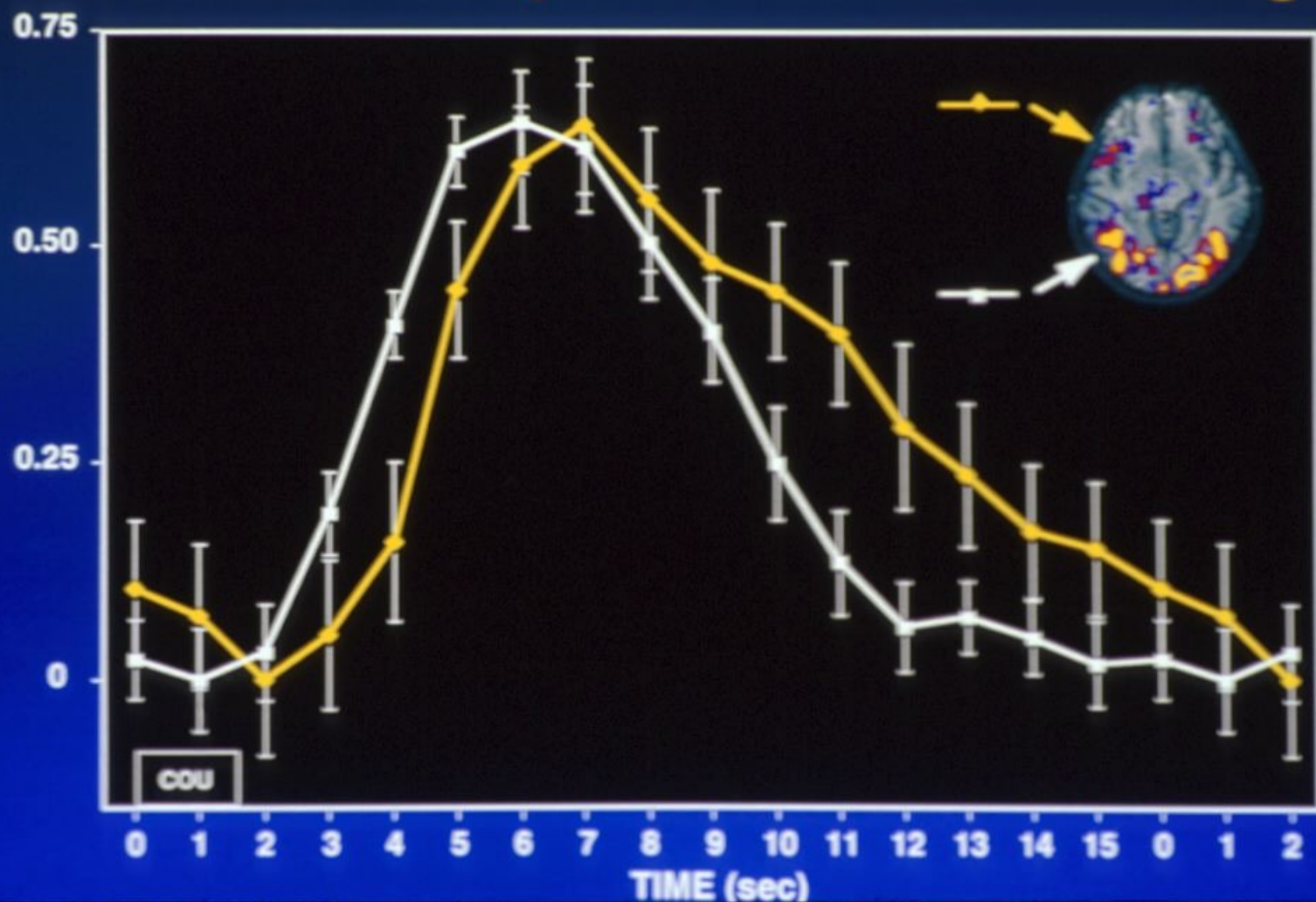
Magnitude



Latency



Time Course Comparison Across Brain Regions



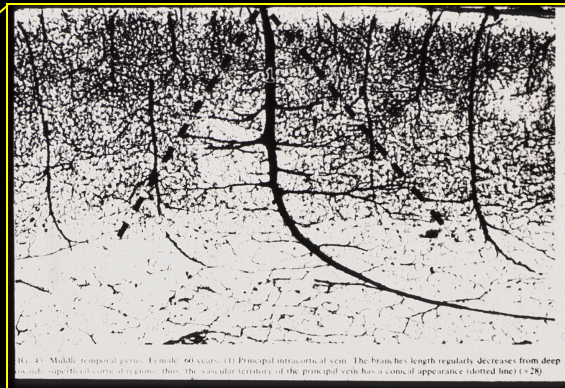
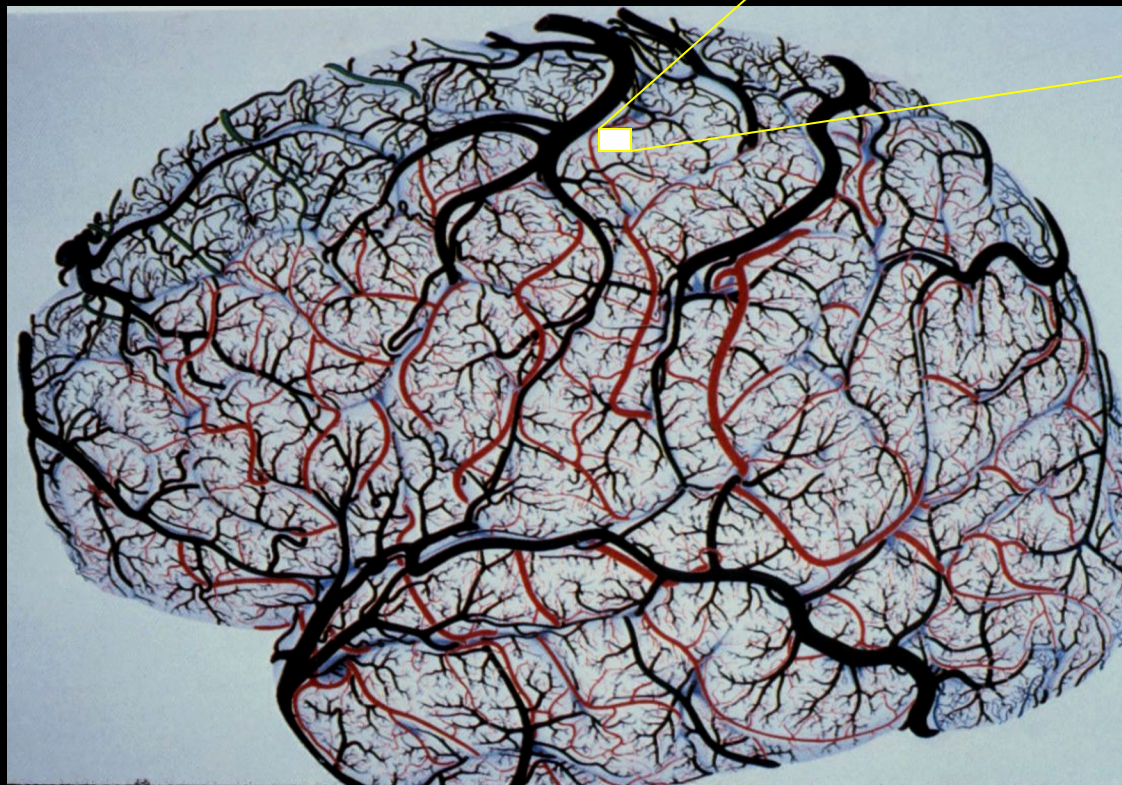
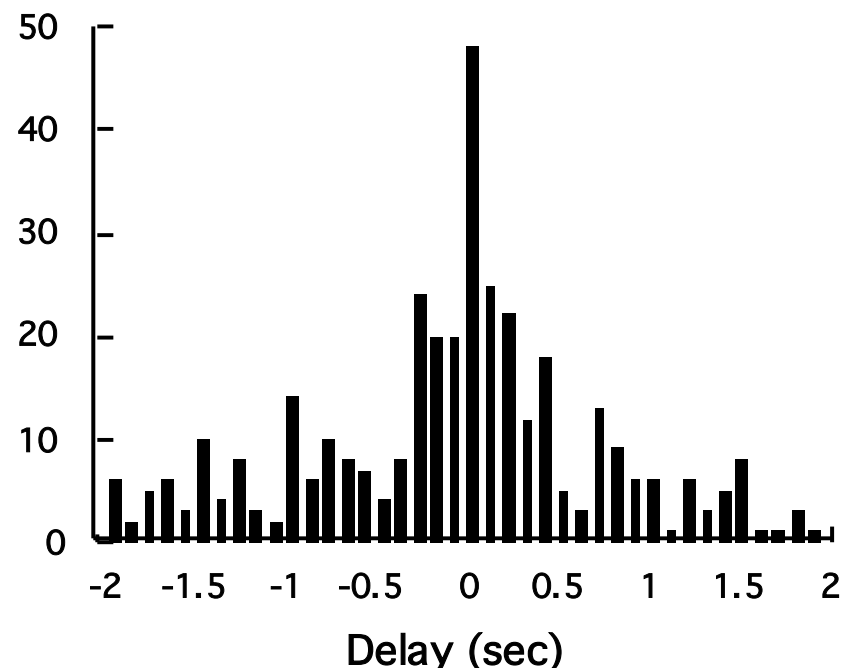
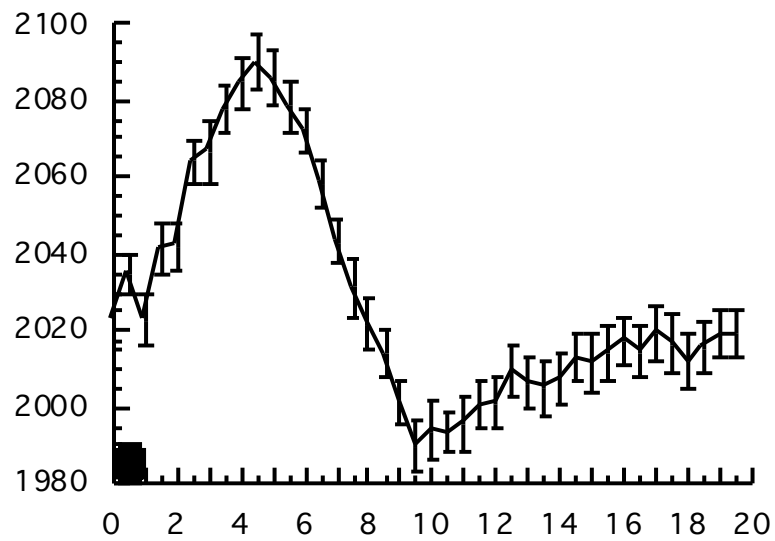
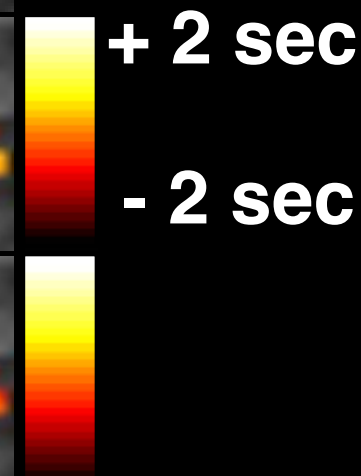
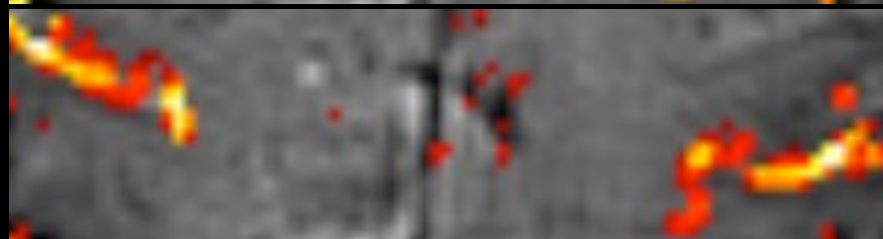
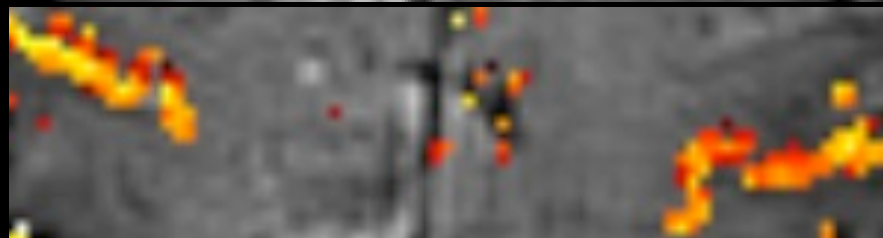


Fig. 41. Middle temporal gyrus. Female, 90 years. (1) Principal intracortical vein. The branches length regularly decreases from deep toward superficial cortical layers. Thus, the vascular territory of the principal vein has a conical appearance (slotted line) (p. 28).

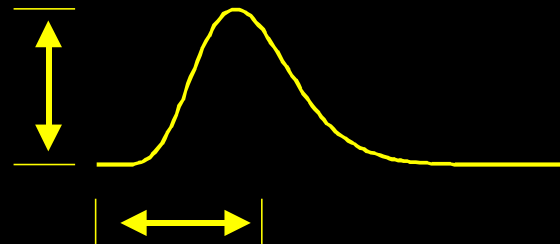
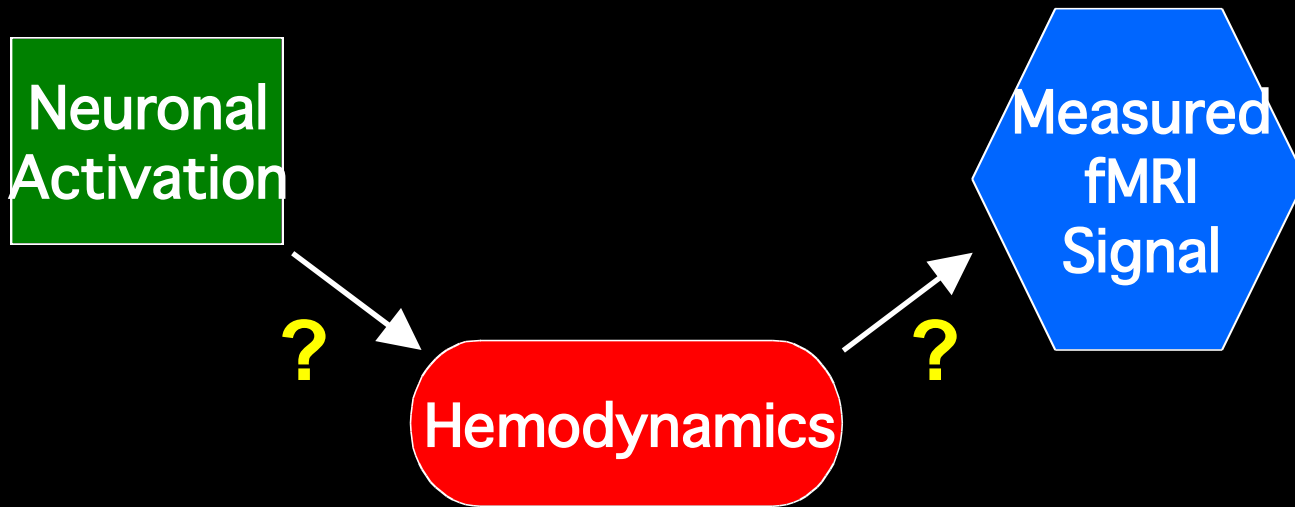
Latency

Magnitude



Temporal Normalization

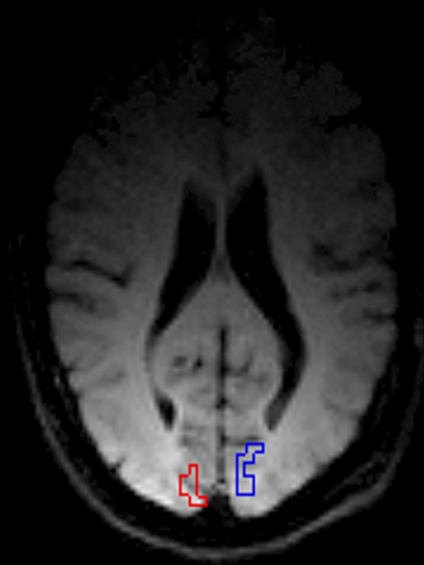
Relative Timing



Physiologic Factors

Regions of Interest Used for Hemi-Field Experiment

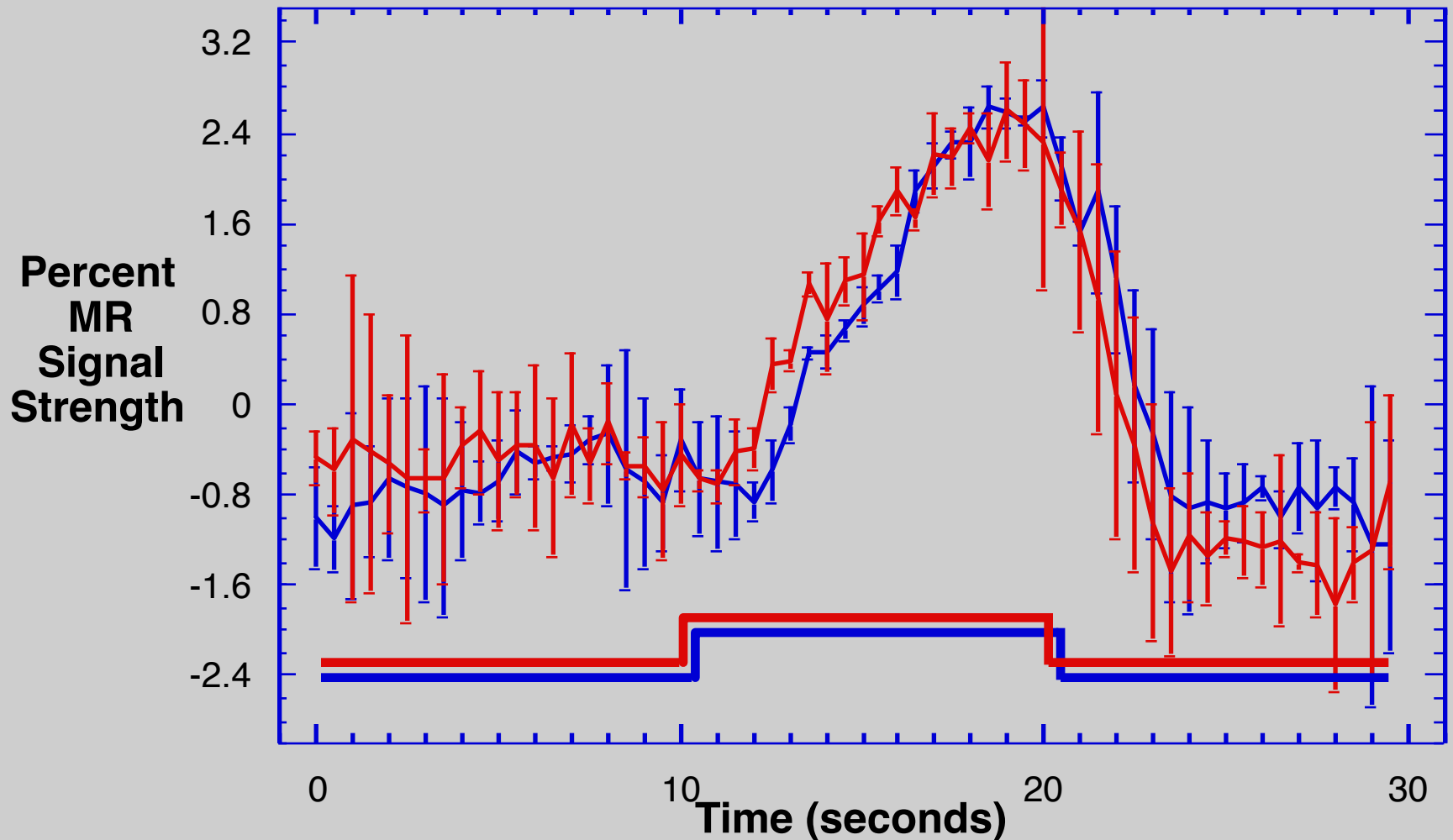
**Right
Hemisphere**



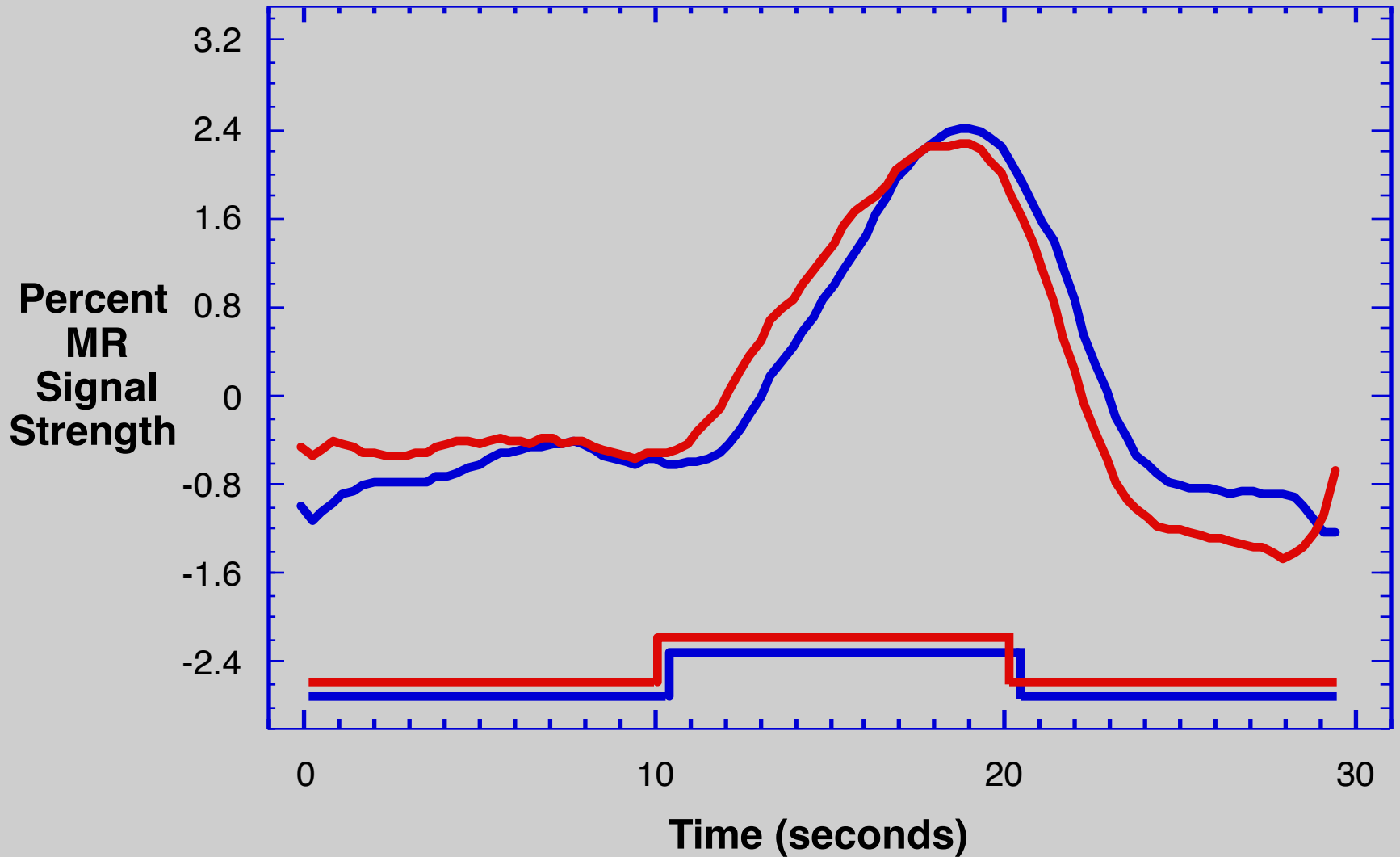
**Left
Hemisphere**

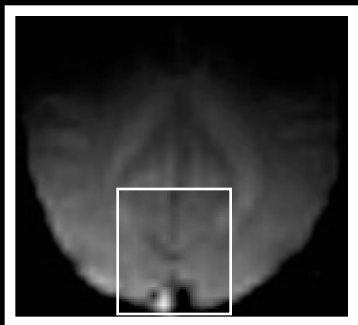
Hemi-field with 500 msec asynchrony

Average of 6 runs Standard Deviations Shown



Average of 6 runs Smoothed Data





500 ms



500 ms



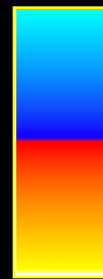
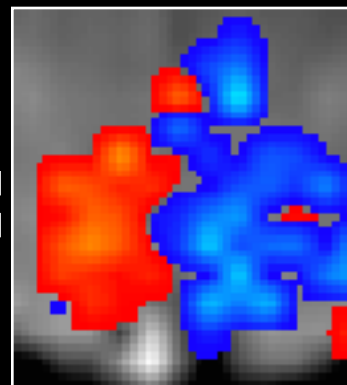
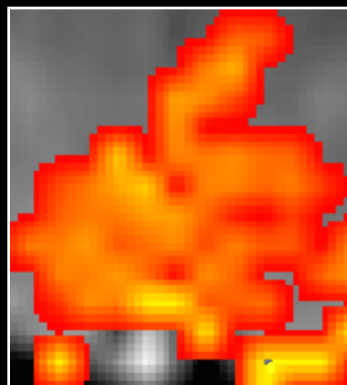
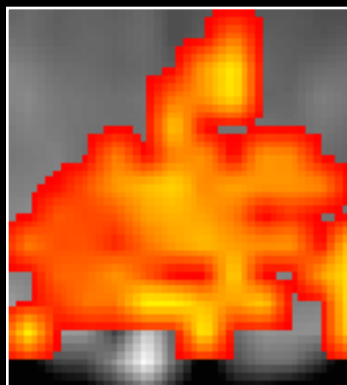
Right Hemifield

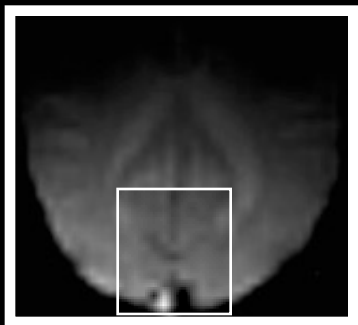
Left Hemifield

+ 2.5 s

0 s

- 2.5 s





250 ms

||



250 ms

||



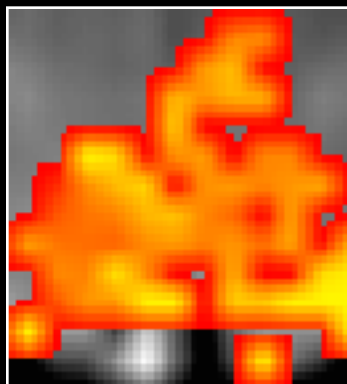
Right Hemifield

Left Hemifield

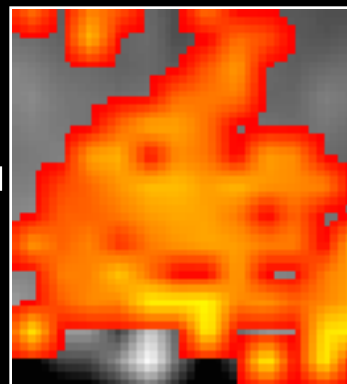
+ 2.5 s

0 s

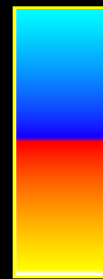
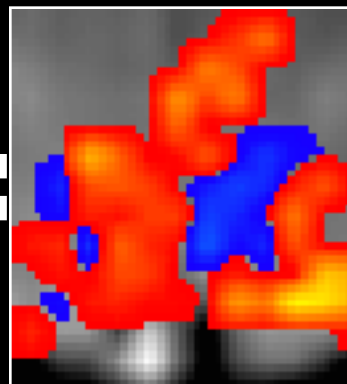
- 2.5 s



-



=



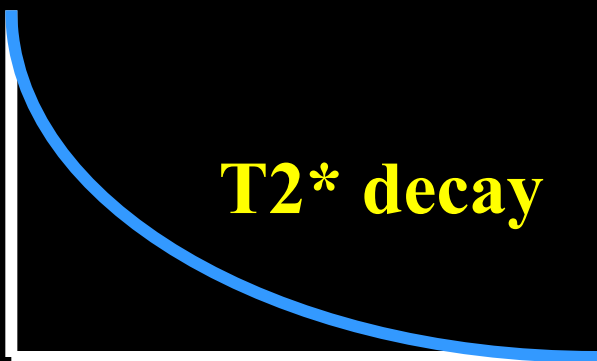
Variables to Optimize

- Information Content
- Sensitivity
- Acquisition Speed
- Resolution
- Image quality

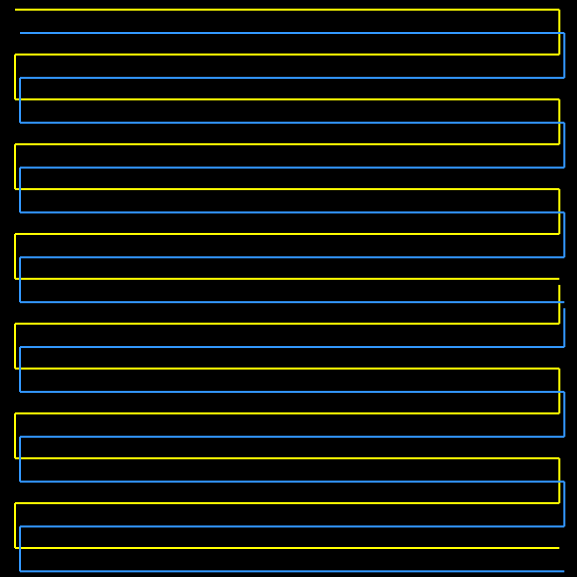
Multishot Imaging



EPI Window 1



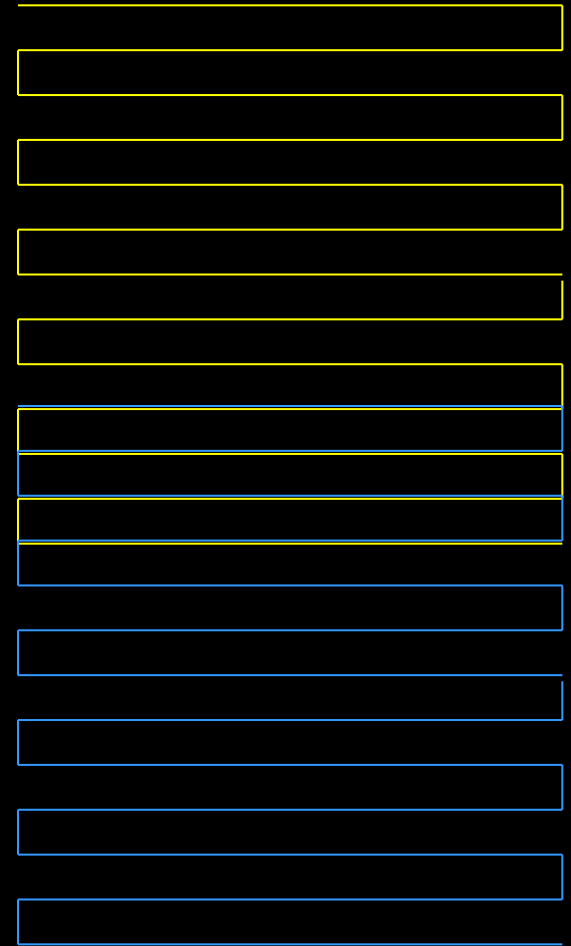
EPI Window 2



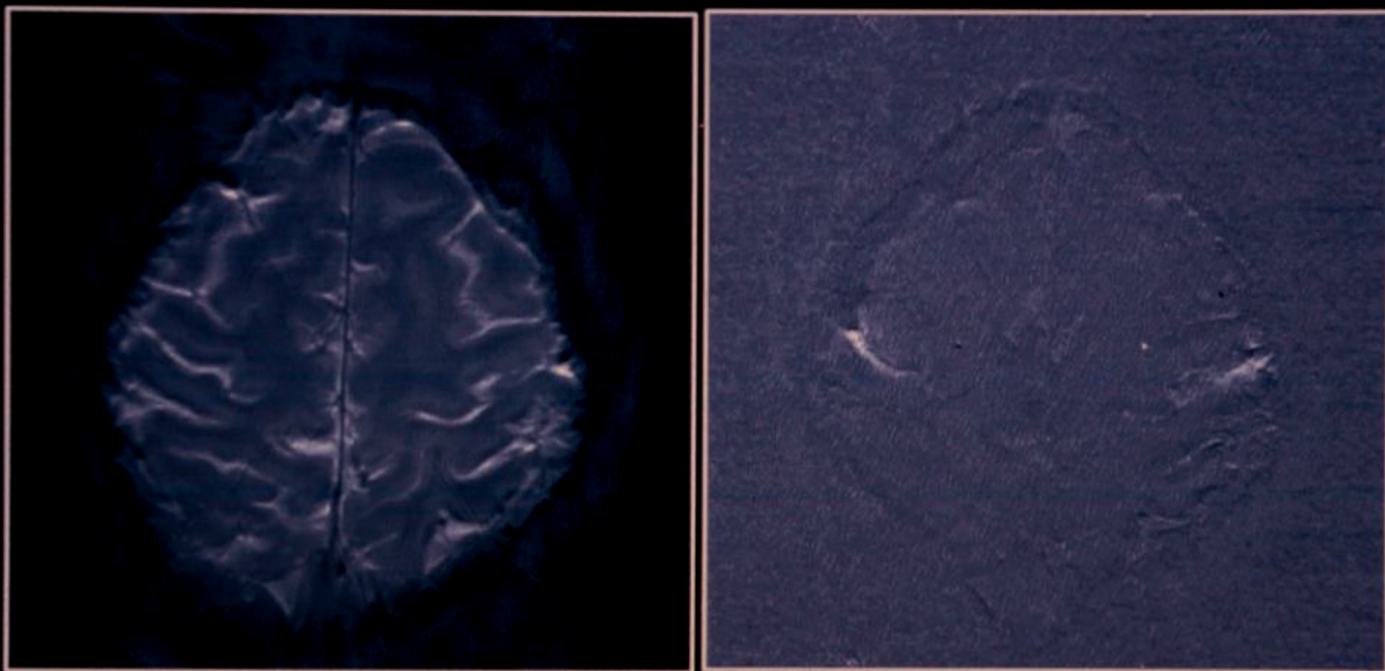
Partial k-space imaging



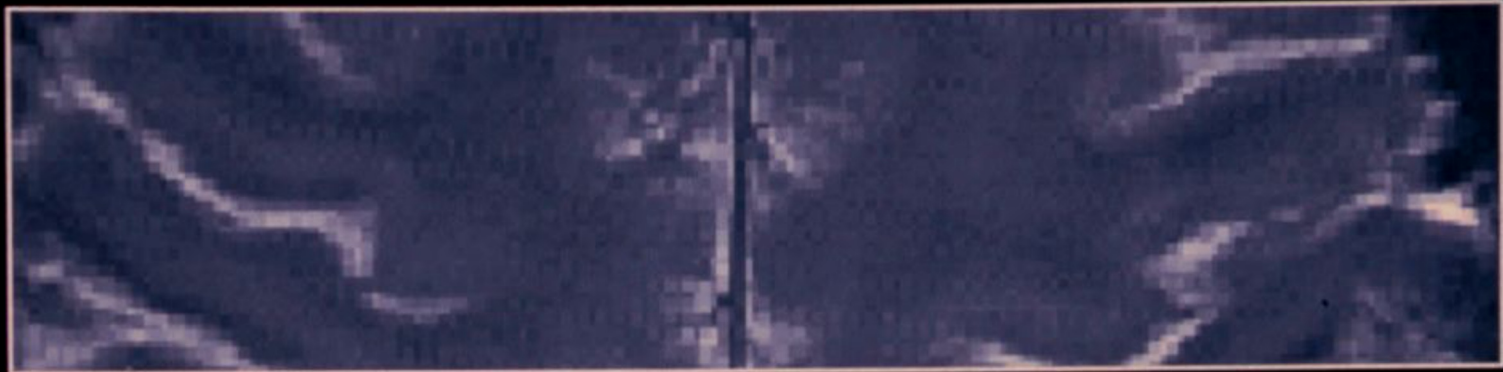
EPI Window



**Single - Shot EPI at 3T:
Half NEX, 256 x 256, 16 cm FOV**



**Single - Shot EPI at 3T:
Half NEX 256 x 256, 16 cm FOV**



Multi Shot EPI

Excitations
Matrix Size

1

64 x 64

2

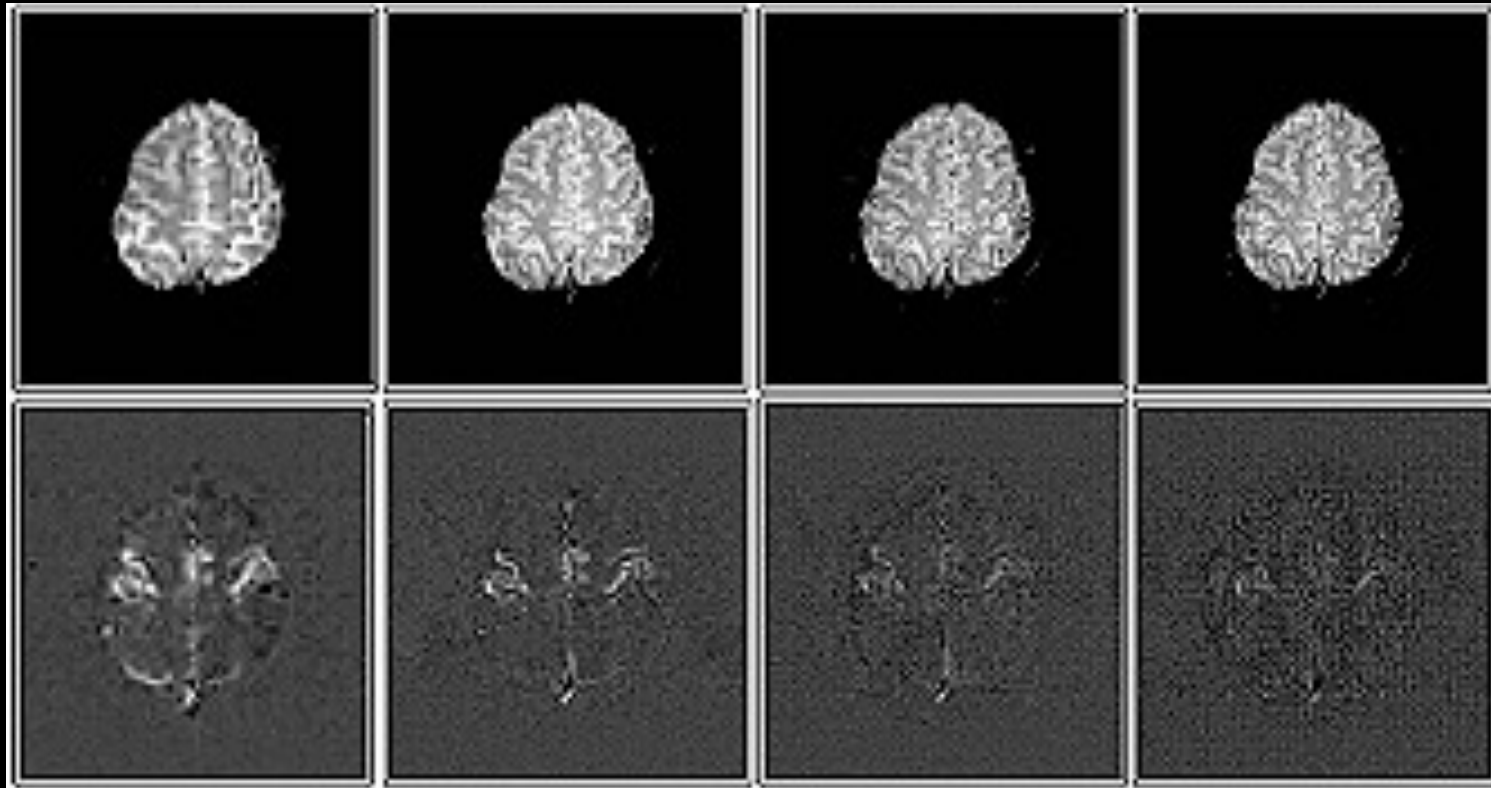
128 x 128

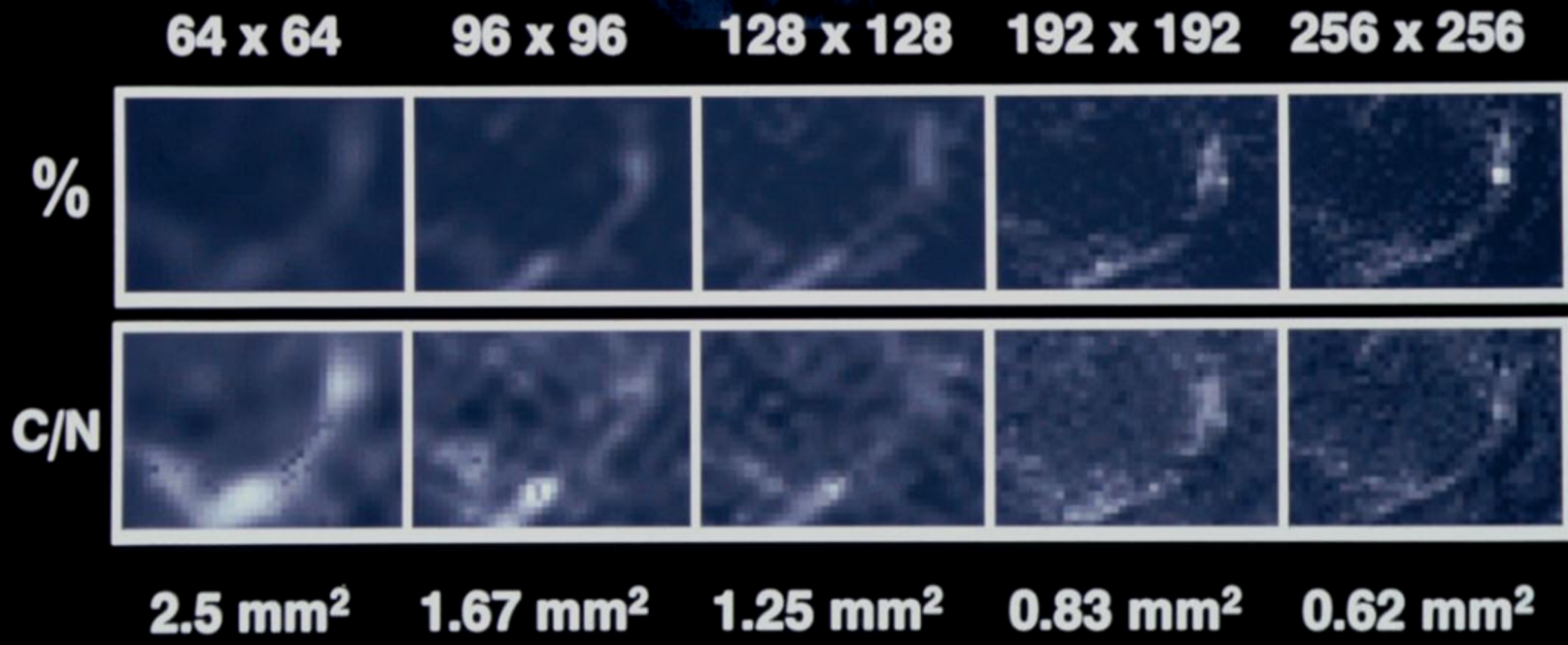
4

256 x 128

8

256

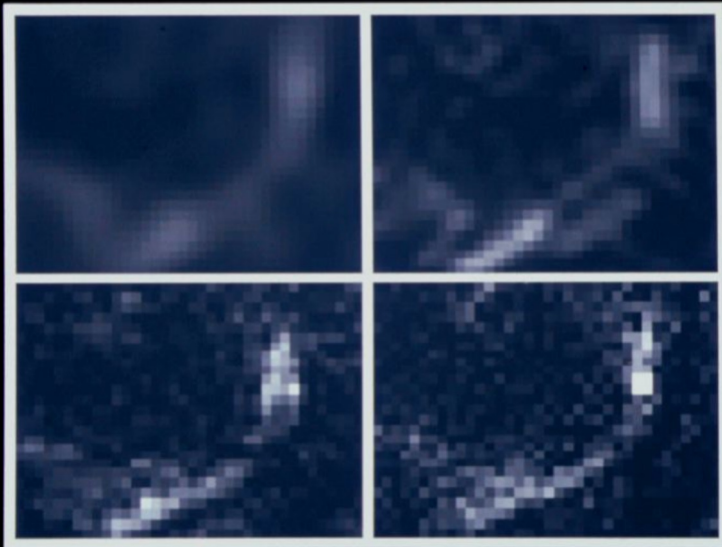




Fractional Signal Change

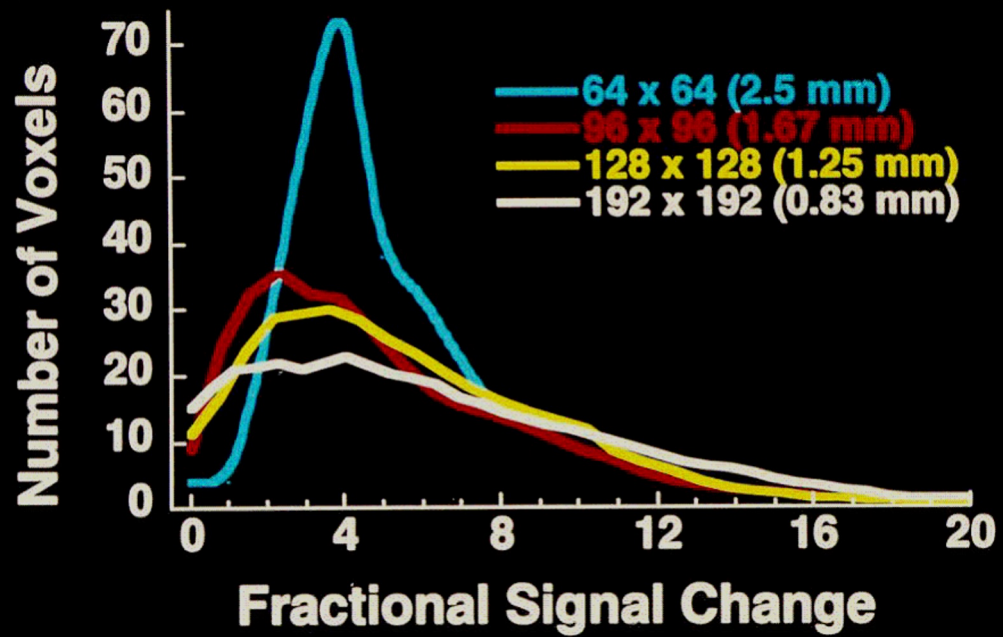
2.5 mm²

1.25 mm²

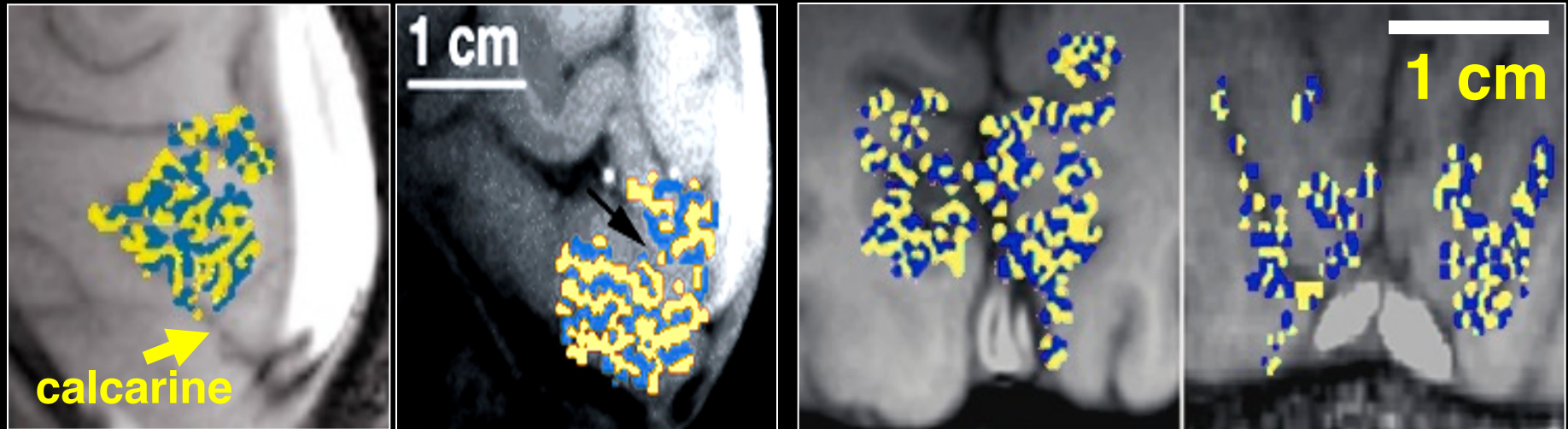


0.83 mm²

0.62 mm²



ODC Maps using fMRI



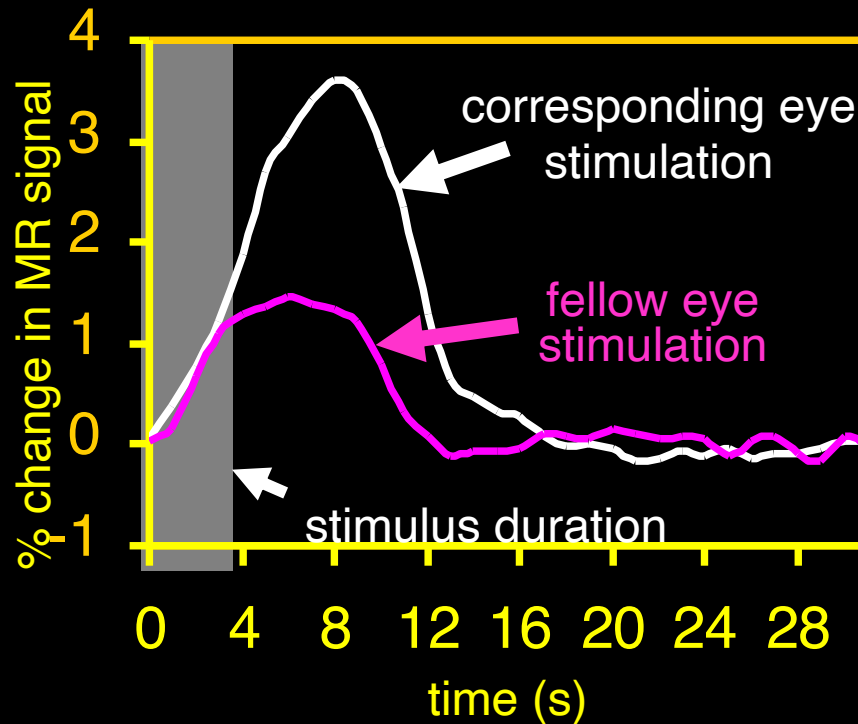
- Identical in size, orientation, and appearance to those obtained by optical imaging¹ and histology^{3,4}.

¹Malonek D, Grinvald A. *Science* 272, 551-4 (1996).

³Horton JC, Hocking DR. *J Neurosci* 16, 7228-39 (1996).

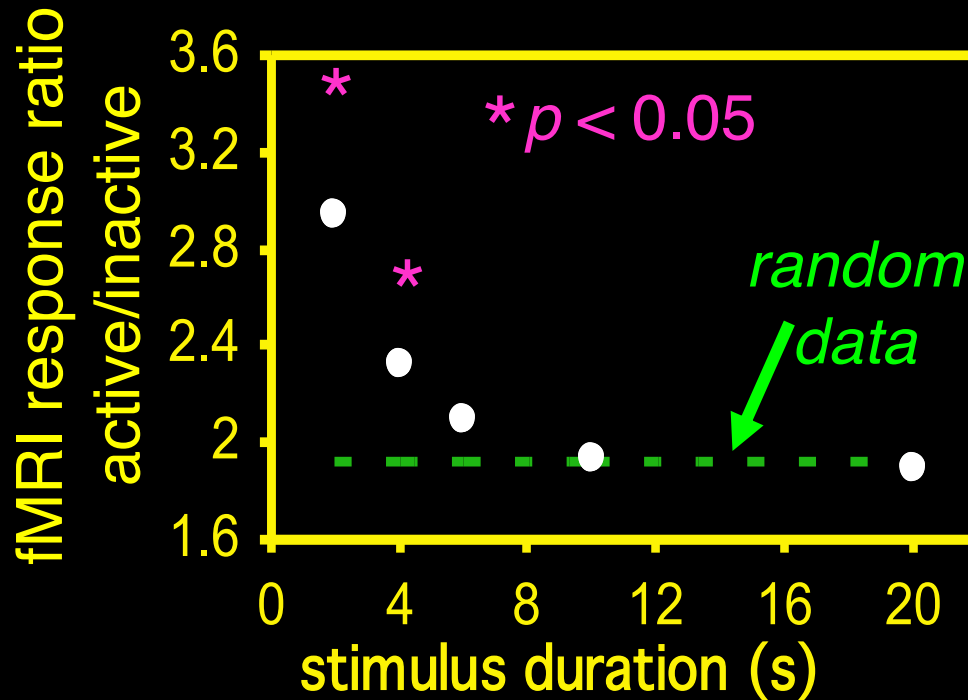
⁴Horton JC, et al. *Arch Ophthalmol* 108, 1025-31 (1990).

fMRI Timecourse within an ODC



- For a 4 second stimulus, the hyperoxic response does not saturate (i.e., does not reach a plateau).
- The ratio of the peak magnitudes of the fMRI responses is nearly 3:1.

Experiment 2: Stimulus Duration



- The saturation of the hyperoxic response does not permit reliable mapping of ODCs.
- ODC maps obtained using the hyperoxic phase of the BOLD fMRI signal *are* reliable when stimulus duration is 4 seconds or less.

Variables to Optimize

- Information Content
- Sensitivity
- Speed
- Resolution
- Image quality

Image Quality

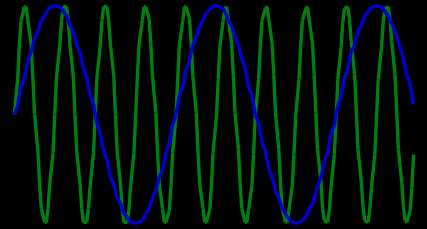
- **Minimizing warping**
 - Shimming
 - Reduced readout window duration

- **Minimizing dropout**
 - Shimming
 - Reduced TE
 - Adjust slice orientation
 - Increase resolution

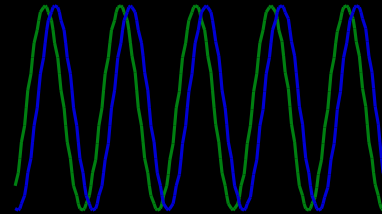
Neuronal Activation Input Strategies

1. Block Design

2. Frequency Encoding

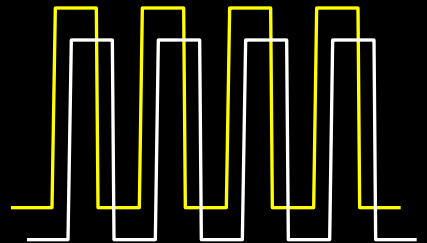


3. Phase Encoding



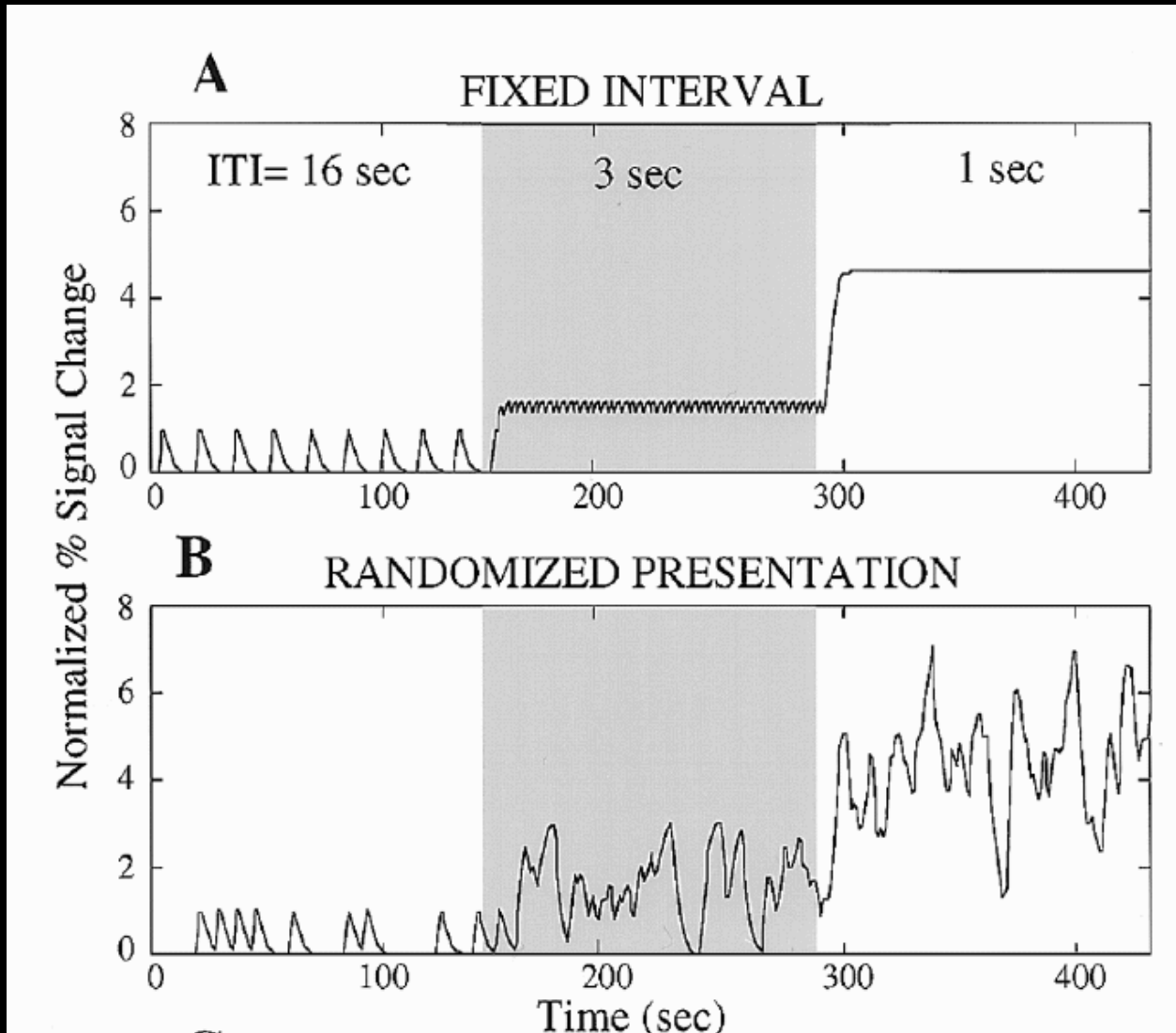
4. Event Related

5. Orthogonal Block Design



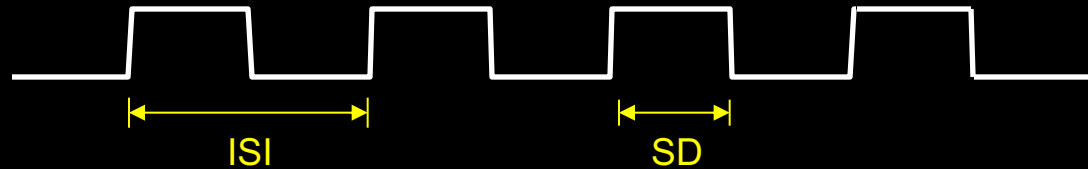
6. Free behavior Design.

M.A. Burock et al. *NeuroReport*, 9, 3735-9 (1998)

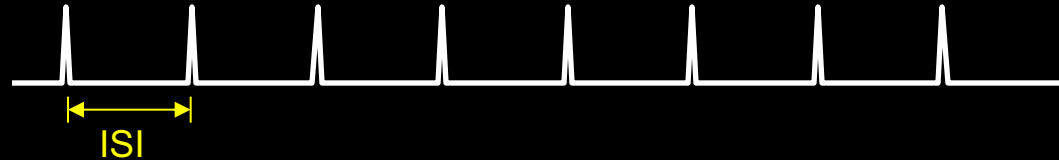


Definitions

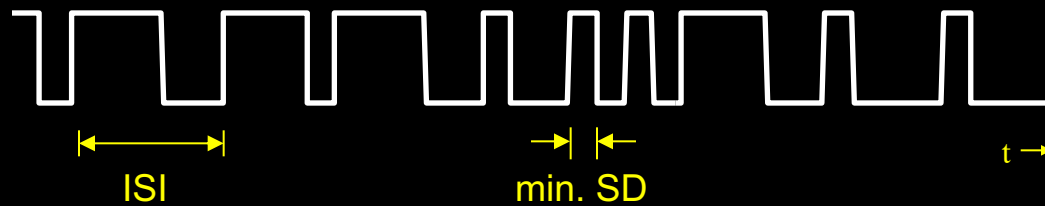
Blocked
Trial



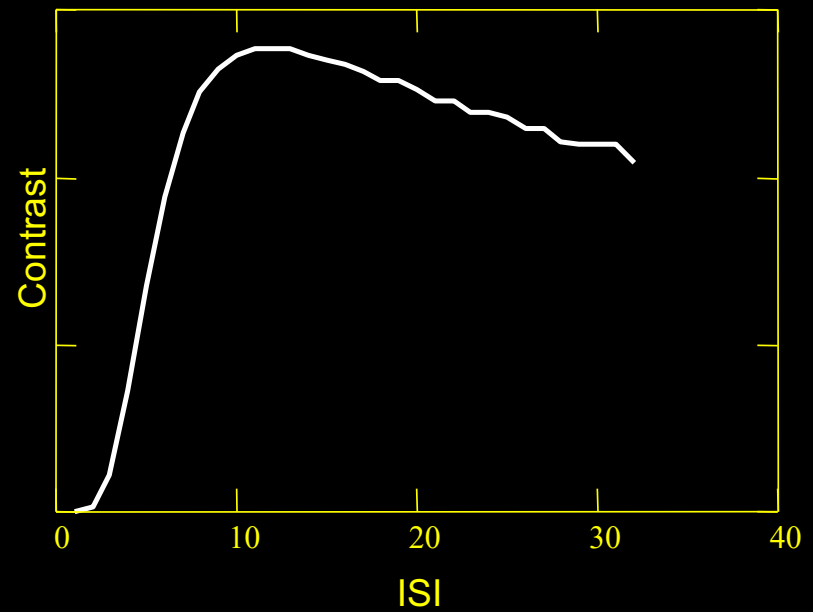
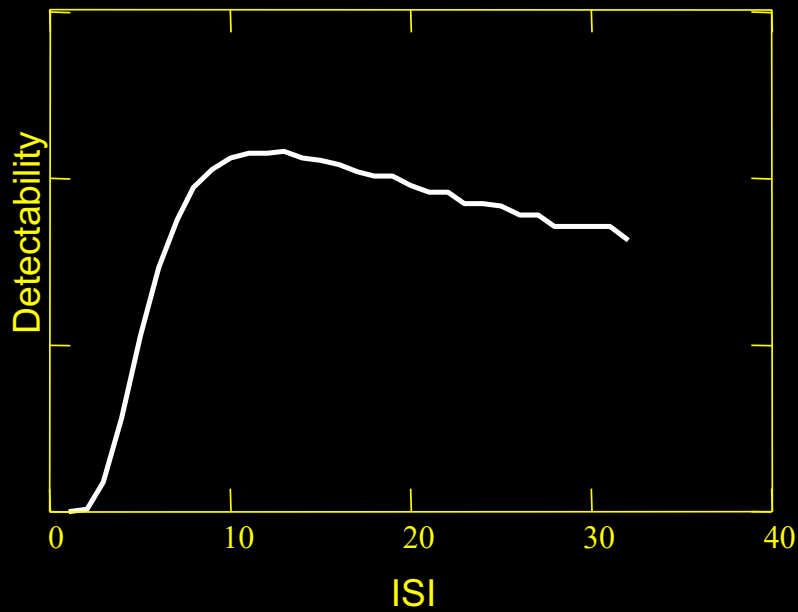
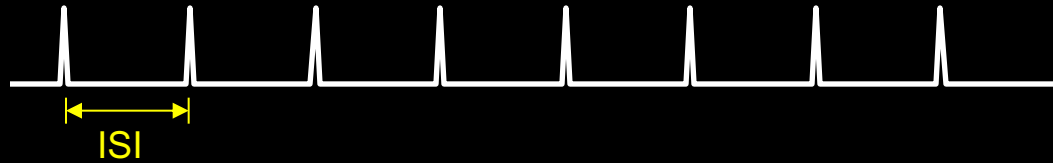
Event-Related
Constant ISI



Event-Related
Variable ISI

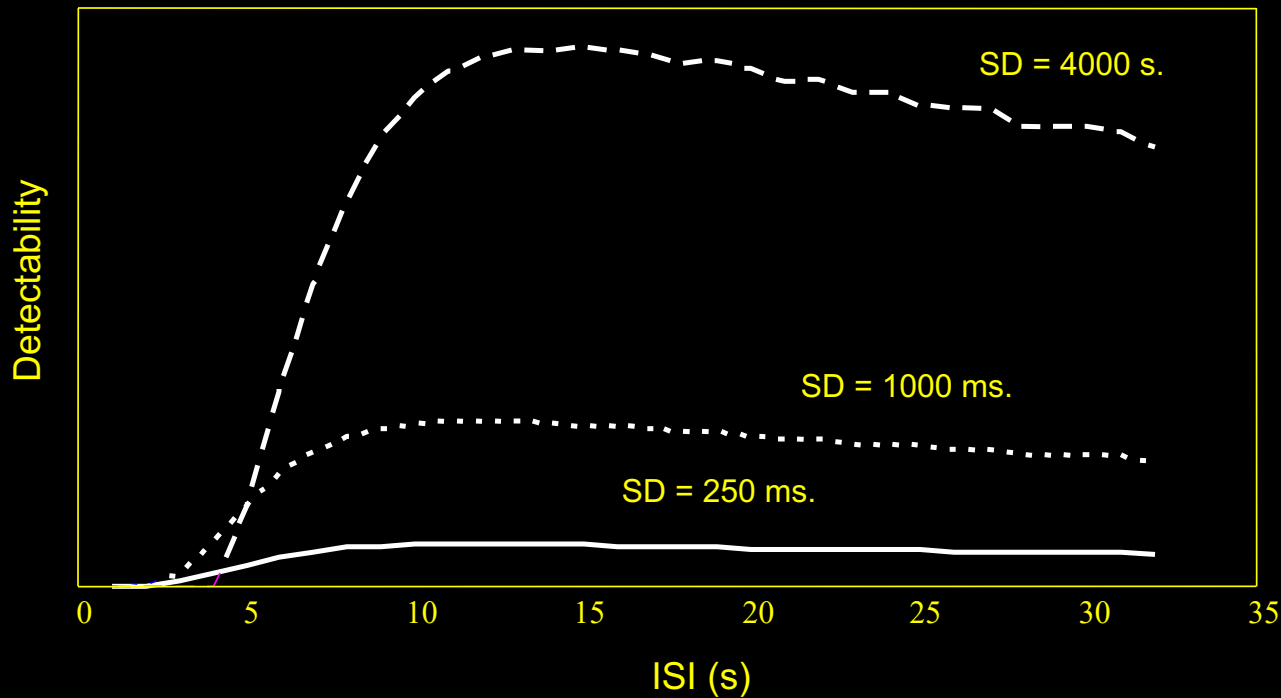
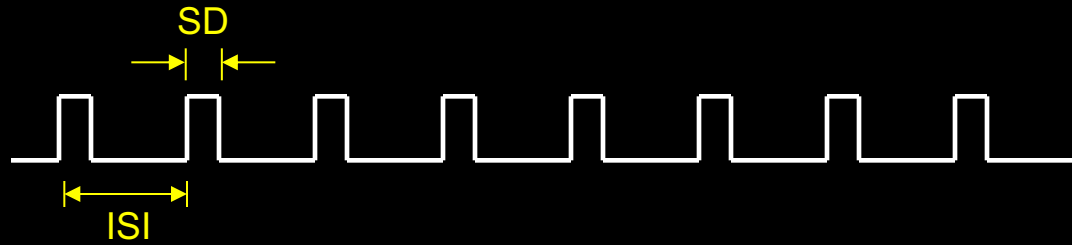


Detection – constant ISI



Optimal detection when there is no overlap

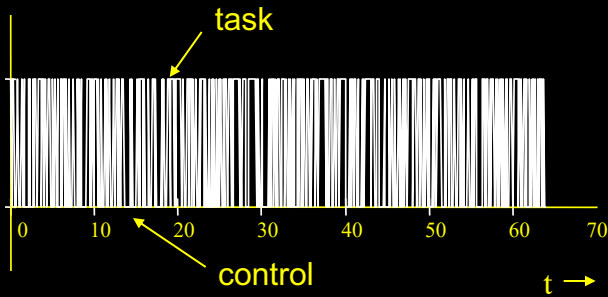
Detection vs. ISI – different SD



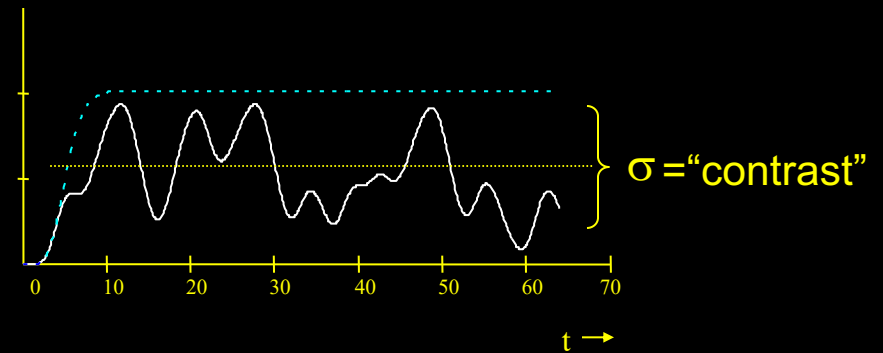
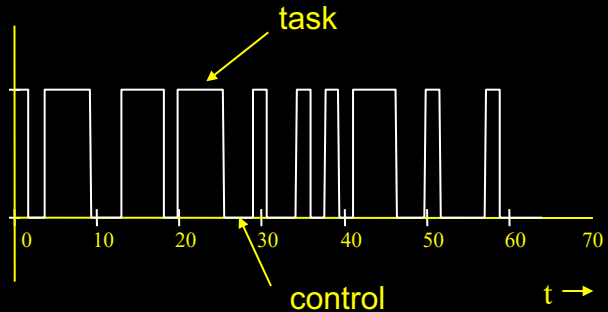
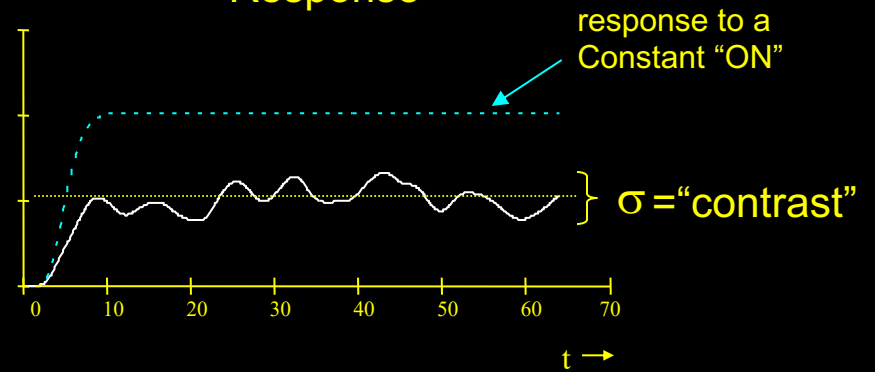
Optimal detection when there is no overlap

Detection: Contrast

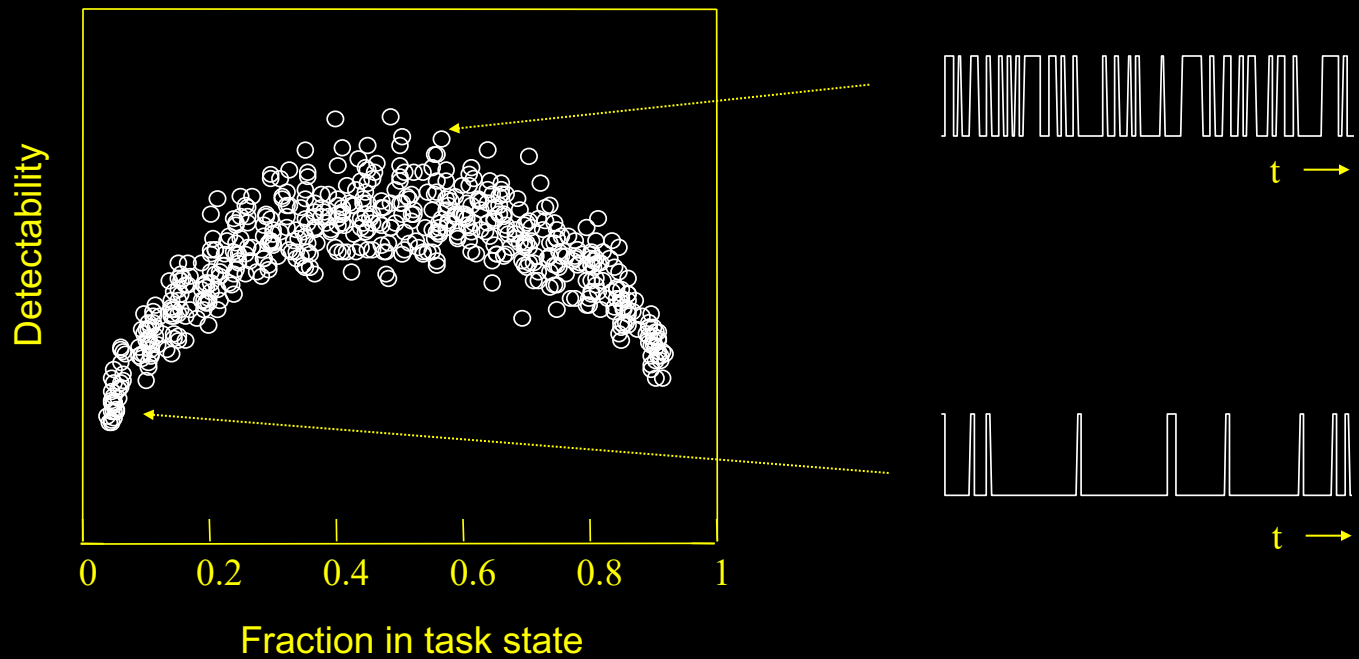
Stimulus



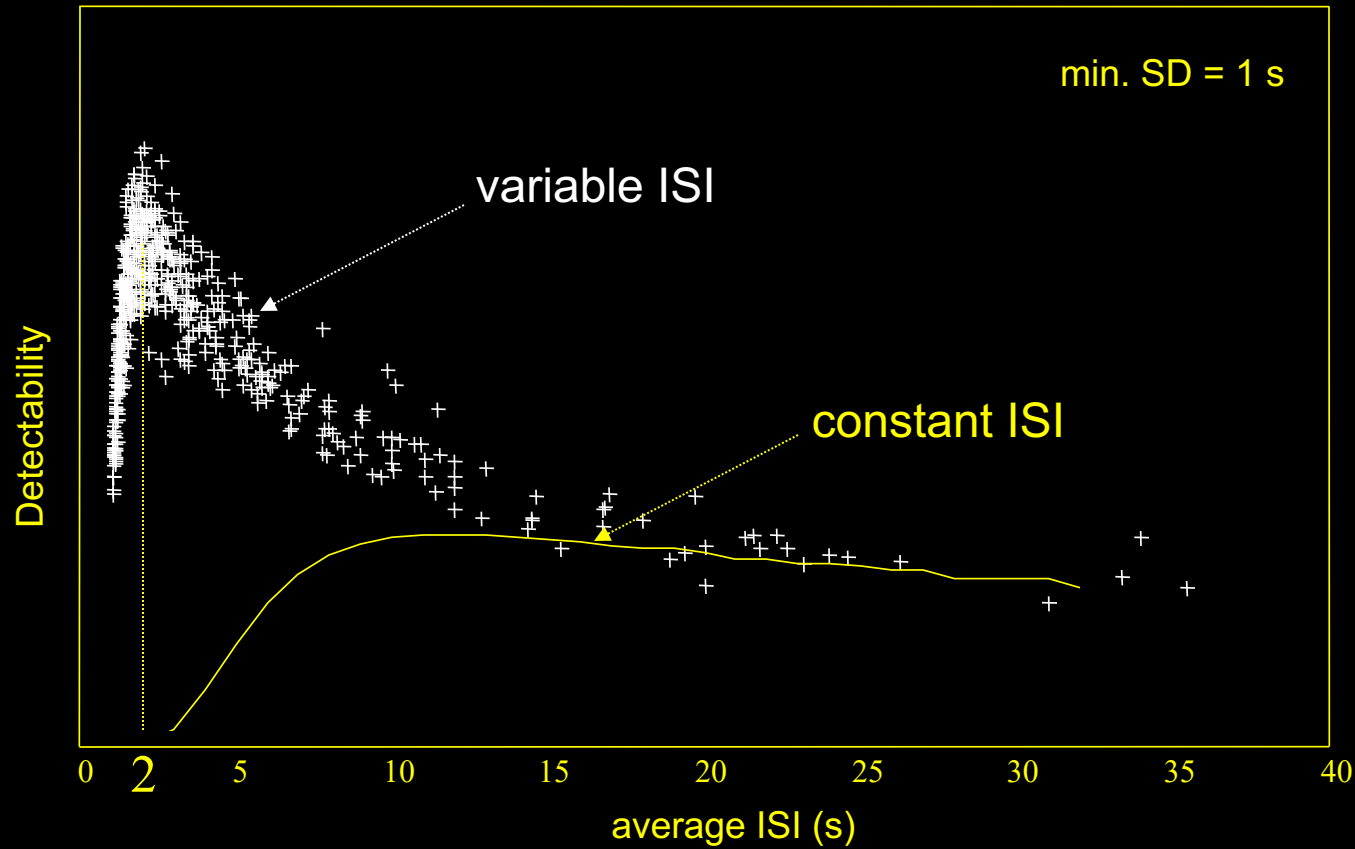
Response



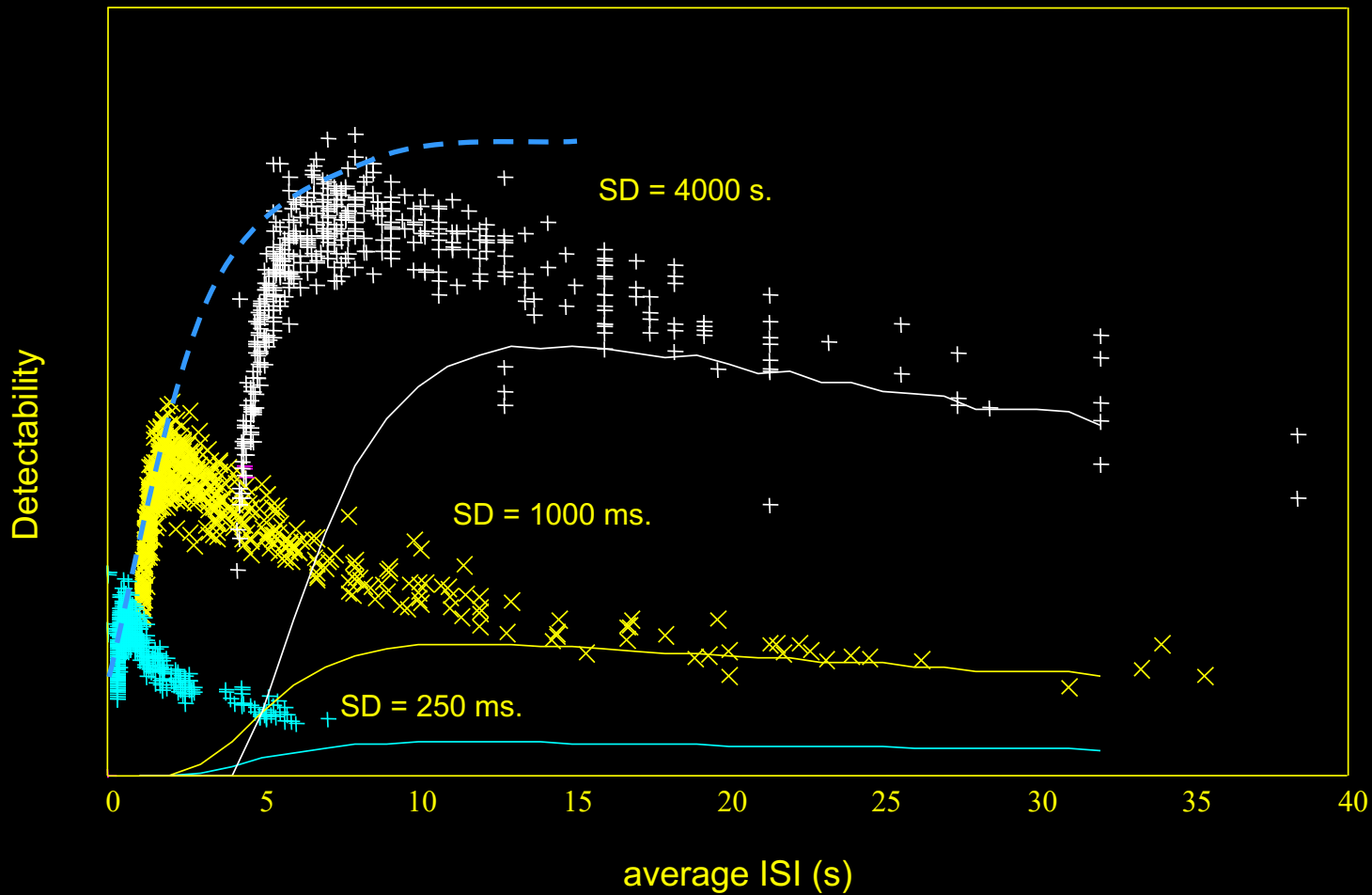
Detection vs. % “on” – variable ISI



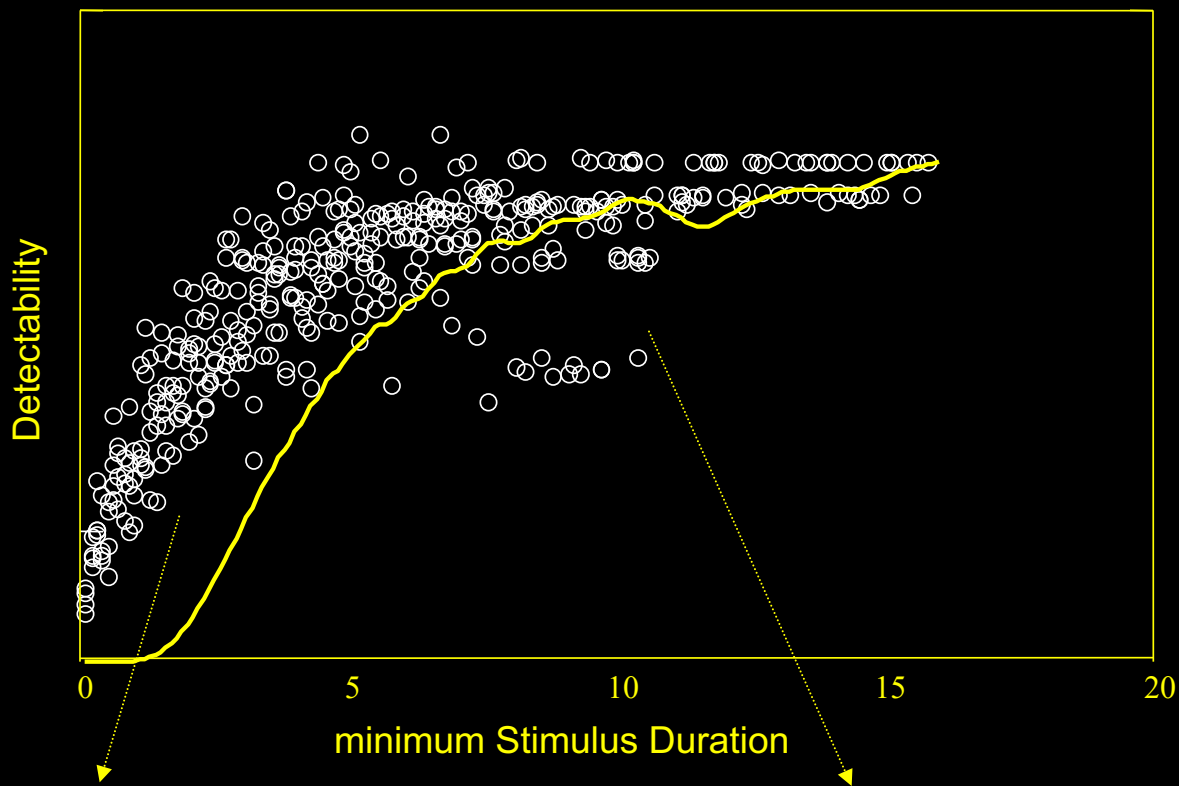
Detection vs. Average ISI



Detection vs. average ISI



Detection – 50% “on”

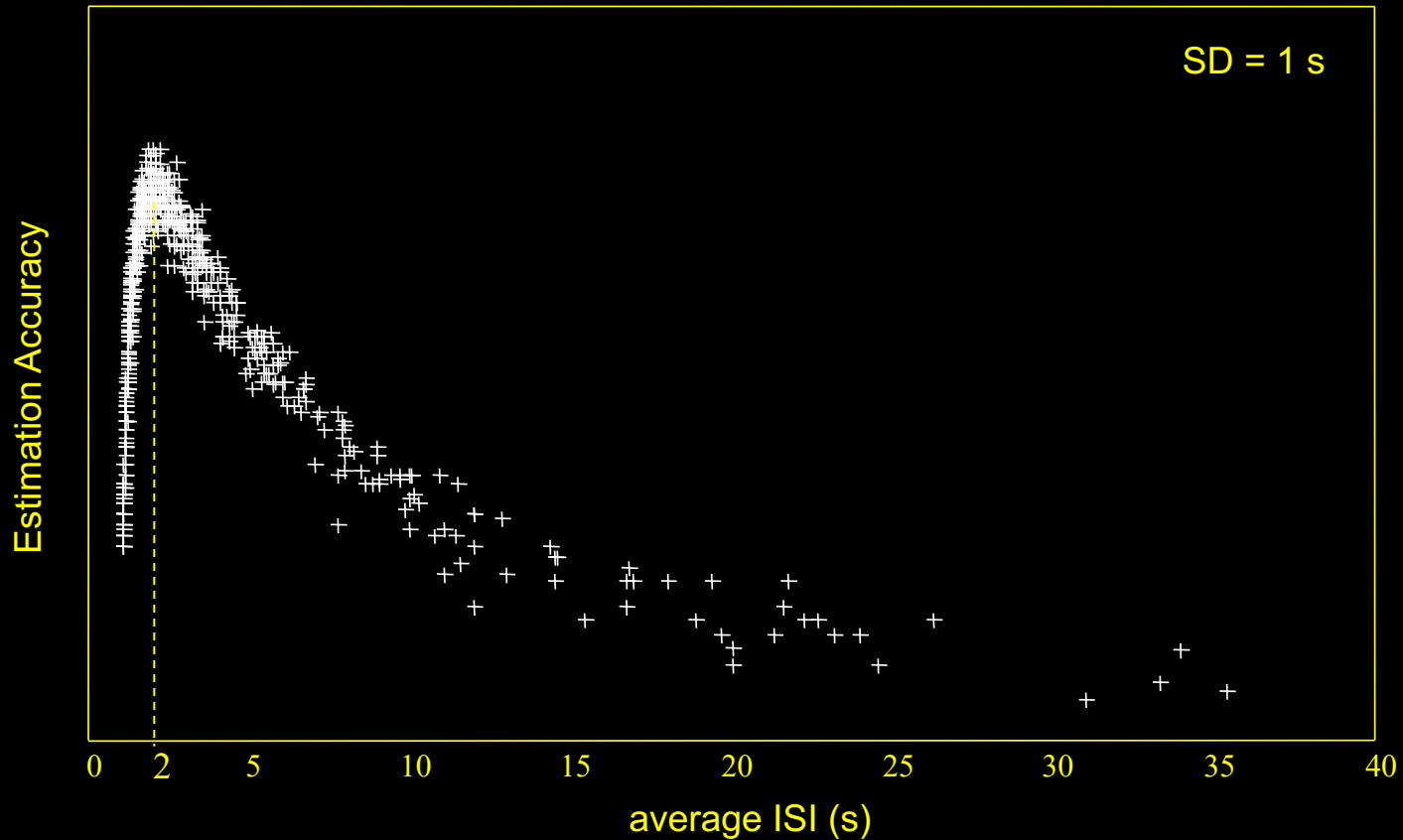


stimulus timing

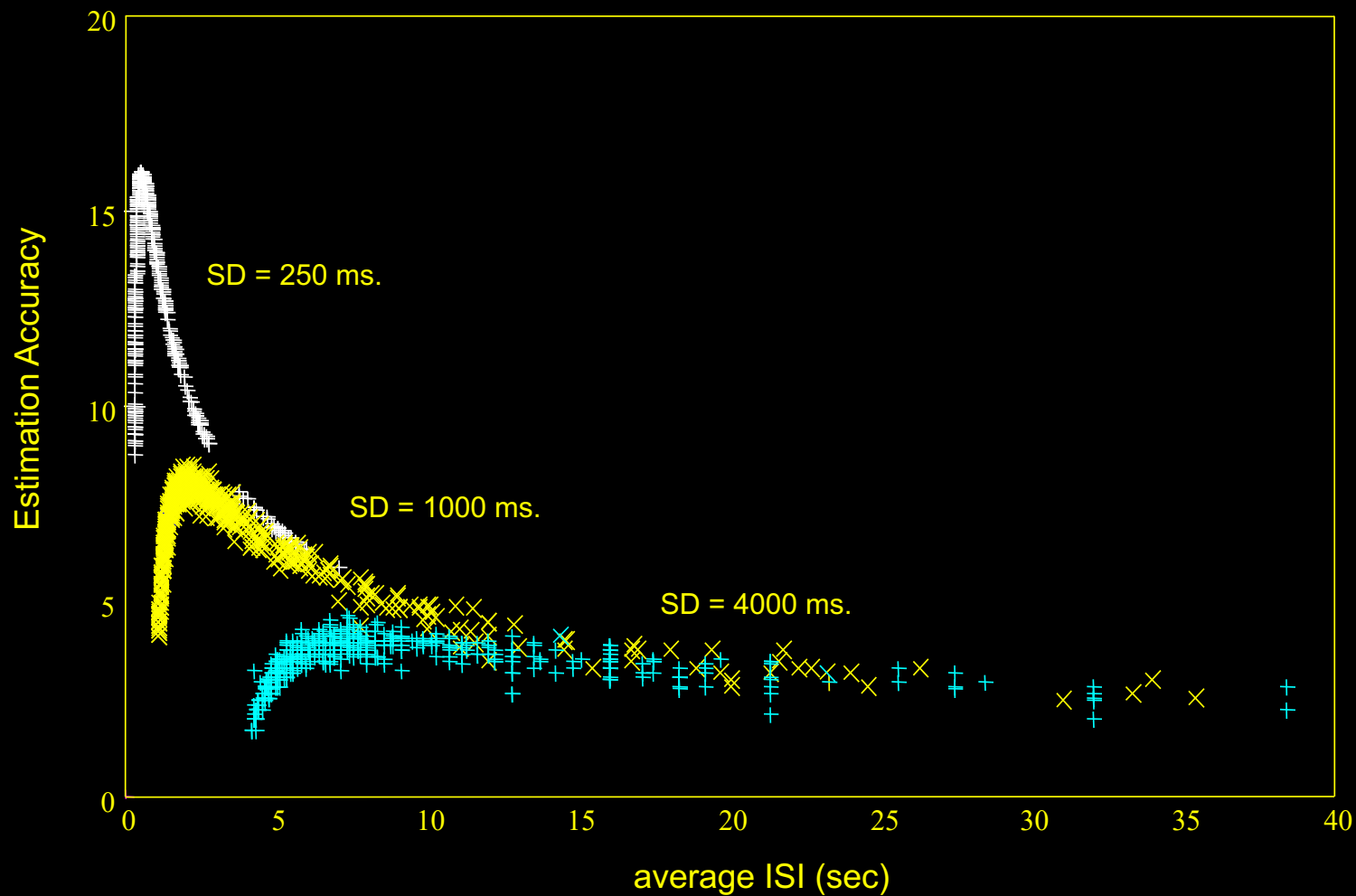


stimulus timing

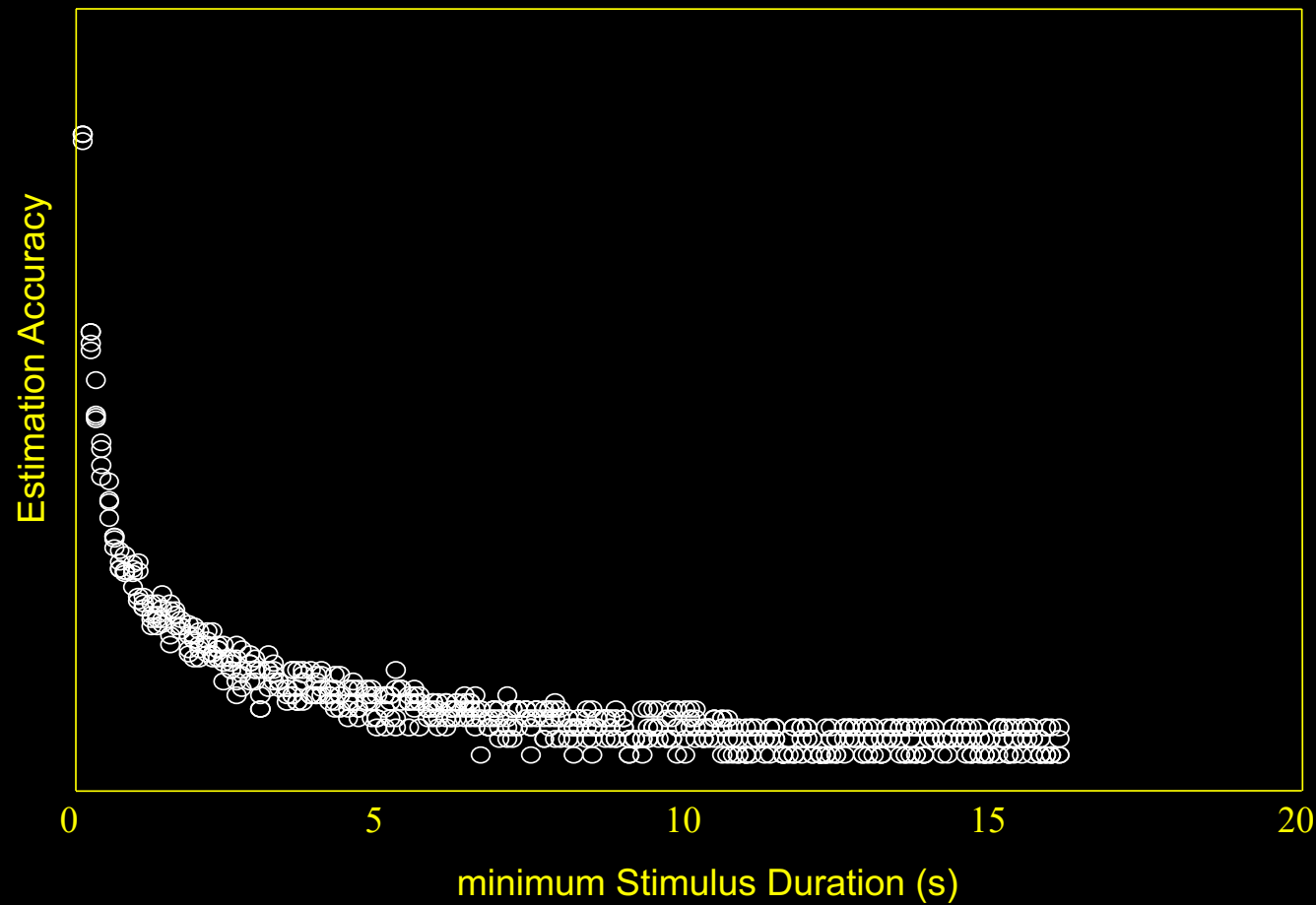
Estimation accuracy vs. average ISI



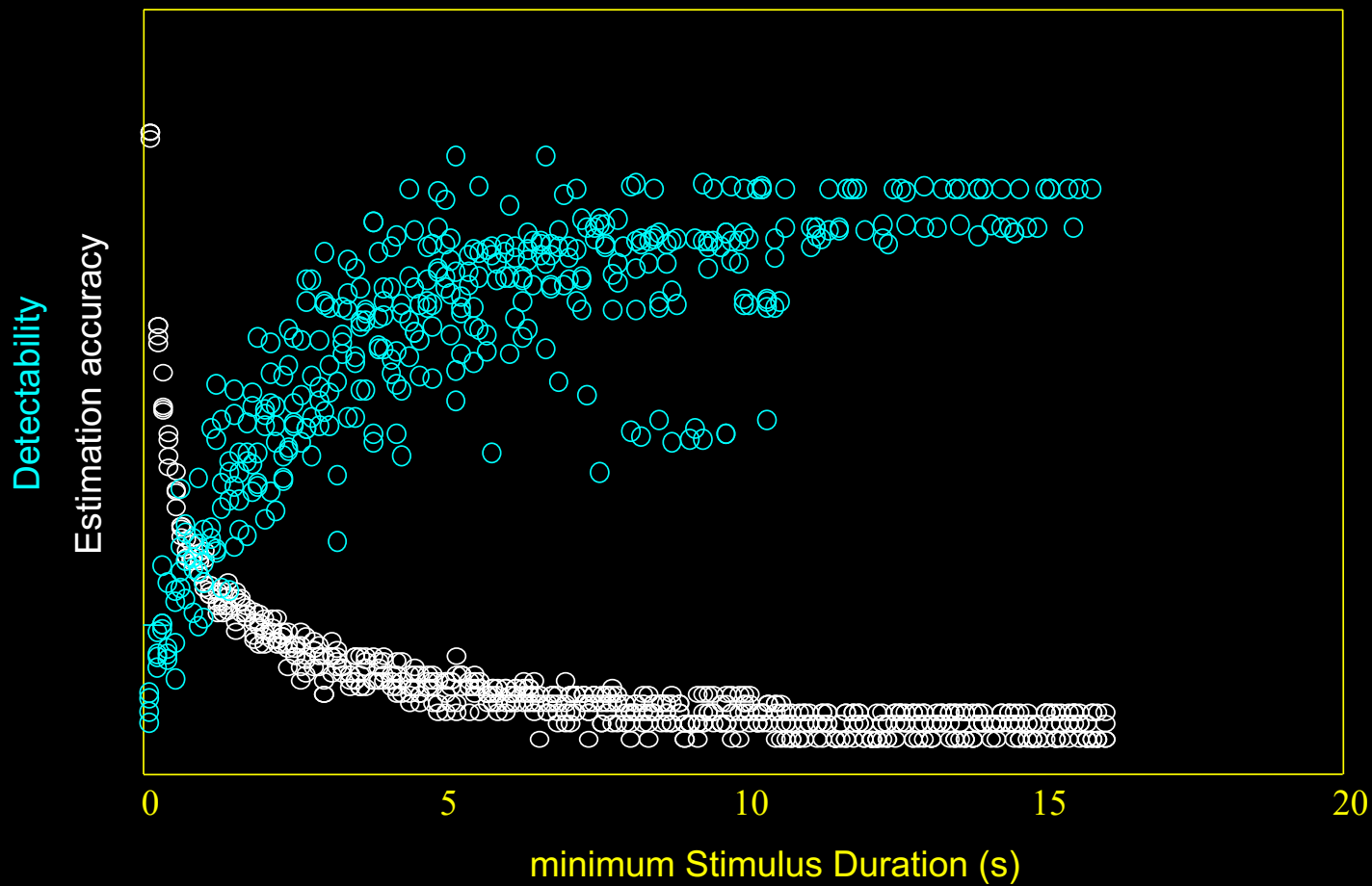
Estimation accuracy vs. average ISI



Estimation accuracy – 50% “on”



Detection and Estimation



Acknowledgements

Robert Savoy

Ravi Menon

Eric Wong

Rick Hoge

&...

Functional Imaging Methods / 3T Group

Staff Scientists:

Sean Marrett
Jerzy Bodurka

Post Docs:

Rasmus Birn
Patrick Bellgowan
Ziad Saad

Clinical Fellow:

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Graduate Student:

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Summer Students:

Hannah Chang
Courtney Kemp



July 7, 2000